## NANO EXPRESS

**Open Access** 



# Prussian Blue Nanoparticle-Labeled Mesenchymal Stem Cells: Evaluation of Cell Viability, Proliferation, Migration, Differentiation, Cytoskeleton, and Protein Expression In Vitro

Jirui Wen<sup>1,4+</sup>, Zhiwei Zhao<sup>1+</sup>, Ruijie Tong<sup>2</sup>, Liwei Huang<sup>3</sup>, Yali Miao<sup>4,5\*</sup> and Jiang Wu<sup>1,5\*</sup>

## Abstract

Mesenchymal stem cells (MSCs) have been used for the treatment of various human diseases. To better understand the mechanism of this action and the fate of these cells, magnetic resonance imaging (MRI) has been used for the tracking of transplanted stem cells. Prussian blue nanoparticles (PBNPs) have been demonstrated to have the ability of labeling cells to visualize them as an effective MRI contrast agent. In this study, we aimed to investigate the efficiency and biological effects of labeled MSCs using PBNPs. We first synthesized and characterized the PBNPs. Then, iCELLigence real-time cell analysis system revealed that PBNPs did not significantly alter cell viability, proliferation, and migration activity in PBNP-labeled MSCs. Oil Red O staining and Alizarin Red staining revealed that labeled MSCs also have a normal differentiation capacity. Phalloidin staining showed no negative effect of PBNPs on the cytoskeleton. Western blot analysis indicated that PBNPs also did not change the expression of  $\beta$ -catenin and vimentin of MSCs. In vitro MRI, the pellets of the MSCs incubated with PBNPs showed a clear MRI signal darkening effect. In conclusion, PBNPs can be effectively used for the labeling of MSCs and will not influence the biological characteristics of MSCs.

Keywords: Prussian blue nanoparticles, Mesenchymal stem cells, Magnetic resonance imaging, Cytotoxicity

## Background

Mesenchymal stem cells, a type of adult stem cell, have the capacity of anti-inflammatory, regenerative potential and can migrate into injured tissues to aid the recovery of damaged function [1]. They can differentiate into multiple cell types under the specific microenvironment and are easily collected from adult and fetal tissue [2]. Thus, mesenchymal stem cells (MSCs) have been used for regenerative medicine and oncology therapy as a

\* Correspondence: miaoyali2006@163.com; jw@scu.edu.cn

<sup>+</sup>Jirui Wen and Zhiwei Zhao contributed equally to this work.

<sup>4</sup>Department of Gynecology, West China Second University Hospital, Sichuan University, Key Laboratory of Birth Defects and Related Diseases of Women and Children (Sichuan University), Chengdu, China

Full list of author information is available at the end of the article

promising tool due to these excellent properties [3, 4]. However, the fate of MSCs after transplanting into the body remains unclear, and non-invasive MSC tracking is necessary in vivo for evaluating the efficiency of transplantation and their fate, properties, and localization [5]. Recently, magnetic resonance imaging (MRI) as an effective technology has been widely obtained to research the structural and functional information of mesenchymal stem cells in vitro and in vivo [6].

In the past years, multiple nanoparticles were used for labeling MSCs as a promising tool for non-invasive imaging of cells to record their distributions and fate in vivo and in vitro, and even used for the treatment of tumors [7]. For example, superparamagnetic iron oxide (SPIO) nanoparticles and quantum dots (QDs) have been used for labeling cells for many years [8, 9]. And fluorescent magnetic nanoparticles (FMNPs) were used



© The Author(s). 2018 **Open Access** This article is distributed under the terms of the Creative Commons Attribution 4.0 International License (http://creativecommons.org/licenses/by/4.0/), which permits unrestricted use, distribution, and reproduction in any medium, provided you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made.

<sup>&</sup>lt;sup>1</sup>West China School of Basic Medical Sciences & Forensic Medicine, Sichuan University, No17, 3rd section, Renmin Nanlu Road, Chengdu 610041, Sichuan, China

for labeling MSCs to realize the targeted imaging and synergistic therapy of gastric cancer cells in vivo [10]. For these novel labels, a careful and complete analysis of cell toxicity is needed because everything has a toxic dose and may perturb downstream cell function [11]. For example, the MRI contrast iron oxide nanoparticles was attributed to the generation of ROS and may cause cell death [12].

Recently, Prussian blue nanoparticles (PBNPs) have been demonstrated that they have potential to be an MRI contrast agent [13–15]. Prussian blue, considered as a practical, economical, safe, and environmently friendly drug, has been approved by the US Food and Drug Administration (FDA) in clinic to therapy the radioactive exposure. Importantly, the PBNPs were highly dispersible and stable in both water and biological mimic environments such as blood serum without the appearance of aggregation within 1 week [16], and have good photothermal stability that could reuse the PBNPs during practical applications [17]. For example, Liang et al. [13] firstly demonstrated that PBNPs with strong absorption in the NIR region can be used as an excellent contrast agent to enhance photoacoustic imaging. PBNPs with uniform size and good colloidal stability can be fabricated from low-cost chemical agents by an easy way.

The PBNPs have been used for labeling some tumor cells as the MRI agent in research [18], but little studies were reported on the application of PBNPs in the MSCs. Here, we report that PBNP-labeled mesenchymal stem cells exhibited normal cell viability, proliferation, migration, cytoskeleton, differentiation, and protein expression in vitro. Further work is needed if this is a reality in vivo and to make sure if directed intralesional delivery of PBNP-labeled MSCs is as critical as cell tracking thought.

## Methods

## Cell Culture

Mouse MSCs C3H10T1/2 were obtained from Nanjing KeyGen Biotech. Inc. Cells were cultured in Dulbecco's modified Eagle's medium (DMEM; Hyclone, USA) supplemented with 10% fetal bovine serum (FBS; Israel) and 1% penicillin-streptomycin (Hyclone, USA) at 37 °C with 5%  $CO_2$  saturation, and the medium was changed every 3 days. After four passages, the cells were used for experiments.

## Preparation of PBNPs

In a typical synthesis, 2.5 mmol of citric acid (490 mg) was first added to a 20 mL 1.0 mM aqueous FeCl<sub>3</sub> solution under stirring at 60 °C. To this solution was dropwise added a 20 mL 1.0 mM aqueous  $K_4$ [Fe(CN)<sub>6</sub>] solution containing the 0.5 mmol of citric acid (98 mg) at 60 °C. A clear bright blue dispersion formed immediately. After 30 min, the solution was allowed to cool to room temperature with the stirring continued for another 5 min at room temperature. Then, an equal

volume of ethyl alcohol was added to the dispersion and centrifuged at 10,000 rpm for 20 min to result the formation of a pellet of nanoparticles. The latter was separated again by the addition of equal volume of ethyl alcohol and centrifugation.

## **Characterization of PBNPs**

The infrared spectroscopy of the synthesized PBNPs were measured using an infrared spectrophotometer (IR; Thermo Fisher Nicolet IS10). Morphology of the synthesized PBNPs was examined by transmission electron microscopy (TEM; JEM 2100F). Field-dependent magnetization of PBNPs was researched using a vibrating sample magnetometer (VSM; Lakeshore 7307). X-ray diffraction (XRD) analysis was performed using Bruker D8 ADVANCE A25X (XRD). The polydisperisty index of the PBNPs was determined by Zetasizer Nano ZS.

## Intracellular Distributions of PBNPs and Ultrastructure of Labeled C3H10T1/2 Cells

Transmission electron microscopy (TEM) was performed to assess the intracellular distributions of PBNPs. After the medium was removed, cells were rinsed with PBS and then digested with 0.25% trypsin. Then, the cells were transferred to a 1.5-mL EP tube to be centrifuged (2000 rpm, 5 min). Then, the supernatant was removed and the cells were fixed by 0.25% glutaraldehyde and 1% osmium acid. After cells were rinsed again, the cells were dehydrated in 50% ethanol, 70% ethanol, 90% ethanol, 90% acetone, and 100% acetone for 20 min each. Then, cells were imbedded at 4 °C overnight. Then, 3% uranium acetate-citrate double staining in sections was performed. Finally, images were collected by TEM.

Scanning electron microscopy (SEM) was done to assess the ultrastructure of labeled C3H10T1/2 cells. After the medium was removed, cells were rinsed with PBS and fixed with 3% glutaraldehyde precooling 4 °C overnight. Then, the cells were rinsed twice with PBS and fixed with 1% osmic acid 4 °C for 1 h. After C3H10T1/2 cells were rinsed again, the cells were dehydrated in ascending graded alcohols (30% ethanol, 50% ethanol, 70% ethanol, 80% ethanol, 90% ethanol, 95% ethanol, and 100% ethanol) for  $2 \times 10$  min each. Then, the cells were immersed in 70%, 80%, 90%, 95%, and 100% acetonitrile solution for 15 min each. Then, vacuum drying and spray coating of gold were performed. Finally, images were collected by SEM.

## Cell Viability Analyses of the PBNPs

Cell viability was evaluated using the MTT (Sigma, USA). Cells were seeded into 96-well plates at  $1 \times 10^3$  cells per well at 37 °C with 5% CO<sub>2</sub> atmosphere. After incubation overnight, the culture medium was replaced by 100 µL fresh medium containing different concentrations of PBNPs (0, 5, 10, 20, 40, and 80 µg/mL), and then cells were cultured for another 1 to 3 days. The culture medium was removed, and the cells were incubated with 20 µL of MTT (5 mg/mL) at 37 °C for 4 h. The precipitated violet dye crystals were dissolved in 150 µL of dimethyl sulfoxide (DMSO; Sigma-Aldrich, USA) for 10 min by shaking gently. The optical density (OD) value was measured at a wavelength of 490 nm using a microplate reader. The results of cells were expressed as percent viable cells.

## **Proliferation Assay**

Comparison with MTT, MTS, WST-1, and XTT, RTCA allows the analysis of the whole period of the experiment and does not require the labeling that negatively affects cell culture experiments [19]. So the xCELLigence system (Roche/ACEA Biosciences) was used to measure cell proliferation in real time. Briefly, cells were seeded into E-Plate-16 (ACEA Biosciences, Inc. San Diego, USA) at  $5 \times 10^3$  cells per well with 150 µL complete medium. After growing 24 h, the medium was replaced by fresh medium containing various concentrations of PBNPs and incubated for another 96 h. This system measured the electrical impedance, which was created by cell attachment on the microelectrode-integrated cell culture plates [20], to provide the quantitative information about the cell number and viability in real time by the RTCA-DP instrument [21]. Cellular proliferation was measured periodically every 15 min for the following 4 days.

## **Real-Time Monitoring of Cellular Migration**

C3H10T1/2 cell migration was measured using a real-time cell invasion and migration (RT-CIM) assay system (ACEA Biosciences, Inc. San Diego, USA). Cells have the ability of increasing the impedance to hence "Cell Index" read-outs when they contact and adhere to the sensors due to the cell migration from the upper chamber into the bottom chamber through the membrane. Simply, cells were seeded in the upper chamber at a density of  $4 \times 10^4$  per well in serum-free medium in the presence of various concentrations of PBNPs. The lower chambers of CIM plates were filled with 165  $\mu$ L complete medium containing 10% FBS. Cell migration was monitored by RTCA DP instrument every 10 min for a period of 100 h. Cell index (CI) was used to reflect the results. The value of CI was derived from the change in electrical impedance as the living cells interact with the biocompatible microelectrode surface in the microplate well to effectively measure cell number, shape, and adherence. The more the number of migrated cells, the larger the cell index.

## Cellular Migration Investigation via Transwell Assay

After being cultured with different concentrations of PBNPs for 48 h, the cells with density of  $2 \times 10^6$  cell/cm<sup>2</sup> were cultured in a Transwell chamber (8 µm pore size; BD FalconTM, USA) for 24 h at 37 °C and 5% CO<sub>2</sub>. After culturing, the inner chamber was cleaned, and the migrated cells on the bottom of the chamber was fixed and stained with 0.1% crystal violet. Each step was followed by washing with PBS for 5 min three times. The migrated cells were photographed at different fields of view using an inverted phase-contrast microscope (CK2, Olympus, Japan).

## In Vitro Cell Differentiation

C3H10T1/2 cell-labeled or unlabeled PBNPs were induced to differentiate into two downstream cell lineages of adipocytes or osteocytes. After cells reached confluence in a six-well plate, cells were cultured in in osteogenic induction medium (10% FBS/DMEM containing 10 nM dexamethasone, 50  $\mu$ M ascorbic acid, 10 mM  $\beta$ -glycerophosphate, Sigma) or adipogenic induction medium (10% FBS/DMEM containing 1  $\mu$ M dexamethasone, 0.5 mM isobutylmethylxanthine, 10  $\mu$ M insulin, Sigma). After 3 weeks, the cells were washed with PBS, fixed with 4% polyoxymethylene, and stained with Alizarin Red or Oil Red O (Sigma). The induced cells were photographed at different fields of view using an inverted phase-contrast microscope (CK2, Olympus, Japan).

## Immunofluorescence Assay for F-actin Visualization

MSCs were cultured with various concentrations of PBNPs at a 24-well plate for 48 h. The cells were fixed with 4% paraformaldehyde for 10 min, permeabilized with 0.2% Triton-100 for 5 min, blocked with 1% BSA in PBS for 30 min at room temperature, and then cultured with phalloidine (1:100, Thermo Fisher Scientific, USA) and DAPI (1:800, Thermo Fisher Scientific, USA) for 30 min at room temperature. Fluorescence microscopy was performed on a Nikon eclipse Ti-S microscope with NIS elements software

## Protein Expression by Western Blot Analysis

The protein expression of the cells was evaluated via Western blot analysis. The MSCs were cultured with the medium containing different concentrations of PBNPs (0, 25, 50  $\mu$ g/mL) on six-well plates for 24 h, washed twice with ice-cold PBS, and scraped in 100  $\mu$ l PIPA buffer (Beyotime) containing protease inhibitors and so-dium orthovanadate (Beyotime, China). After 30 min, the samples were centrifuged at 14,000 rpm for 10 min at 4 °C, then the protein concentrations of the samples were determined using BCA kit (Beyotime, China). The same amount of proteins were electrophoresed in 10%

SDS-PAGE gels (Beyotime, China) and transferred to PVDF membrane (GE Healthcare). The membranes were blocked with 5% milk in Tris-buffered saline with Tween20 (TBST) at room temperature for 2 h and then incubated with anti- $\beta$ -catenin (1:1000, CST, USA), anti-vimentin (1:1000, Abiocode), and anti- $\beta$ -actin (1:1000, CST, USA) overnight at 4 °C. The membranes were washed three times for 5 min each and then incubated with the appropriate secondary antibodies for 2 h at room temperature. Signals were detected with ECL and ECL-plus (Beyotime, China) and exposed to Molecular Image<sup>®</sup> ChemiDoc<sup>™</sup> XRS+ system (Bio-Rad Inc., USA) with Image Lab<sup>™</sup> Software using enhanced chemiluminescence.

## Cellular Imaging Investigation of Cellular Labeling Efficiency via MRI

MSCs were treated with different concentrations (25 and 50  $\mu$ g/mL) of PBNPs, and the control cells were cultured with completed medium without PBNPs for 48 h, washed three times with PBS buffer, trypsinized, collected, and then embedded in 1 mL 1% (*w*/*v*) agarose



solution for imaging studies. Additionally, the MSCs labeled with 50  $\mu$ g/mL PBNPs were induced to osteogenic differentiation for 14 days, then were examined the MRI signal effect. The T2-weighted imaging was performed using an inversion recovery gradient echo sequence with TE = 23 ms, TR = 400 ms, NEX = 2.0, a slice thickness of 2 cm, a FOV of 20 × 20 cm, and matrix size of 384 × 256.

## **Statistical Analysis**

The results were expressed as mean  $\pm$  SD of at least three independent experiments performed in triplicate. Treatment groups were compared using one-way analysis of variance (ANOVA) and Student's *t* test was used. *p* < 0.05 was accepted as a significant difference.

## **Results and Discussion**

## PBNP Characterization

Transmission electronic microscopy (TEM) was performed to characterize the PBNPs (Fig. 1a), which have a diameter of 20-25 nm. For the morphology, the PBNPs showed a cuboidal structure. Figure 1b shows the infrared spectroscopy of the synthesized PBNPs. The PBNPs exhibited a typical absorption peak of Fe<sup>3+</sup>-CN around 2085.23 nm, which was in agreement with that of PBNPs. Field-dependent magnetization measurement was further used to study the magnetic properties of the PBNPs. Figure 1c shows magnetization curves of the PBNPs at room temperature, which demonstrated superparamagnetism of the PBNPs. Figure 1d shows the diffraction peaks at 200, 220, 400, and 420, which corroborated with the XRD pattern of PBNPs. Additionally, the polydisperisty index of PBNPs was 0.16, which indicated a uniform particle size distribution.

## Cellular Uptake and Cytotoxicity of PBNPs

To further confirm the cellular uptake of the PBNPs to MSCs, cellular micromorphology of the above C3H10T1/2 cells treated with and without the PBNPs was studied. Figure 2 shows SEM and TEM images of C3H10T1/2 cells after the incubation for 48 h with and without the PBNPs. From the SEM images, the ultrastructure of the labeled C3H10T1/2 cells did not have obvious changes when compared with the control C3H10T1/2 cells. From the TEM images, the control C3H10T1/2 cells without the incubation with the PBNPs exhibited a typical cellular micromorphology with obvious cellular microstructures. Yet, after incubation with the PBNPs, random distribution of the PBNPs was clearly observed in the cytoplasm of the C3H10T1/2 cells. And some PBNPs appeared to be localized in vesicles within the cytoplasm of the cells. Although the random distribution of the PBNPs was observed in the cytoplasm of the C3H10T1/2 cells, the exact mechanism of intracellular uptake was unclear. We propose that the internalization of the PBNPs in C3H10T1/2 cells may occur via a similar mechanism as the previous study demonstrated, which had reported that different inorganic nanoparticles including Prussian blue-Poly(L-lysine), gold, silver, and metaloxides can be readily taken up by cells via endocytosis [15, 22, 23].

To evaluate the cytotoxicity and the cell viability assay in MSCs, MTT method was performed. The cells were incubated for 1 to 3 days at 37 °C under 5% CO<sub>2</sub> with various concentrations of PBNPs suspended in DMEM. Three independent trials were conducted, and the averages and standard deviations were reported. Figure 3 shows that the viability of MSCs treated with PBNPs (5,



Fig. 2 SEM and TEM images of the C3H10T1/2 cells after the incubation with different concentrations of PBNPs for 48 h. a SEM images. b TEM images. ↑, intracellularly distributed PBNPs

10, 20, 40, 80  $\mu$ g/mL) was relative to the control cells at 24 to 72 h, respectively. The results indicated that the PBNPs were non-toxic to cells treated with the same amount of PBNPs as MTT. Furthermore, a real-time proliferation assay using the xCELLigence instrument was used for investigating the growth curves of MSCs. Results showed that the growth curves of MSCs were not significantly influenced by these concentrations of PBNPs (Fig. 4a), and the cell viabilities were counted and showed in Fig. 4b after treating in 24, 48, 72, and 96 h. These results suggest that PBNPs have no effect on the proliferation of MSCs.

## **Cell Migration Capability**

Migration of MSCs treated with various concentrations of PBNPs was tested using Transwell assay and a new technique, RT-CIM assay system. From the Transwell assay, the labeled cells showed no obvious changes in migration. By using the RT-CIM assay system, cell migration was monitored in real time, which reflected a more accurate data and could predict cell migration capability more accurately. From the RT-CIM assay system, although at the beginning of the labeling, the labeled cells migrated slowly than the unlabeled cells. But at 72 and 96 h, there was no significant difference in cell migration between labeled cells and unlabeled cells, indicating that high concentrations of PBNPs did not affect MSC motility (Fig. 5).

## In Vitro Cell Differentiation

The pluripotency of labeled and unlabeled MSCs was investigated by Alizarin Red and Oil Red O staining. Figure 6 shows that labeled MSCs can be successfully differentiated into adipocytes and osteocytes as the unlabeled MSCs did. These results suggest that the PBNPs did not interfere with the cells' differentiation capacity, which kept the pluripotency of labeled MSCs.

## Influence of the Labeling PBNPs on the Cytoskeleton

To investigate the effect of PBNPs on the cytoskeleton of MSCs, immunofluorescence assay of F-actin was used. The phalloidin staining shows no alteration of the red actin filaments of the cytoskeleton after labeling for 48 h compared with unlabeled MSCs. A comparison of the integrity and distribution of actin filaments in the labeled and unlabeled cells for 48 h revealed no alterations (Fig. 7).

## Western Blot Analysis

Wnt signaling pathways play an important role in the regulation of cell proliferation, differentiation, apoptosis, tissue formation, and the stem cell fate [24]. So, β-catenin is the functional protein of MSCs. Additionally, the vimentin is the mesenchymal biomarker and is also the functional protein of MSCs [25]. These two proteins related with the biological function of MSCs. The expressions of  $\beta$ -catenin and vimentin were evaluated by Western blot analysis. Figure 8 shows that the expression of  $\beta$ -catenin and vimentin of MSCs treated with various concentrations of PBNPs for 48 h had no significant changes compared with the expression of MSCs treated with no PBNPs. These results indicated that PBNPs cannot change the expression of β-catenin and vimentin of MSCs, which showed the stability of biological function of MSCs after treatment with PBNPs.



Wen et al. Nanoscale Research Letters



(2018) 13:329



## In Vitro MRI

MSCs, like other stem cells, have the potential to differentiate bone, cartilage, fat, muscle, and cardiac cells, which have become an important source for regenerative medicine. And tracking the migration and outcome of MSCs is so important to evaluate the role and outcome of exogenous MSCs in defect repair. Magnetic resonance imaging (MRI) helped to observe MSCs after clinical administration, and MRI contrast agent is necessary. The potential of PBNPs used as an effective T2-weighted cellular MRI contrast



Fig. 6 In vitro cell differentiation of cells with or without PBNPs. Oil Red O staining for adipocyte and Alizarin Red staining for osteocytes. Images were obtained 3 weeks after labeling (magnification × 200)



agent has been demonstrated [14], and some other studies also demonstrated the surface modification of PBNPs enhances its performance in MRI [17, 26]. Currently, PBNP labeling has been used in a variety of cells. Dumont et al. described PBNPs as agents for MRI and fluorescencebased imaging of pediatric brain tumors [27]; Perera et al. developed the gadolinium-incorporated PBNPs for the early detection of tumors in the gastrointestinal tract [28]; and Cano-Mejia et al. combined Prussian blue nanoparticle (PBNP)-based photothermal therapy (PTT) with anti-CTLA-4 checkpoint inhibition to treat neuroblastoma [29]. However, there is rarely related reports on PBNP-labeled MSCs. Additionally, whether there is any negative influence on cell function and viability of MSCs after labeling PBNPs remains unclear

To investigate whether the PBNPs have the ability to enhance the T2-weighted MRI contrast of cells, we incubated the MSCs with or without PBNPs and examined the MRI signal effect. To monitor the temporal stability of labeling and to investigate whether the PBNPs would lose its imaging capability when the MSCs differentiated, we incubated the MSCs with PBNPs and induced the MSCs to osteogenic differentiation for 14 days then examined the MRI signal effect. As shown in Fig. 9, the pellets of the MSCs incubated with PBNPs showed a clear MRI signal darkening effect and the SI value of the labeled MSCs had obvious difference with unlabeled MSCs. Notably, the labeled MSCs also showed a clear MRI signal darkening effect when differentiation is induced. These results demonstrated that PBNPs had the potential to be used as an effective T2 contrast agent for cellular imaging of MSCs and can offer long-term retention of the contrast agent even after the cell differentiation.





There are many published data of MSCs labeled with magnetic nanoparticles (MNPs), but the application of MNPs was limited by their cytotoxicity. When delivering MNPs to target tissue, the majority of MNPs often distribute in the liver and spleen, so the toxicity of MNPs cannot be neglected [30]. For example, Costa C found that SPIONs could produce cytotoxicity to neuronal cells and glia cells [31]. As we mentioned above, the PBNPs showed no detectable cytotoxicity and had no effects on the cell characteristics of MSCs including cyto-skeleton, cellular morphology, and functional protein. Thus, the strength of using PBNPs as an effective T2-weighted cellular MRI contrast agent would be demonstrated in terms of the cytotoxicity.

## Conclusions

In summary, we introduced the PBNPs to the tracking of mesenchymal stem cells and studied the survival, migration potential, and cell characteristics of MSCs after being labeled with the PBNPs. Furthermore, we also demonstrated the potential of PBNPs as an effective T2-weighted MRI contrast agent for the cellular MRI of MSCs. PBNPs can be effectively used for the labeling of MSCs and will not influence the biological characteristics of MSCs. This conclusion paved a new road for the label of MSCs.

### Abbreviations

DMEM: Dulbecco's modified Eagle's medium; DMSO: Dimethyl sulfoxide; FBS: Fetal bovine serum; MRI: Magnetic resonance imaging; MSC: Mesenchymal stem cell; NIR: Near infrared; OD: Optical density; PBNP: Prussian blue nanoparticle; TEM: Transmission electron microscopy; VSM: Vibrating sample magnetometer

## Acknowledgements

The authors thank the National Natural Science Foundation of China and Foundation of Sichuan Provincial Science and Technology Program for the financial support of this study.

### Funding

Funding was received from the following:

- 1. National Natural Science Foundation of China (Grant No. 11262020)
- 2. Foundation of Sichuan Provincial Science and Technology Program (Grant Nos. 2016SZ0020, 2014FZ0074, and 2014SZ0002-15).
- 3. Sichuan University Graduate Research Innovation Fund (2018YJSY095).
- Chengdu technological innovation research and development project (2018-YF05-00195-SN).

#### Availability of Data and Materials

We are also trying to make the availability of research data more transparent. So, at the same time, supporting data will be available to editors and peer reviewers at the time of submission for the purposes of evaluating the manuscript and the future researches. All the data is applicable, and all the materials are promptly available to others without undue qualifications.

#### Authors' Contributions

ZZ and RT designed the experiment. JW and ZZ carried out the experiment. JW and YM analyzed the data and the analysis tools. JW, ZZ, and RT wrote the manuscript. LH assisted with the proofing of the manuscript. All authors read and approved the final manuscript.

#### **Competing Interests**

The authors declare that they have no competing interests.

## **Publisher's Note**

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

#### Author details

<sup>1</sup>West China School of Basic Medical Sciences & Forensic Medicine, Sichuan University, No17, 3rd section, Renmin Nanlu Road, Chengdu 610041, Sichuan, China. <sup>2</sup>College of Pharmaceutical and Biological Engineering, Shenyang University of Chemical Technology, Shenyang, China. <sup>3</sup>West China School of Stomatology Medicine, Sichuan University, Chengdu, China. <sup>4</sup>Department of Gynecology, West China Second University Hospital, Sichuan University, Key Laboratory of Birth Defects and Related Diseases of Women and Children (Sichuan University), Chengdu, China. <sup>5</sup>Deep Undergroud Space Medical Center, West China Hospital, Sichuan University, No.17, 3rd Section, Renmin Nanlu Road, Chengdu 610041, Sichuan, China.

## Received: 1 February 2018 Accepted: 24 September 2018 Published online: 22 October 2018

#### References

- Li L, Jiang J (2011) Regulatory factors of mesenchymal stem cell migration into injured tissues and their signal transduction mechanisms. Front Med 5: 33–39.
- Tarnowski M, Sieron AL (2006) Adult stem cells and their ability to differentiate. Med Sci Monit 12:RA154–RA163.
- Kariminekoo S, Movassaghpour A, Rahimzadeh A, Talebi M, Shamsasenjan K, Akbarzadeh A (2016) Implications of mesenchymal stem cells in regenerative medicine. Artif Cells Nanomed Biotechnol 44:749–757.
- Zimmerlin L, Park TS, Zambidis ET, Donnenberg VS, Donnenberg AD (2013) Mesenchymal stem cell secretome and regenerative therapy after cancer. Biochimie 95:2235–2245.

- Hossain MA, Chowdhury T, Bagul A (2015) Imaging modalities for the in vivo surveillance of mesenchymal stromal cells. J Tissue Eng Regen Med 9: 1217–1224.
- Zhang M, Liu X, Huang J, Wang L, Shen H, Luo Y et al (2017) Ultrasmall graphene oxide based T1 MRI contrast agent for in vitro and in vivo labeling of human mesenchymal stem cells. Nanomedicine. Volume 14, Issue 7, Pages 2475-2483.
- Patel S, Lee KB (2015) Probing stem cell behavior using nanoparticle-based approaches. Wiley Interdiscip Rev Nanomed Nanobiotechnol 7:759–778.
- Higuchi Y (2012) Development of fluorescent labeling methods for stem cells. J Pharm Soc Jpn 132:433–439.
- Wu X, Hu J, Zhou L, Mao Y, Yang B, Gao L et al (2008) In vivo tracking of superparamagnetic iron oxide nanoparticle-labeled mesenchymal stem cell tropism to malignant gliomas using magnetic resonance imaging. Laboratory investigation. J Neurosurg 108:320–329.
- Li C, Ruan J, Yang M, Pan F, Gao G, Qu S et al (2015) Human induced pluripotent stem cells labeled with fluorescent magnetic nanoparticles for targeted imaging and hyperthermia therapy for gastric cancer. Cancer Biol Med 12:163–174.
- 11. Wang J, Jokerst JV (2016) Stem cell imaging: tools to improve cell delivery and viability. Stem Cells Int 2016:9240652.
- Valdiglesias V, Kilic G, Costa C, Fernandez-Bertolez N, Pasaro E, Teixeira JP et al (2015) Effects of iron oxide nanoparticles: cytotoxicity, genotoxicity, developmental toxicity, and neurotoxicity. Environ Mol Mutagen 56:125–148.
- Liang X, Deng Z, Jing L, Li X, Dai Z, Li C et al (2013) Prussian blue nanoparticles operate as a contrast agent for enhanced photoacoustic imaging. Chem Commun 49:11029–11031.
- Fu G, Liu W, Feng S, Yue X (2012) Prussian blue nanoparticles operate as a new generation of photothermal ablation agents for cancer therapy. Chem Commun 48:11567–11569.
- Kim T, Lemaster JE, Chen F, Li J, Jokerst JV (2017) Photoacoustic imaging of human mesenchymal stem cells labeled with Prussian blue-poly(l-lysine) nanocomplexes. ACS Nano 11:9022–9032.
- Shokouhimehr M, Soehnlen ES, Hao J, Griswold M, Flask C, Fan X et al (2010) Dual purpose Prussian blue nanoparticles for cellular imaging and drug delivery: a new generation of T1-weighted MRI contrast and small molecule delivery agents. J Mater Chem 20:5251–5259.
- Cheng L, Gong H, Zhu W, Liu J, Wang X, Liu G et al (2014) PEGylated Prussian blue nanocubes as a theranostic agent for simultaneous cancer imaging and photothermal therapy. Biomaterials 35:9844–9852.
- Chen Y, Wu L, Wang Q, Wu M, Xu B, Liu X et al (2016) Toxicological evaluation of Prussian blue nanoparticles after short exposure of mice. Hum Exp Toxicol 35:1123–1132.
- LTR Ş, Albeniz GR, Dinç BR, Albeniz I (2017) iCELLigence real-time cell analysis system for examining the cytotoxicity of drugs to cancer cell lines (review). Exp Ther Med. Volume 14, Issue 3, Pages 1866-1870.
- Irelan JT, Wu MJ, Morgan J, Ke N, Xi B, Wang X et al (2011) Rapid and quantitative assessment of cell quality, identity, and functionality for cellbased assays using real-time cellular analysis. J Biomol Screen 16:313–322.
- Xing JZ, Zhu L, Jackson JA, Gabos S, Sun XJ, Wang XB et al (2005) Dynamic monitoring of cytotoxicity on microelectronic sensors. Chem Res Toxicol 18: 154–161.
- Lu J, Ma S, Sun J, Xia C, Liu C, Wang Z et al (2009) Manganese ferrite nanoparticle micellar nanocomposites as MRI contrast agent for liver imaging. Biomaterials 30:2919–2928.
- Pan D, Caruthers SD, Hu G, Senpan A, Scott MJ, Gaffney PJ et al (2008) Ligand-directed nanobialys as theranostic agent for drug delivery and manganese-based magnetic resonance imaging of vascular targets. J Am Chem Soc 130:9186–9187.
- Jing Y, Zhang JC, Li ST, Zhao JH, Wang J, Han XF et al (2015) Wnt/beta-catenin pathway might underlie the MET in trans- differentiation from MSC to MSCderived neuron. Zhongguo Ying Yong Sheng Li Xue Za Zhi 31:572–576.
- Li YY, Choy TH, Ho FC, Chan PB (2015) Scaffold composition affects cytoskeleton organization, cell-matrix interaction and the cellular fate of human mesenchymal stem cells upon chondrogenic differentiation. Biomaterials 52:208–220.
- Zhu W, Liu K, Sun X, Wang X, Li Y, Cheng L et al (2015) Mn2+-doped prussian blue nanocubes for bimodal imaging and photothermal therapy with enhanced performance. ACS Appl Mater Interfaces 7:11575–11582.

- Dumont MF, Yadavilli S, Sze RW, Nazarian J, Fernandes R (2014) Manganesecontaining Prussian blue nanoparticles for imaging of pediatric brain tumors. Int J Nanomedicine 9:2581–2595.
- Perera VS, Chen G, Cai Q, Huang SD (2016) Nanoparticles of gadoliniumincorporated Prussian blue with PEG coating as an effective oral MRI contrast agent for gastrointestinal tract imaging. Analyst 141:2016–2022.
- Cano-Mejia J, Burga RA, Sweeney EE, Fisher JP, Bollard CM, Sandler AD et al (2017) Prussian blue nanoparticle-based photothermal therapy combined with checkpoint inhibition for photothermal immunotherapy of neuroblastoma. Nanomedicine 13:771–781.
- Li X, Wei J, Aifantis KE, Fan Y, Feng Q, Cui FZ et al (2016) Current investigations into magnetic nanoparticles for biomedical applications. J Biomed Mater Res A 104:1285–1296.
- Costa C, Brandao F, Bessa MJ, Costa S, Valdiglesias V, Kilic G et al (2016) In vitro cytotoxicity of superparamagnetic iron oxide nanoparticles on neuronal and glial cells. Evaluation of nanoparticle interference with viability tests. J Appl Toxicol 36:361–372.

## Submit your manuscript to a SpringerOpen<sup>®</sup> journal and benefit from:

- Convenient online submission
- ► Rigorous peer review
- Open access: articles freely available online
- High visibility within the field
- Retaining the copyright to your article

Submit your next manuscript at ► springeropen.com