



Impact of binder as a formulation variable on the material and tableting properties of developed co-processed excipients

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Abstract

The functionality of a co-processed excipient is usually derived from its composition and the proportion of each excipient that is incorporated to yield a composite excipient. The aim of this study was to assess the impact of binder as a formulation variable on the material and tableting properties of developed co-processed excipients containing gelatin (SGS) and microcrystalline cellulose (SMS) as binders respectively in the same proportion. Two co-processed excipients, SGS and SMS were generated by combining tapioca starch (90%), gelatin or microcrystalline cellulose (7.5%) and colloidal silicon dioxide (2.5%) using the co-fusion method. Particle size analysis and morphological assessment were carried out by light microscopy and scanning electron microscopy (SEM) respectively. DSC analysis was performed to evaluate the thermal behaviour of both materials and flow properties were assessed by measuring parameters like angle of repose, bulk and tapped densities, Carr's index and Hausner's ratio. Compaction behaviour of both materials was determined using Heckel and Walker equations and the compressibility–tableting–compactibility (CTC) profile for each material was obtained. Particulate and bulk-level properties of SGS and SMS revealed spherical-shaped, free-flowing powders characterized by a glass transition event typical of amorphous polymers. Compaction analysis demonstrated greater degree of plastic deformation with SMS resulting in better tableting properties with respect to tensile strength and disintegration time. The outcome of the study shows that the choice of binder used in the formulation of a co-processed excipient plays a crucial role in defining the material and tableting properties of the co-processed excipient.

Keywords Binder · Gelatin · Microcrystalline cellulose · Co-processed excipients

1 Introduction

The success of a tableting operation requires the inclusion of functional excipients to the formulation. Excipients play the traditional role of ensuring that active pharmaceutical ingredients are processed into suitable dosage forms that will deliver the drug to the intended site of action after administration. Hence, the manufacturability, stability,

bioavailability and efficacy of the drug are influenced by the presence of excipients in a formulation. The necessity for excipients with improved functionality has driven the research in the area of novel excipient development to increase the range of excipients that are available for pharmaceutical development.

Many of these researches have led to the commercialization of novel excipients like Prosolv® (JRS Pharma),

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Ludipress® (BASF) and StarLac® (Roquette Pharma). Currently, attention is being paid to direct compression (DC) as the preferred method of tableting because it addresses most of the limitations encountered with the conventional method of wet granulation. This has steered the development of novel excipients greatly towards those that possess direct compression functionality. Only a few single excipients exist with direct compression functionality and on the top of the list is microcrystalline cellulose (MCC) which has been classified as a dry binder in the formulation of tablets by dry granulation and direct compression [1]. All other excipients that are employed in direct compression tableting are a combination of two or more excipients known as co-processed excipients. Co-processing is a particle engineering technique that facilitates the development of a composite excipient with improved functionality [2–4]. The performance attributes of a co-processed excipient are usually determined by the composition of the co-processed excipient with respect to the primary excipients used as well as the proportion of each primary excipient in the co-processed excipient [3, 5]. Research into co-processing of excipients has yielded products with diverse functionalities and performance attributes. These functionalities include orally disintegrating ability [6, 7], improved dilution potential [8], rapid disintegration [9], enhanced direct compression functionality [10], multifunctional excipient [4, 8], improved tableability [11], and improved dispersibility [12].

Binders are important materials included in the formulation of tablets to facilitate bonding of powder particles during granulation. They ensure the agglomeration and cohesion of the granules to each other, promoting appropriate compactibility and free-flowing properties [13]. Depending on their mode of incorporation in tablet formulation, binders are classified as solution binders (hydroxypropyl methylcellulose, gelatin and polyvinylpyrrolidone) or dry binders (microcrystalline cellulose). Binders have been known to modulate the compressibility of a tablet formulation and so has become a candidate material in co-processing to improve the functionality of excipients with poor compressibility. To overcome the relative poor compactibility of lactose, co-processed excipient based on the combination of α -lactose monohydrate (a brittle material) and plastic binders (microcrystalline cellulose and polyvinyl pyrrolidone) have been developed with considerable success [10]. Similarly, a study carried out by Wang et al. (2015) demonstrated an improvement in the tableability of lactose when co-processed with hydroxypropyl methylcellulose (HPMC E3) and crospovidone (PVPP). Other studies related to improving the direct compression potential of starches has been achieved by co-processing with binders like acacia [14, 15]. In the present study, two co-processed excipients composed

of tapioca starch and colloidal silicon dioxide but differing in the binder content were generated by co-fusion. The aim of the study was to assess the impact of binders differing in their mode of incorporation on the material and tableting properties of the generated co-processed excipients. Gelatin was selected as an example of a solution binder while microcrystalline cellulose was chosen as a dry binder. Both binders were incorporated in the same proportion in their respective formulations.

2 Materials and methods

Tapioca starch was obtained as a gift sample from Quality Starch and Chemicals (Tamil Nadu, India), Microcrystalline cellulose (Avicel PH 112, FMC Biopolymer, Philadelphia, PA), Gelatin (May and Baker Ltd, England) and colloidal silicon dioxide (Cab-o-Sil®, Cabot GmbH, Germany). All other materials used were of analytical grade.

2.1 Preparation of co-processed excipients (SGS and SMS)

Co-processing of excipients was carried out using the method described by Adeoye and Alebiowu [16] with modifications. A 40% w/w suspension of tapioca starch (TS) was prepared by dispersing 90 g of tapioca starch (TS) in 135 mL distilled water. Gelatin (7.5 g) and colloidal silicon dioxide (2.5 g) were added to the suspension and stirred for 5 min. Further mixing was continued on a shaker water bath (Julabo SW 23, Seelbach, Germany) set at 54 ± 2 °C/60 rpm for 15 min. The mixture was allowed to equilibrate at 25 ± 2 °C and homogenized at a speed of 11,000 rpm (Ultra Turrax T 25 basic Ika® Werke, India) for 5 min, it was then dried partially at 25 ± 2 °C for 2 h before being finally dried in the Fluid bed dryer (Retsch TG 100, Germany) at 40 °C for 10 min. The co-processed excipient (SGS) obtained was screened through a sieve (500 μ m) and stored in an air-tight container kept in a desiccator containing phosphorous pentoxide (P_2O_5) prior to characterization studies. The entire process was repeated to prepare SMS containing microcrystalline cellulose (MCC) as binder.

2.2 Particle size analysis

Particle size analysis was carried out for SGS and SMS using a Leica DMLP light microscope (Leica, Microsystems Wetzlar GmbH, Wetzlar, Germany). The diameter corresponding to the length along the longest axis was measured for each particle and a minimum of 500 particles were counted for each material. Particle size was expressed as d_{10} , d_{50} , and d_{90} corresponding to 10, 50 and 90% of cumulative undersize particles respectively.

2.3 Scanning electron microscopy (SEM)

The shape and surface morphology of both materials were examined using a scanning electron microscope (S-3400, Hitachi Ltd., Tokyo, Japan) operated at an excitation voltage of 15 kV. The samples were prepared by mounting on a steel stage using a double-sided adhesive tape and sputter-coated with gold prior to image capture at various magnifications.

2.4 Differential scanning calorimetry

Thermal analysis of the materials was evaluated using DSC, Model Q2000 (TA Instruments, New Castle, DE USA). Prior to analysis, the DSC instrument was calibrated using high purity indium standard and continuously purged with dry nitrogen flowing at 50 ml/min. Powder samples weighing about 5 mg each of SMS and SGS were heated in standard Tzero aluminium pans at 20 °C/min from 25 to 300 °C. Data analysis was performed using Universal[®] Analysis 2000 (version 4.5A) software. Modulated differential scanning calorimetry (MDSC) scan was carried out to obtain a better resolution of the glass transition event from the reversing heat flow signal.

2.5 Angle of repose

Angle of repose of both powders was measured using the granulate flow tester (GTB, Erweka, Germany). The powder sample (20 g) was poured at 45° into a stainless-steel funnel and allowed to flow out through the orifice measuring 10 mm in diameter unto a flat surface. The height of the conical heap of powder was measured automatically using an integrated driven laser system and the angle of repose calculated using the formula, $\theta = \tan^{-1} h/r$. A mean of three replicates was recorded as the angle of repose.

2.6 Bulk, tapped and true densities

The volume occupied by 20 g powder of each sample poured into a 100 mL measuring cylinder of a tapped density tester (USP tap density apparatus, Electro lab, Mumbai, India) was recorded as the bulk volume. The tapped volume was obtained by tapping the contents of the measuring cylinder to constant volume according to the USP II method. Bulk and tapped volumes were obtained in triplicate and were used to calculate the bulk and tapped densities. Hausner ratio (HR) and Carr's index (CI) were calculated for each sample using the bulk and tapped densities and the results were expressed as mean \pm standard deviation.

True density (ρ_T) of both materials was determined by the gas displacement technique using the Helium

Pycnometer (Pycno 30, Smart Instruments, India). Measurements were taken in triplicate at 25 ± 2 °C/ $40 \pm 2\%$ RH and the mean \pm standard deviation was recorded.

2.7 Compaction studies

The compaction behaviour of both powders was evaluated using out-of-die analysis. Tablets weighing 400 mg were compressed individually at pressures ranging from 35–300 MPa on a Hydraulic Carver Press (Model 3912, Carver Inc., USA) using 13 mm flat-faced punches. Prior to compression, the die cavity was lubricated with a dispersion of magnesium stearate in ethanol. The compacts were held for 30 s at maximum pressure during the last stage of compression leading to detachment and ejection of the tablet. After ejection, the tablets were kept in a desiccator for 24 h to allow for elastic recovery. The tablet parameters of weight, thickness and crushing strength were measured for each tablet and the following equations (Eqs. 1, 2, 3, 4 and 5) were used to calculate volume (V), apparent density (ρ_A), relative density (D), porosity (ϵ) and tensile strength (TS) respectively.

$$V = \pi r^2 h \quad (1)$$

$$\rho_A = \frac{W}{\pi r^2 h} \quad (2)$$

$$D = \frac{\rho_A}{\rho_T} \quad (3)$$

$$\epsilon = 1 - D \quad (4)$$

$$TS = \frac{2F}{\pi dt} \quad (5)$$

where r corresponds to the radius of the die, h is the thickness of the tablet, W is the weight of the tablet, F is the crushing strength and d is the diameter of the die.

The parameters obtained above were fitted into Heckel [17] and modified Walker [18, 19] equations (Eqs. 6 & 7) respectively to generate the corresponding compaction plots.

$$\ln \left(\frac{1}{1-D} \right) = KP + A \quad (6)$$

$$V' = -W' \log P + V_{sp'} \quad (7)$$

The compressibility plot (porosity against compaction pressure), compactibility plot (Tensile strength against porosity) and tabletability plot (tensile strength against compaction pressure) were also generated for each material.

2.8 Tableting

Tablets (400 mg) were prepared by compressing directly a powder blend of ibuprofen and the co-processed excipient (SGS or SMS) (1:1) on a Rimek rotary tablet press (Mini II D, Karnavati Engineering Pvt. Ltd., India) fitted with flat-faced 12-mm punch and die tooling. The compaction force was kept constant for both batches of tablets. The tablets were kept for 24 h after compression to allow for elastic recovery before evaluation of tablet properties. The following properties of tablets were evaluated according to BP specifications [20].

2.9 Weight uniformity

The weight of twenty randomly selected tablets from each batch of tablets was obtained using an analytical scale (Mettler-Toledo AG 285, Switzerland) and the mean and standard deviation of each sample was recorded.

2.10 Tablet thickness

The thickness of ten tablets chosen at random from each batch was measured using a digital micrometre screw gauge (Mitutoyo, Japan) and a mean of ten replicates was recorded with standard deviation.

2.11 Crushing strength

The breaking force required to crush a tablet along its diameter was determined using a tablet hardness tester (TBH 20, Erweka, Germany). An average of six replicates was obtained for each batch and the tensile strength (T_s) was computed using the equation,

$$T_s = \frac{2F}{\pi dt}$$

where F is the crushing strength (N), d and t are diameter and thickness respectively.

2.12 Friability

Tablet friability was evaluated using a Friabilator (EF-2, Electro lab, India). Ten tablets were weighed initially, placed in the friabilator and allowed to rotate at 25 rpm for 4 min. The tablets were re-dusted, re-weighed and the difference in tablet weight was determined. Friability was calculated as follows:

$$\% \text{friability} = \frac{W_i - W_f}{W_i} \times 100$$

where W_i and W_f are the initial and final weights of tablets respectively.

2.13 Disintegration time

The disintegration time of six tablets sampled at random for each batch was determined using a disintegration apparatus (ED-2L, Electro lab, India) as described in the British Pharmacopoeia [20].

2.14 Determination of disintegration efficiency ratio (DER)

The disintegration efficiency ratio (DER) was determined using the relationship,

$$DER = \frac{C_s/F_R}{D_T}$$

where C_s , F_R and D_T are crushing strength, friability and disintegration time respectively.

2.15 *In vitro* dissolution studies

In vitro dissolution studies were conducted using the dissolution tester (USP) (TDT-08L, Electro lab, India). The USP Apparatus II (paddle) method was adopted as recommended by USP [21]. Phosphate buffer (pH 7.2; 900 mL) was prepared and used as the dissolution medium. One tablet from each formulation was dropped into the dissolution medium (37 ± 0.5 °C) and the apparatus set to rotate at 50 rpm for 60 min. Aliquots of 5 mL were withdrawn at specific time intervals and replaced with equal volume of phosphate buffer (pH 7.2) maintained at the same temperature as that of the dissolution medium. Each withdrawn sample was filtered using a 0.2 μ membrane disc filter and suitably diluted with phosphate buffer (pH 7.2). The diluted samples were assayed for ibuprofen by reading the absorbance at 221 nm using the UV/VIS spectrophotometer (Lambda 35, PerkinElmer, USA) and the amount of drug released was calculated using the regression data equation ($y = 0.0951x$, $R^2 = 0.9981$) obtained from the calibration curve of ibuprofen. The dissolution profile of ibuprofen was determined by plotting a graph of percentage drug released against time.

2.16 Statistical analysis

Data analysis was carried out in Microsoft Excel using the analytical tool, ANOVA: Single factor to evaluate the differences in tableting properties of both materials. Differences in tableting properties of both materials were considered significant at $p \leq 0.05$.

3 Results

Particle size analysis of the two co-processed excipients is presented in Table 1. Comparing the d_{10} , d_{50} and d_{90} parameters, particle size of SGS was approximately twice as large as that of SMS. A narrow particle size distribution was obtained for SMS due to its lower span value of 1.26.

Figure 1a, b displays the SEM pictures of SGS and SMS respectively. Both materials are characterized by spherical-shaped particles with several particles showing a deviation from sphericity. Surface morphology reveals that the SGS particles appear smoother than those of SMS. The images of SGS and SMS reveals a homogeneous dispersion of the interacting excipients resulting in the formation of a single composite excipient with minimal appearance of discrete primary particles of the individual excipients.

Thermal analysis of SGS and SMS represented by the DSC curve in Fig. 2 shows a characteristic glass transition event occurring in the reversing heat flow signal for both materials. The onset of glass transition was slightly lower for SGS occurring at a temperature of 251.53 °C compared to 254.02 °C obtained for SMS.

The powder properties of SGS and SMS are presented in Table 2. Both powders demonstrated good flow behaviour on account of the low values obtained for AR, CI and HR.

Table 1 Particle size analysis of SGS and SMS using microscopy

| Material | $D_{10}(\mu)$ | $D_{50}(\mu)$ | $D_{90}(\mu)$ | Span |
|----------|---------------|---------------|---------------|------|
| SGS | 77.5 | 145 | 289 | 1.46 |
| SMS | 44 | 75.5 | 139.5 | 1.26 |

SGS Co-processed excipient containing gelatin as binder

SMS Co-processed excipient containing microcrystalline cellulose as binder

The BD and TD obtained for SMS was greater than that of SGS indicating a greater degree of packing in the powder bed.

The true density of both powders did not differ significantly although SGS was observed to have a slightly higher value of 1.45 g/cm³ than that of SMS. There was, however, a remarkable difference in their swelling index (SI) as SMS was found to swell about 4 times more than SGS.

Table 3 is a summary of the compaction parameters derived from Heckel and Walker analysis (Fig. 3). The mean yield pressure (P_y) resolved as the inverse of the slope of the linear portion of the Heckel plot was found to be lower for SMS compared to SGS indicating a higher degree of plasticity. The total degree of densification of the powder bed at the early stages of compression was quantified as the D_A parameter. The extent of densification occurring as a result of particle rearrangement (D_A) was seen to be higher for SGS (0.745) than that of SMS (0.614). Densification attributed to particle motion and filling of the die at low pressures (D_ρ) on the other hand, was higher for SMS compared to SGS. This is consistent with the values of bulk and tapped densities obtained for SMS which was significantly higher than that of SGS. However, densification contributed by particle fragmentation at low pressures (D_B) was higher for SGS in relation to SMS indicating that lower amount of plastic deformation occurred during compression. This agrees with the higher yield pressure obtained for SGS. The Walker's W' coefficient of compressibility indicates that SMS is more compressible than SGS owing to the higher value obtained as compressibility coefficient (W') for SMS (Table 3).

The compaction behaviour of the two materials was also evaluated using the compressibility-tabletability-compactibility (CTC) profile presented in Fig. 4a–c. The compressibility plot (Fig. 4a) relates the effect of compression pressure on porosity and shows a gradual decline in

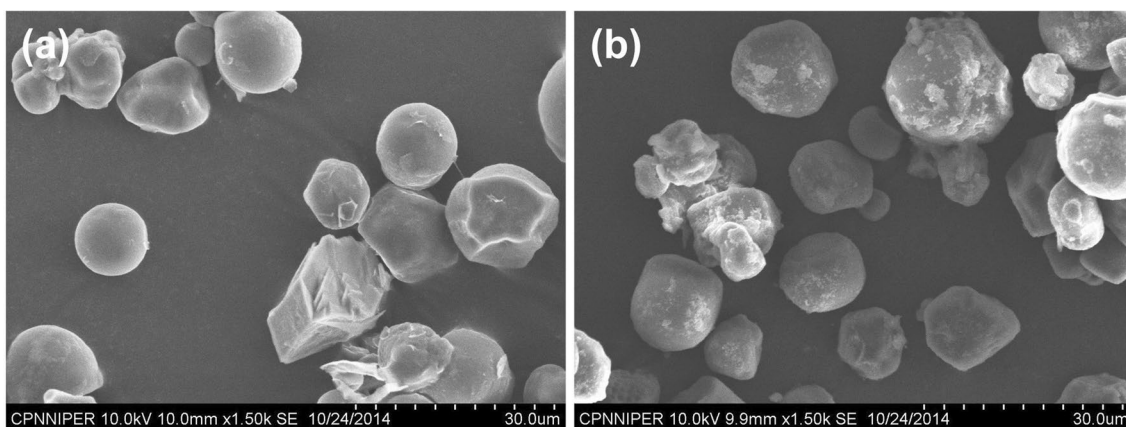


Fig. 1 SEM images of **a** SGS and **b** SMS

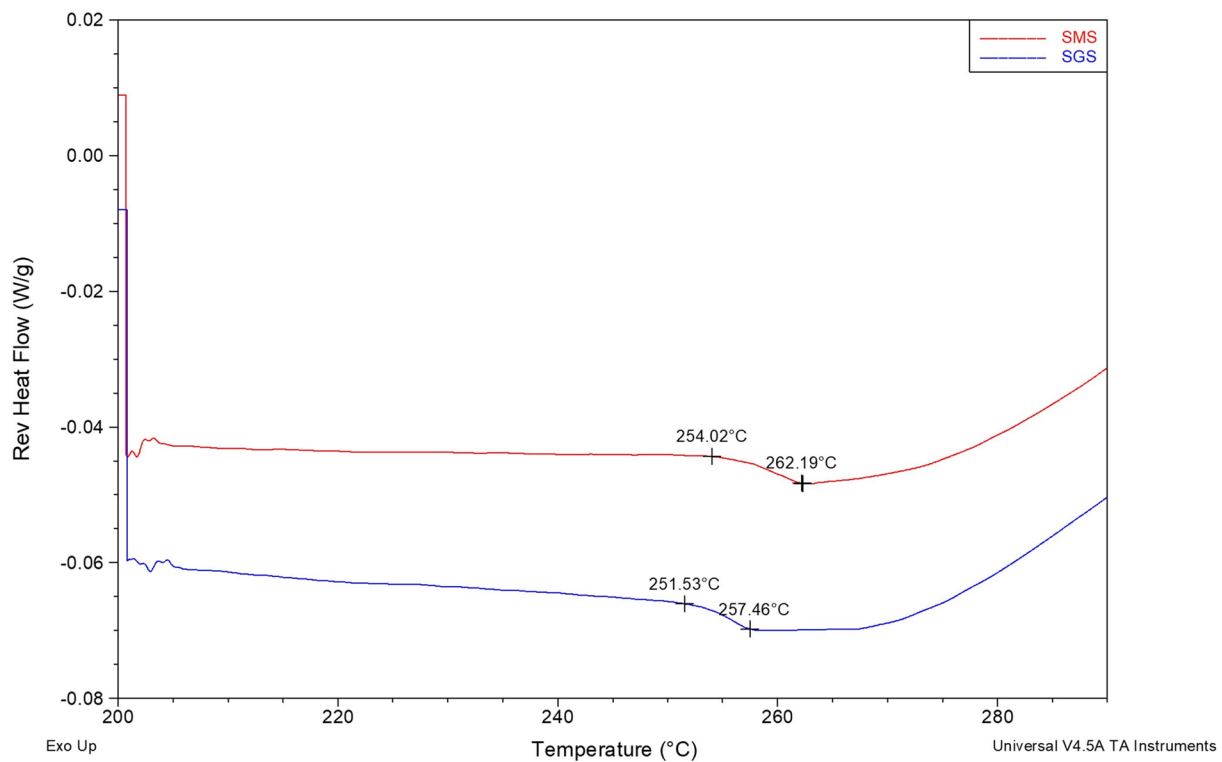


Fig. 2 DSC overlay of SGS and SMS

Table 2 Powder properties of SGS and SMS

| Material | AR (°) | BD (g/mL) | TD (g/mL) | PD (g/mL) | CI (%) | HR | SI (%) |
|----------|------------|-------------|-------------|-------------|-------------|-------------|--------------|
| SGS | 21.6 (0.3) | 0.48 (0.01) | 0.57 (0.02) | 1.45 (0.02) | 14.4 (4.53) | 1.17 (0.06) | 10.15 (1.49) |
| SMS | 22.1 (0.2) | 0.54 (0.02) | 0.67 (0) | 1.43 (0.03) | 19.6 (2.53) | 1.24 (0.04) | 45.69 (1.94) |

AR angle of repose; BD bulk density; TD tapped density; PD particle (true) density; CI Carr’s index; HR Hausner’s ratio; SI Swelling index

Table 3 Heckel and Walker parameters for SGS and SMS

| Material | P_y | D_A | D_0 | D_B | W' |
|----------|--------|-------|-------|-------|-------|
| SGS | 200 | 0.745 | 0.393 | 0.352 | 29.64 |
| SMS | 128.21 | 0.614 | 0.469 | 0.145 | 41.04 |

porosity for both materials as the compression pressure increases. Lower levels of porosity were obtained for SGS at pressures ranging from 35–150 MPa but beyond 150 MPa, lower levels were obtained for SMS corresponding to greater compressibility at higher pressures.

The compactibility plot (Fig. 4b) shows the relationship between tensile strength and porosity of compacts. For both materials, tensile strength increased with decreasing porosity. The tensile strength of SGS compacts were higher at all porosities (0.1–0.4). At porosities below 0.1, tensile strength values of SMS were observed to be higher

than those of SGS. Compacts of SMS produced the lowest porosity value at maximum compaction pressure. The tableting profile for both materials represented by a plot of tensile strength against compression pressure (Fig. 4c) shows that tensile strength increased as the compression pressure increased. Higher tensile strength values were obtained with SGS at low and intermediate pressures. However, a maximum limit was reached for SGS at 200 MPa while the tensile strength of SMS continued to rise with increasing pressure beyond 200 MPa.

The tableting properties of SGS and SMS are summarized in Table 4. The mean weight and thickness parameters of tablets for both materials were similar. There were significant differences in the crushing strength, tensile strength and disintegration time of tablets from both materials at $p < 0.05$. It was observed that SMS produced stronger tablets that disintegrated faster than those of SGS.

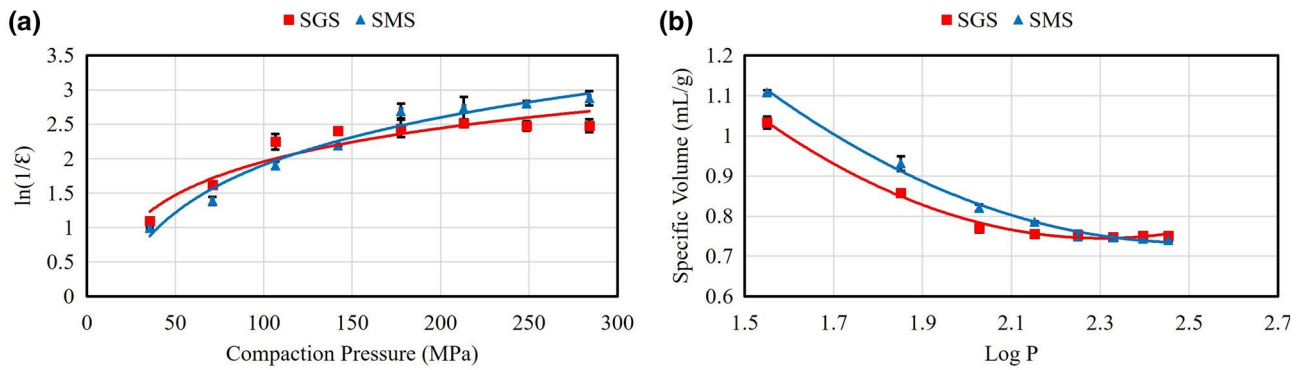


Fig. 3 a Heckel and b Walker plots of SGS and SMS

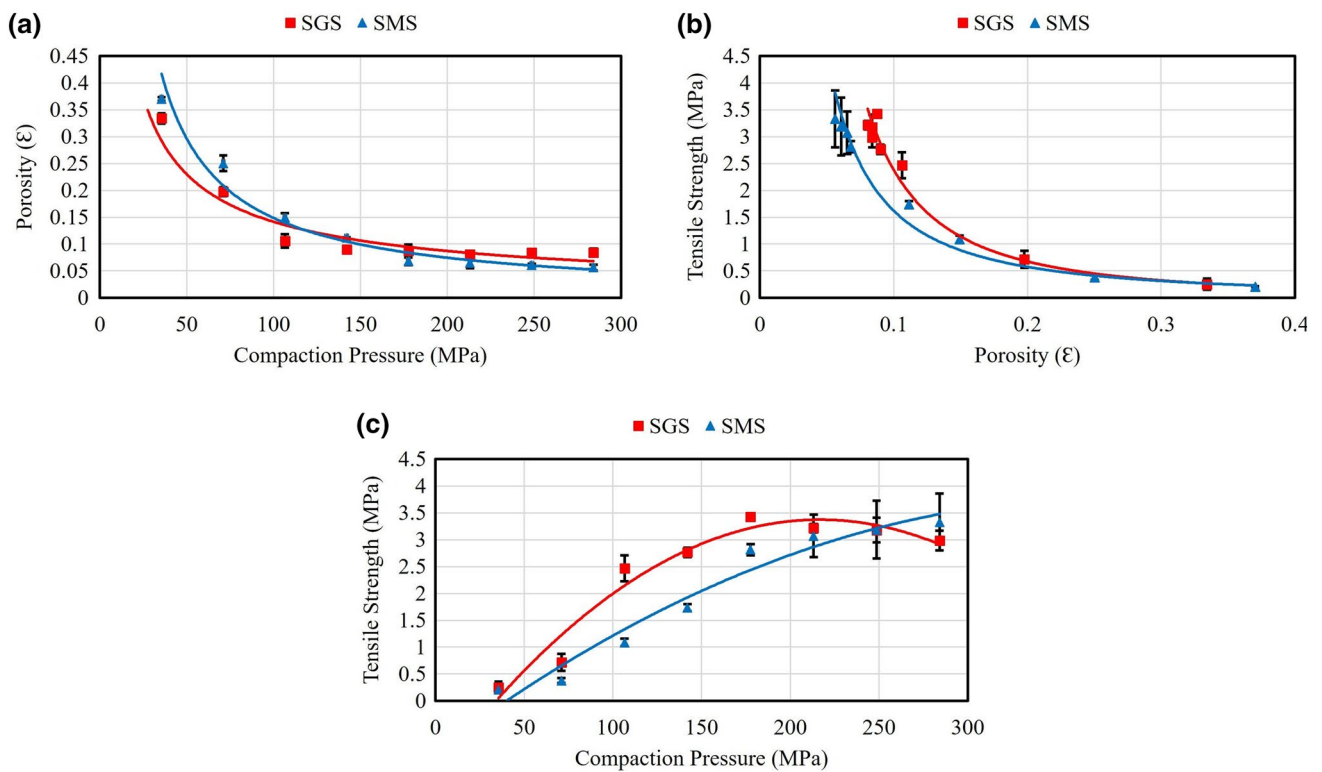


Fig. 4 CTC plots of SGS and SMS. a Compressibility plot, b Compactibility plot and c Tableability plot

Table 4 Physical properties of tablets prepared using SGS and SMS as DC excipients

| Material | Weight (mg) | Thickness (mm) | CS (N) | TS (MPa) | DT (min) | FR (%) | DER | T _{50%} (min) |
|----------|--------------|----------------|------------|------------|------------|-------------|--------|------------------------|
| SGS | 399.7 (4.22) | 3.43(0.03) | 79.38(7.7) | 1.23(0.12) | 0.32(0.04) | 0.57 (0.07) | 435.20 | 5 |
| SMS | 399.4 (6.81) | 3.43(0.05) | 91.5(4.04) | 1.42(0.06) | 0.16(0.03) | 0.59 (0.04) | 969.28 | 4 |

CS Crushing strength; TS Tensile strength; DT Disintegration time; FR Friability; DER Disintegration efficiency ratio; T_{50%} Time taken to attain 50% drug release

The DER for both materials shows that SMS had a much higher value implying a better balance of disintegrating and binding properties. Friability did not differ widely for both materials and the time taken to attain 50% of drug release was faster with SMS compared to SGS. The dissolution plot (Fig. 5) shows a similar release pattern for both materials.

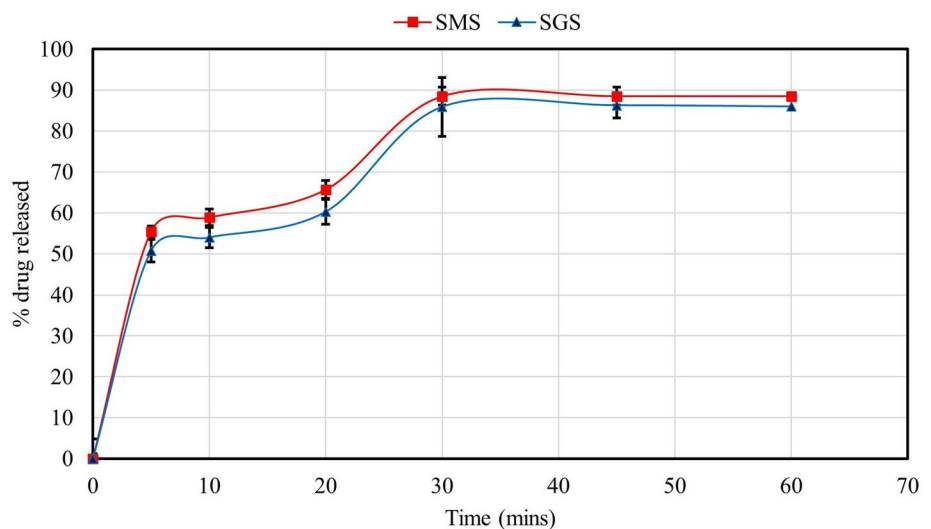
4 Discussion

The principal objective of co-processing is to engineer the functionality of existing excipients for a desired application in solid dosage form development. It is necessary therefore to make rational selection of the interacting excipients that will encapsulate the desired attributes in the composite excipient [3, 22]. In our study, gelatin (GEL) and microcrystalline cellulose (MCC) were chosen as models of wet and dry binders respectively in the preparation of SGS and SMS. One key attribute of co-processed excipients that is modulated during development is the particle size [23, 24] which contributes significantly to the functionality of the co-processed excipient [8, 11]. Bulk properties of flow and compressibility has been enhanced as a result of particle size modification [25, 26]. The difference in particle size observed for SGS and SMS can be attributed to the type and mode of incorporation of the binder during co-processing. Gelatin has been used traditionally as a binding agent in the formulation of tablets by wet granulation [27]. Hence, its propensity to increase particle size significantly was higher due to its agglomerating effect resulting in the cohesion of powder particles by the formation of liquid bridges which led to particle size enlargement [28]. On the other hand, microcrystalline cellulose does not exert that agglomerating effect that

leads to increase in particle size because of its inability to form liquid bridges during processing [1]. As a result, particles of SGS were significantly larger in size than those of SMS. This suggests that the type of binder incorporated in the formulation of co-processed excipients influences to a reasonable degree the particle size of the composite excipient generated.

Co-processing of excipients did not alter significantly the particle shape of the parent excipient, tapioca starch as the particles of SGS and SMS maintained the characteristic spherical shape of tapioca starch [29, 30]. The percentage proportion of the binders (7.5%) employed in this study may not have been sufficient enough to cause a deviation in the sphericity of tapioca starch considering that the particle shapes of gelatin and microcrystalline cellulose are irregular and fibrous respectively [5, 31]. However, there seems to be slight modifications of the surface morphology of SMS as the particles appeared to have what looked like deposits on its surface. This may be ascribed to the presence of colloidal silicon dioxide (CSD) which remained largely on the surface of SMS particles as opposed to the integration of CSD into the particle structure of SGS as a result of the binding effect of gelatin (Fig. 1). The deposits of CSD on the surface of SMS particles may be responsible for the superior swelling action and rapid disintegration time exhibited by SMS. This concurs with the findings of Rojas and Kumar (2011) who related the rapid disintegrating action of silicified microcrystalline cellulose II to the deposition of CSD on the surface of the co-processed excipient resulting in rapid ingress of water and subsequent disintegration (< 2 min). Particle shape has been implicated in the bulk flow of powders as spherical shaped particles tend to flow better due to limited interparticulate friction [32]. The flow properties of SMS and SGS were observed to be excellent flow with respect to the indices

Fig. 5 *In vitro* drug-release profile of SGS and SMS



of angle of repose, Carr's index and Hausner's ratio and this is consistent with their spherical particle shape.

The appearance of a base-line shift in the DSC curves of SGS and SMS corresponds to a glass transition (T_g) event (Fig. 2) and this implies that both materials are predominantly amorphous. Amorphous or glassy polymers do not generally display a sharp melting point; instead, they soften over a wide temperature range. The difference in T_g obtained for both materials though not significant can be attributed to the difference in composition of the co-processed excipients. A lower T_g was obtained for SGS possibly because gelatin degrades at temperatures exceeding 40 °C [33] while microcrystalline cellulose degrades at temperatures exceeding 100 °C. Glass transition temperature (T_g) for linear organic polymers range from -100 to ≥ 300 °C [34]. From a pharmaceutical standpoint, T_g is an important factor for solid dosage forms. For solid dosage forms, amorphous polymers are expected to remain solid at room temperature or at the storage temperature to ensure the stability of the product. The high T_g of both materials will guarantee the stability of products prepared using these materials as excipients. Furthermore, a less crystalline or amorphous polymer is preferred in solid dosage formulations because they facilitate the release of drugs compared to crystalline polymers that impede the release of drugs because they display barrier properties [34].

The flow properties exhibited by both materials confirm the efficacy of co-processing as a particle engineering technique in improving the flow functionality of excipients with poor flowability status. This is in agreement with several other studies carried out that demonstrated improvement in flowability as a result of co-processing [4, 7, 24, 35]. Improvement in powder flow could be attributed to the increase in particle size and the spherical shape recorded for both materials. The ability of powders to flow well during tableting is a necessary requirement for materials that are designed for direct compression because they exclude the processing step of granulation that imparts flowability to the powder blend. Most direct compression formulations usually consist of the excipient in higher proportions (60–95%), hence the ability of this excipient to flow greatly influences the flow behaviour of the powder blend. Enhanced flow of the powder blend will result in tablets with uniform weight and content which conforms to quality attributes of robust tablets. The remarkably higher swelling index for SMS relative to SGS (Table 2) may be associated with the high intra-particulate porosity of microcrystalline cellulose which promotes swelling by means of capillary action [1] coupled with the deposition of CSD on the surface of SMS particles as shown by the SEM image (Fig. 1). On the other hand, the limited swelling profile of SGS could be linked to the formation of a

non-porous gel by gelatin that prevents further uptake of water [5]. Swelling is an established mechanism by which some disintegrants exert their action [36]. Tablets containing SMS were found to disintegrate faster than those containing SGS thereby validating its superior swelling profile.

The ability of a material to form solid compacts or tablets is quantified by its mechanical properties [37]. Mechanical properties of a powder relates to its response to applied pressure during compression [38]. Powders under the effect of an external mechanical stress are subject to either elastic deformation, plastic deformation, viscoelastic deformation, or fragmentation as the main mechanism for deformation [39]. Plastic deformation has been recognized as the most important deformation mechanism that facilitates tablet formation [39]. According to Heckel analysis, materials having a relatively low yield pressure (P_y) undergo a greater degree of plastic deformation during compression. A lower yield pressure was obtained for SMS implying a higher degree of plasticity (Table 3). Plasticity has been associated with a material's ability to undergo irreversible deformation during compression that leads to the formation of permanent bonds that are retained after decompression and elastic recovery during tableting [40]. The low yield pressure recorded for SMS has been linked to the ability of microcrystalline cellulose to undergo plastic deformation during compression due to the presence of slip planes in its micro structure [1]. On the other hand, a higher degree of particle fragmentation (D_b) was recorded for SGS which correlates with the higher yield pressure (P_y) obtained for the same material (Table 2). Materials that have high propensity for particle fragmentation are usually brittle and hard, thereby resisting compression leading to particle breakage and subsequent plastic deformation at higher yield pressures [41]. The higher yield pressure of SGS may be related to the brittle fracture tendency of gelatin [27]. Like the Heckel model, the Walker profile also provides information about the plasticity of a material [42]. The higher the absolute Walker coefficient (W'), the more readily the powder reduces its volume, and therefore the more compressible and plastic it is. The higher W' of SMS shows that it readily undergoes plastic deformation during compression compared to SGS. This is consistent with the findings of Heckel analysis.

Tabletability has been used as a performance indicator to study the compaction behaviour of pharmaceutical powders and is usually defined by the contributing factors of compressibility and compactibility [43]. Compressibility refers to the ability of a material to undergo volume reduction when pressure is applied and can be graphically illustrated as a porosity–pressure relationship [44]. The application of pressure to a powder bed in a confined space initiates particle rearrangement that leads to the filling of the pore spaces, deformation and reduction

in volume thereby increasing the packability and density of the powder [38]. When this happens, particles are brought near each other thereby increasing bonding area. The bonding area–bonding strength model proposed by Sun (2011) provides the correlation to compressibility and compactibility. The minimal difference observed in the compressibility profile of both materials may be attributed to the deformation mechanism exhibited by both materials during compression. Lower porosity levels obtained at higher pressures for SMS demonstrates higher compressibility which is related to its greater degree of plastic deformation as seen in the Heckel analysis. With respect to tableability, compressibility of the material contributes the bonding area over which inter-particulate bonds are generated thus higher compressibility and consequent larger bonding area was obtained for SMS relative to SGS. Compactibility is the ability of a material to form tablets of sufficient tensile strength under the effect of densification and is strongly correlated with the strength of inter-particulate bonds in the compact (bonding strength). The bonding strength of each material increased with decreasing porosity (Fig. 4b); much lower levels of porosity (<0.1) were obtained for SMS giving rise to compacts with higher tensile strength. The higher bonding strength observed with SMS may be linked to a stronger interfacial adhesion occurring during bonding [45]. In addition, the presence of microcrystalline cellulose in the particle structure of SMS could have facilitated the formation of hydrogen bonds between adjacent particles contributing to the higher tensile strength obtained for SMS compacts at lower porosity. Other factors that may have influenced the compactibility of both materials include properties like the particle size and shape [37]. Tableability is basically known as the capacity of a powdered material to be transformed into a tablet of specified strength under the effect of compaction pressure [46]. The differences observed in the tableability profiles of both materials reflected the differences in their compressibility and compactibility profiles. Hence, the tableability of each material was governed by their respective compressibility and compactibility profiles. The continuous rise in tableability of SMS even at pressures beyond 200 MPa implies that bonding area and bonding strength increased with higher loads. Hence, there was reduced tendency for elastic recovery during decompression and after ejection. However, the tableability of SGS was observed to plateau at 200 MPa but weakened at higher pressures possibly due to the phenomenon known as “over compression”. This arises when maximum compressibility has been attained by compaction and further increase in pressure does not lead to an increase in bonding area. If a higher pressure does not result in more plastic deformation, the stored elastic energy would increase because of the additional load applied on the powder as a

result of higher pressure. Elastic recovery of particles during decompression then breaks the bonds and compromises tablet strength. The higher the compaction pressure is, the greater is the deterioration/weakening of tableability, because of the more significant elastic recovery [45].

The differences recorded in the tableting profile of SGS and SMS with respect to the crushing strength and disintegration time can be attributed to the material attributes of both excipients. Due to the high degree of plasticity observed with SMS, tablets containing SMS were observed to have higher crushing strength due to superior bonding area and bonding strength developed during compression. However, disintegration of the tablets (containing SMS) was faster and this correlates with its high swelling capacity which was about 4 times more than that of SGS. Higher values of DER for SMS implies that a better balance of mechanical and disintegrating properties was attained. Hence, the use of SMS as a directly compressible excipient in tablet formulation will not exert a negative effect on tensile strength or disintegrating profile of the tablets [47]. The two co-processed excipients evaluated showed similarities in the tableting profile and functionality and this is consistent with the requirements for an ideal DC excipient. Differences observed in physical and mechanical properties of the excipients can be ascribed to the incorporation of different binders in their formulation.

5 Conclusion

This study has revealed that the material and tableting properties of the co-processed excipients developed were consistent with the type of binder used in its formulation. Particle size of the co-processed excipients was influenced by the aggregating ability of the binder used in its preparation with SGS containing gelatin as binder giving rise to composite particles with larger particle diameter. The co-processed excipient containing microcrystalline cellulose as binder (SMS) demonstrated a higher degree of plasticity during compaction leading to the formation of tablets with better compactibility and tableability owing to the excellent plastic deformation profile of MCC. Tablets with rapid disintegration time were produced with SMS as a result of the better swelling property of MCC compared to gelatin. The rational selection of a binder in the formulation of co-processed excipient is one critical factor to be considered during its development.

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Conflict of interest On behalf of all authors, the corresponding author states that there is no conflict of interest.

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