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Inflammatory biomarkers and pendelluft magnitude in ards patients transitioning from controlled to partial support ventilation

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The transition from controlled to partial support ventilation is a challenge in acute respiratory distress syndrome (ARDS) patients due to the risks of patient-self-inflicted lung injury. The magnitude of tidal volume (V_T) and intrapulmonary dyssynchrony (pendelluft) are suggested mechanisms of lung injury. We conducted a prospective, observational, physiological study in a tertiary academic intensive care unit. ARDS patients transitioning from controlled to partial support ventilation were included. On these, we evaluated the association between changes in inflammatory biomarkers and esophageal pressure swing (ΔP_{es}), transpulmonary driving pressure (ΔP_{L}), V_{T} , and pendelluft. Pendelluft was defined as the percentage of the tidal volume that moves from the non-dependent to the dependent lung region during inspiration, and its frequency at different thresholds (-15, -20 and -25%) was also registered. Blood concentrations of inflammatory biomarkers (IL-6, IL-8, TNF-α, ANGPT2, RAGE, IL-18, Caspase-1) were measured before (T_0) and after 4-h (T_4) of partial support ventilation. Pendelluft, ΔP_{es} , ΔP_{l} and V_{T} were recorded. Nine out of twenty-four patients (37.5%) showed a pendelluft mean \ge 10%. The mean values of ΔP_{es} , ΔP_L , and V_T were – 8.4 [– 6.7; – 10.2] cmH₂O, 15.2 [12.3–16.5] cmH₂O and 8.1 [7.3–8.9] m/kg PBW, respectively. Significant associations were observed between the frequency of high-magnitude pendelluft and IL-8, IL-18, and Caspase-1 changes ($T_0/$ T_4 ratio). These results suggest that the frequency of high magnitude pendelluft may be a potential determinant of inflammatory response related to inspiratory efforts in ARDS patients transitioning to partial support ventilation. Future studies are needed to confirm these results.

The transition from controlled to partial support ventilation or spontaneous modes is necessary for withdrawing mechanical ventilation in the acute respiratory distress syndrome (ARDS). Both ventilatory strategies preserve diaphragmatic contraction and allow spontaneous breathing (SB). Likewise, SB favors less sedation as well as improvements in ventilation/perfusion matching, dorsal ventilation, gas exchange, hemodynamics, and attenuate ventilator-induced diaphragmatic dysfunction, among other beneficial effects¹⁻⁴. However, under certain conditions, SB has been demonstrated to cause or enhance lung injury and could therefore complicate the weaning⁵⁻⁸.

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Nevertheless, there is no definitive evidence that P-SILI mechanisms such as pendelluft may effectively promote lung injury in humans. An additional challenge to advance our understanding of pendelluft is that we lack a validated approach to quantify it in magnitude and frequency, both of which may theoretically influence the impact of pendelluft on lung injury.

In the present study, we aimed to determine the potential contribution of pendelluft, esophageal pressure swing (ΔP_{es}) , transpulmonary driving pressure (ΔP_L) , and tidal volume (V_T) to acute lung injury, assessed by changes in inflammatory biomarkers in plasma, during the transition from controlled to partial ventilatory support.

Methods

Study population. We assessed patients with moderate-severe ARDS on protective mechanical ventilation (MV) for more than 48 h, hemodynamically stable, under moderate-light sedation (Richmond Agitation-Sedation Scale (RASS) -2 to -3) and without paralytic agents. Patients younger than 18 years old, pregnant, with contraindications to place EIT, central nervous system injury, new sepsis or moderate-severe metabolic acidosis, were excluded.

Study protocol. In this physiological study we prospectively monitored ARDS patients transitioning from controlled to partial support ventilation with esophageal manometry and EIT and we applied a systematic approach to measure pendelluft. In parallel, we analyzed the changes in representative biomarkers of acute lung injury to determine whether the development of pendelluft was associated with an increase in any of these biomarkers (Supplementary Figure S1).

Baseline respiratory mechanics and PEEP titration. Before initiating SB, respiratory system compliance was calculated by dividing V_T by the difference between plateau pressure and total positive end-expiratory pressure (PEEP), under volume-controlled mode with VT of 6 ml/kg of predicted body weight (PBW) and respiratory rate to keep PaCO₂ 5.3–6.6 kPa. Optimal PEEP was defined as the PEEP associated with the lowest combination of collapse and overdistension according to EIT¹¹. The patients were maintained at a semi-recumbent position (30° to 45°) during the study protocol. Further details are provided in the supplementary file.

Mechanical ventilation settings. The ventilator mode was switched from volume-control ventilation (VCV) to biphasic positive airway pressure mode (BiVent, Servo-i ventilator Maquet) after detection of a regular patient's respiratory rate (RR) (\geq 10 bpm). BiVent was applied during 4-h with a target of 10–50% of spontaneous ventilation relative to total minute ventilation (Supplementary Method S1). *Pressure-high* was adjusted for V_T of 6 ml/kg PBW and *Pressure-low* for optimal PEEP according to EIT; *T-high* with 0.8–1.0 s duration and *T-low* to maintain the same RR as in VCV.

Respiratory mechanics during SB. Airway pressure (P_{aw}), esophageal pressure (P_{es}), and transpulmonary pressure (P_L) were registered synchronously with EIT monitoring using a pneumotachometer (FluxMed MBMED*). P_L was calculated as the difference between P_{aw} and P_{es} . The correct position of the esophageal catheter (Neurovent Research Inc*, Canada) was confirmed¹² (Supplementary Method S1).

Ventilatory cycle and pendelluft. Regional ventilation changes were analyzed in four regions-of-interest (ROI) with similar height from non-dependent to dependent regions using EIT (Enlight 1800, Timpel*, Brazil). Because controlled, spontaneous, and mixed cycles coexist in BiVent, an algorithm was implemented to define each ventilatory cycle (Supplementary Figure S2). We analyzed ventilatory cycles for the last 10-min of each monitoring hour. Pendelluft magnitude was defined as the percentage of the normalized V_T that moves from non-dependent to dependent regions during inspiration in each ventilatory cycle (expressed in negative values). The mean of pendelluft magnitude was obtained and the pendelluft frequency was estimated as the proportion of cycles presenting pendelluft magnitudes above specific cut-off points (-15, -20, -25%, expressed as "-0.15", "-0.20", "-0.25" in Fig. 1 and Supplementary Figure S3).

Biomarkers. Pre-specified inflammatory mediators related to acute lung injury and ventilator-induced lung injury (VILI) (pro-inflammatory cytokines [IL-6, IL-8, TNF- α], biomarkers of lung epithelial [The receptor for advanced glycation end products, RAGE] and endothelial [angiopoietin-2, ANGP2] injury, and representative biomarkers of inflammasome activation [IL-18, Caspase-1])¹³⁻²³ were measured in serum by ELISA (Human magnetic Luminex screening assay and Human Caspase-1/ICE quantikine ELISA kit) at baseline (T₀) and after 4 h on BiVent mode (T₄) (Supplementary Method S3).

Statistical Analysis. Summary statistics of pendelluft magnitude were estimated. For each patient, the pendelluft frequencies were calculated from the four 10-min monitoring periods. Friedman analysis was performed



Figure 1. Histograms of inspiratory dyssynchrony (pendelluft) at different magnitudes. X axis corresponds to the magnitude of pendelluft and Y axis, to the percentage of ventilatory cycles with certain magnitude of pendelluft. The negative value of pendelluft represents the lost volume in non-dependent region during inspiration, expressed as fraction. The vertical red dotted line delimits the pendelluft with high magnitude cutoff -0.2 (i.e. 20% of lost volume in non-dependent region during inspiration). (A) corresponds to Subject #2, a patient with a pendelluft mean of -0.2 (-20%), who presented high frequency of high-magnitude pendelluft. (B) corresponds to Subject #23, a patient with pendelluft mean of -0.02 (-0.2%), who presented low frequency of high-magnitude pendelluft.

to compare changes in the pendelluft frequencies, ΔP_{es} , ΔP_{L} , and V_T during the four observation periods. The Wilcoxon signed-rank test was used to compare the biomarkers at T_0 and at T_4 .

To evaluate the individual association between ΔP_{es} , ΔP_L , V_T , and pendelluft frequency with each biomarker ratio [(biomarker at T_4)/(biomarker at T_0)], simple linear regression models were fitted. To study the independence of associations between pendelluft and ratios while controlling for ΔP_{es} , ΔP_L and total and regional V_T , multiple linear regressions were fitted. All the analyses were performed using R statistical software (R Foundation for Statistical Computing, Vienna, Austria).

Ethics approval and consent to participate. This study was performed in accordance with the Declaration of Helsinki. The Institutional Review Board reviewed and approved the study (approval number N.027/2016, Comité Ético Científico Hospital Clínico Universidad de Chile). Written informed consent was obtained from all patient's next of kin. All methods were performed in accordance with the relevant guidelines and regulation.

Results

We included twenty-four ARDS patients of which 14 were males, with a median age of 63 [54–67] years and with body mass index of 29 [23–32] kg m⁻². Before enrollment their worst exchange values were median PaO_2/FiO_2 of 16.4 [12–20] kPa and worse sequential organ failure assessment (SOFA) score of 12 [9–14] with six patients treated with prone positioning. At the study entry, MV time was 6.5 [4–11] days, gas exchange and lung mechanics were already improving in most patients. Twelve patients presented with patchy, 4 with diffuse, and 8 with lobar computed tomography attenuations (Supplementary Table S1).

The pendelluft magnitude and its frequency for different cut-offs on hourly basis and the overall period are shown in Table 1. Nine patients (37.5%) showed a volume displacement mean \geq 10% from non-dependent to dependent region during inspiration (i.e. mean pendelluft). Pendelluft frequency was lower at higher cut-off points of magnitude (19 [3.8–32]% at pendelluft₁₅, 10 [2–23]% at pendelluft₂₀, and 3 [1–15]% at pendelluft₂₅). ΔP_{es} , ΔP_{L} , and V_T were – 8.5 [–10.1; –6.6] cmH₂O, 15.1 [12.2–16.7] cmH₂O and 8.1 [7.2–8.8] m/kg PBW, respectively. None of these respiratory variables significantly changed during the study period (Table 1). Respiratory rate and total minute ventilation were 24 (19.6–25.9) bpm and 10.2 (8.8–12.0) L/min, respectively; both remained stable through the 4-h period (*p*-value = 0.809 and *p*-value = 0.951, respectively).

The overall cohort plasma concentration of the biomarkers did not change between T_0 and T_4 with the exception of TNF- α that decreased (Supplementary Figure S4). Nevertheless, some individual patients did exhibit an increase in biomarkers concentrations. The main results of single regression models for biomarkers ratios and mean pendelluft magnitude, frequency of different pendelluft magnitudes, or respiratory variables are shown in Fig. 2, Fig. 3 and Additional File 1 Table 2. There was only a trend in correlations between IL-18 and Caspase-1 ratios and the mean pendelluft magnitude (R² 0.147 and *p*-value 0.064 for both biomarkers), but a significant association was observed between these biomarkers (and IL-8) and the frequency of high-magnitude pendelluft. The R², estimate (β), and level of significance (*p*-value) increased as pendelluft magnitude became higher

Variable	H ₁ [Median (IQR)]	H ₂ [Median (IQR)]	H ₃ [Median (IQR)]	H ₄ [Median (IQR)]	Global [Median (IQR)]	<i>p</i> -value
ΔP_{es} (cmH ₂ O)	-7.8 (-12.4; -6.5)	-9.0 (-12.2; -6.1)	-8.5 (-10.2; -6.6)	-8.3 (-10.0; -2.6)	-8.5 (-10.1; -6.6)	0.905
$\Delta P_L (cmH_2O)$	15.2 (12.0–17.0)	14.8 (12.3–18.1)	14.0 (11.8–16.0)	13.7 (11.8–16.6)	15.1 (12.2–16.7)	0.714
V _T (mL/kg)	7.9 (6.8–8.7)	8.2 (7.0–9.6)	8.1 (7.0-8.9)	8.0 (6.9–8.8)	8.1 (7.2–8.8)	0.538
pendelluft _{MEAN} (%)	-5 (-11; -3)	-7 (-11; -3)	-7 (-12; -2)	-7 (-13; -3)	-7 (-11; -3)	0.752
pendelluft ₋₁₅ (%)	10.8 (2.7–29.3)	14.0 (2.7–32.7)	17.9 (1.6–36.7)	17.9 (4.0-39.0)	19.1 (3.8–32.2)	0.153
pendelluft ₋₂₀ (%)	3.9 (1.1–18.7)	8.4 (0.4–21.3)	8.3 (0.6–20.3)	9.7 (1.3-24.6)	10.0 (2.1–22.7)	0.643
pendelluft ₋₂₅ (%)	2.5 (0.0-7.2)	2.5 (0.0-9.8)	1.8 (0.2–8.2)	3.3 (0.2–10.4)	3.0 (1.2–15.2)	0.844

Table 1. Respiratory variables, mean pendelluft magnitude and pendelluft frequency at different magnitudes, during the study period. H₁, H₂, H₃ and H₄ represent the last 10-min of each monitoring hour within the 4-h study period; Global is the average between H₁, H₂, H₃ and H₄; pendelluft_{MEAN} represents the mean of pendelluft magnitude and pendelluft_{.15}, pendelluft_{.20}, and pendelluft_{.25}, the pendelluft frequency at magnitudes – 15, – 20, and – 25%, respectively, measured in each time of monitoring; ΔP_{es} : negative deflection of esophageal pressure (P_{es}) from the onset of inspiratory effort during the ventilatory cycle; ΔP_L , tidal change in transpulmonary pressure, calculated as airway pressure (P_{aw}) minus P_{es}, between the maximum and minimum values of the ventilatory cycle: Both, ΔP_{es} and ΔP_L , were measured in cmH₂O; V_T (mL/kg PBW): tidal volume measured in mL/kg of predicted body weight.

(from 15 to 25%) (Fig. 2). We did not observe association between other cytokines and the mean and frequency of pendelluft at any magnitude (Supplementary Table S2). Likewise, no significant associations were observed between biomarkers and global respiratory variables, with the exception of a positive correlation between RAGE ratio and ΔP_L (Fig. 3 and Supplementary Table S2).

To explore whether pendelluft may be mediator in the pathway between global parameters and inflammatory biomarkers, simple regressions were fitted. The mean pendelluft magnitude and frequencies at different pendelluft magnitudes were associated with V_T at the dependent lung regions but not with total V_T . We did not observe significant associations between pendelluft and ΔP_{es} nor ΔP_L suggesting that pendelluft frequency might be only partially influenced by these variables (Supplementary Table S3). Even more, when ΔP_{es} , ΔP_L , and V_T were included as covariates in multiple linear regressions for the biomarkers ratios, the observed associations between pendelluft₂₀₋₂₅ frequency and IL-8, IL-18, and Caspase-1 were only slightly attenuated, presenting stronger associations than the global parameters as evidenced by the magnitude of the t-statistic (Table 2).

Discussion

In the present physiological study, we found that in ARDS patients transitioning from controlled to partial support ventilation: (1) the overall concentration of inflammatory biomarkers did not change consistently, although a subgroup of patients exhibited an increase in some inflammatory biomarkers; (2) the frequency of high-magnitude pendelluft was the parameter best associated with the increase in specific inflammatory biomarkers (IL-8, IL-18, and Caspase-1), independently of ΔP_{es} , ΔP_{L} , and V_{T}

The present study describes for the first time in humans the association of high-magnitude pendelluft with the increase of specific inflammatory mediators related to VILI. The absence of a significant correlation between pendelluft and global variables, such as ΔP_{es} , ΔP_L and V_T provides evidence for the current hypothesis of pendelluft as a regional phenomenon which may be related to a local change in pleural pressure^{10,24,25}.

Not all patients developed high-magnitude pendelluft (Fig. 1) or increased inflammatory biomarkers, but the association between both was positive and significant. Indeed, we observed a progressive increase in \mathbb{R}^2 , in the estimate (β), and in the level of significance (*p*-value) in relation to the increase in the cut-off points of pendelluft magnitude from 15 to 25% with the IL-8, IL-18 and Caspase-1 ratios. This suggests that the inflammatory response is triggered above a certain threshold of pendelluft in the same way as non-protective MV. High-magnitude pendelluft causes overstretch in lung regions during tidal inflation and it is known that cyclic stretch upregulates IL-8 in a strain-dependent manner¹⁵ and thus provides a potential explanation for the association between the frequency of high-magnitude pendelluft and the increase in IL-8. This cytokine is the major chemoattractant for neutrophils¹⁶ and the release of IL-8 is considered to play an important role in the inflammatory response and progression of VILI in patients with ARDS¹⁷.

A parallel increase in IL-18 and Caspase-1 in association with the frequency of high-magnitude pendelluft suggests a common pathway related to the inflammasome activation. IL-18 and caspase-1 have been shown to play a fundamental role in the spread of lung injury in experimental studies and in critically ill patients^{18–21}. Even more, an elevated level of serum IL-18 has a suggested association with worse prognosis in patients with ARDS^{18,19}. The use of MV with high V_T (for a few hours) has been shown to increase the expression of IL-18 and Caspase-1 in lung tissue and plasma¹⁹. The mechanical stress produced by MV on the lung parenchyma is capable of triggering the production of reactive oxygen species in mitochondria from activated alveolar macrophages, which activate the inflammasome leading to the processing and maturation of Pro IL-1β and Pro IL-18^{20,21}.

The decision to assess inflammatory changes through the ratio of biomarker levels at T_0 and T_4 was based in the large inter-individual variability reported in previous studies^{13–24}, as well as, the expectation that only a subgroup of patients would have intense inspiratory efforts. In addition, we believe that the biomarker ratio,



Figure 2. Scatter plots and regression analysis between (**A**) IL-8, (**B**) IL-18, (**C**) Caspase-1 ratios and frequencies of pendelluft magnitude -15, -20 and -25%. Biomarker ratio [(biomarker at T₄)/(biomarker at T₀)] and the mean of pendelluft frequencies at different cut-off points of pendelluft magnitude (-15, -20 and -25%), through the 4 h period of observation, were obtained for each patient. Pendelluft.₁₅: mean of pendelluft frequency at magnitude of -15%; Pendelluft.₂₀: mean of pendelluft frequency at magnitude of -20%; Pendelluft.₂₅: mean pendelluft frequency at magnitude of -25%. ΔP_{es} : mean of negative deflection of esophageal pressure from the onset of inspiratory effort during the ventilatory cycle; ΔP_L : mean of tidal change in transpulmonary pressure. V_T : tidal volume.

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by representing a relationship is sensitive to changes, discriminates the most relevant interactions and allows a more personalized analysis²⁶.

Remarkably, there was a low frequency of high-magnitude pendelluft at the SB onset. Three potential causes may explain these findings: (1) In this study, we used a personalized titration of "optimal" PEEP according to EIT to reduce lung collapse¹¹. The titrated PEEP may reduce the neuromuscular efficiency as suggested by recent physiologic studies^{27,28}; (2) The ventilatory mode used (BiVent) usually generates lower tidal volumes and transpulmonary pressure than fully synchronized or partially synchronized pressure-targeted modes despite similar settings on the ventilator and patient's effort²⁹ and has shown to be a safe and potentially beneficial ventilatory strategy³⁰⁻³³. We applied a similar ventilatory strategy to that used in a randomized controlled trial with BiVent (*BiRDS study, ClinicalTrials.gov Identifier: NCT01862016*). (3) Finally, the sedation was titrated to



Figure 3. Scatter plots and regression analysis between (**A**) IL-8, (**B**) IL-18, (**C**) Caspase-1 ratios, and respiratory variables. Biomarker ratio [(biomarker at T₄)/(biomarker at T₀)] and the mean values by patient of ΔP_{es} , ΔP_L and V_{Tb} through the 4 h period of observation, were obtained for each patient ΔP_{es} : mean of negative deflection of esophageal pressure (P_{es}) from the onset of inspiratory effort during the ventilatory cycle; ΔP_L : mean of tidal change in transpulmonary pressure. Only the association between ΔP_{es} and ΔP_L and the pendelluft ²⁵ frequency was significant ($R^2 0.202$ and *p*-value = 0.047). Several patients presented pendelluft of higher magnitude at lower than – 15 and 20 cmH₂O of ΔP_{es} and ΔP_L , respectively.

maintain RASS - 2 to - 3 and SB up to 50% of the total minute ventilation, which was successfully obtained and remained between 35 and 50% in all patients. In this scenario, which may be considered partially inhibitory of strong inspiratory efforts, no associations were found between the percentage of SB over total minute ventilation and pendelluft magnitude or inflammatory biomarkers.

P-SILI may be more likely when intense inspiratory efforts occur in severe ARDS ("solid-like" lungs), compared to mild ARDS ("fluid-like" lungs)^{34,35}. In the present study, all patients had moderate to severe ARDS upon admission to the ICU. However, at the time of inclusion, patients had remained on MV for over a week on average and thus: gas exchange, lung disease, and lung mechanics were already improving in most patients. Nevertheless, high-magnitude pendelluft was observed in some patients despite protective values of ΔP_{es} , ΔP_{L} , and V_{T} . Both the global parameters and pendelluft may share some common mechanisms and thus the observed associations are

Predictor	Estimate	R ²	t-value	<i>p</i> -value					
Model 1: IL-8 ratio = $\beta_0 + \beta_1^* \text{pend}_{20} + \beta_2^* \Delta P_{es}$									
pendelluft-20	1.485	0.085	1.398	0.177					
ΔP_{es}	0.018		0.494	0.626					
Model 2: IL-8 ratio = $\beta_0 + \beta_1^* \text{pend}_{20} + \beta_2^* \Delta P_L$									
pendelluft ₋₂₀	1.324	0.075	1.286	0.212					
ΔP_L	0.002		0.056	0.956					
Model 3: IL-8 ratio = $\beta_0 + \beta_1 * \text{pend}_{25} + \beta_2 * \Delta P_{es}$									
pendelluft-25	4.631	0.228	2.492	0.021					
ΔP_{es}	0.037		1.079	0.292					
Model 4: IL-8 ratio = $\beta_0 + \beta_1^* \text{pend}_{25} + \beta_2^* \Delta P_L$									
pendelluft_25	3.942	0.188	2.200	0.039					
ΔP_L	-0.011		-0.266	0.793					
Model 5: IL-18 ratio = $\beta_0 + \beta_1^* \text{pend}_{20} + \beta_2^* \Delta P_{es}$									
pendelluft_20	0.553	0.169	1.949	0.065					
ΔP _{es}	-0.001		-0.083	0.934					
Model 6: IL-18 ratio = $\beta_0 + \beta_1^* \text{pend}_{20} + \beta_2^* \Delta P_L$									
pendelluft_20	0.558	0.169	2.038	0.054					
ΔP_L	0.001		0.086	0.932					
Model 7: IL-18 ratio = $\beta_0 + \beta_1^* \text{pend}_{25} + \beta_2^* \Delta P_{es}$									
pendelluft ₋₂₅	1.577	0.355	3.309	0.003					
ΔP_{es}	0.005		0.601	0.554					
Model 8: IL-18 ratio = $\beta_0 + \beta_1^* \text{pend}_{25} + \beta_2^* \Delta P_L$									
pendelluft_25	1.500	0.348	3.327	0.003					
ΔP_L	-0.037		-0.370	0.715					
Model 9: Caspase-1 ratio = $\beta_0 + \beta_1 * \text{pend}_{20} + \beta_2 * \Delta P_{es}$									
pendelluft_20	1.025	0.235	1.856	0.078					
ΔP_{es}	-0.021		-1.112	0.279					
Model 10: Caspase-1 ratio = $\beta_0 + \beta_1^* \text{pend}_{20} + \beta_2^* \Delta P_L$									
pendelluft-20	1.141	0.225	2.131	0.045					
ΔP_L	0.021		0.978	0.339					
Model 11: Caspase-1 ratio = $\beta_0 + \beta_1^* \text{pend}_{25} + \beta_2^* \Delta P_{es}$									
pendelluft_25	2.611	0.336	2.659	0.001					
ΔP_{es}	-0.012		-0.646	0.525					
Model 12: Caspase-18 ratio = $\beta_0 + \beta_1 * \text{pend}_{25} + \beta_2 * \Delta P_L$									
pendelluft-25	2.728	0.334	2.952	0.008					
ΔP_L	0.012		0.654	0.520					

Table 2. Effect of ΔP_{es} and ΔP_L on associations between pendelluft₂₀₋₂₅ frequencies and biomarker ratios. Pendelluft₂₀ and pendelluft₂₅ represent the pendelluft frequency at magnitudes of – 20% and – 25%, respectively. ΔP_{es} : negative deflection of esophageal pressure (P_{es}) from the onset of inspiratory effort during the ventilatory cycle; ΔP_L , tidal change in transpulmonary pressure, calculated as airway pressure (P_{aw}) minus P_{es} , between the maximum and minimum values of the ventilatory cycle; V_T (mL/kg PBW): tidal volume measured in mL/kg of predicted body weight.

attenuated when including both variables in the multivariate model, but the signal from pendelluft was a stronger predictor of inflammatory response and it might be mediated by specific pathways unrelated to global parameters.

Study Limitations. Our findings must be interpreted with caution due to several limitations such as: (1) the small sample size; (2) the use of BiVent mode with optimized PEEP and analgosedation enough to maintain spontaneous ventilation up to 50% of total minute ventilation, which may have avoided high-magnitude pendelluft and a stronger inflammatory response; (3) the short period of spontaneous ventilation; (4) the potential effect of simultaneous phenomena acting as confounders on biomarkers changes; (5) the study does not allow to infer whether the changes in IL-18, Caspase 1 and IL-8 plasma concentrations observed in patients with high-magnitude pendelluft were indeed produced in the lung; and, (7) the lack of validation of the results of pendelluft in the absence of a unified definition of the phenomenon.

For all the above, the present study should be considered as a pilot exploratory and hypothesis generating study. Further research is needed to assess the role of pendelluft in clinical practice. However, to the best of our knowledge, this is the first attempt to explore the association between pendelluft and inflammation in subjects with ARDS during the first hours of spontaneous ventilation.

Conclusions

In conclusion, in ARDS patients transitioning from controlled to partial support ventilation high-magnitude pendelluft was independently associated with an increase in specific inflammatory biomarkers related to VILI (IL-8, IL-18 and Caspase-1). The development of pendelluft may be a potential determinant of P-SILI at the spontaneous ventilation onset. Future studies are needed to confirm this conclusion.

Data availability

All data generated or analyzed during this study are included in this published article and its supplementary information file.

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Author contributions

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Competing interests

The authors declare no competing interests.

Additional information

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