NANO EXPRESS

Open Access



Influence of Carbon Nanotubes and Its Derivatives on Tumor Cells In Vitro and Biochemical Parameters, Cellular Blood Composition In Vivo

Olena M. Perepelytsina^{1*}, Andriy P. Ugnivenko¹, Alexey V. Dobrydnev², Olga N. Bakalinska³, Andrii I. Marynin⁴ and Mychailo V. Sydorenko¹

Abstract

The aim of the proposed work was to analyze the toxicity of oxidized carbon nanotubes (CNTox), functionalized by doxorubicin (CNT-Dox) and fluorescein (CNT-FITC) on cell and organism level. The cytotoxic effect of CNTox, CNT-Dox, and CNT-FITC was analyzed on tumor cells in vitro (2-D, 3-D cultures) and on Balb2/c mice model in vivo. As a result, it was demonstrated the possibility of doxorubicin immobilization on the surface of CNT and controlled release of doxorubicin (Dox) from the surface of CNT. Dox immobilization coincident with decreasing cytotoxic effect CNT-Dox compared with free Dox. Breakdown of peptide bonds with CNT surface led to the release of doxorubicin and dosedependent enhancement of the cytotoxic effect of CNTs and Dox. The combined cytotoxic effect from CNTs, Dox, and trypsin on the survival of tumor cells was shown. At the organism level, it was investigated the effect of the obtained nanostructures on the state of hepatic enzymatic system, the protein metabolism, and cell blood composition of the experimental animals. CNTox influence in vivo model was statistically the same as control. CNT-Dox demonstrated lower total organism toxic effect compared to the pure doxorubicin. Deviations in the cell blood composition indicated a general toxic effect of CNT-Dox, but it was more moderate compared with of pure doxorubicin. From the data obtained, we concluded that binding CNTs with doxorubicin allows reducing toxicity of the doxorubicin on the general biochemical indicators of blood and violations in the blood cells composition in vivo. At the same time, the combined effect of CNTs and doxorubicin after drug release allowed us to achieve greater efficacy in suppressing tumor growth in vitro.

Keywords: Multi-walled carbon nanotubes, Nanotoxicity, Multicellular tumor spheroids, Doxorubicin, Hepatic function, Cell blood composition

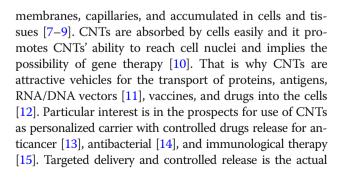
PACS: 61.46+w61.48+c61.48De87.15-v87.64-t

Background

One of the most striking and promising applications of carbon nanotubes is medicine. Carbon nanotubes (CNTs) are characterized by unique chemical and biological properties [1-5]. CNTs have a large surface area that allows them to attach a wide range of biological substances [6]. In addition, CNTs are able to penetrate through cell

¹Department for Biotechnical Problems of Diagnostic IPCC, Nauky str.,42/1, Kiev 03028, Ukraine

Full list of author information is available at the end of the article





© The Author(s). 2018 **Open Access** This article is distributed under the terms of the Creative Commons Attribution 4.0 International License (http://creativecommons.org/licenses/by/4.0/), which permits unrestricted use, distribution, and reproduction in any medium, provided you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons license, and indicate if changes were made.

^{*} Correspondence: olenaquail@gmail.com

problem of the modern use of drugs, especially with cytotoxic properties. The exact mechanism of drug release ensures an effective concentration of the active substance in the target tissue with a minimal concentration in others. It would reduce the dose of the drug with maintaining its effectiveness and diminution of harm from side effects. Currently, there are various ways of purposeful drug delivery, such as delivery using liposomes [16], polymeric micelles and dendrimers [17], biodegradable particles [18], and other nanoparticles [19]. But recent experiments have demonstrated a lot of benefits from using CNTs in delivering drugs compared to other nanoparticles [20, 21]. One of them is that CNTs with fairly large and active surface that can be filled with the desired chemical substance, ranging from small molecules to proteins, antibodies, and RNA/ DNA. Open ends of CNTs make the inner volume and surface accessible for functionalization. So, the large surface area of CNTs provides a lot of binding sites for different type of functionalization. At the same time with prospects of CNTs, there are some problems with low solubility of CNTs, ability for aggregation, hydrophilic qualities, long half-life, and influence on whole organism [22]. According to the literature, the introduction of CNTs into the body of experimental animals is accompanied with accumulation of CNT and its derivatives in the organs of the digestive tract, spleen, kidneys [23], muscles [24], and lung tissue [25]. On the next step, CNTs influence on the activity of metabolic and inflammatory processes [25, 26], state of immunity system [27], and survival of experimental animals [28]. Nevertheless, these problems are the subject of active research for further advancement in the use of carbon nanotubes. The advantages of CNTs as nano-vectors for drug delivery have been convincingly demonstrated in a number of studies. Authors of [29, 30] reported that specific nanotubes may be less harmful than nano-carriers for drugs. It has also been shown that simple functionalization (-OH, -COOH, -NH, PEG) [31] or encapsulation of the CNTs [22], increases the water solubility, improves bioavailability, and reduces toxicity of CNTs. And the introduction of CNTs to mice with a transplanted tumor may be effective against targeted transformed tissue and led to decreasing of tumor volume and to increasing animal survival [32].

At the base of previous investigations [33], we assumed that active antitumor substance (doxorubicin) could be immobilized on the surface of carbon nanotube peptide bonds. The resulting compound, carbon nanotubes which were functionalized by doxorubicin (CNT-Dox), could reduce cytotoxic properties of CNT as doxorubicin (Dox). At the same time, the disintegration of the treated construct may allow to realize the cytotoxic properties CNT and Dox. Thereby, it is possible to achieve increasing the antitumor activity of both substances. Therefore, the aim of present study was to determine the cytotoxic effect of CNTs-Dox construct in the presence of protease (trypsin) in vitro. We analyzed the impact of CNTs and its derivatives on tumor cells in 2D and 3D cell model, in vitro. The other aim was to investigate the influence of the obtained compounds (CNTs, CNTox, and CNT-Dox) on the activity of hepatic enzyme system, proteins turnover, and on cellular blood composition in vivo. So, the authors realized a complex estimation of the toxicity, bioavailability, and effectiveness of the use of CNTs and their derivatives against tumors of gastrointestinal tract.

Methods

Cell line of Caucasian colon adenocarcinoma grade II carcinoma (HT29) was used as experimental cell model in 2D (monolayer) and 3D (spheroid) system in vitro. The line was purchased from Bank of cell lines and tissues of animals Kavetsky' Institute of experimental pathology, oncology, and radiobiology NAS Ukraine. The cells were handled in standard cell culture conditions (95% humidity, 5% CO₂ in air; 37 °C) in DMEM full medium with 10% FBS under laboratory containment level 2.

Synthesis, Oxidation, and Functionalization of CNT

The initial Multi-walled carbon nanotubes (MWCNTs) were obtained by chemical vapor deposition (propylene and hydrogen with Mo/Fe/Al₂O₃ as catalyst). Synthesized MWCNTs had 10–30 layers, internal diameter 5–15 nm, external diameter 10–60 nm, length 20–500 μ m, specific surface area 120 m²/g and bulk density 5–50 g/l [33].

Purification of MWCNTs from the metal/catalyst was performed by HF treatment. Elimination of amorphous carbon from carbon nanomaterials was realized by oxidation in air at 450–500 °C. The crude sample containing MWCNTs reacted with oxygen from air and created carbon dioxide or carbon monoxide. Some amount of carbon deposit has been obtained after HF (aqua) dissolution of the catalyst support was oxidized in air at 450–500 °C. An air flow quartz tubular reactor was used for this procedure for 130–150 min. We analyzed and described physical and chemical characteristics of obtained MWCNTs in previous work [33].

Scanning electron spectroscopy (SEM) of MWCNTs (JEOL SL6060LA, Japan) was used to determine the structural characteristics of MWCNTs. After immobilization of the ligands, the morphology was not changed.

Oxidation of MWCNTs

On the next step, the purified carbon nanotubes (CNTs) were oxidized in 70% HNO_3 at 99 °C for 4 h and then washed with distilled water and 10% NH_4OH solution for 12 h. As a result, carbon nanomaterial oxides MWCNTox (CNTox) were synthesized. After that, CNTs were washed thrice with dH_2O to neutral pH. The acidic sites on CNT surface were regenerated with 0.1 M HCl solution. The

resulting oxidized CNTs-ox were separated by centrifugation, rinsed extensively, and re-suspended in dH_2O water.

Preparation of CNT-Dox Particles

The task of the next step was to immobilize Dox hydrochloride (Dox, Teva Nederland B.V, Netherlands) on the surface of MWCNTs particles. To functionalize the surfaces of oxidized CNTs (200 mg) by amino containing Dox-lactose monohydrate, they were incubated with bifunctional linking agent-N-cyclohexyl-N'-(2 morpholinoethyl) carbodiimide metho-p-toluenesulfonate (C 1011, Sigma Aldrich, USA) during 15 min at room temperature (Fig. 1a). After that, 100 mg DOX-lactose monohydrate was added into 10 ml of 0.15 M phosphate buffer pH 6.5 to each nanocarbon materials. The mixture was allowed to react at 30 °C for 24 h. In such conditions, covalent binds between Dox and CNTs were formed (Fig. 1b). The composition were collected by centrifugation at 10,000 rpm 15 min and washed with dH₂O thrice. Supernatants were used for detection concentration of free DOX by spectrophotometer. Immobilization of FITS on CNT surface was provided by scheme shown on Fig. 2a, b.

Preparation of Stable Suspensions of MWCNTs

The colloidal suspension of MWCNTs was carried out in two stages. In the first stage, carbon nanomaterials have been subjected to ultrasonic treatment in phosphate saline buffer (PBS) using an ultrasonic disperser UZDN—2 T. The processing modes were I = 10 mA, R = 22 kHz, duration—30 min. In the second stage, the resulting hydrosol was dispersed by the centrifugation at room temperature.

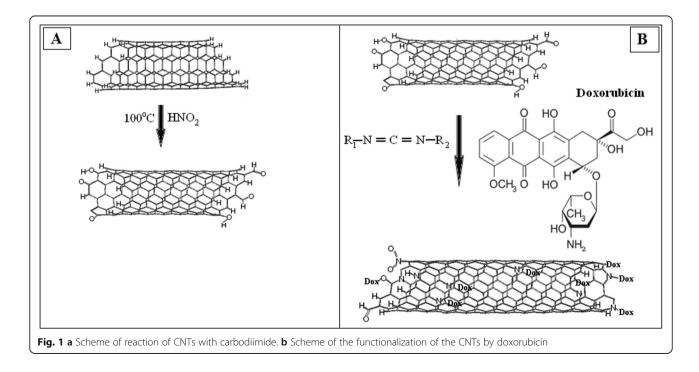
The process includes several centrifugation cycles. So, the hydrophilic dissolving SWCNTs fraction was selected this way. Before adding to the suspension cultured cells, solutions of MWCNTs were sterilized by boiling during 30 min. Derivatives of CNTs (CNT-Dox and CNT-FITC) were sterilized by 100-fold concentration of PSGA (Penicillin: Streptomycin: Gentamycin: Amphotericin).

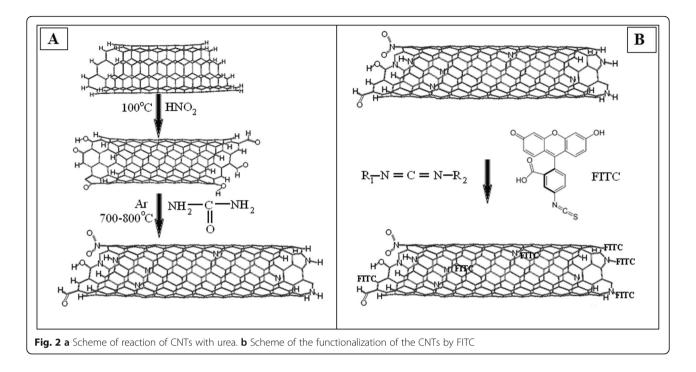
Zeta Potential of Suspensions of Nanotubes

Zeta potential of samples were measured by electrophoretic light scattering (M3-PALS). For measurements, the Zetasizer Nano ZS analyzer, manufactured by Malvern Instruments (Malvern, UK), was used. Experiments were carried out at 25 °C with seven repeats. To measure the samples, a universal submersible electrode (Universal Dip Cell) ZEN1002 and polystyrene cuvettes (DTS001), a light source—an H-Ne 633 nm laser, were used.

FTIR Spectroscopy

The chemical composition of the obtained nanomaterials was investigated by Fourier-transform infrared (FTIR) spectroscopy. IR spectra were determined by FTS 7000e Varian FTIR spectrometer. Samples for analysis were prepared by grinding in a mill a mixture of ~ 1 mg of CNTs and 150 mg of spectrally pure KBr. Samples were prepared by using a press with a pressure force of $3.0-3.5 \times 10^3 \text{ kg/cm}^2$. The samples were dehydrated by heating at a temperature of 600 °C for 60 min. Pre-shot spectra of KBr were preliminary obtained, after that they were subtracted from the spectra of the samples. All spectra was analyzed according catalog of Spectrometric





Identification of Organic Compounds [34]. For comparison, samples of MWCNTs oxidized (CNT-O), MWCNTs functionalized by doxorubicin (CNT-D), and MWCNTs functionalized by fluorescent label (CNT-F) were used. All processing and conditions, of samples and concentration, were the same for three materials.

Colorimetric Assay of Doxorubicin Release from CNTs Surface

To evaluate the amount of free Dox after immobilization on CNMs and the effectiveness of the Dox release, the ability of free Dox to fluorescent at a wavelength of 495 nm was used [35]. Active concentration of Dox in Dox hydrochloride was 16.7% *w/w*. For the purpose of drawing the calibration lines, Dox Teva 20 mg/ml with ten dilutions to 8×10^{-3} mg/ml was used. Then, the fluorescence of free Dox was measured in supernatant from complexes DOX with CNTs by spectrophotometric plate reader Multiscan (Labsystem, Finland).

Functional Groups Concentration in CNT-DOX, CNT-FITC Particles

For Dox immobilizations, 1 g of MWCNTs in 1 ml dH_2O was used. The amount of Dox-TEVA was 100 mg of (16.7 mg of active Dox) in 1 ml dH_2O . The amount of free Dox in supernatant after reaction was 0.37 mg or 2.2% from active substances. Thus, we made the conclusion that 16.23 mg of DOX was immobilized on 1 g of CNTox. For FITC percent of immobilization was low. Then, 8.35 mg of FITC was immobilized on 1 g of CNTox in 1 ml dH_2O . Effectiveness of functionalization

was 1.62% w/w for CNT-DOX and 0.84% w/w for CNT-FITC. Further calculation of concentrations CNT-Dox and CNT-FITC are based on these data.

Cytotoxic Assay of CNT Derivatives on 2-D and 3-D Cell Model

The cytotoxicity of Dox, CNTs, CNT-FITC, and CNT-Dox was evaluated against HT29 tumor cell using MTT assay. MTT test based on conversion of 3-[4,5-dimetltiazol-2]-2,5-dipheniltetratetrazolium salts to formazan crystals by NAD(P)H-dependent mitochondrial oxidoreductase enzymes in alive cells. Protocol was described by T. Mosmann [36]. In brief, 1×10^4 HT29 were seeded in 96-well plates and cultured in full culture medium for 12 h. Then, current culture medium was replaced by culture medium containing CNTox (sample #1), MWCNTs (sample #2), CNT-Dox (sample #3), Dox (sample #4), and CNT-FITC (sample #5). Concentrations of samples # 1, 2, 3, 5 were 12.5–25–50–100–200 µg/ml, stock concentration of sample #4 was 20 µg/ml, end concentration from 1 to 10 µg/ml. Cells were cultured in full medium and were used as control. After 24 h of incubation, cells were analyzed with MTT by colorimetric assay. To 100 µl of cells suspension, we added 20 µl MTT solution (5 mg/ml PBS, Sigma). After that, cells were incubated with MTT during 4 h in standard conditions. Then, samples were centrifuged under 1500 g, during 5 min, and supernatant was extracted. In all, wells were added 10 µl DMSO (Sigma) for MTT crystals dilution and 20 µl of 25 mM glycine. The absorbance of reacted

solution was measured at 540 nm on spectrophotometric plate reader Multiscan (Labsystem, Finland).

Multicellular Tumor Spheroids Generation

HT29 cells multi-cellular tumor spheroid (MTS) (3D culture) as model system of tumor micrometastasis was cultured by well-established method which was described earlier [33]. Briefly, cell suspension were counted using Trypan blue and planted an equal number of cells $(5 \times 10^4 \text{ cells/ml})$. The 3D cell culture was maintained in DMEM (Sigma, USA) medium with 10% FBS (Sigma, USA) in standard conditions (95% humidity, 5% CO₂ in air, 37 °C). Generation of MTS was performed by technology which was developed in our laboratory. The cultivation of tumor cells were maintained for 24 h in 24-well plates coated with 1% agar in culture medium with 0.24% of carboxy-methyl-cellulose. For investigating the dependence of the size and number of MTS on the concentration and type of CNTs, MTS was generated in the presence of various concentrations of CNTs. Before MTS generation to the cell cultures, CNTs solution in PBS was added in culture to the end concentration as described previously for MTT assay. Further cultivation was conducted during 48 h at a constant rotation of plates on orbital shaker (80 rpm). At the next stage, micro photo images were taken by "dark field" method. Overall, more than 120 images were done. Then, the volume of all MTS, which were on the files, was calculated with the use Axio Vision Rel 4.7 program, Zeiss. We used the formula of Rolf Bjerkvig: $V = 0.4 \cdot a \cdot b^2$, where geometric sizes of the spheroids (b < a) [37]. The visualization of the results was carried out on a Stemy 2000C microscope, Zeiss.

Analysis of the Impact of CNTs on Hepatic Enzyme System, Proteins Turnover, and on Cellular Blood Composition In Vivo

The procedures involving the animals and their care were conformed to the European directive 2010/63 EU, approved by the local Animal Experimentation Ethics Committees (Protocol №1 21.10.2016). In order to analyze the influence of the obtained substances on the general condition of the organism homeostasis, a series of experiments in vivo was conducted. In vivo studies mice of the Balb/2a line were used. Male and female mice were equal in the groups, aged 6-8 weeks, ten for each group. Mice were housed in cages with steel wire tops and corn-cob beddings and maintained in a controlled atmosphere with 12/12 dark/light cycle, temperature of 22 $^{\circ}C \pm$ 3 °C, and humidity of 50-70%, with free access to food and fresh water. Thus, four groups of mice were formed. Group 1: intact animals were treated with 200 µl of PBS, control. Group 2: mice were treated with CNTox in dose 1.5 mg/kg. Group 3: mice were treated with CNT-DOX in dose 1.5 mg/kg. And in group 4, mice were treated doxorubicin in dose 20 mg/kg. Mice received CNT parenteral in 200 μ l of PBS, every 3 days, during 4 weeks. Doxorubicin was administered intraperitoneally, once every 3 days, at a concentration of 20 mg/kg body weight.

Serum Biochemical Analysis

One month later, mice were withdrawn from the experiment. Cardiac blood samples were immediately collected from dead animals. Blood was taken from animals at the same time from 10 to 11 a.m. For plasma, blood was incubated for 40 min at 37 °C and then centrifuged (20 min, 2000 rpm). Then biochemical parameters, total protein, albumin, aspartate aminotransferase (AST) and alanine aminotransferase (ALT), alkaline phosphatase (ALP), were determined in the plasma with diagnostic kits (Cormay, Warsaw, Poland). Experiments were carried out by unified laboratory protocols on the semi-automatic biochemical analyzer FP-901M (Labsystems, Finland). Cellular blood composition was determined on a hematological analyzer Mindray BC-3000 Plus, China.

Statistical Analysis

For statistical analysis of 3D culture, all cell aggregates were sorted into groups according to size from 1×10^{-4} mm³ to 1×10^{-2} mm³ with step in 1×10^{-3} mm³. Then number on MTS in each group and median of MTS volume for each group were estimated. All measurements were repeated three times. For micro statistic assay normally distributed random variables, we used the Student's coefficient for small population. The indicated *p* value was **p* ≤ 0.05 or ***p* ≤ 0.01.

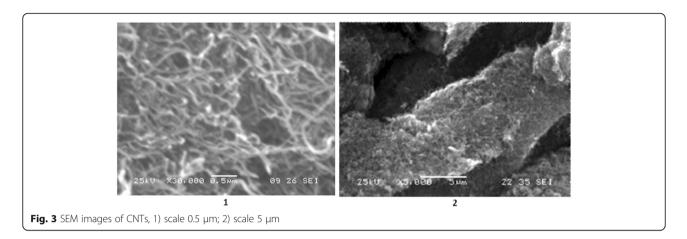
Results and Discussion

Scanning Electron Microscopy of MWCNTs

According to protocol [38], the average diameter of CNTs was 10–20 nm and specific surface area determined by argon desorption was 200–400 m²/g. Bulk density within 20–40 g/dm³. In particular, the agglomerates in the form of the entangled tubes with dimensions of 20–500 μ m are obtained during an industrial CNT production applying CVD method (Fig. 3).

Zeta Potential of Suspensions of Nanotubes

CNTox and CNT indicate significant stability to aggregation, which directly depends on the value of the zeta potential. CNT-DOX has a smaller zeta potential than CNTox and CNT, and high reproducibility of the measurement, which indicates the homogeneity of the particles (Table 1). A small value of the zeta potential of CNT-FITC can indicate significant particle sizes or their small concentrations, as indicated by the high noise ratio at measurement.



FTIR Spectroscopy of CNTs, CNT-Dox, and CNT-FITC

The bindings between CNTox and doxorubicin (DOX) and fluorescein (FITC) were estimated on the basis of infrared spectral data as demonstrated in Fig. 4.

The presence of a strong band at $v = 3311 \text{ cm}^{-1}$ (CNT-O) and $v = 3451 \text{ cm}^{-1}$ (CNT-D) attributed to the CON-H coupling fluctuations, as well as the presence of a strong band at $v = 1634 \text{ cm}^{-1}$ (CNT-O) and $v = 1631 \text{ cm}^{-1}$ (CNT-D) attributed to the O-CNH bonding vibrations, which clearly indicates the type of amide bond between CNT and Dox. Also, IR showed the absorption of C-H bonds which is located at 2969–2834 cm⁻¹ and a broad band at 1460–1407 cm⁻¹ from the C-O-H fragment. Thus, we can conclude that as a result of chemical reactions, CNTs were functionalized with an antitumor drug (doxorubicin) and a fluorescent label (FITC).

Cytotoxicity of CNTs at Different Stages of Functionalization on Monolayer and Spheroids Cell Growth Models

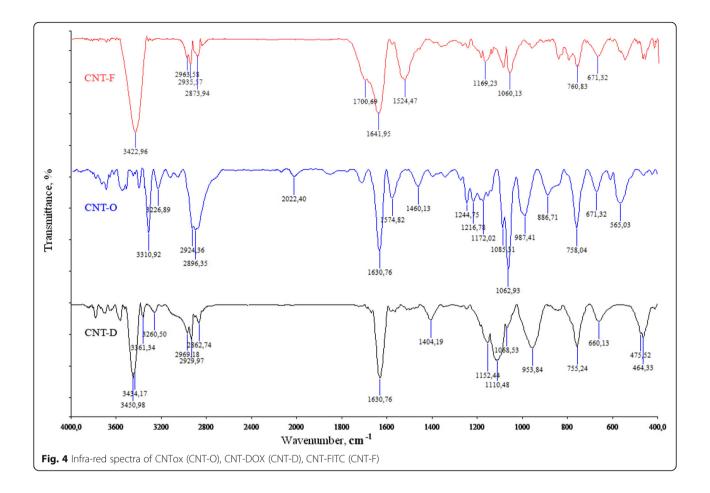
The next step was to determine the cytotoxicity of oxidized CNTs (CNTox), CNTs functionalized with doxorubicin (CNT-Dox), and fluorescent label (CNT-FITC). The results of the MTT test on monolayer culture of HT29 are shown in Fig. 5.

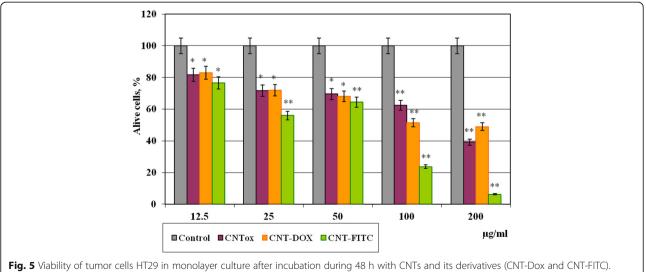
As a result, it was demonstrated that CNTox, CNT-Dox, and CNT-FITC have a moderate cytotoxic effect at concentrations of 12.5 μ g/ml (81%). Increasing CNTox concentration from 25 to 50 and 100 μ g/ml led to dose-dependent decreasing the viability of tumor cells to 71.8–69.6–62.5%

Table 1 Zeta potential of CNT samples at dilution 1:10

-		
Sample	Zeta potential, mV	
CNTox	-27.0 ± 2.42	
CNT	-28.7 ± 1.51	
CNT-DOX	-13.9 ± 0.67	
CNT-FITC	-2.24 ± 1.17	

accordingly compared with control. At concentration of CNTox up to 200 µg/ml, the viability of HT29 decreased to 39.2%. At that time, CNT-Dox at low concentrations (12.5-50 µg/ml) did not show statistically significant cytotoxicity, compared with CNTox. At high concentrations (200 µg/ml), CTN-Dox had even less cytotoxicity than CNTox (50%). At the same time, CNTs, functionalized with fluorescein, had a relatively higher cytotoxic effect on tumor cells. After incubation with CNT-FITC in concentration of 25 μ g/ml, HT29 cell survival reduced to 55% and at 100-200 µg/ml to 23 and 7% respectively. Thus, in that case, CNTs played the role of rather inert cell substrate. More than that, CNTs immobilized Dox and reduced Dox cytotoxicity. In previous studies [33], we have demonstrated that primary nanotubes have hydrophobic qualities, moderate cytotoxic effect, and stimulate the formation of a large number of cellular aggregates. According to the literature [39], surface charge of CNTs changes during the oxidation. CNTs become more hydrophilic, and it leads to the formation of smaller aggregates and increase CNTs cytotoxic effect. The data we receive in previous study confirms this tendency. CNTox reduced survival of tumor cells by at least 60% compared to control, CNT-Dox at 45%, and CNT-FITC at 97% (at 200 µg/ml). Explanation of the obtained data may be in reports of the other authors that functional ligands, in most cases, change the surface zeta potential of CNTs, stimulate solubility of CNTs, and increase cell penetration of CNTs [40]. The ability of CNTs to form aggregates after oxidation and functionalization decreases, while the permeability through the cell membrane increases and the reactivity of cellular organelles increases. More than that, CNT-Dox, at high concentrations, has lower cytotoxic effect than CNTox. At the same time, according to the obtained data, it can be assumed that the peptide bond keeps doxorubicin on the surface of the CNT. Peptide bond between CNTs and Dox is sufficiently stable in cell culture conditions. It does not break down and take doxorubicin in inactive form. At the same time, fluorescein-sodium molecular (C₂₀H₁₂O₅), a ligand of the





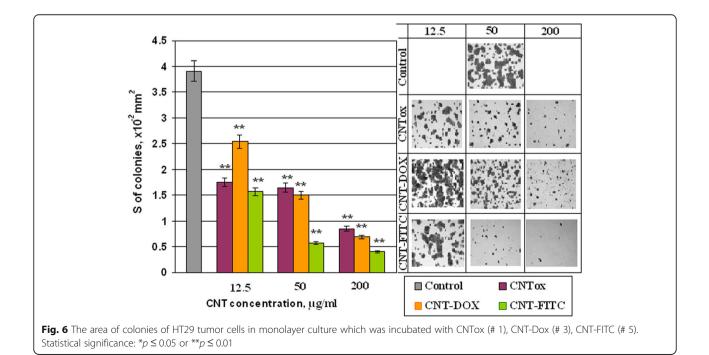
Statistical significance: * $p \le 0.05$ or ** $p \le 0.01$

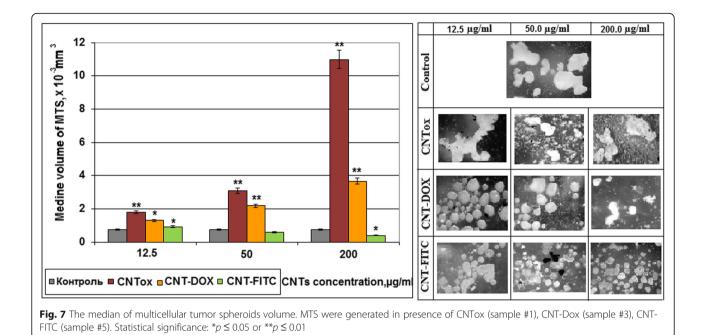
size of 332.311 g/mol, quite easily dissociates from the surface of the CNTs and enters the cells. In results, there are irreversible violations of DNA structures, nuclei, and mitochondria [41].

To verify the cytotoxicity of CNTs and its derivatives and impact on adhesive properties of tumor cells, the area of the HT29 cell 2D colonies was analyzed. The results are shown in Fig. 6. It was demonstrated that CNTs and their derivatives have an influence on adhesive ability of tumor cells and formation of tumor cells colonies in monolayer culture. Incubation of tumor cells with CNTox (sample # 1) at concentrations of 12.5, 50.0, and 200 µg/ml led to dose-dependent decreasing of 2D cell colonies at 55.2%, 57.8%, and 78.3% accordingly, compared with control. At the same time, the sample of CNT-Dox (sample # 3) at the same concentrations did not cause such effect. The area of 2D colonies reduced by 34.8%, 61.6%, and 82.4% respectively. The CNT-FITC (sample #5) demonstrated the largest influence on tumor cells in monolayer culture. The area of 2D colonies after incubation with CNT-FITC decreased at 59.8%, 85.2%, and 89.8%, respectively. It should be noted that the results obtained have the same tendency as MTT-assay. But the results of the MTT analysis did not show such a significant cytotoxic effect. The resulting discrepancies may be the result of non-cytotoxic effects of CNTs on the cell colony, and, partly, anti-adhesive influence. Previously, we have demonstrated that CNTs have less cytotoxic ability then anti-adhesion. According to our data, CNTs stimulate migration of tumor cells into suspension

fraction and formation of multicellular tumor spheroids (MTS). The sensitivity of cells to antitumor agents in monolaver and spheroid cultures is different. That is why on the next step, we investigated the formation of MTS by tumor cells HT29 in the presence of CNTox, CNT-Dox, and CNT-FITC. The concentrations of CNTs were the same as in previous experiments. In Fig. 7, it was demonstrated that CNTox (sample # 1) are able to stimulate the formation of MTS. Increasing of CNTox concentration is accompanied with dose-dependent increasing of median volume of MTS. At concentration CNTox from 12.5, 50, 200 µg/ml, median volume of MTS increases from 1.79 to 2.18 and 10.98 mm³; it is almost ten times. Derivatives of CNTs do not cause such effect on tumor cells. CNT-Dox (sample # 3) stimulates formation of MTS in 2.83 times. At the same time, incubation of 3D tumor cell culture with CNT-FITC (sample # 5) leads to a 2.4-fold decrease of MTS volume.

It is noteworthy that in most experiments, CNT-Dox has not such cytotoxic effects on tumor cells, both in 2D and in 3D culture, which could be compared with the effect of a single doxorubicin. The mechanism of cytotoxic action of doxorubicin is based on penetration into the cell nucleus and intercalation between nucleotide pairs, violation of replication and DNA repair, protein synthesis and, as a result, cell death. The cause of the reduction of cytotoxic effect of the CNT-Dox may be the binding of the doxorubicin with CNT surface through peptide bonds. It prevents Dox dissociation from CNT surface and Dox penetration into the cell and cellular



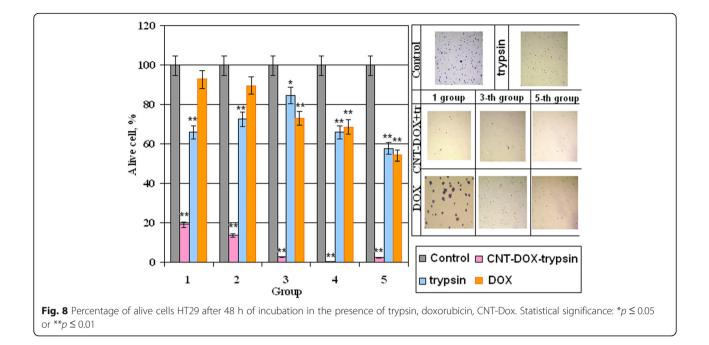


organelles. This fact may let to deliver the compound to certain tissues without causing a negative effect on "non-target" objects.

In this case, the next step of the study was controlled release of doxorubicin. For peptide bonds breaking, we used the commonly known peptidase trypsin as the release agent. The effect of trypsin on the Dox release from the surface of the CNT was investigated by spectral analysis. Since the free doxorubicin has a fluorescence peak at 495 nm, bounded doxorubicin has no such ability. It was analyzed how the increasing of trypsin concentration affected on concentration of free doxorubicin. The results are shown in our previous work [42]. Shortly, it was demonstrated that increasing the concentration of 0.05% trypsin from 11 to 20% in culture medium contributed to an increasing the concentration of free doxorubicin from 3.13 to 6.55 μ g/ml. A further increasing the concentration of trypsin to 60% did not lead to increasing in free doxorubicin. However, the concentration of trypsin by about 66% stimulated release again and led to increasing the concentration of doxorubicin in two times, to 11.38 μ g/ ml. Thus, it was concluded that 0.05% trypsin has several effective concentrations. Under these conditions, peptide bonds between doxorubicin and CNT were broken and doxorubicin was released. Therefore, to analyze how CNT-Dox influence the tumor cells after Dox release, we incubated tumor cells in the w/o fetal bovine serum (FBS) nutrient medium with trypsin and in the presence of CNT-Dox. The survival of tumor cells was determined using the MTT test. The ratio of the nutrient medium, trypsin, concentration of CNT-Dox, and doxorubicin are given in Table 2. The results of incubation HT29 during 48 h are demonstrated on Fig. 8. Cell viability in the presence of trypsin—blue columns, alone doxorubicin—orange columns, and CNT-Dox with trypsin-pink columns. In results, it has been found that the simultaneous use of trypsin and CNT-Dox significantly increased the cytotoxic effect of CNT and doxorubicin compared to the separately use of these substances. So doxorubicin alone at concentrations from 0.05 to 1.0 µg/ml causes a dose-dependent decreasing the percentage of living HT29 cells from 7.18 to 45.7% relative to control (Fig. 8, orange columns). Incubation of CNT-Dox at concentrations of 20.0 to 1.25 µg/ml with trypsin at concentration from 0 t0 70% led to a dose-dependent decreasing in the percentage of living cells from 80.9 and 99.8% respectively (Fig. 8, pink columns). At the

Table 2 Concentrations of trypsin, Doxorubicin, CNT-DOX, and nutrient medium for MTT-assay, after incubation during 48 h

Groups	DMEM w/o FBS, µl	Trypsin in DMEM w/o FBS, μl	CNT-Dox, µg/ml	Doxorubicin, µg/ml
1	100	0	20	0.05
2	50	50	10	0.125
3	45	55	5	0.25
4	38	62	2,5	0.5
5	30	70	1,25	1.0



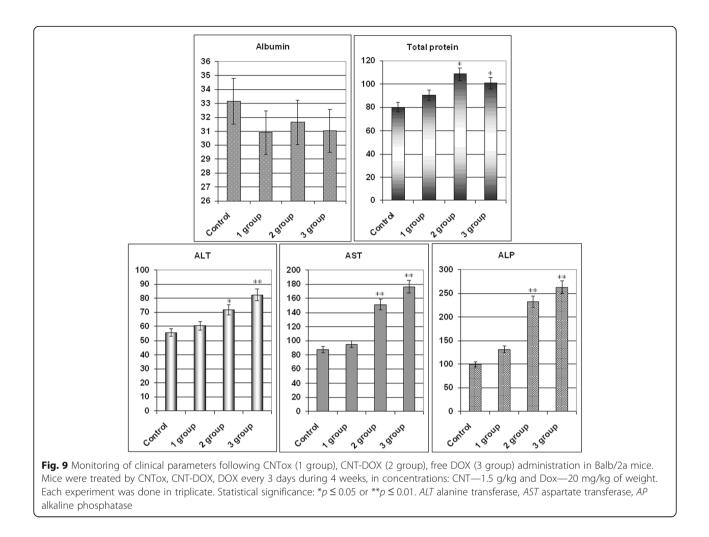
same time, incubation with trypsin alone leads to decreasing percentage of living cells only by 34.0–42.0% (Fig. 8, blue columns). Thus, we can conclude that we observe the synergistic effect of CNT-DOX and trypsin. Each individual component has a small cytotoxic effect on cells, and together the cytotoxic potential of substances increases several times.

As functional groups (Dox) were attached to CNTs surface by peptide bonds as, in vivo Dox release will be realized in organs of the gastrointestinal tract with an increased content of proteases, peptidases. In organism, proteases are used for various metabolic processes. Acid proteases secreted into the stomach (such as pepsin) and serine proteases present in duodenum (trypsin and chymotrypsin) enable us to digest the protein in food [43]. Other proteases are present in leukocytes (elastase, cathepsin G) and play several different roles in metabolic control. This is one of the fastest "switching on" and "switching off" regulatory mechanisms in the physiology of an organism. By complex cooperative action, the proteases may proceed as cascade reactions, which result in rapid and efficient amplification of an organism's response to a physiological signal. Therefore, the authors suggest that CNT-Dox construction will be the most effective in the case of stomach, pancreas, liver, and small intestine cancer localization in case of parenteral administration of drug.

Influence of CNTs and Their Derivatives on Cell Blood Composition, Hepatic Enzyme System, and Proteins Turnover In Vivo

To determine the impact of the CNTox and CNT-Dox on the protein metabolism and the state of the hepatic

enzyme system, the level of albumin (Al), total protein (Tp), alanine aminotransferase (ALT), aspartate aminotransferase (AST), and alkaline phosphatase (ALP) was determined. Data are given in Fig. 9a, b. As a result, it was noted that CNT-Dox and Dox have influence on the hepatic enzymes activity, namely on the AST and ALP. AST level increased in mice serum from 1 group for 21.6%, 2 group for 93.9%, and 3 group for 126.4% compared with control. At the same time, the activity of ALP increased in mice serum from 1 group for 23.5%, 2 group for 119.1%, and 3 group for 147.8%. CNTox administration did not show statistically significant changes in AST, ALT, and ALP levels. In addition, it should be noted that CNTox, Doxorubicin, and CNT-Dox slightly increased the level of total protein in the blood of experimental animals. So, we found that systematic introduction of CNTox have not influence on mice serum enzyme profile. And opposite, administration of CNT-Dox and Dox had toxicity influence and induced a chronic hepatic damage. Notably, symptoms of hepatitis had more manifestation after Dox treatment than CNT-Dox. To determine possible inflammatory processes and systemic effects of CNTox, CNT-Dox on the state of blood cells composition, it was analyzed the blood cell formula of the experimental animals. The results are shown in Table 3. Obtained data are in good agreement with the well-known manifestations of doxorubicin's hematological toxicity: anemia (decreased red blood cells, hemoglobin, hematocrit), thrombopenia (platelet count), neutropenia (decrease in the number of granulocytes). Interestingly, that it was demonstrated the same direction of the changes of practically all hematological parameters in the 1 (CNTox), 2 (CNT-Dox), and 3 (Dox)



groups of animals. However, the change in the 2 and 3 groups of animals was statistically significant accordingly to control and 1 group. In the 2 group (CNT-Dox), it was found pronounced decreasing of the monocyte content related to the system of phagocyte mononuclear cells and cell's immune response (9.5% and 0.12×10^9 /l in control, 4.6% and 0.06×10^{9} /l in 2 group, and 4.55 and 0.05×10^{9} /l in 3 group). Animals of 2 and 3 groups demonstrated reducing the content of granulocytes (neutrophils) (12.6 and 0.16×10^9 /l in control and 8.5% and 0.2×10^9 /l in 2 group and 8.05 and 0.16×10^{9} /l in 3 group). The number of lymphocytes, both in percentage and absolute, increased in 2 and 3 groups (77.9% and 0.97×10^9 /l in control and 86.9% and 2.0×10^{9} /l in 2 group and 87.8% and 2.3×10^{9} /l in 3 group). The main function of the lymphocytes is recognition of the antigen and participation in the adequate immunological response of the body. T lymphocytes perform regulatory and effectors functions. B lymphocytes take part in humoral immunity, providing immunoglobulins in response to stimulation of other people's antigens. So, it can be assumed that an increase in the index of lymphocyte content in experimental 1, 2, and 3 groups can be associated with the introduction of foreign antibodies (CNTs) and/or tissue distraction [44]. Some decrease in the absolute number of leukocytes in 2 $(1.2 \times 10^9/l)$ and 3 $(0.85 \times 10^9/l)$ 10^{9} /l) groups compared with the 1 group of animals $(2.0 \times 10^{9}/l)$ can be regarded as the result of a gradual accumulation of the reversal of toxic effects of Dox. It is described the reaction of WBC in experimental animal groups as well-known toxic hematologic impact from doxorubicin in the development of leucopenia. The analysis of indicators reflecting the number and state of RBC (erythrocytes and hemoglobin) also showed the same trend of misbalance in the 2 and 3 groups of animals. Statistically significant thrombocytopenia and anemia are more indicative in animals of 2 and 3 groups: the number of erythrocytes $(5.54 \times 10^{12}/l \text{ in control}, 3.97 \times 10^{12}/l \text{ in 2 group, and})$ 3.12×10^{12} /l in 3 group), the amount of hemoglobin (78 g/dl for intact animals, 55.5 g/dl for 2 group, and 46.2 g/dl for 3 group), hemoglobin (25.25% for intact animals and 16.75% for 2 group and 15.12% for 3 group). The amount of erythrocytes decreased but the average

	Control	CNTox	CNT-Dox	Dox
Leukocytes, 10 ⁹ /I	1.25	2.0	1.2	0.85
Lymphocytes, 10 ⁹ /l	0.97	1.75	2.0	2.3
Lymphocytes, %	77.9	86.7	86.9	87.8
Monocytes, 10 ⁹ /l	0.12	0.09	0.06	0.05
Monocytes, %	9.5	7.15	4.6	4.5
Granulocytes, 10 ⁹ /l	0.15	0.20	0.20	0.16
Granulocytes, %	12.6	9.15	8.5	8.0
Hemoglobin, g/dl	78.0	72.5	55.5	46.2
Erythrocytes, 10 ¹² /l	5.54	4.96	3.97	3.12
Hematocrit, %	25.25	21.25	16.75	15.12
Av. vol. erythrocyte	45.5	42.9	42.65	42.15
Av. hemoglobin per erythrocyte, lg	14.05	14.55	14.2	13.01
Av. concentration of hemoglobin per erythrocytes, g/dl	309.5	340.5	335.5	336.2
Thrombocytes, 109/l	27.0	25.5	14.0	12.05

Table 3 Composition of the formed blood elements in the experimental animals after 4 weeks of administration of CNTox and CNT-Dox

content of hemoglobin in one erythrocyte did not decrease. And, as a result, concentration of hemoglobin per one erythrocyte increased. Analysis of the RBW counts let us suggest that in 2 and 3 group of animals, there are several processes: decreasing the formation of erythrocytes in the bone marrow, the acceleration of erythrocyte destruction, the violation of the structure of membranes of red blood cells, and molecular defects (oxidation) of hemoglobin. Thrombocytopenia $(27 \times 10^9/l \text{ in intact animals, } 14.0 \times 10^9/l \text{ in intact animals, } 10^9/l \text{ in in$ $10^{9}/l$ in 2 group, and $12.05 \times 10^{9}/l$ in 3 group), a dose-dependent reversible myelosuppression, leucopenia and granulocytopenia (neutropenia) are the predominant manifestations of doxorubicin hematologic toxicity and is the most common acute dose-limiting toxicity of this drug. The direction of changes in the platelet content in the blood of experimental animals treated with CNTox and CNT-Dox is the same; however, significantly more pronounced in the group of animals receiving free Dox.

Thus, according to our results from in vivo experiments, it was demonstrated that systematic introduction of CNTox have not influence on mice serum enzyme profile and protein turnover. And opposite, administration of CNT-Dox and Dox had toxicity influence and induced a chronic hepatic damage. More than that, dose-dependent reversible myelosuppression, leucopenia, and granulocytopenia (neutropenia) was shown for the group of animals receiving free Dox. This predominant manifestation of hematologic toxicity was less pronounced in the group of animals receiving free CNT-Dox and CNTs. So, we can assume that, in the case of parenteral administration of CNT-Dox under action of gastric juice peptidases, CNT-Dox particles breaks up into free CNT and Doxorubicin. After that, Doxorubicin enters to the stomach cells and partly in the bloodstream. That also causes the specified effect on blood cells composition. For modeling Dox release in vivo, trypsin were used in vitro.

One of the goals of this investigation was to minimize the side effects of carbon vehicle on the body. Previously, the authors demonstrated that CNTs may be a potential threat to tumor development due to its ability to stimulate cell migration and support cells in suspension fraction [33]. In this case, CNTs themselves play a role of artificial extra cellular matrix. Another way CNTs can stimulate suspension cells to aggregation. If this process will be coincident with antitumor drug accumulation on CNTs surface, CNTs will attract substrate-independent cells and kill them. Simultaneously, it was found that pure CNTs did not have statistically significant cytotoxicity to tumor cells. So, CNTs alone are not dangerous as cytotoxic agents and can act as carrier for antitumor drugs to target cells. Then, studies were conducted to the functionalization of the CNTs by antitumor antibodies. It was demonstrated that CNTs are able to carry on the surface not only the Dox but also specific tumor antibodies-anti EGFr [42]. Under the action of trypsin, Dox was released and realized strong cytotoxic effect on tumor cells. Recent studies have shown the synergy cytotoxic effect of CNTs and Doxorubicin after release from CNT-Dox construct in the presence of trypsin. Such effect was not demonstrated by CNTs and Dox separately. Therefore, the benefits from the use of CNTs seems in the usage CNTs as vehicle for antitumor antibody and drug. On the other hand, the negative effects of Doxorubicin, like many other early antitumor drugs,

are totally cytotoxic effects. Binding of the Dox to the CNTs partially blocks it. This effect allows ensuring local accumulation of the Dox in the focus of tumor activity with subsequent release and action. Thus, greater efficacy can be achieved with a smaller dose of administration. This effect can be achieved only if there are tumor-specific antibodies on the surface of the CNTs. The possibility of creating such construct was demonstrated by the authors in previous work. Undoubtedly, that CNTs dissemination, accumulation, and Dox effective should be tested on mixed culture in vitro and on a tumor model in vivo. For this purpose, synthesized CNT-FITC was created and conducted. The ability of the CNTs to act as an extra-cellular matrix and the significance of this process for the "tumor-body" system should be tested on the animal model. The effectiveness of the drug will be investigated on the model of Ehrlich carcinoma and colon rectal carcinoma [44]. The distribution of CNTs in the tissues of the body will be investigated using the construct created by the CST-FITC, as was mentioned in this work. The accumulation of CNTs in the tissues of the organs of the gastrointestinal system, namely the stomach, liver, and intestines, will be analyzed by histological assay. These studies are already conducted by the authors.

According to Shang-Lin Wang [4] and our data, free doxorubicin causes similar side effects, but more pronounced than CNT-Dox. Other authors reported that toxicity effect of CNTs depends on way of administration, dose, and time of exposure and varies according to the size and type of the cells [45-49]. Settling of CNTs in the tissues of the liver, kidneys, and stomach with prolonged exposure can cause oxidative stress, DNA damages, compromise cell proliferation, necrosis of tissues, and chronic inflammation [50]. According to Manna [51], CNTs can cause oxidative stress and compromise cell proliferation. In the case of in vitro studies, the cytotoxicity of CNT highly depends on the degree of CNTs purification, functionalization, size, and surface charge [52-55]. According to our results and previous data, the obtained CNTs did not demonstrate a significant cytotoxic effect [33]. More than that, our data let us suggest that there is a combined cytotoxic effect of CNTs and DOX that occurs as in vitro. That is why we assumed that obtained CNTs can be used against tumor cells, in case of the target accumulation of CNTs/CNT-Dox in tumor tissue. However, mechanisms of the cytotoxic effect of CNTs are not completely clear. Some authors suggested that CNT particles activate NF-kappaB pathway depending on the dose and that the mechanism of activation was due to activation of stress-related kinases [51]. Other authors reported that CNTs have a direct pro-apoptotic effect in vitro in different cancer cell lines and tumor cells obtained from surgical specimens [56], CNTs able to modify fatty acids in cell membranes [57] or erythrocyte membrane damage [58]. For further investigation of accumulation CNTs in cells and tissue, we plan to use CNT-FITC composite.

Other unclear questions are as follows: what is the prolonged impact of CNTs/CNT-Dox on organism level and how does it stimulate accumulation CNTs/CNT-Dox in tumor tissue? To investigate the influence of chronical introduction of CNTs/CNT-Dox, long-time studies on model of transplanted or initiated tumors of various localizations will be realized. Other authors analyzed the distribution of nanotubes throughout the body of mice after pulmonary exposure [59]. In results, accumulation of MWCNTs was documented in several organs, including notably the white pulp of the spleen and the bone marrow. The CNTs usually deposit in the liver, spleen, or lungs after they have served their purpose from where they are expelled gradually out of the body through the renal excretion route [60]. Zhao and Liu reported that accumulation of CNTs in the body can lead to granulomatous inflammation or alveolar septal thickening. Zhuang Liu et al. reported that SWNT-PTX affords higher efficacy in suppressing tumor growth than clinical Taxol[®] in a murine 4T1 breast-cancer model, owing to prolonged blood circulation and tenfold higher tumor paclitaxel (PTX) uptake by SWNT delivery likely through enhanced permeability and retention [61]. Accumulation of CNTs in the target tissue can be enhanced by placing on the CNTs surface specific antibodies which over expressed by tumor cells. The possibility of using antibodies for the targeted delivery of nanostructured preparations has been described by many authors [62, 63].

Conclusion

In 2D culture CNTox concentration from 25 to 50 and 100 µg/ml led to dose-dependent decreasing the viability of tumor cells to 71.8-69.6-62.5% accordingly compared with control. At concentration of CNTox up to 200 µg/ ml, the viability of HT29 decreased to 39.2%. At that time, CNT-Dox at concentrations 12.5-25-50 µg/ml did not show statistically significant cytotoxicity, compared with CNTox. At high concentrations (200 µg/ml), CTN-Dox had even less cytotoxicity than CNTox (50%). After incubation with CNT-FITC in concentration of 25 μ g/ml, HT29 cell survival reduced to 55% and at 100-200 µg/ml to 23 and 7% respectively. In 3D culture, increasing of CNTox concentration is accompanied with dose-dependent increasing of median volume of MTS. At concentration CNTox from 12.5, 50, 200 µg/ml median volume of MTS increases from 1.79 to 2.18 and 10.98 mm³. CNTs-Dox and CNT-FITC did not cause such effect on tumor cells. Doxorubicin alone at concentrations from 0.05 to 1.0 μ g/ml causes a dose-dependent decrease in the percentage of living HT29 cells from

7.18 to 45.7% relative to control. Incubation CNT-Dox at concentrations of 20.0 to 1.25 µg/ml with trypsin at concentration from 0 to 70% led to a dose-dependent decreasing the percentage of living cells from 80.9 and 99.8% respectively. At the same time, incubation with trypsin alone leads to decreasing percentage of living cells only by 34.0-42.0%. So, the synergistic effect of CNT-DOX and trypsin was observed. Each individual component has a small cytotoxic effect on cells, and together the cytotoxic potential of substances increases several times. In vivo, systematic introduction of CNTox have not influence on mice serum enzyme profile. And opposite, administration of CNT-Dox and Dox had toxicity influence and induced a chronic hepatic damage, thrombocytopenia, a dose-dependent reversible myelosuppression, leucopenia, and granulocytopenia (neutropenia). Notably, symptoms of hepatitis had more manifestation after Dox treatment than CNT-Dox.

So, the possibility of targeted delivery and controlled release of any highly toxic drug with the use of CNT depends on strategies of reducing toxicity of CNTs and realizing potential of CNTs and anti-tumor drugs "in right place in right time." According to the data obtained by authors and literature, it is possible. Our data support the assumption that this approach allows to reduce toxicity of the doxorubicin on the general biochemical indicators of blood and violations in the blood cells composition. At the same time, doxorubicin releasing is realized under certain conditions. And combined effect of CNTs and doxorubicin let us achieve greater efficacy in suppressing tumor cell growth in vitro.

Abbreviations

Al: Albumin; ALP: Alkaline phosphatase; ALT: Alanine aminotransferase; AST: Aspartate aminotransferase; CNT-Dox: Carbon nanotubes which were functionalized by doxorubicin; CNT-FITC: Carbon nanotubes which were functionalized by fluorescein; CNTox: Oxidized carbon nanotubes; CNTs: Carbon nanotubes; Dox: Doxorubicin; FTIR: Fourier-transform infrared spectroscopy; MTS: Multi-cellular tumor spheroid; MWCNTs: Multi-walled carbon nanotubes; PTX: Paclitaxel; Tp: Total protein

Acknowledgements

We are deeply grateful to Dr. Kudriyvec, who kindly provided us with standardized tumor cell line HT29 and their characterization.

Funding

This study was supported by "Integrated multidisciplinary scientific research program of the National Academy of Sciences of Ukraine Molecular and cellular biotechnologies for the needs of medicine, industry and agriculture", Grant No. 18/17-B.

Availability of Data and Materials

The authors declare that materials, data, and associated protocols are promptly available to readers without undue qualifications in material transfer agreements. All data generated or analyzed during this study are included in this article.

Authors' Contributions

OMP and MVS contributed to study design. OMP performed the experiments, analyzed the data, and wrote the manuscript, the cytotoxicity and biochemical analysis. ONB provided synthesis of MWCNTs, CNT-Dox, and CNT-FITC. AU took part in experiments, data analyzing, and wrote the manuscript. AVD ensured

FTIR assay. OMP provided 3D culture experiments and hematological data analyzes. AIM realized zeta potential assay and interpretation. All authors read and approved the final manuscript.

Competing Interests

The authors declare that they have no competing interests.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.

Author details

¹Department for Biotechnical Problems of Diagnostic IPCC, Nauky str.,42/1, Kiev 03028, Ukraine. ²Chemistry Department, Taras Shevchenko National University of Kiev, Lva Tolstoho str. 12, Kiev 01033, Ukraine. ³Chuiko Institute of Surface Chemistry NAS of Ukraine, 17 General Naumov str., Kiev 03164, Ukraine. ⁴National University of Food Technologies, 68, Volodymyrska str., Kiev 01601, Ukraine.

Received: 19 January 2018 Accepted: 27 August 2018 Published online: 12 September 2018

References

- Rodriguez RD, Toader M, Hermann S, Sheremet E, Müller S, Gordan OD, Yu H, Schulz SE, Hietschold M, Zahn DRT (2012) Nanoscale optical and electrical characterization of horizontally aligned single-walled carbon nanotubes. Nanoscale Res Lett 7:682
- Liu Y, Liang X, Wang S, Hu K (2016) Electrospun poly(lactic-co-glycolic acid)/ multiwalled carbon nanotube nanofibers for cardiac tissue engineering. J Biomater Tissue Eng 6:719–728
- Venkatesan J, Pallela R, Kim SJ (2014) Dispersion of single walled carbon nanotubes in marine polysaccharides for bone tissue engineering. J Biomater Tissue Eng 4:501–505
- Xue Y, Holt S, Elsevier BV (2017) Chapter 11—carbon nanotubes for biomedical applications. In: Industrial Applications of Carbon Nanotubes, Micro and Nano Technologies, pp 323–346
- Khan AJ, Khan RA, Singh VM, Newati SJ, Yusuf M (2013) In silico designed, self-assembled, functionalized single-walled carbon nanotubes and, deoxyribose nucleic acids (f-SW-CNT-DNA) bioconjugate as probable... J Bionanosci 7(5):530–550
- Saifuddin N, Raziah AZ, Junizah AR (2013) Carbon nanotubes: a review on structure and their interaction with proteins. J Chem 2013:1–18
- Costa PM, Bourgognon M, Wang JT, Al-Jamal KT (2016) Functionalised carbon nanotubes: from intracellular uptake and cell-related toxicity to systemic brain delivery. J Control Release 241:200–219
- Lacerda L, Russier J, Pastorin G, Herrero MA, Venturelli E, Dumortier H, Al-Jamal KT, Prato M, Kostarelos K, Bianco A (2012) Translocation mechanisms of chemically functionalised carbon nanotubes across plasma membranes. Biomaterials 33(11):3334–3343 Shows how different functionalization schemes on CNT can affect their uptake by mammalian cells
- Karimi M, Solati N, Ghasemi A, Estiar MA, Hashemkhani M, Kiani P, Mohamed E, Saeidi A, Taheri M, Avci P, Aref AR, Amiri M, Baniasadi F, Hamblin MR (2015) Carbon nanotubes part II: a remarkable carrier for drug and gene delivery. Expert Opin Drug Deliv 12(7):1089–1105
- Hilder TA, Hill JM (2009) Modeling the loading and unloading of drugs into nanotubes. Small 5:300–308
- 11. Ramos-Perez V, Cifuentes A, Coronas N, de Pablo A, Borros S (2013) Modification of carbon nanotubes for gene delivery vectors. Methods Mol Biol 1025:261–268
- 12. Basu B, Mehta GK (2014) Carbon nanotubes: a promising tool in drug delivery. Int J Pharm Bio Sci 5:533–555
- Zhang W, Zhang Z, Zhang Y (2011) The application of carbon nanotubes in target drug delivery systems for cancer therapies. Nanoscale Res Lett 6:555
- Ugnivenko AP, Perepelitsina OM, Sydorenko MV, Ostapchenko LI (2017) Carbon nanotubes in delivery of bioactive substances. J Bionanosci 11(6): 531–547
- Sur A, Pradhan B, Banerjee A, Aich P (2015) Immune activation efficacy of indolicidin is enhanced upon conjugation with carbon nanotubes and gold nanoparticles. PLoS One 10(4):e0123905
- 16. Allen TM, Cullis PR (2013) Liposomal drug delivery systems: from concept to clinical applications. Adv Drug Deliv Rev 65:36–48

- Miyata K, Christie RJ, Kataoka K (2011) Polymeric micelles for nano-scale drug delivery. React Funct Polym 71:227–234
- Mahapatro A, Singh DK (2011) Biodegradable nanoparticles are excellent vehicle for site directed in-vivo delivery of drugs and vaccines. J Nanobiotechnol 9:55
- 19. Sagnella S, Drummond C (2012) Drug delivery a nanomedicine approach. Aust Biochem 43:5–7
- Elhissi AMA, Ahmed W, Hassan IU, Dhanak VR, D'Emanuele A (2012) Carbon nanotubes in Cancer therapy and drug delivery. J Drug Deliv 2012:837327
- 21. Zhang Y, Bai Y, Yan B (2010) Functionalized carbon nanotubes for potential medicinal applications. Drug Discov Today 15(11–12):428–435
- Pastorin G (2009) Crucial functionalizations of carbon nanotubes for an improved drug delivery: a valuable option? Expert opinion. Pharm Res 26: 746–769
- Principi E, Girardello R, Bruno A, Manni I, Gini E, Pagani A, Grimaldi A, Ivaldi F, Congiu T, De Stefano D, Piaggio G, de Eguileor M, Noonan DM, Albini A (2016) Systemic distribution of single-walled carbon nanotubes in a novel model: alteration of biochemical parameters, metabolic functions, liver accumulation, and inflammation in vivo. J Nanomed 11:4299–4316
- Maes HM, Stibany F, Giefers S, Daniels B, Deutschmann B, Baumgartner W, Schäffer A (2014) Accumulation and distribution of multiwalled carbon nanotubes in zebrafish (Danio rerio). Environ Sci Technol 48(20): 12256–12264
- Jacobsen NR, Møller P, Clausen PA Saber AT, Micheletti C, Jensen KA, Wallin H, Vogel UB (2017) Biodistribution of carbon nanotubes in animal models. Basic Clin Pharmacol Toxicol 121:30–43
- Dong J, Ma Q (2015) Advances in mechanisms and signaling pathways of carbon nanotube toxicity. Nanotoxicology 9(5):658–676
- Thurnherr T, Brandenberger C, Fischer K, Diener L, Manser P, Maeder-Althaus X, Kaiser JP, Krug HF, Rothen-Rutishauser B, Wick P (2011) A comparison of acute and long-term effects of industrial multiwalled carbon nanotubes on human lung and immune cells in vitro. Toxicol Lett 200(3):176–186
- Yang S-T, Luo J, Zhou Q, Wang H (2012) Pharmacokinetics, metabolism and toxicity of carbon nanotubes for biomedical purposes. Theranostics 2(3): 271–282
- Bhirde AA, Patel V, Gavard J, Zhang G, Sousa AA, Masedunskas A, Leapman RD, Weigert R, Gutkind JS, Rusling JF (2009) Targeted killing of cancer cells in vivo and in vitro with EGF-directed carbon nanotube-based drug delivery. ACS Nano 3:307–316
- Zhao D, Alizadeh D, Zhang L, Liu W, Farrukh O, Manuel E, Diamond DJ, Badie B (2011) Carbon nanotubes enhance CpG uptake and potentiate anti-glioma immunity. Clin Cancer Res 17(4):771–782
- Hadidi N, Kobarfard F, Nafissi-Varcheh N, Aboofazeli R (2011) Optimization of single-walled carbon nanotube solubility by noncovalent PEGylation using experimental design methods. Int J Nanomedicine 6:737–746
- Podesta JE, Al-Jamal KT, Herrero MA, Tian B, Ali-Boucetta H, Hegde V, Bianco A, Prato M, Kostarelos K (2009) Antitumor activity and prolonged survival by carbon-nanotube-mediated therapeutic siRNA silencing in a human lung xenograft model. Small 5(10):1176–1185
- Yakymchuk OM, Perepelytsina OM, Rud AD, Kirian IM, Sydorenko MV (2014) Impact of carbon nanomaterials on the formation of multicellular spheroids by tumor cells. Phys Status Solidi A 211(12):2778–2784
- Silverstein RM, Webster FX, Kiemle DJ, Bryce DL (2015) Spectrometric identification of organic compounds, 8th edn. Wiley and Sons, New York, p 455
- Dai X, Yue Z, Eccleston ME, Swartling J, Slater NK, Kaminski CF (2008) Fluorescence and lifetime imaging of free and micellarencapsulated doxorubicin in living cells. Nanomedicine 4(1):49–56
- Mosmann T (1983) Rapid colorimetric assay for cellular growth and survival: application to proliferation and cytotoxic assayas. J Immunol Methods 65: 55–63
- Bjerkvig R (1992) Spheroid culture in cancer research. Boca Raton, FL: CRC Press, p 335
- Yanchenko V, Sementsov Yu, Melezhyk A (2004) Method of obtaining of catalysts for CVD of carbon nanotubes. Ukrainian Pat. Application 20041008154, Int. Cl.7 C01B11/00, D01F9/12
- Eatemadi A, Daraee H, Karimkhanloo H, Kouhi M, Zarghami N, Akbarzadeh A, Abasi M, Hanifehpour Y, Joo SW (2014) Carbon

nanotubes: properties, synthesis, purification, and medical applications. Nanoscale Res Lett 9:393

- Rotoli BM, Bussolati O, Bianchi MG, Barilli A, Balasubramanian C, Bellucci S, Bergamaschi E (2008) Non-functionalized multi-walled carbon nanotubes alter the paracellular permeability of human airway epithelial cells. Toxicol Lett 178(2):95–102
- Shityakov S, Salvador E, Pastorin G, Förster C (2015) Blood–brain barrier transport studies, aggregation, and molecular dynamics simulation of multiwalled carbon nanotube functionalized with fluorescein isothiocyanate. J Nanomed 10:1703–1713
- Perepelytsina OM, Yakymchuk OM, Sydorenko MV, Bakalinska ON (2016) Functionalization of carbon nanomaterials surface by doxorubicin and antibodies to tumor markers. Nanoscale Res Lett 11(1):314
- Oda K (2012) New families of carboxyl peptidases: serine-carboxyl peptidases and glutamic peptidases. J Biochem 151(1):13–25. https://doi.org/10.1093/jb/ mvr129 PMID 22016395
- 44. Eferl R, Casanova E (eds) (2015) Mouse models of cancer. Methods and protocols. Humana Press. https://doi.org/10.1007/978-1-4939-2297-0
- 45. Yu Y, Zhang Q, Mu Q, Zhang B, Yan B (2008) Exploring the immunotoxicity of carbon nanotubes. Nanoscale Res Lett 3:271
- Wang S-L, Lee J-J, Taiching AL (2016) Comparison of efficacy and toxicity of doxorubicin and mitoxantrone in combination chemotherapy for canine lymphoma. Can Vet J 57(3):271–276
- 47. Erdely A, Dahm M, Chen BT, Zeidler-Erdely PC, Fernback JE, Birch ME, Evans DE, Kashon ML, Deddens JA, Hulderman T, Bilgesu SA, Battelli L, Schwegler-Berry D, Leonard HD, McKinney W, Frazer DG, Antonini JM, Porter DW, Castranova V, Schubauer-Berigan MK (2013) Carbon nanotube dosimetry: from workplace exposure assessment to inhalation toxicology. Part Fibre Toxicol 10(1):53
- Lindberg HK, Falck GC, Singh R, Suhonen S, Järventaus H, Vanhala E, Catalán J, Farmer PB, Savolainen KM, Norppa H (2013) Genotoxicity of short singlewall and multi-wall carbon nanotubes in human bronchial epithelial and mesothelial cells in vitro. Toxicology 313(1):24–37
- Fu G, Zhu L, Yang K, Zhuang R, Xie J, Zhang F (2016) Diffusion-weighted magnetic resonance imaging for therapy response monitoring and early treatment prediction of photothermal therapy. ACS Appl Mater Interfaces 8: 5137–5147
- Kobayashi N, Izumi H, Morimoto Y (2017) Review of toxicity studies of carbon nanotubes. J Occup Health 59(5):394–407
- Manna S, Sarkar S, Barr J, Wise K, Barrera E, Jejelowo O, Ramesh G (2005) Singlewalled carbon nanotubes induces oxidative stress and activates nuclear transcription factor-xB in human keratinocytes. Nano Lett 5:1676–1684
- Haniu H, Saito N, Matsuda Y, Tsukahara T, Takanashi S, Maruyama K, Kato H (2014) Biological responses according to the shape and size of carbon nanotubes in BEAS-2B and MESO-1 cells. Int J Nanomedicine 17:1979–1990
- Hu X, Cook S, Wang P, Hwang HM, Liu X, Williams QL (2010) In vitro evaluation of cytotoxicity of engineered carbon nanotubes in selected human cell lines. Sci Total Environ 408:1812–1817
- 54. Schinwald A, Donaldson K (2012) Use of back-scatter electron signals to visualise cell/nanowires interactions in vitro and in vivo; frustrated phagocytosis of long fibres in macrophages and compartmentalisation in mesothelial cells in vivo. Part Fibre Toxicol 9(1):1
- Manke A, Luanpitpong S, Dong C, Wang L (2014) Effect of fiber length on carbon nanotube-induced fibrogenesis. Int J Mol Sci 15:7444–7461
- Garcia-Hevia L, Valiente R, Gonzalez J, Fernandez-Luna JL, Villegas JC, Fanarraga ML (2015) Anti-cancer cytotoxic effects of multiwalled carbon nanotubes. Curr Pharm Des 21(15):1920–1929
- Yang F, Jiang Q, Xie W, Zhang Y (2017) Effects of multi-walled carbon nanotubes with various diameters on bacterial cellular membranes: cytotoxicity and adaptive mechanisms. Chemosphere 185:162–170
- Kartel MT, Chernykh VP, Ivanov LV, Gordienko EA, Kovalenko SN, Gubin YI, Nardid OA, Smolyaninova EI (2011) Mechanisms of the cytotoxicity of carbon nanotubes. Chem Phys Technol Surf 2(2):182–189
- Czarny B, Georgin D, Berthon F, Plastow G, Pinault M, Patriarche G, Thuleau A, L'Hermite MM, Taran F, Dive V (2014) Carbon nanotube translocation to distant organs after pulmonary exposure: insights from in situ 14Cradiolabeling and tissue Radioimaging. ACS Nano 8(6):5715–5724
- Zhao X, Liu R (2012) Recent progress and perspectives on the toxicity of carbon nanotubes at organism, organ, cell, and biomacromolecule levels. Environ Int 40:244–255

- Liu Z, Chen K, Davis C, Sherlock S, Cao Q, Chen X, Dai H (2008) Drug delivery with carbon nanotubes for in vivo cancer treatment. Cancer Res 68(16):6652–6660
- 62. Beech R, Shin SJ, Smith JA, Kelly KA (2013) Mechanisms for targeted delivery of nanoparticles in cancer. Curr Pharm Des 19(37):6560–6574
- 63. Bi Y, Hao F, Yan G, Teng L, Lee RJ, Xie J (2016) Actively targeted nanoparticles for drug delivery to tumor. Curr Drug Metab 17(8):763–782

Submit your manuscript to a SpringerOpen[⊗] journal and benefit from:

- ► Convenient online submission
- ► Rigorous peer review
- ► Open access: articles freely available online
- ► High visibility within the field
- ► Retaining the copyright to your article

Submit your next manuscript at ► springeropen.com