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The relationship between HbA_{1c} and ultrasound plaque textures in atherosclerotic patients

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Abstract

Objective: Diabetes mellitus (DM) is associated to the morphological and componential characteristics of atheromatous plaques. It has proven that plaque textures are related to plaque components and beneficial for atherosclerotic risk stratification. The aim of this study is to compare plaque textures in patients with and without DM, and examine the relationship between HbA_{1c} levels and the ultrasound plaque textures in atherosclerotic patients.

Methods: A total of 136 participants (among them 66 are diabetic and 70 are non-diabetic) suffering from carotid plaques were included. About 300 texture features were extracted from the ultrasound images of plaques using the algorithms of histogram, absolute gradient, run-length matrix, gray-level co-occurrence matrix, autoregressive model and wavelet transform, respectively. Thirty optimal features were selected by the Fisher coefficient and the mutual information measure. The most discriminating feature (MDF) was obtained from the linear discriminant analysis for the optimal features. Linear regression model was performed to investigate the relationship between HbA_{1c} and MDF. The receiver operating characteristics (ROC) curve was further developed to validate the relation between the estimated HbA_{1c} (models output) and diabetes status.

Results: A total of 12 texture features showed statistical difference between patients with and without DM. The MDF was significant higher in non-diabetic patients (0.326 ± 0.049) than diabetic patients (-0.346 ± 0.052) ($p < 0.001$). The optimal regression model ($r = 0.348$, $p < 0.001$) for HbA_{1c} included a constant ($p < 0.001$) and the MDF ($p < 0.001$). The areas under ROC curve used to estimate HbA_{1c} was 0.828.

Conclusions: The results indicate that there is a quantitative relationship between the HbA_{1c} levels and plaque textures in ultrasonic images of atherosclerotic patients, which may suggest that texture analysis of the ultrasonic image of plaque is a promising method for evaluating the cardiovascular risk caused by DM in patients with plaques.

Keywords: Ultrasound imaging, Carotid plaque, Texture, HbA_{1c}, Cardiovascular disease

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Background

Diabetes mellitus (DM) enable to accelerate atherosclerosis and increase the risk of cardiovascular diseases [1, 2]. Carotid intima-media thickening (IMT) measured by ultrasound imaging and carotid artery elasticity evaluated by ultrasound radio frequency technology have been utilized for assessing the impact of DM on the plaques [3, 4]. These schemes, however, ignore some essential information about the plaque surface and morphology. Substantial evidences have indicated that quantitative textural analysis of the medical images can provide more useful diagnostic information [5], and is useful for atherosclerotic risk stratification [6]. Thus, it is significant to characterize carotid plaques using textures in patients with and without DM, which may help to evaluate the risk of cardiovascular events caused by DM.

DM are associated with the morphological and the componential characteristics of carotid plaques [3, 7]. In previous studies, Wilhjelm et al. [8] found that texture features of the ultrasound plaques was correlated with the histologically determined relative volume of soft materials. Niu et al. [9] indicated that texture features extracted from ultrasound images of the carotid arterial wall were useful in identifying arterial surface roughness. Rakebrandt et al. [10] reported that there are five texture classes match with the plaque contents including fibrin, elastin, calcium, haemorrhage and lipid. The above studies may imply that some plaque textures are different in patients with and without DM. Furthermore, HbA_{1c} is a risk factor for cardiovascular diseases in type 2 diabetes [11], and is related to the mortality in heart failure patients with diabetes [12]. However, few studies have investigated the relationship between HbA_{1c} and plaque textures.

The aim of this study is to compare plaque textures in patients with and without DM, and examine the relationship between HbA_{1c} levels and plaque textures in atherosclerotic patients.

Subjects and methods

Subjects

A total of 136 subjects (among them 66 are diabetic and 70 are non-diabetic) suffering from carotid plaques were investigated in present study. From October 2011 to February 2015, the patients received carotid artery examination at the department of ultrasound, the third affiliated hospital of Sun Yat-sen University. All participants provided the written informed consent. The study protocol was approved by the Institutional Review Board of the third affiliated hospital of Sun Yat-sen University (Guangzhou, China).

In this study, the diagnostic criteria for diabetes are defined as fasting plasma glucose (FPG) level of ≥ 7.0 mmol/L, and/or 2-h plasma glucose value

of ≥ 11.1 mmol/L, and/or HbA_{1c} level of ≥ 6.5 %, and/or treatment with either hypoglycemic agents or insulin [13, 14]. Patients with acute or chronic infectious disease, alcohol or drug abuse, retinopathy, or uncontrolled hypertension were excluded. Information regarding age, gender, total number of plaques, systolic blood pressure (SBP), diastolic blood pressure (DBP), body mass index (BMI), total cholesterol, triglyceride, low density lipoprotein cholesterol, high density lipoprotein cholesterol, lipoprotein, apolipoprotein A1, apolipoprotein B100, FPG, HbA_{1c} and medication use were collected.

Carotid ultrasonography

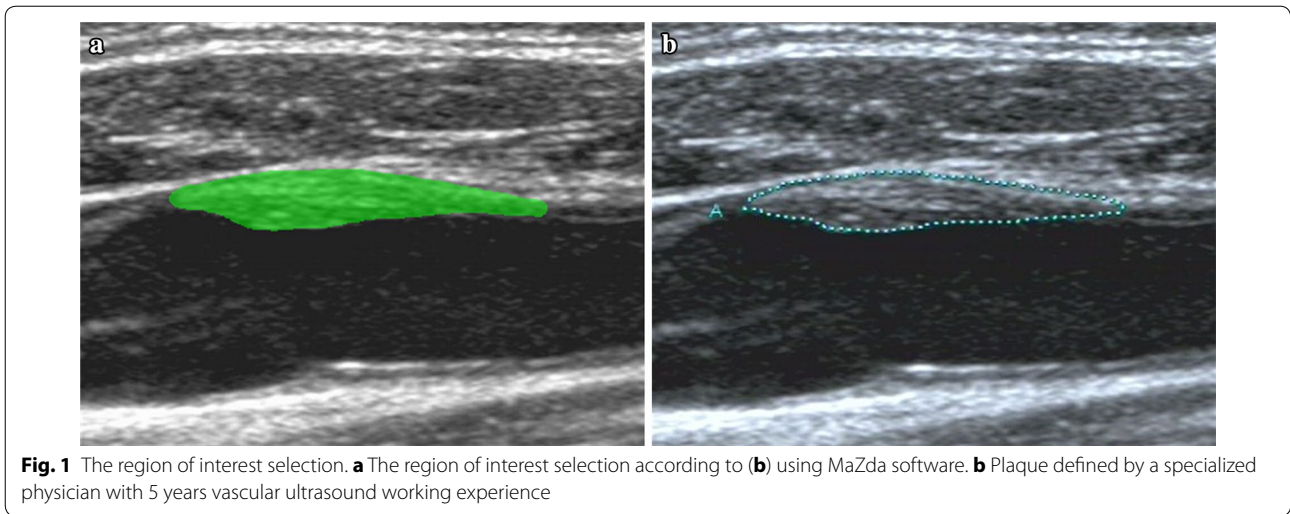
The study was performed by a specialized physician with 5 years vascular ultrasound working experience using a Toshiba AplioXG SSA-790A ultrasound Platform equipped with a 5–12 MHz linear-array transducer (PLT-805AT) and Esaote MyLab90 ultrasound Platform equipped with a 4–13 MHz linear-array transducer (LA523). The carotid artery was examined with the head tilted slightly upward in the mid-line position. The transducer was manipulated so that the near and far walls were parallel to the transducer footprint, and the lumen diameter was maximized in the longitudinal plane.

To improve the comparability of the plaque images obtained by different ultrasound systems at different settings, all images were standardized according to the scheme proposed by Sabetai et al. [15] before texture analysis. Furthermore, it is more clinically significant to focus on echolucent plaques, since these plaques are more potentially unstable than echo-rich plaques [16]. Gray-scale median (GSM) analysis is an objective and reproducible method for evaluating the echogenicity of carotid plaque [15]. In case there were multiple plaques in one individual, the plaques with the lowest GSM value among them was selected as the representative for the following texture analysis [17]. Two operators performed the GSM measurement independently, and the interoperator reproducibility was evaluated with a *kappa* value. The disagreement of the two operators were discussed and re-evaluated, then an agreement was finally achieved.

Many studies have shown that carotid intima-media thickening (IMT) is a high risk factor of the future cardiovascular events [18–20]. Maximum IMT (Plaque-IMT-max) was defined as the greatest axial thickness among the plaques in the carotid arteries [21, 22], and was measured in this study.

Texture analysis

MaZda is an effective tool for texture analysis and offers an approach for texture feature extraction, selection and reduction [23]. In MaZda, we can draw regions of interest with arbitrary shapes, as shown in Fig. 1. It provides six



various algorithms, such as histogram, absolute gradient, run-length matrix, co-occurrence matrix, autoregressive model and wavelet for features extraction [5, 23]. In present study, about 300 texture features of carotid plaques were extracted using MaZda, as shown in Table 1.

Texture feature selection and reduction

In order to select optimal features among the large number of texture features of the plaques from diabetic and non-diabetic patients, the methods based on Fisher coefficient and mutual information measure were used to select 15 optimal features, respectively. Furthermore, linear discriminant analysis (LDA) was implemented for the combined feature set, and the most discriminating features (MDF) were obtained.

Fisher coefficient

Fisher coefficient is defined as a ratio of between-class scatter D to within-class variance V [24]:

$$F = \frac{D}{V} = \frac{\frac{1}{1 - \sum_{k=1}^K P_k^2} \sum_{k=1}^K \sum_{j=1}^K P_k P_j (\mu_k - \mu_j)^2}{\sum_{k=1}^K P_k \nu_k} \quad (1)$$

where μ_i , ν_i and P_i denote the mean, the variance and the priori probability of class i , respectively. Texture features with larger Fisher coefficient are selected as optimal features.

Mutual information measure

Mutual information (MI), a measure of dependence between two random variables, is defined as [25]:

$$MI(X, Y) = H(X) + H(Y) - H(X, Y) \quad (2)$$

where X and Y are random variables, H is the entropy. In case of X stores values of texture features and Y stores the classification decision. Then, a large MI between X and Y means that X is a useful texture features for classification. Then the MI for each texture features f_i is calculated by [25, 26]:

$$MI(f_i, d) = \sum_{d=1}^{N_b} \sum_{k=1}^{N_c} P(f_i^d, c_k) \log_2 \left[\frac{P(f_i^d, c_k)}{P(f_i^d)P(c_k)} \right] \quad (3)$$

where $d = c_1, c_2, \dots, c_{N_c}$ means the class category, N_c is the total number of class, N_b is the number of histogram

Table 1 Texture features

<i>Histogram</i>	(1) mean, (2) variance, (3) skewness, (4) kurtosis and (5) percentiles 1, 10, 50, 90 and 99 %
<i>Absolute gradient</i>	(1) mean, (2) variance, (3) skewness, (4) kurtosis and (5) percentage of pixels with nonzero gradient
<i>Run-length matrix</i>	(1) run-length nonuniformity, (2) grey-level nonuniformity, (3) long-run emphasis, (4) short run emphasis and (5) fraction of image in runs. Parameters computed for horizontal, 45° vertical and 135° orientation
<i>Co-occurrence matrix</i>	(1) angular second moment, (2) contrast, (3) correlation, (4)sum of squares, (5) inverse difference moment, (6) sum average, (7) sum variance, (8) sum entropy, (9) entropy, (10) difference variance and (11) difference entropy. Parameters are computed for 4 orientations: (a, 0), (0, a), (a, a), (a, -a) and 5 distances: a = 1, 2, 3, 4, 5; between image pixels
<i>Autoregressive model</i>	(1) model parameter vector includes 4 parameters and (2) standard deviation of the driving noise
<i>Wavelet</i>	(1) Energy of wavelet coefficients in low-frequency subbands, (2) horizontal high-frequency subbands, (3) vertical high-frequency subbands and (4) diagonal high-frequency subbands at successive scales

bins used for feature discretization, f_i^d denotes discretized value of f_i .

Linear discriminant analysis

LDA is a useful method for feature reduction [24]. The aim of LDA is to find a transform matrix W such that the ratio of determinants $\frac{|W^T S_B W|}{|W^T S_W W|}$ is maximized. Where S_B and S_W are the between-class scatter matrix and the within-class scatter matrix. These matrices can be given as formulas (4, 5).

$$S_B = \frac{1}{M} \sum_{k=1}^{N_c} M_k (x_i^{(k)} - u^{(k)}) (x_i^{(k)} - u^{(k)})^T \quad (4)$$

$$S_W = \frac{1}{M} \sum_{k=1}^{N_c} \sum_{i=1}^{M_k} (x_i^{(k)} - u^{(k)}) (x_i^{(k)} - u^{(k)})^T \quad (5)$$

where $X_i^{(k)}$ denotes the i -th pattern in class k ($i = 1, 2, \dots, M_k$), $k = 1, 2, \dots, N_c$, $u^{(k)}$ is the mean vector of class k . It has proved that such a transform matrix Φ is composed of eigenvectors corresponding to largest eigenvalues of $S_W^{-1} S_B$. The MDF can be obtained when the original data is transformed by the means of matrix Φ as formula (6).

$$MDF_i = \Phi^T (x_i - u) \quad (6)$$

Statistical analysis

All statistical analysis was performed with PASW Statistics 18 and p less than 0.05 was considered statistically significant. All values were presented as the mean value \pm SD, or real number of patients with the percentage in parentheses. Independent sample t test was used to examine the baseline clinical parameters between the diabetic and non-diabetic patients. Pearson correlation analysis was conducted to investigate the relationship between HbA_{1c} and the variables including age, BMI, total number of plaques, SBP, DBP, plaque-IMTmax and MDF. Linear regression analysis was carried out by considering the HbA_{1c} as a dependent variable and regarding the MDF as independent variable. The optimized regression model was obtained to estimate the HbA_{1c}. Further, the receiver operating characteristics (ROC) curve was developed to test the relationship between the estimated HbA_{1c} (models output) and diabetes status.

Results

Baseline characteristics of study participants

Table 2 describes the baseline characteristics of the study population ($n = 136$), which includes 66 patients with DM (age, mean \pm SD, 67.8 ± 10.0 years) and 70 patients without DM (age, mean \pm SD, 69.4 ± 9.8 years). The

BMI (23.9 ± 3.1 vs 22.0 ± 2.8 kg/m², $p = 0.001$), triglyceride (1.90 ± 1.57 vs 1.31 ± 0.89 , $p = 0.009$ mmol/L), HbA_{1c} (8.87 ± 2.25 vs 5.50 ± 0.41 %, $p < 0.001$) and FPG (10.76 ± 4.26 vs 5.14 ± 0.70 mmol/L, $p < 0.001$) were significantly different in patients with and without DM. In the DM group, the ratio of patients using oral hypoglycemic agent, insulin, both oral hypoglycemic agent and insulin, and no drug for treatment were 50 % ($n = 33$), 21.2 % ($n = 14$), 9.1 % ($n = 6$), and 19.7 % ($n = 13$).

Plaques selection

There was a good agreement between the two operators in selecting the plaque with the lowest GSM value in one individual with multiple plaques. The interoperator reproducibility was 97.79 % ($kappa$ value = 0.965), and the 3 controversial plaques were discussed and re-evaluated, then eventually an agreement was achieved.

Texture selection and reduction

A total 30 optimal features were selected based on the Fisher coefficient and the mutual information measure. Among the optimal features, 12 features (7 feature extracted by run-length matrix and 5 features extracted by wavelet) were considered to be statistically different in patients with and without DM, as shown in Table 3. In order to reduce the number of the optimal features, LDA was further performed to gain the MDF. The MDF (-0.035 ± 0.052 vs 0.033 ± 0.050 , $p < 0.001$) showed significant difference in the diabetic and the non-diabetic patients.

Pearson correlation of the study variables with HbA_{1c}

Pearson correlation analysis was implemented to examine the relationship between HbA_{1c} and the variables including age, BMI, total number of plaques, SBP, DBP and MDF. Table 4 indicates that the HbA_{1c} is positively correlated with BMI ($r = 0.182$, $p = 0.034$), whereas HbA_{1c} is negatively correlated with the MDF ($r = -0.348$, $p < 0.001$).

Linear regression model for HbA_{1c}

Table 5 shows that the optimal model for HbA_{1c} ($r = 0.348$, $p < 0.001$) is achieved by stepwise regression method. The model included a constant ($p < 0.001$) and the MDF ($p < 0.001$). The optimized regression equation can be described as formula (7) to estimate the HbA_{1c}.

$$\text{Estimated HbA}_{1c} = -13.297 * x_1 + 7.136 \quad (7)$$

where x_1 is the MDF.

Further, the ROC curve was developed to validate the relationship between the estimated HbA_{1c} and diabetes status, and the area under the ROC curve was 0.828 (Fig. 2).

Table 2 Baseline characteristics of 136 subjects

Characteristics	Diabetes (n = 66)	Non-diabetes (n = 70)	t	p
Age, mean (SD)	67.8 ± 10.0	69.4 ± 9.8	-0.972	0.333
Male gender, n (%)	43 (65)	46 (66)	0.068	0.946
Total number of plaques	2.1 ± 1.2	2.0 ± 1.1	0.533	0.104
Hypertension, n (%)	43 (65)	44 (63)	0.277	0.783
CHD, n (%)	18 (27.3)	22 (31.4)	-0.528	0.598
SBP (mm Hg)	136.9 ± 19.0	139.1 ± 22.0	-0.642	0.522
DBP (mm Hg)	75.8 ± 9.2	76.7 ± 12.8	0.465	0.643
BMI (kg/m ²)	23.9 ± 3.1	22.0 ± 2.8	3.437	0.001
Total cholesterol (mmol/L)	4.78 ± 1.20	4.46 ± 1.17	-1.548	0.116
Triglyceride (mmol/L)	1.90 ± 1.57	1.31 ± 0.89	2.677	0.009
HDL-cholesterol (mmol/L)	1.05 ± 0.28	1.13 ± 0.34	-1.484	0.140
LDL-cholesterol (mmol/L)	3.04 ± 0.97	2.86 ± 1.06	1.023	0.308
Lipoprotein A (mg/L)	211.9 ± 219.2	284.9 ± 288.7	-1.652	0.101
Apolipoprotein A1 (g/L)	1.29 ± 0.31	1.31 ± 0.26	-0.362	0.718
Apolipoprotein B100 (g/L)	1.20 ± 0.47	1.17 ± 1.23	0.163	0.871
HbA _{1c} (%)	8.87 ± 2.25	5.50 ± 0.41	11.940	<0.001
FPG (mmol/L)	10.76 ± 4.26	5.14 ± 0.70	10.611	<0.001
Plaque-IMTmax (mm)	2.4 ± 0.8	2.5 ± 0.8	-0.635	0.527

Data are presented as the mean value ±SD or percentage of subjects

CHD coronary heart disease, SBP systolic blood pressure, DBP diastolic blood pressure, BMI body mass index, HDL-cholesterol high density lipoprotein cholesterol, LDL-cholesterol low density lipoprotein cholesterol, FPG fasting plasma glucose

Table 3 Statistically different features between diabetic and non-diabetic plaques

Features	Non-diabetes (n = 70)	Diabetes (n = 66)	Fisher	MI	t	p
WavEnLH_s-4	756.21 ± 418.35	522.48 ± 385.45	0.342	0.109	3.383	0.001
Vertl_Fraction	0.883 ± 0.056	0.847 ± 0.096	0.213	0.036	2.630	0.010
135dr_ShrtrREmp	0.921 ± 0.037	0.893 ± 0.0716	0.25	0.066	2.866	0.005
Vertl_ShrtrREmp	0.915 ± 0.040	0.886 ± 0.072	0.243	0.046	2.810	0.006
WavEnLL_s-2	16,327 ± 4554	13,092 ± 7191	0.229	0.055	2.2733	0.007
WavEnLL_s-1	16,327 ± 4559	13,474 ± 7337	0.224	0.041	2.705	0.008
WavEnLH_s-3	465.39 ± 275.86	343.30 ± 247.33	0.220	0.039	2.712	0.008
135dr_Fraction	0.892 ± 0.052	0.858 ± 0.091	0.213	0.040	2.627	0.010
45dgr_ShrtrREmp	0.918 ± 0.038	0.892 ± 0.073	0.210	0.038	2.606	0.011
WavEnLL_s-3	15,479 ± 4811	12,802 ± 7299	0.193	0.069	2.510	0.014
Horzl_ShrtrREmp	0.816 ± 0.095	0.757 ± 0.169	0.191	0.048	2.491	0.014
45dgr_Fraction	0.887 ± 0.053	0.854 ± 0.095	0.184	0.040	2.444	0.016
MDF	0.033 ± 0.050	-0.035 ± 0.052	-	-	7.712	<0.001

WavEnLH_s-3 and WavEnLH_s-4 are energy of wavelet coefficients in vertical high-frequency subbands at scale 3 and 4; WavEnLL_s-1, WavEnLL_s-2 and WavEnLH_s-3 are energy of wavelet coefficients in low-frequency subbands at scale 1, 2 and 3; 45dgr_Fraction, Vertl_Fraction and 135dr_Fraction are fraction of image in runs computed for 45°, vertical and 135° orientation; Vertl_ShrtrREmp, Horzl_ShrtrREmp, 45dgr_ShrtrREmp, Vertl_ShrtrREmp and 135dr_ShrtrREmp are short run emphasis computed for horizontal, 45° vertical and 135° orientation

MDF most discriminating feature, MI mutual information

Table 4 Pearson correlation of the study variables with HbA_{1c}

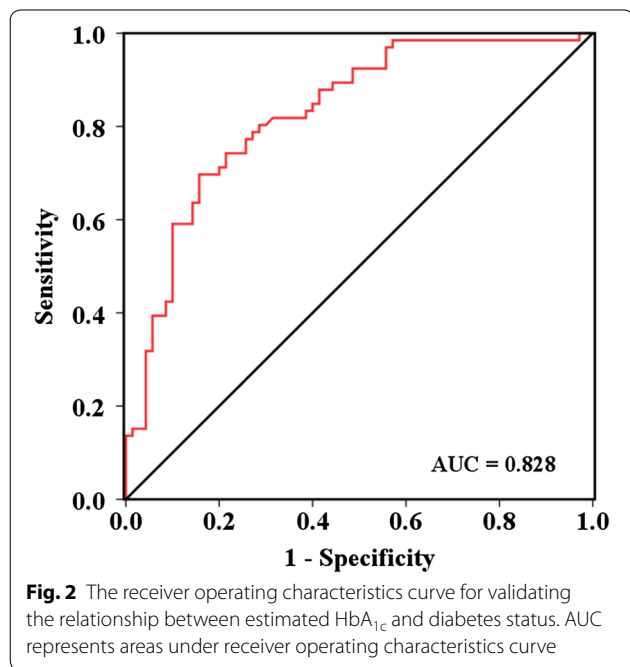
		Age (year)	BMI (kg/m ²)	TNP	SBP (mmHg)	DPB (mmHg)	Plaque-IMTmax (mm)	MDF
HbA _{1c} (%)	Pearson	-0.123	0.182	-0.022	-0.071	0.084	-0.097	-0.348
	p	0.155	0.034	0.795	0.408	0.333	0.262	<0.001

BMI body mass index, TNP total number of plaques, SBP systolic blood pressure, DPB diastolic blood pressure, MDF most discriminating feature

Table 5 Linear regression model of HbA_{1c} with the coefficients of the variables involved

Model	Variables/constant	Coefficients	P	95.0 % confidence interval	
				Lower bound	Upper bound
HbA _{1c} ($r = 0.392, p < 0.001$)	Constant	7.136	<0.001	6.766	7.506
	MDF	-13.297	<0.001	-19.407	-7.186

MDF most discriminating feature



Discussion

In this study, a total of 12 texture features showed significant difference in diabetic and non-diabetic patients. Previous studies indicated that MD impacted the vascular structure and function [27, 28], increased the IMT of common carotid artery [3], and modified the relationships between carotid plaque calcium, composition and inflammation [7]. The textural differences may be a candidate parameter reflecting the morphological and compositional differences of the carotid plaques in patients with and without DM. The texture features including the fraction of image in runs computed for 45°, vertical and 135° orientation, and the short run emphasis computed for horizontal, 45°, vertical and 135° orientation were statistically higher in non-diabetic patients than diabetic patients. The fraction of image in runs is a measurement of the percentage of image pixels that are part of any of the runs considered for the matrix computing and it should have a low value for images with linear structure [5, 29]. Moreover, the short run emphasis, a feature emphasizing the short runs, is a measure of the

proportion of short runs occurring in the image [5, 29]. Given the above, it may suggest that diabetes tend to impact plaques with a linear structure in the surface.

In previous studies, Virmani et al. [30] indicated that the BMI was significantly higher in diabetic patients ($30.5 \pm 7.41 \text{ kg/m}^2$) than in non-diabetic patients ($26.6 \pm 5.4 \text{ kg/m}^2$) ($p = 0.001$). Nozue et al. [31] showed that BMI was significantly different in the participants with MD or not (25.3 ± 3.9 vs $23.8 \pm 2.7 \text{ kg/m}^2$, $p = 0.01$). Marso et al. [32] indicated that the median triglycerides in acute coronary syndrome patients with MD was 144 mg/dL, whereas that in patients without MD was 101 mg/dL ($p < 0.001$). In the study of Lee et al. [33] reported that the median triglycerides in subjects with HbA_{1c} ranged from 3.6 to 5.2, from 5.3 to 5.4, from 5.6 to 5.7, and from 5.8 to 6.4 were 109.1, 116.1, 120.2, and 127.9 mg/dL, respectively ($p < 0.001$). These findings are consistent with our results, in which the BMI (23.9 ± 3.1 vs $22.0 \pm 2.8 \text{ kg/m}^2$, $p = 0.001$) and triglycerides (1.90 ± 1.57 vs $1.31 \pm 0.89 \text{ mmol/L}$, $p = 0.009$) are statistically different in the patients with and without DM.

Ultrasound IMT measurements were considered as a strong predictor of future cardiovascular events [18–20]. Recent studies suggested that the increased IMT was not an independent predictor of plaque development [34, 35]. Compare with carotid IMT, carotid plaque predicts cardiovascular events more accurately [36, 37]. In this study, the carotid plaque-IMTmax showed no statistical difference in patients with and without DM (2.4 ± 0.8 vs $2.5 \pm 0.8 \text{ mm}$, $p = 0.527$), whereas the MDF was significant higher in diabetic patients (0.033 ± 0.050) than in non-diabetic patients (-0.035 ± 0.052) ($p < 0.001$). It may suggest that the MDF is more effective than carotid plaque-IMTmax in illustrating the difference of plaques in patients with and without DM. Additionally, MDF make it possible to evaluate the stability of the plaque. Compared with the conventional features (i.e. plaque-IMTmax) that are evaluated visually, the MDF is an abstract feature that extracted from texture features without visual evaluation.

HbA_{1c} testing reflects the average plasma glucose over the previous 2–3 months [38]. Mukai et al. [39] indicated that the crude average of the maximum carotid

intima-media thickness increased significantly with rising quartiles of HbA_{1c}. Daida et al. [40] examined the association between HbA_{1c} and plaque regression, and suggested that plaque regression was less pronounced in patients with high HbA_{1c} levels compare with those with low levels. In present study, we found a relationship between the HbA_{1c} levels and plaque textures in atherosclerotic patients, which may be useful for evaluating the impact of long-term blood glucose level on the carotid plaques. Furthermore, Eeg-Olofsson et al. [11] indicated that higher HbA_{1c} levels increased the risks of cardiovascular disease, coronary heart disease and total mortality. Ikeda et al. [41] showed that HbA_{1c} was an independent risk factor for cardiovascular disease. The relationship between the MDFs and HbA_{1c} may suggest that the MDFs can be used to assess cardiovascular risk, which may elevate the value of B-mode ultrasonography examination.

The main limitation was that this method could be applied only to patients with carotid plaques. The atheromatous plaque, however, was a common complication of diabetes and had a high prevalence in population [42, 43]. Besides, the number of subjects was relatively small in this study. A longitudinal, prospective study utilizing carotid ultrasound evaluation in a large number of diabetic patients with plaques is required to assess the precise prognostic value of plaque textures in determining future cardiovascular events caused by DM.

Conclusion

In conclusion, the results of present study indicated that the textures of the carotid plaques were statistically different in patients with and without DM. The relationship between the HbA_{1c} levels and plaque textures may suggest that texture analysis of the ultrasound images of carotid plaques is a promising method to evaluate the risk of cardiovascular events caused by DM in patients with plaques.

Abbreviations

DM: diabetes mellitus; MDF: most discriminating feature; ROC: receiver operating characteristics; IMT: intima-media thickening; FPG: fasting plasma glucose; SBP: systolic blood pressure; DBP: diastolic blood pressure; BMI: body mass index; GSM: gray-scale median; Plaque-IMTmax: maximum intima-media thickening; LDA: linear discriminant analysis; MI: mutual information; CHD: coronary heart disease; HDL-cholesterol: high density lipoprotein cholesterol; LDL-cholesterol: low density lipoprotein cholesterol; WavEnLH_s-3 and WavEnLH_s-4: energy of wavelet coefficients in vertical high-frequency subbands at scale 3 and 4; WavEnLL_s-1, WavEnLL_s-2 and WavEnLH_s-3: energy of wavelet coefficients in low-frequency subbands at scale 1, 2 and 3; 45dgr_Fraction, VertL_Fraction and 135dr_Fraction: fraction of image in runs computed for 45°, vertical and 135° orientation; VertL_ShrtrEmp, Horzl_ShrtrEmp, 45dgr_ShrtrEmp, VertL_ShrtrEmp and 135dr_ShrtrEmp: short run emphasis computed for horizontal, 45°, vertical and 135° orientation; TNP: total number of plaques.

Authors' contributions

XWH, YLZ, RQZ, HRZ and LLN took part in the design of this study, collected and analyzed the data, interpreting the data, wrote the manuscript. LM

participated analytical methods, interpretation of results, wrote the manuscript. MQ, WZ participated analytical methods, interpretation of results. All authors were involved in making revisions to the manuscript. Finally, all authors reviewed the manuscript. All authors read and approved the final manuscript.

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Competing interests

The authors declare that they have no competing interests.

Availability of data and materials

The datasets during and/or analysed during the current study available from the corresponding author on reasonable request.

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