




Multiparametric prostate MRI and structured reporting: benefits and challenges in the PI-RADS era

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Abstract

Prostate cancer (PCa) is the second most frequent cancer diagnosis in men and the sixth leading cause of cancer death worldwide with increasing numbers globally. Therefore, differentiated diagnostic imaging and risk-adapted therapeutic approaches are warranted. Multiparametric magnetic resonance imaging (mpMRI) of the prostate supports the diagnosis of PCa and is currently the leading imaging modality for PCa detection, characterization, local staging and image-based therapy planning. Due to the combination of different MRI sequences including functional MRI methods such as diffusion-weighted imaging (DWI) and dynamic contrast-enhanced MRI (DCE-MRI), mpMRI enables a high sensitivity and specificity for the detection of PCa. The rising demand for individualized treatment strategies requires methods to ensure reproducibility, completeness, and quality of prostate MRI report data. The PI-RADS (Prostate Imaging Reporting and Data System) 2.1 classification represents the classification system that is internationally recommended for MRI-based evaluation of clinically significant prostate cancer. PI-RADS facilitates clinical decision-making by providing clear reporting parameters based on clinical evidence and expert consensus. Combined with software-based solutions, structured radiology reports form the backbone to integrate results from radiomics analyses or AI-applications into radiological reports and vice versa. This review provides an overview of imaging methods for PCa detection and local staging while placing special emphasis on mpMRI of the prostate. Furthermore, the article highlights the benefits of software-based structured PCa reporting solutions implementing PI-RADS 2.1 for the integration of structured data into decision support systems, thereby paving the way for workflow automation in radiology.

Keywords Prostate cancer · Multiparametric magnetic resonance imaging · Structured reporting · PI-RADS · Radiomics

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Abbreviations

ADC	Apparent diffusion coefficient
AFS	Anterior fibromuscular stroma
AI	Artificial intelligence
AUC	Area under the curve
BCR	Biochemical recurrence
BPH	Benign prostate hyperplasia
CDSS	Clinical decision support systems
CT	Computed tomography
DCE	Dynamic contrast-enhanced
DRE	Digital rectal examination
DWI	Diffusion-weighted imaging
EPE	Extraprostatic extension
MDSS	Multifactorial decision support system
MpMRI	Multiparametric MRI
MRS	MR spectroscopy
PCa	Prostate cancer

PI-RADS	Prostate imaging reporting and data system
PSA	Prostate-specific antigen
PSAD	Prostate-specific antigen density
PSMA	Prostate-specific membrane antigen
PZ	Peripheral zone
SVI	Seminal vesicle invasion
SVM	Support vector machine
TRUS	Transrectal ultrasound
TURP	Transurethral resection of the prostate
T2w	T2-weighted
TZ	Transition zone

Introduction

Prostate cancer (PCa) is the most commonly diagnosed cancer type in men in the Western world [1], imposing specific requirements for prostate imaging which are essential for the development of risk-adapted therapy approaches. Application of PSA testing in early PCa diagnosis has led to the detection of an increasing number of prognostically favorable cases with low-tumor stages [1]. Nevertheless, there is still a considerable number of highly aggressive primary tumors with possible extraprostatic extension (EPE) and lymph node (LN) or bone/distant metastases in the early stages of the disease.

In the past, the usage of MRI in PCa diagnosis has been limited. Its primary use was restricted to patients with PCa as an abdominal staging test, and for the evaluation of EPE. Despite adequate anatomic evaluation using morphological MRI sequences, especially for EPE detection in T2-weighted imaging (T2w), MRI showed suboptimal potential for the detection of clinically insignificant PCa [2].

However, the role of MRI in PCa diagnosis has evolved in the last decade: with the addition of novel imaging sequences, such as dynamic contrast-enhanced MRI (DCE), diffusion-weighted imaging (DWI), and MR spectroscopy (MRS), functional information was added to the anatomical image data provided by T2w. Therefore, mpMRI was established as a principle non-invasive imaging technique to support PCa diagnosis, characterization, surveillance, and biopsy guidance. The implementation of a multiparametric MRI protocol led to a migration of PCa detection into earlier stages of the disease providing additional information about tumor aggressiveness in addition to anatomical information [3].

Within this article, a detailed overview of appropriate PCa detection, structured reporting, and subsequent PCa analysis focusing on an MRI-guided pathway within the course of the disease is given. We discuss the added diagnostic value and clinical significance of mpMRI of the prostate in combination with structured reporting according to the PI-RADS v2.1 classification that, in combination

with radiomics analyses, forms the basis for the prospective implementation of artificial intelligence (AI) into the clinical reporting workflow.

Imaging methods for prostate cancer detection

TNM classification and tumor staging

TNM classification of PCa is based on the current UICC classification [4, 5]. The tumor stages T1–2 N0 M0 describe locally confined PCa, whereas locally advanced PCa encompasses the stages T3–4 N0/+ and M0. Therefore, locally advanced PCa includes tumors that extend the prostate capsule (T3a), infiltrate the seminal vesicles (T3b) or neighboring structures (e.g., rectum and urinary bladder, T4), or expansions as locoregional LN metastases (N+) without distant metastases. Higher Gleason score distribution, a higher proportion of clinical T2 disease (or higher), as well as extraprostatic extension (EPE) and the incidence of perineural invasion are associated with positive surgical resection margins and thus, higher biochemical recurrence rates (BCR) with a worse prognosis, respectively [6]. Within a prospective study investigating 1308 PCa patients, multivariate Cox's proportional hazards regression analysis clearly outlined T3 stages (with presence of ECE) as an independent pathological risk factor for BCR prediction in comparison to pathological T2 stages ($p < 0.001$) [6].

Clinical practice guidelines propose using the results obtained during primary diagnosis to determine local tumor extent (T stage). The currently used clinical terminology suggests a differentiation between “locally confined” and “locally advanced” PCa generally referring to DRE without specifying further conditions. Due to increasingly improved therapeutic strategies, medical imaging is of high relevance for the detection of primary PCa as well as for staging of locally advanced PCa considering the presence of EPE, potential lymphogenic or bone/distant metastases [7]. Different approaches for the determination of local tumor extent and the identification of distant metastases exist within the clinical workflow. In addition to DRE and PSA testing, non-invasive imaging techniques such as TRUS, CT, mpMRI are used. Besides that, positron emission tomography (PET)—ideally in combination with CT (PET/CT) and mpMRI—can be applied. After bioptic detection of tumor tissue, metastases can be diagnosed through bone scintigraphy, which should be performed in symptomatic patients independent of PSA level, ISUP grade, or clinical stage according to the Guideline Working Panel of the European Association of Urology. In addition, PET/CT has gained increasing clinical relevance because of its added diagnostic value to detect BCR, either as local tumor recurrence or with presence of

LN or bone metastases [8, 9]. Gupta et al. demonstrated a superior diagnostic accuracy for the detection of lymph node metastases using ^{68}Ga -PSMA PET-CT in comparison to mpMRI with 95.1% vs. 90.5%, respectively ($p = 0.001$) [9].

Transrectal ultrasonography (TRUS)

TRUS is used to determine prostate volume and is applied as a first diagnostic test in patients with increased PSA levels to explore PCa localization in addition to its guiding function for systematic or targeted punch biopsies when PCa is suspected. In prior studies, the diagnostic accuracy to localize PCa was rated significantly inferior in comparison to more advanced imaging modalities such as MRI [10, 11]. A retrospective study of 90 PCa patients demonstrated a significantly higher diagnostic accuracy to detect and especially localize PCa using mpMRI in comparison to TRUS biopsy within the base (AUC 0.81 vs. 0.61), mid gland (0.75 vs. 0.68), and apex (0.70 vs. 0.67) in a mixed model analysis ($p < 0.0001$) [11].

A high proportion of PCa cannot be detected sufficiently through TRUS due to their heterogeneous appearance, with isoechoic tumors being the most common form on ultrasound imaging. For this reason—and to increase diagnostic accuracy—10 to 12, systematic core biopsies are considered as standard-of-care, and are recommended by the Guideline Working Panel of the European Association of Urology (EAU) [10, 12]. The probability of malignancy for a suspicious lesion detected by TRUS varies between 17 and 57% [13]. Despite these benefits, complications of TRUS-guided prostate biopsies should not be neglected. While the risk for rectal bleeding ranges from 1.3 to 5.8%, inflammation occurs in up to 4% of patients [12]. Although TRUS enables a volumetric characterization of the prostate as well as the assessment of EPE in some cases, TRUS is not recommended as a staging method for locally advanced PCa by the EAU [10].

Multiparametric magnetic resonance imaging (mpMRI)

MpMRI describes the combination of anatomic and functional sequences in MRI and is nowadays mainly composed of morphological T2w imaging, DWI, and DCE imaging (i.e., dynamic contrast-enhanced MRI) [14]. The diagnostic value for PCa detection lies in the variety of possible image contrasts that allow structural imaging and (functional) assessment of healthy and pathologically altered tissue. High-resolution T2w sequences allow the most accurate visualization of the zonal prostate anatomy, the capsule, and assessment of local tumor extension. For the detection of EPE, including seminal vesical invasion (SVI) and infiltration of the neurovascular bundles, T2w imaging achieves a diagnostic accuracy for the detection of

EPE of up to 0.74 [15, 16]. The detection rate of PCa using T2w sequences is impaired by signal intensity changes based on post-inflammatory, post-therapeutic, and atrophic tissue changes, particularly in the peripheral zone (e.g., in the context of chronic prostatitis). Overall, morphologic T2w sequences are sensitive (ranging from 88 to 91% depending on the study) but not specific (ranging from 61 to 67%) for the detection of prostate cancer [14, 17, 18]. Combining different MRI techniques including functional MRI methods, DCE-MRI, and DWI leads to higher sensitivity and specificity for the detection of PCa [19–21].

DWI is based on the motility of water molecules within the tissue. Due to the high cell density of tumor tissue, the motility of water molecules is impaired, which enables the differentiation between tumor and normal tissue using DWI. The extent of impaired diffusion can be quantified via apparent diffusion coefficient (ADC) maps (Fig. 1). Thereby, the degree of diffusion restriction allows a qualitative and quantitative assessment of the aggressiveness and clinical significance of PCa. Nowak et al. demonstrated that ADC measures achieved AUC values of up to 78.9% for discriminating between lesions with Gleason scores < 7 vs. Gleason scores ≥ 7 [21].

DCE-MRI (perfusion imaging) consists of multiple fast T1-weighted (T1w) sequences after a bolus injection of gadolinium-based contrast media. Perfusion imaging allows the examination of contrast agent accumulation within specific areas of the prostate. Perfusion depends on the characteristics of small vessels in the tissue. Since the formation of new vessels (neovascularization) is a common feature of tumors by which their high nutrient requirements are met, tumor tissues show strong blood circulation in these imaging modalities. Thus, PCa may display an early and strong enhancement as well as a fast wash-out of contrast agents (wash-out phenomenon) compared to benign tissue [22–24].

Currently, mpMRI of the prostate is the leading imaging method for the detection, characterization, and assessment of local tumor extent of PCa. If MRI is applied as a first diagnostic test before TRUS-biopsy, it enables the detection of up to 18% more cases of clinically significant PCa while simultaneously sparing one in four men the primary biopsy [25]. According to the EAU guidelines [7], mpMRI of the prostate is particularly recommended before biopsies in biopsy naïve patients or for patients with prior negative biopsy and consistent suspicion of PCa (Fig. 2). It reaches high diagnostic accuracy in the detection of PCa especially in anterior regions and areas near the apex of the prostate that can be challenging to detect via TRUS or TRUS-guided biopsies since up to 80% of lesions identified in the distal apex were shown to be PCa positive at targeted biopsy and may have been missed on TRUS-guided systematic biopsy only [17, 25].

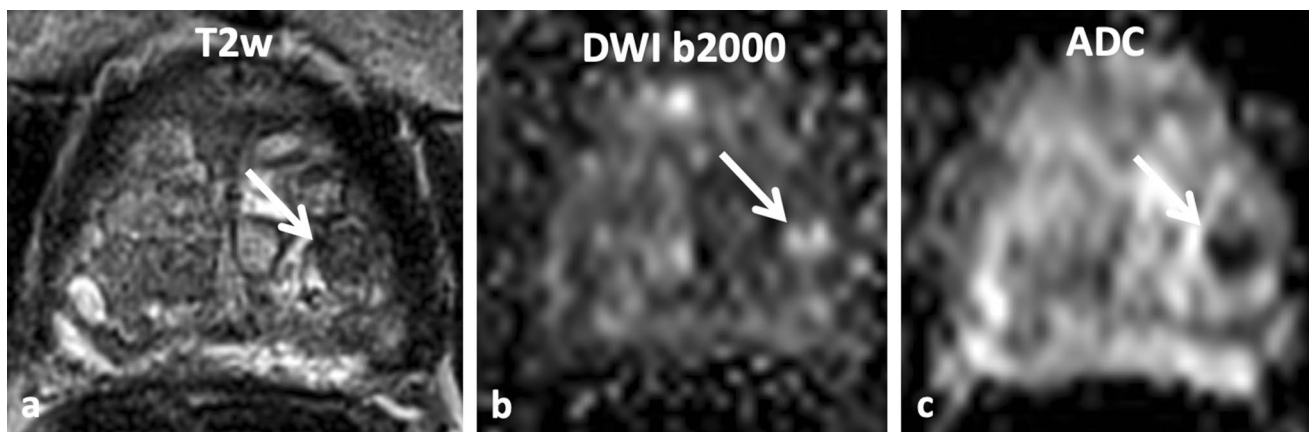


Fig. 1 72-year-old patient with PSA levels of 6.4 ng/ml. **a** T2w-hypointense lesion without complete encapsulation (arrow) consistent with a T2w score of 2 (PI-RADS v2.1). **b, c** The atypical nodular lesion shows strong diffusion restriction including hyperintense signal intensities at high b2000 value images and corresponding low signal

intensities in ADC maps (arrows in **b, c**) consistent with a DWI score of 4 (PI-RADS v2.1). The overall PI-RADS score (v2.1) is 3. MRI ultrasound fusion biopsy of this moderately suspicious prostate lesion reveals an acinar adenocarcinoma (Gleason 4+3=7b, ISUP grade 3)

Local tumor staging using mpMRI

MpMRI is the gold standard for local T-staging of PCa [17]. It is superior to common methods like TRUS and DRE for the assessment of local tumor extent and EPE [18, 26]. A clear advantage of MRI in comparison to other imaging techniques is the possibility of high-resolution depictions of prostate morphology, its capsule, and its neighboring organs. While the transition zone is predominantly evaluated using T2w imaging, the peripheral zone is predominantly evaluated using DWI according to the PI-RADS v2.1 guideline (Table 1). The tumor stage T2 refers to carcinomas that are restricted to the prostate and do not show signs of EPE (Fig. 3), whereas T3 carcinomas extend beyond the prostate capsule (T3a) or show SVI (T3b), either with continuous tumor spread into the seminal vesicles along the excretory ducts or via secondary invasion of the seminal vesicles after macroscopic EPE [27]. The T4 stage describes a direct tumor infiltration into adjacent organs such as rectum or urinary bladder infiltration.

Although the evaluation of EPE on mpMRI should be interpreted with caution [15], a majority of patients with aggressive tumors, especially intermediate- and high-risk PCa, show a significantly higher risk of capsule infiltration and EPE as assessed within a retrospective study with 1045 PCa patients [16]. Lee et al. evaluated only a limited preoperative staging accuracy of EPE for high pathological stages (\geq T3) with an overall sensitivity and specificity of 52.6% and 82.1%, respectively [16]. Reliable signs of EPE on MRI are the obliteration of the rectoprostatic angle or an infiltration/asymmetry of the neurovascular bundles (T3a). Furthermore, the length of capsular contact has been shown to be more sensitive for the detection of EPE than subjective

assessments [28–30]. Mehralivand et al. reported that curvilinear contact length to the capsule of more than 1.5 cm (EPE grade 1), capsular bulge/irregularity (EPE grade 1), both features together (EPE grade 2) or a frank breach of the prostatic capsule with or without invasion of adjacent structures (EPE grade 3) are associated with a higher risk of pathologically confirmed EPE: grade 1 with 24.3%, grade 2 with 38.2%, grade 3 with 66.1%, respectively [28]. EPE of the tumor at the prostate apex with infiltration of the urethral sphincter can also be assessed and is of high clinical relevance since infiltration of the urethral sphincter can lead to urinary incontinence after radical prostatectomy [31].

Assessment of EPE through mpMRI by an experienced radiologist has a negative predictive value of 94–96% and a positive predictive value of up to 79% [32–36]. Although a majority of recent studies suggests only moderate sensitivities of 49–57% for the detection of EPE, mpMRI demonstrated very high specificities of 74–91% [16, 37, 38]. Sensitivity and specificity for the detection of SVI are comparable with 44% and 95%, respectively [16]. MRI-based assessment of EPE in the tumor stage pT3 is impaired when no macroscopic signs of periprostatic fat infiltration or obliteration of the rectoprostatic angle are present [39]. Another reason for the low sensitivity of different imaging approaches to detect EPE is the lack of visualization methods of initial microscopic extracapsular extension. Jager et al. demonstrated a significant increase in the detection rate of EPEs from 14 to 100% depending on the infiltration depth into the extraprostatic fat (< 1 mm vs. > 3 mm) [40].

LN metastases are present in up to 60% of patients with locally advanced prostate cancer. However, a meta-analysis of 24 studies [41] demonstrated only a poor sensitivity of 32% (22–56%) and a moderate specificity of 82%

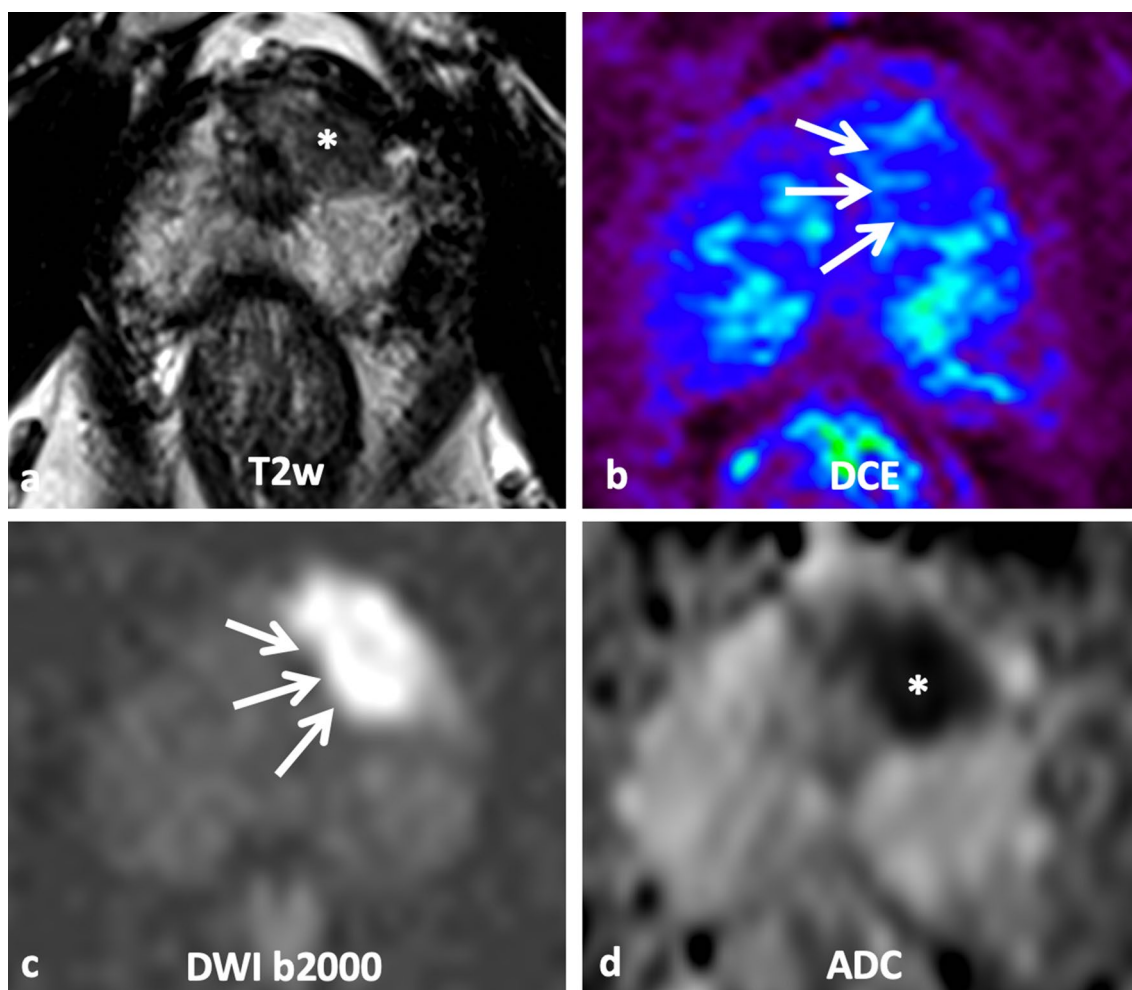


Fig. 2 Prostate cancer in a 54-year-old patient following two consecutive negative TRUS biopsies. **a** Axial T2w and **c, d** DWI/ADC images: the tumor (* or arrows), scored as PI-RADS 5 lesion, is localized within the left anterior peripheral zone (PZa) of the apex and shows focal T2w-signal hypointensity with strong diffusion

restriction **b** DCE imaging does; however, not exhibit suspicious enhancement dynamics (DCE–). Targeted MRI ultrasound fusion biopsy revealed an acinar adenocarcinoma (Gleason score 4+5=9, ISUP grade 5)

(79–83%) for the detection of locoregional LN metastases through mpMRI. Similarly, contrast-enhanced CT showed a poor sensitivity of up to 42% and a specificity of up to 82% for the detection of locoregional LN metastases [41]. In contrast, PET/CT, ideally conducted as PSMA-PET/CT, represents one of the most sensitive imaging modalities for the detection of LN (and distant) metastases and is most commonly applied for the post-treatment setting [10, 42]. As highlighted in a recent meta-analysis, PSMA-PET/CT demonstrates a high sensitivity and high specificity of up to 77% and 97% for advanced PCa detection in a per-patient analysis [43]. Nevertheless, the detection rate for LN metastases through PSMA-PET/CT in a primary staging setting prior to radical prostatectomy also reveals moderate success rates with sensitivities of 33–65% and specificities of 98–100%, respectively [44].

MRI-guided fusion biopsy

Ideally, prostate biopsies detect clinically significant PCa while sparing non-relevant, indolent tumors. Under the current standard-of-care, tissue cores are obtained in a systematic manner through TRUS-guided biopsies, a technique first described by Hodge et al. [45]. However, it was shown to suffer from both poor sensitivity and specificity as a standalone diagnostic test for clinically significant PCa [25, 46, 47]. Within the PROMIS trial, mpMRI was more accurate than TRUS-biopsy in terms of both sensitivity (93% vs. 48%) and negative predictive value (89% vs. 74%) for the detection of clinically significant prostate cancer ($p < 0.0001$) [25].

By combining mpMRI with ultrasound methods as targeted fusion biopsies, these deficits have been overcome

Table 1 Summary of differences in lesion scoring for PI-RADS v2.1 (2019) vs. PI-RADS v2.0 (2015) for the assessment of clinically significant prostate cancer

	Score	PI-RADS v2.1	PI-RADS v2.0
T2WI:transitional zone	1	Normal appearing TZ (rare) or a round, completely encapsulated nodule (“typical nodule”)	Homogeneous intermediate signal intensity (normal)
	2	A mostly encapsulated nodule or a homogeneous circumscribed nodule without encapsulation (“atypical nodule”) or homogeneous mildly hypointense area between nodules	Circumscribed hypointense or heterogeneous encapsulated nodule(s) (BPH)
	3	Heterogeneous signal intensity with obscured margins; includes others that do not qualify as 2, 4 or 5	
	4	Lenticular or non-circumscribed, homogeneous, moderately hypointense and < 1.5 cm in greatest dimension	
	5	Lenticular or non-circumscribed, homogeneous, moderately hypointense and ≥ 1.5 cm in greatest dimension or definite extraprostatic extension/invasive behavior	
T2WI:peripheral zone	1	Uniform hyperintense signal intensity (normal)	
	2	Linear or wedge-shaped hypointensity or diffuse mild hypointensity, usually indistinct margin	
	3	Heterogeneous signal intensity or Non-circumscribed rounded, moderate hypointensity; includes others that do not qualify as 2, 4 or 5	
	4	Circumscribed, homogeneous moderate hypointense focus/mass confined to prostate and < 1.5 cm in greatest dimension	
	5	Circumscribed, homogeneous moderate hypointense focus/mass confined to prostate and ≥ 1.5 cm in greatest dimension or definite extraprostatic extension/invasive behavior	
DWI: peripheral zone or transitional zone	1	No abnormality on ADC, high <i>b</i> value DWI	
	2	Linear/wedge-shaped hypointense on ADC and/or Linear/wedge-shaped hyperintense on high <i>b</i> value DWI	Indistinct hypointense on ADC
	3	Focal (discrete and different from the background) hypointense on ADC and/or Focal hyperintense on high <i>b</i> value DWI May be markedly hypointense on ADC or markedly hyperintense on high <i>b</i> value DWI, but not both	Focal mildly/moderately hypointense on ADC and Isointense/mildly hyperintense on high <i>b</i> value DWI
	4	Focal markedly hypointense on ADC and Markedly hyperintense on high <i>b</i> value DWI < 1.5 cm in greatest dimension	
	5	Focal markedly hypointense on ADC and Markedly hyperintense on high <i>b</i> value DWI ≥ 1.5 cm in greatest dimension or definite extraprostatic extension/invasive behavior	

Table 1 (continued)

	Score	PI-RADS v2.1	PI-RADS v2.0
DCE-MRI: peripheral zone or transitional zone	+	Focal, and earlier than or contemporaneously with enhancement of adjacent normal prostatic tissues and corresponds to suspicious finding on T2w and/or DWI	
	–	No early or contemporaneous enhancement or Diffuse multifocal enhancement not corresponding to a focal finding on T2w and/or DWI or Focal enhancement corresponding to a lesion demonstrating features of BPH on T2w (including features of extruded BPH in the PZ)	No early enhancement or Diffuse enhancement not corresponding to a focal finding on T2w and/or DWI or Focal enhancement corresponding to a lesion demonstrating features of BPH on T2w

recently. In addition to implementing a triage test that increases diagnostic accuracy of PCa detection, mpMRI allows to perform mapped and targeted fusion biopsies of suspicious index lesions in addition to systematic but blind samplings [48, 49]. As demonstrated in recent trials, MRI-TRUS fusion biopsies may prevent up to 27% of patients from unnecessary biopsies when compared to systematic TRUS-guided biopsies [25]. Kasivisvanathan et al. demonstrated that the detection rate of clinically significant PCa can be increased with use of targeted biopsies in comparison to standard TRUS-guided biopsies (38% vs. 26%; $p = 0.005$) while simultaneously reducing overdiagnosis of clinically insignificant cases (9% vs. 22%; $p < 0.001$) [47].

Diagnostic accuracy of mpMRI can be further improved by including additional clinical parameters such as PI-RADS, PSA, prostate volume, age, and DRE results [50]. For instance, performing systematic TRUS-guided biopsies in men with PI-RADS category 1 or 2 will on average detect 8% of clinically significant PCa cases and at the same time overdiagnose 18% of patients with insignificant PCa [51]. Therefore, two out of three PCa diagnoses would lead to overtreatment and potential risk of increased patient morbidity. Diagnostic yields for significant PCa increase with higher PI-RADS categories growing from 12 to 21% over 39–48% to 72–73% for PI-RADS categories 3, 4, and 5, respectively [52, 53]. In case of MRI-guided fusion biopsies, these favorable diagnostic results for PI-RADS categories > 3 are further emphasized even when performing targeted biopsies alone, as this was the case for the above-mentioned Precision trial (with 12% increased detection rates for significant PCa and 13% decreased diagnosis of indolent, non-significant tumors) [47]. While some studies suggest that targeted biopsies alone will overlook up to 18% of cases of clinically significant tumors which would have been detected in systematic TRUS-guided biopsies, most of

these additional tumors are often found in sextants adjacent to the lesion identified by mpMRI indicating that factors such as inaccurate sampling and tumor heterogeneity should be taken into account [49, 51]. In conclusion, evidence is accumulating for multiple benefits of MRI-guided biopsy approaches compared to TRUS-guided biopsies as the standard-of-care. Especially in combination with radiological expertise reflected by structured reporting systems—such as PI-RADS—mpMRI and targeted biopsies do not only perform with significantly increased sensitivity and specificity for the detection of clinically significant PCa, but also reduce the number of men who need to undergo primary biopsies altogether.

Structured reporting and radiomics analysis of prostate cancer

Report standardization

The written radiology report is the most common method of communication between radiologists and their stakeholders, who rely on a report with information that will enable clinical decision-making. However, recent studies show gaps in medical imaging report completeness, yet a good quality report is essential for patient care. According to the Institute of Medicine, quality of care can be defined as the degree to which health services for individuals and populations increase the likelihood of desired health outcomes [54]. The radiological report has an impact on all quality dimensions, especially on appropriateness, efficiency, safety, and patient-centered care. A standardized way to communicate reporting results is important to avoid miscommunication, which can be caused by insufficient clinical information provided by the referring physician or a lack of feedback on the

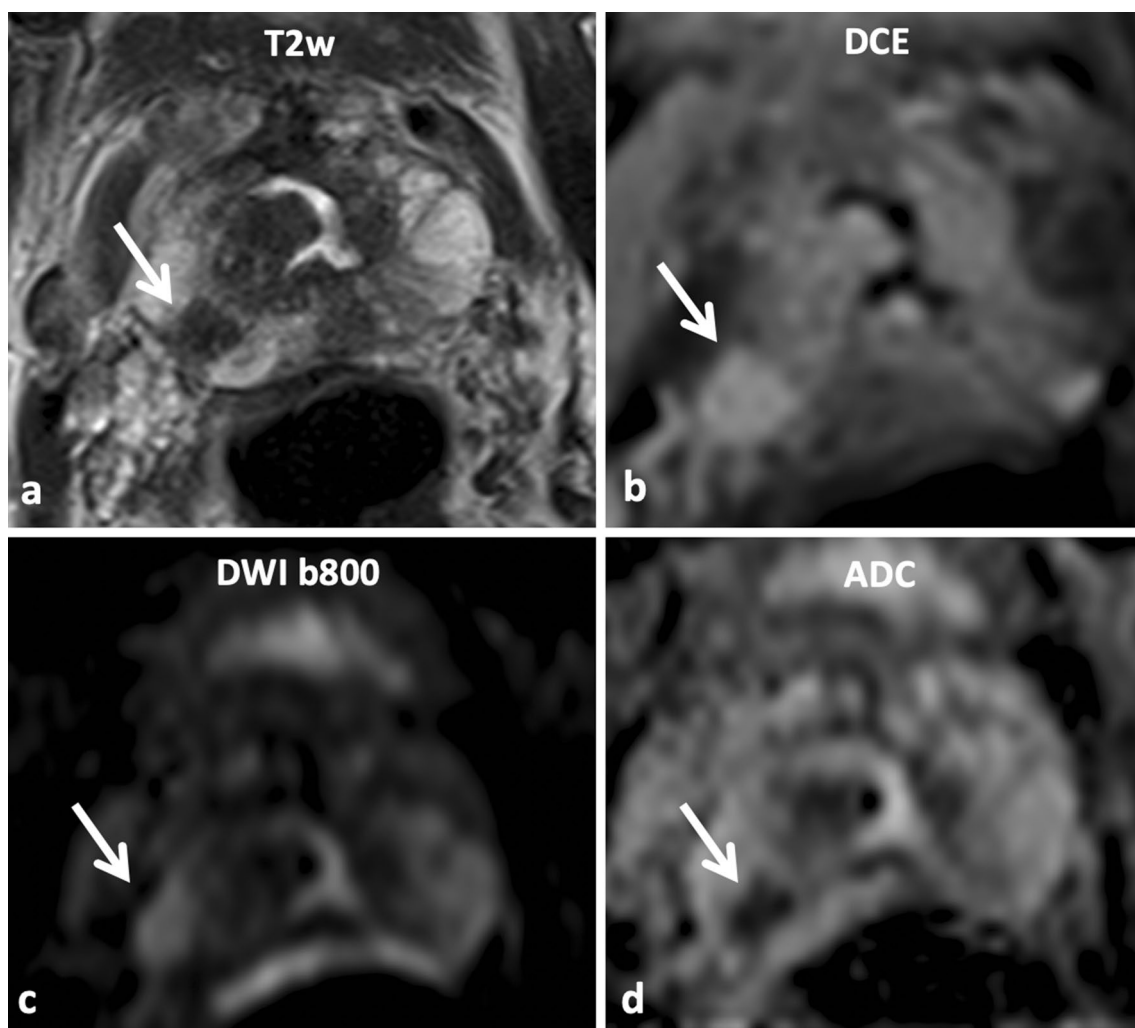


Fig. 3 Prostate cancer in a 78-year-old patient after transurethral resection of the prostate (TURP) and PSA level of 6.3 ng/ml. **a** Axial T2w sequence. The tumor is located on the right side within the PZ (mid gland, arrow). **b** DCE reveals strong early enhancement. **c** DWI ($b=800$) and **d** ADC map show significant diffusion restriction. The

lesion has a maximal diameter of 1.0 cm without extracapsular extension revealing an overall PI-RADS score of 4 (v2.1, 2019). MRI ultrasound fusion biopsy demonstrates an acinar adenocarcinoma (Gleason score $4+4=8$, ISUP grade 4)

examination requisition. Structured reporting has developed as a possible solution which narrows the communication quality gap in medicine through standardized integration of feedback into the communication process.

Synoptic reporting depicts the most advanced form of structured reporting since it incorporates discrete fields and fully analyzable data based on radiological ontologies, which in return increase the reproducibility, completeness, and quality of report data for analyses. In a recent survey, > 90% of radiologists and urologists preferred verbal descriptions of confidence levels and structured prostate MRI reports over free text [55]. Furthermore, structured reporting templates improved the sensitivity of prostate MRI for clinically significant PCa in the peripheral zone (PZ) from 53 to 70% [56]. Published documented benefits of structured prostate

MRI reporting include increased perceived clinical impact of report, improved reproducibility, and improved communication [57, 58]. As such, the use of a specified lexicon to convey ideas such as levels of confidence in the diagnosis of EPE may improve communication and help referring clinicians [59]. Structured reporting encompasses qualitative descriptors based on expertise and has become a priority for many radiological societies, including the European Society of Radiology, the Radiological Society of North America (RSNA), and other organizations such as Cancer Care Ontario [60].

As an example, the RSNA provides RadReport as a web-based reporting application [61] including a prostate MRI reporting template which was constructed based on surveys of radiologists and urologists. For prostate MRI, the

majority of surveyed radiologists indicated that contrast dose and type, magnetic field strength, coil type, and any medications administered describe essential report components [55, 62]. While these kinds of web-based applications do extract advantages from structured reporting, their restricted integration into existing radiological application systems and missing integration into the workflow at all limits their added value. Additionally, a variety of report solutions vary significantly in levels of complexity and content, rendering them unsuitable for synoptic reporting.

Synoptic reporting requires a solution that enables the integration of structural decision trees based on the input of various stakeholders. By combining structural decision trees with reporting systems, such as PI-RADS, successful communication during the clinical decision-making process can be achieved. Another example of structured radiology reporting are web-based software tools, which interactively transform radiological and clinical findings into structural decision trees (Figs. 4 and 5); therefore, providing the necessary infrastructure for process automation to be integrated into the routine workflow. Along with the improved accessibility and evaluability of clinical data, this facilitates the deployment of radiomics and artificial intelligence to support clinical decision-making [3]. However, successful implementation of advanced software applications requires distinct technical set-ups which cannot be provided in all clinical settings.

PI-RADS version 2.1

With the rise of MRI usage in PCa diagnosis, characterization, and monitoring, the need for standardized reporting has dramatically increased over the last decade. To address this issue, the European Society of Urogenital Radiology (ESUR) induced the initiative for PI-RADS v1 in 2012, a major structured reporting system for prostate mpMRI preferred by over 80% of radiologists and urologists [55, 63]. Over the last years, PI-RADS evolved to decrease complexity within the scoring system, define minimum technical parameters for improved result comparability, decrease variability in score interpretations, and augment sensitivity and specificity for the detection of clinically significant PCa.

PI-RADS generates a score from 1 to 5, ranging from very low to very high probability of clinically significant PCa (Fig. 6). In spring 2019, the revised PI-RADS version 2.1 was introduced to resolve limitations which were identified in the previous PI-RADS versions (see Fig. 6 for the summarized PI-RADS v2.1 algorithm). One major focus for the changes of PI-RADS v2.0 to v2.1 lays in adapted diagnostic criteria for lesions in the transition zone (TZ) of the prostate, particularly affecting the assessment of PI-RADS category 1–3 lesions (Table 1). While PI-RADS v2.0 was able to enhance its accuracy from 81 to 93% and

its sensitivity from 76 to 96% for TZ lesions compared to PI-RADS v1 [64], diagnosis of TZ lesions remained challenging compared to lesions within the PZ (Table 1). Therefore, more detailed criteria for nodules within the TZ were introduced in PI-RADS v2.1 leading to improved diagnostic accuracy and reduced interpretation variabilities in this area [3]. For instance, nodules commonly associated with age-related benign prostatic hyperplasia (BPH) were previously assigned as PI-RADS category 2 lesions, whereas PI-RADS v2.1 now classifies these nodules into PI-RADS category 1 on T2w imaging (Fig. 7a). In addition, PI-RADS v2.1 places special emphasis on DWI scoring to increase the overall PI-RADS category, in particular for the lower T2w imaging categories PI-RADS 2 (Fig. 7b) and PI-RADS 3 (Fig. 6 and Table 1) [3]. PI-RADS v2.0 enabled the upgrade of a T2w PI-RADS 3 lesion to a PI-RADS 4 lesion in case of a DWI PI-RADS category of 5. With PI-RADS v2.1, DWI now has the added ability to upgrade a TZ PI-RADS 2 lesion to a PI-RADS 3 lesion in case of a DWI assessment of 4 or 5 [63] (Fig. 1). Following DWI assessment, PZ PI-RADS 3 and 4 lesions may be distinguished utilizing DCE (Fig. 6), which is considered positive if focal early or contemporaneous enhancement is present correlating with a T2 or DWI abnormality (Table 1). In general, an overall suspicion category according to PI-RADS should always be summarized within the radiological report as well as the assignment of a PI-RADS score per lesion. This also accounts for benign focal lesions (such as BPH nodules) as well as for diffuse geographic signal hypointensities which may be classified as (chronic) prostatitis (Fig. 8).

The updated PI-RADS v2.1 classification also includes more information for identifying and classifying cancers in the anterior fibromuscular stroma (AFS) (Fig. 9) as well as in the central zone located as a pyramidal T2 hypointense structure within the prostate base. Especially for these regions, the detection of significant diffusion restriction (ideally using high b values $> 1400 \text{ mm}^2$) as well as suspicious perfusion characteristics of a suspicious lesion on DCE (such as type 2 or type 3 curves) point toward the presence of PCa [63].

A further expansion of PI-RADS v2.1 includes specifications for the use of biparametric MRI over mpMRI, thereby omitting DCE-MRI for selected clinical cases, which provides several benefits: it does not only allow to perform prostate MRI faster and with reduced costs, but also spares the use of contrast agents, thereby avoiding potential gadolinium retentions. However, in some cases, mpMRI is superior to bpMRI due to the improvement of sensitivity provided by DCE-MRI [22–24]. For instance, it was shown that upgrading lesions from PI-RADS category 3 to category 4 based on DCE scores—in this case for PI-RADS v2.0—resulted in an increased detection of lesions with a Gleason score ≥ 7 in up to a third of the patients [24]. Consequently, the PI-RADS

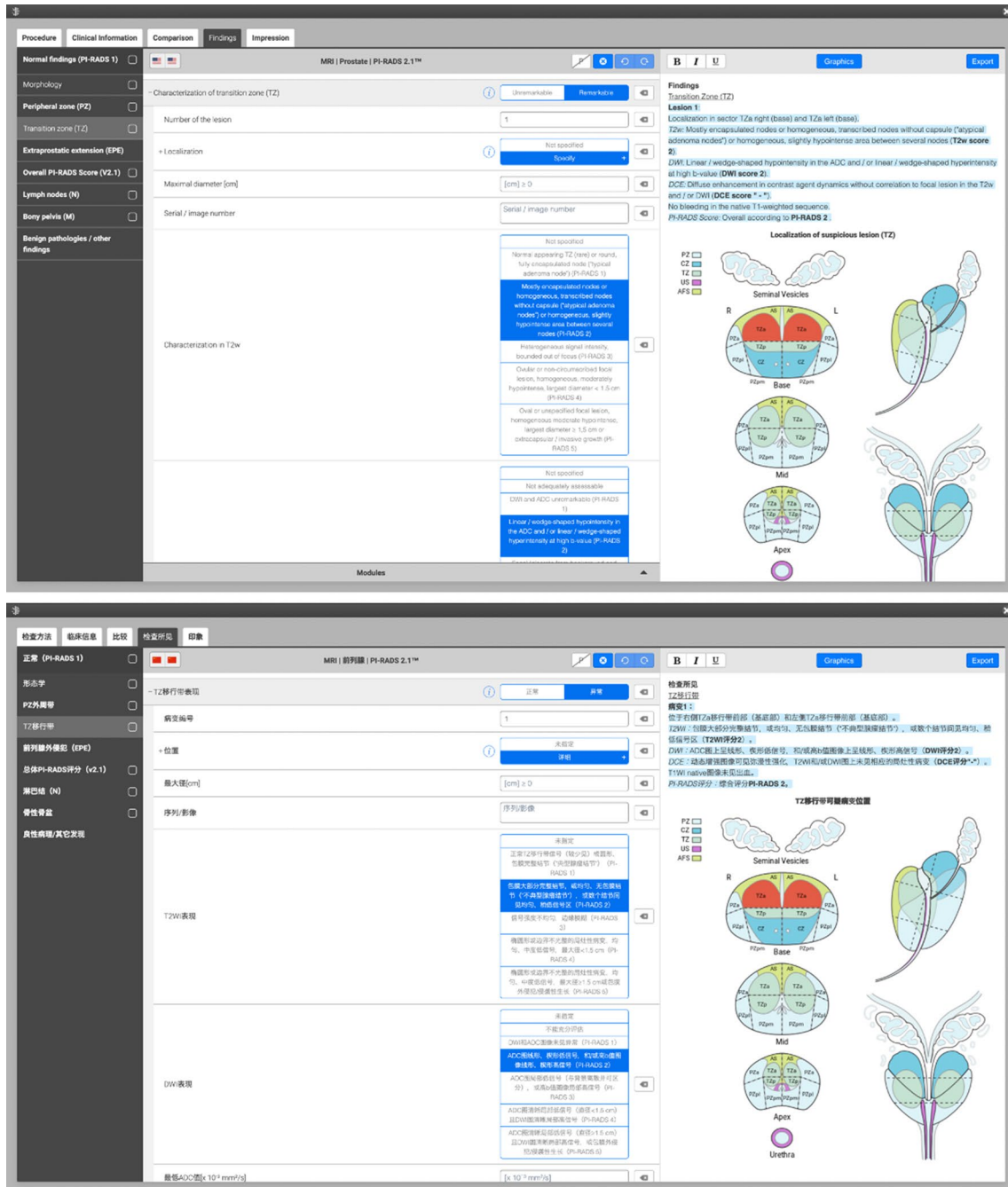


Fig. 4 Structured PI-RADS v2.1 reporting template in English (above) and Chinese (below), exemplarily shown for an interactive web-based software tool which includes a structured decision tree and

automatically generated text output with graphical support to enhance interdisciplinary communication and provide clinical decision support

committee provides five scenarios for which mpMRI should be preferred in comparison to bpMRI:

1. Patients with prior negative biopsies in combination with unexplained raised serum PSA levels and those in active surveillance under evaluation for fast PSA doubling times or changes in clinical/pathological status.

2. Men with persistent suspicion for harboring clinically significant PCa who have undergone a previous, negative bpMRI. In this case, not missing any clinically significant PCa has highest priority.
3. Patients with either prior prostate interventions (e.g., TRUS, BPH therapy, radiotherapy) or with prior drug/hormonal therapies (e.g., testosterone, 5-alpha reduc-

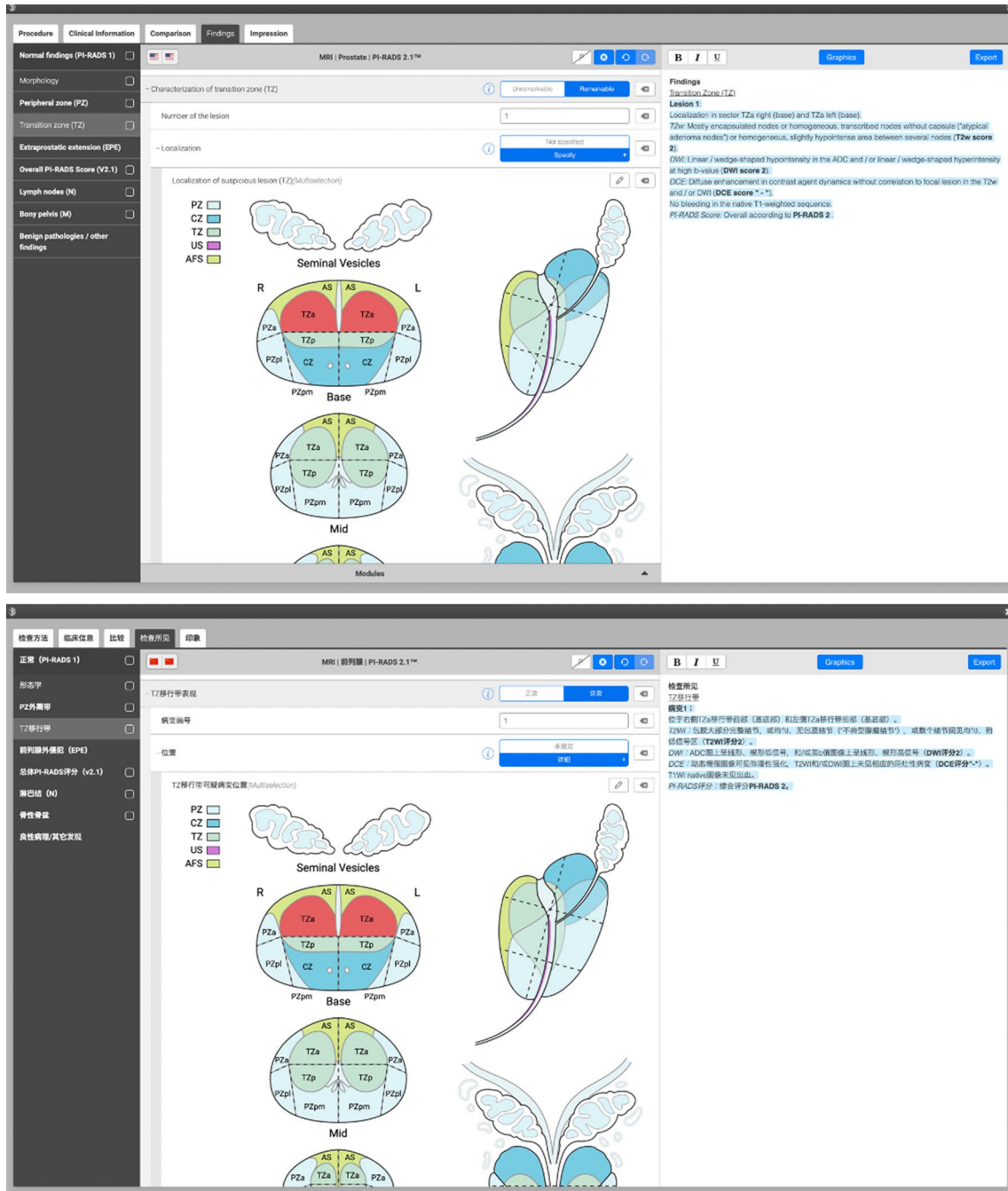


Fig. 5 PI-RADS v2.1 reporting template from an interactive web-based software tool displaying the English (above) and Chinese (below) structured reporting sections. The structured decision tree includes the possibility to select the lesion location from the updated

sector map according to PI-RADS v2.1 recommendation, now also including the posteromedial PZ (PZpm) at the base of the prostate as separate sectors

- tase) which are known for changes in prostate morphology.
4. Biopsy-naïve men with a strong family history, known genetic predispositions, elevated urinary genomic scores, and higher than average risk calculator scores for clinically significant PCa.

5. Patients with a hip implant or other considerations that can be expected to yield degraded DWI.

Other changes in the revised PI-RADS v2.1 include alterations in the sector maps used to compartmentalize the prostate into sub-regions. With the addition of two

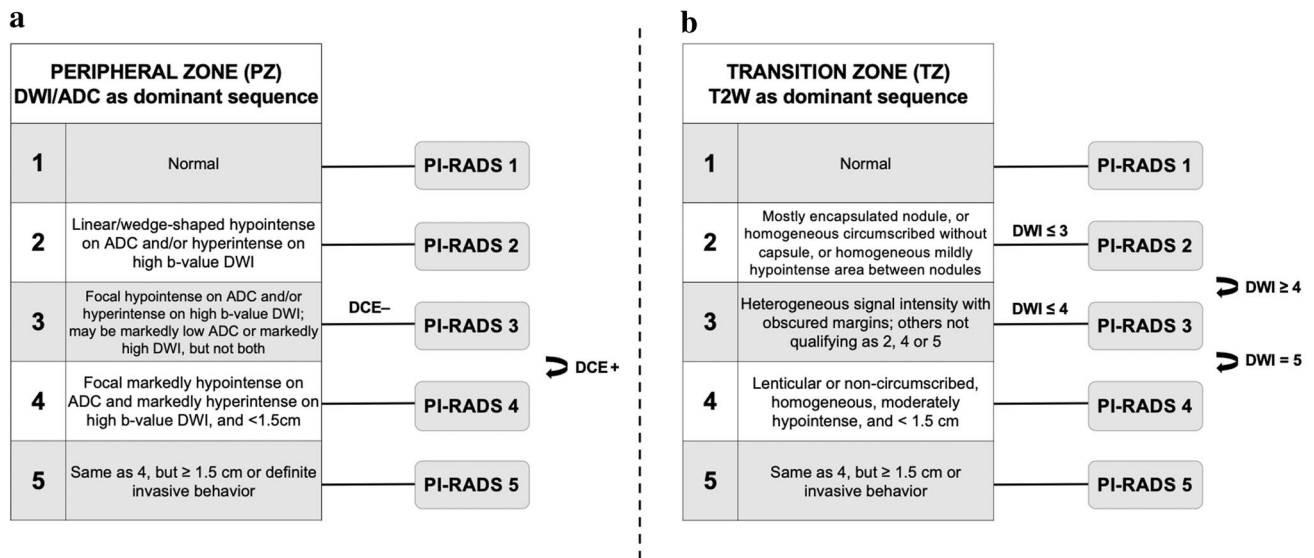


Fig. 6 Simplified PI-RADS v2.1 algorithm for determining the likelihood of clinically significant PCa in a given patient. The PI-RADS system classifies imaging features into five scores with increasing probability of clinically suspicious PCa. This classification relies on DWI as the dominant sequence for the PZ and T2w imaging for

the TZ. Note that positive enhancement in an otherwise PI-RADS 3 lesion of the PZ upgrades that lesion to PI-RADS 4. Similarly, the DWI characteristics of PI-RADS 2 and 3 lesions in the TZ can increase the overall PI-RADS score

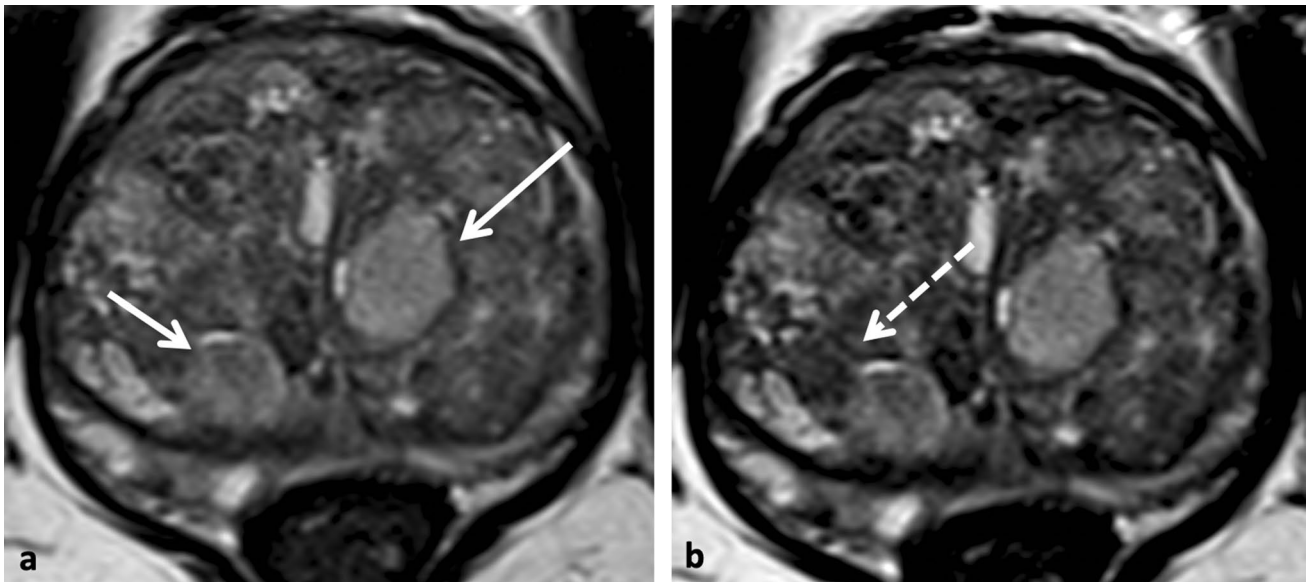


Fig. 7 Enlarged prostate gland of a 71-year-old patient with PSA levels of 15 ng/ml. Axial T2w shows heterogeneous nodular changes in the case of BPH without a suspicious index lesion. **a** Adenomatous nodules (arrows) exhibit a circular hypointense capsule consistent

with a PI-RADS score of 1 (v2.1, 2019). **b** Heterogeneous, hypointense signal attenuation between the adenomatous nodules are in accordance with a PI-RADS score of 2 (dashed arrow). The enlarged TZ leads to compression of the PZ

regions to the PZ at the level of the base—the medial right and left posterior PZpm—the sector map is composed of 41 sectors in total (38 within the prostate gland, two corresponding to the seminal vesicles, and one corresponding to the membranous urethra). So far, surveyed practicing

radiologists prefer using image series and number, PZ vs. TZ anatomy, and apex/mid gland/base terminology to localize lesions. Although usage of the PI-RADS sector map is recommended by the PI-RADS committee, it is currently not preferred in all clinical centers, with only

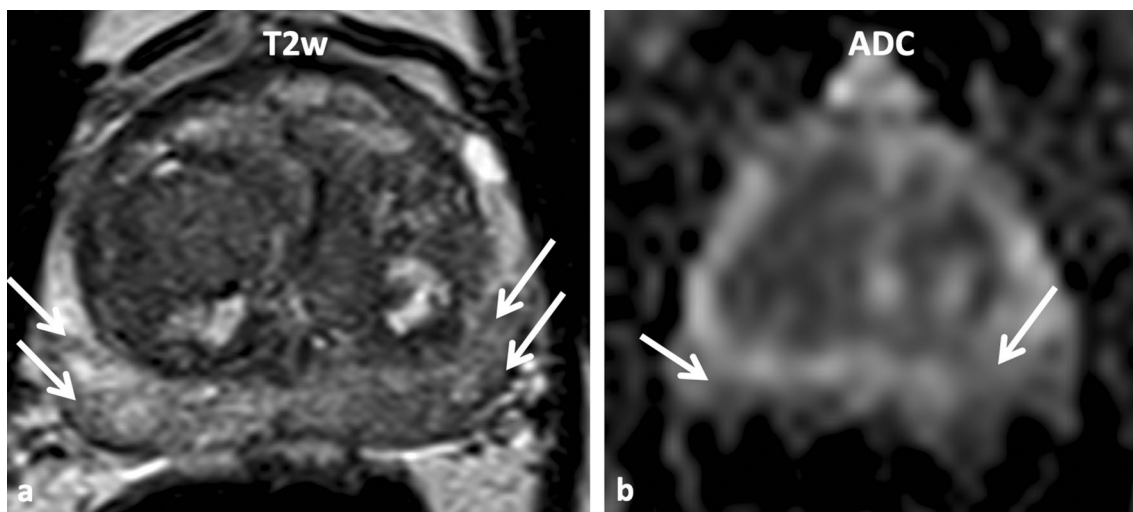


Fig. 8 65-year-old patient with undulating PSA levels between 5 and 7 ng/ml and clinical suspicion of PCa. **a** Axial T2w and **b** ADC map demonstrate bilateral streaky signal hypointensities with non-focal

character (arrows) according to PI-RADS 2 (v2.1, 2019). Histology following non-target TRUS biopsy confirms chronic prostatitis, no cancer was detected

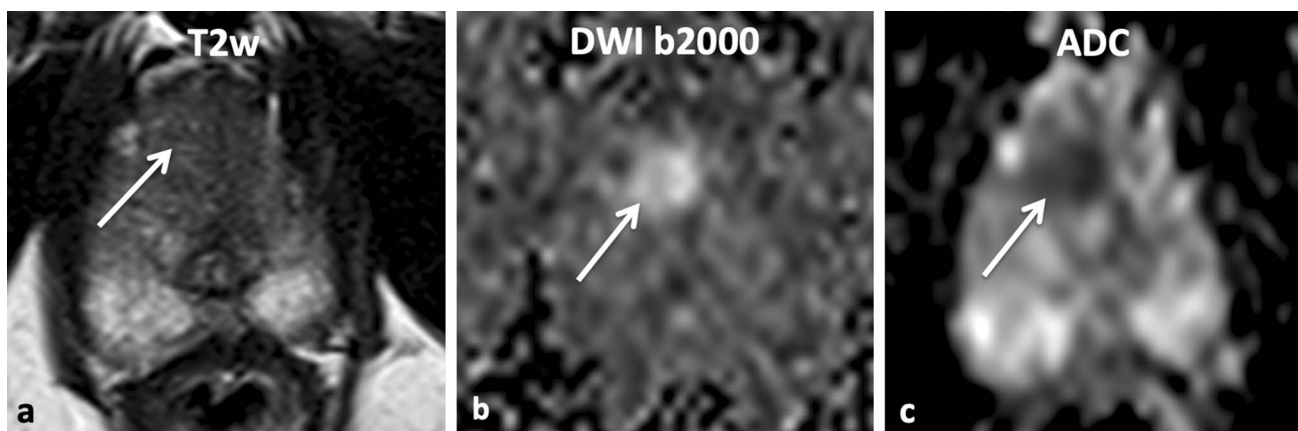


Fig. 9 66-year-old patient (PSA level 7 ng/ml) with prostate cancer presenting as an indistinct T2w hypointense area **a** measuring 1.0 cm (arrows). The lesion is located in the anterior portion of the TZ and involves the AFS. **b** Axial DWI ($b=2000$) and **c** ADC map reveal strong diffusion restriction. Due to AFS involvement, TZ-criteria need to be deployed for lesion scoring according to PI-RADS v2.1:

The lesion is scored with a T2w score of 3 and DWI score of 4. Overall, this leads to a PI-RADS score of 3 (v2.1). MRI ultrasound fusion biopsy of this suspicious lesion reveals an acinar adenocarcinoma (Gleason 3+4=7a, ISUP grade 2). Two prior TRUS biopsies did not detect prostate cancer presence most likely due to its anterior location close to the apex

one in ten radiologists endorsing this type of reporting method [62].

To ensure consistency and comparability, new guidelines for the measurement of total prostate volume and technical specifications regarding the acquisition of T2w, DWI, and DCE-MRI have been introduced with PI-RADS v2.1. As such, it is recommended to explicitly state within the report that the exam was PI-RADS-compliant [63].

In summary, PI-RADS v2.1 was established to reduce variability in mpMRI interpretation with focus on lesion

scoring within the TZ, address the potential use of bpMRI for lesion assessment, revise the sector map, clarify technical features to simplify exam performance, and adjust as well as unify prostate volume measurements. These modifications aim to further strengthen the role of PI-RADS scoring in mpMRI, thereby increasing its value in prostate cancer diagnosis, characterization, and clinical decision-making as PI-RADS represents an established semantic biomarker which can be extracted from radiological reports.

Radiomics

Radiomics refers to the high-throughput analysis of quantitative image features from standard-of-care medical imaging aiming for prediction of certain clinical markers (clinical survival, radiosensitive phenotypes, or genomic features). This enables data extraction and application in clinical decision support systems by which diagnostic, prognostic, and predictive accuracy is enhanced. As such, the overall aim of radiomics is to reveal disease characteristics that cannot be captured by the naked eye, thereby improving disease diagnostics and treatment. For instance, in the case of PCa detection and classification, it was shown that a radiomics model using extracted features from mpMRI showed superior predictive performance when compared to parameters such as PI-RADS category, mean ADC, or DRE findings. While the radiomics model alone achieved a mean AUC of 0.78, an ensembled radiomics model—which included PI-RADS categories, DRE findings, and PSA density—resulted in an increased mean AUC of 0.89 for the prediction of PCa presence [65]. In order for radiomics to develop, its full potential and to progress as a field from research to clinical routine, a minimum standard of quality regarding image acquisition, image segmentation, feature extraction, and radiomics modeling via machine-learning methods must be achieved. Overall, a whole multitude of factors drastically influences the performance of radiomics-based decision support systems. Thereby, these factors affect outcome predictions, diagnostic accuracy, and therapy planning. In this process, standardization is a crucial step by which robustness and performance of these radiomics-based decision support systems can be achieved [66]. Currently, the field of radiomics lacks standardized evaluation of both scientific integrity and clinical relevance of different radiomics investigations. Thus, distinct evaluation criteria and reporting guidelines need to be established for radiomics to mature as a discipline [66].

Structured reporting of radiological findings describes a powerful tool by which this goal can be achieved. PI-RADS incorporates technical specifications and parameters required for standardized imaging. This approach ensures that comparability is given on the level of medical image acquisition itself, enhancing reproducibility and performance of radiomics-based systems. In addition, these structured reporting systems provide access to semantic features, which—when combined with radiomics data—significantly increase the predictive value of radiomics data sets [67].

In summary, structured reporting systems provide a framework by which standardization, accessibility, and completeness of radiological data are increased, thereby paving the way for high-quality data acquisition and complementary radiomics analysis. As such, they yield direct influence on diagnosis, prognosis, and clinical decision-making [56, 66, 67].

Clinical implications

Role of mpMRI

Regarding its clinical relevance, mpMRI has become widely accepted as a reliable imaging technique for the detection and diagnosis of PCa. The increasing application of mpMRI in combination with PI-RADS v2.1 intends to prevent unnecessary biopsies in primary diagnostics, as it enables the assessment of suspicious lesions and their local extent. Despite a tendency to underestimate the size of PCa when correlated with histological analysis [68, 69], mpMRI facilitates the conduct of targeted biopsies (e.g., as MRI ultrasound fusion biopsy), which improves pre-therapeutic risk stratification of PCa patients. Assessment of local tumor extent of PCa through mpMRI aids in determining further urological therapeutic concepts. In some European institutions, MRI is used for surgical planning prior to radical prostatectomy. In this case, MRI can facilitate the surgical decision for nerve-sparing surgery to preserve the neurovascular bundles. A recent study assessing positive surgical resection margins within a cohort of 382 patients that underwent radical prostatectomy revealed that TZ tumors were more likely to extend to the apical (37%) and anterior (22%) margins, especially in case of bladder neck involvement (37%), whereas PZ tumors were more likely to extend to the posterolateral (47%) and also apical (44%) resection margins, the latter accounted as the most common site of positive surgical margins, respectively [70].

Despite the potential of mpMRI to prove apical positivity as a significant preoperative predictor of a positive surgical margin, image-based evidence of external urethral sphincter infiltration is essential for further surgical planning to maximize the membranous urethra length [19, 31].

Standardized application of mpMRI in combination with distinct biopsy procedures allows precise therapy planning for surgical as well as for focal therapeutic procedures (e.g., high-intensity focused ultrasound or cryotherapy) and brachytherapy [71–73]. As part of advanced PCa screenings with a high rate of low-risk cancers, personalized therapy approaches have gained more significance due to lower complication rates when compared to more aggressive therapy approaches [74]. Over the last decades, mpMRI has been increasingly used for radiotherapy planning of locally advanced PCa in addition to CT to define the exact target volume for radiation treatment. Comparative studies indicate that target volumes for radiation therapy based on MRI findings can be reduced by 30% as anatomic structures of the apex and posterior gland as well as their surroundings can be determined more precisely in comparison to CT [75, 76]. The American Urological

Association and the American Society for Radiation Oncology recommend that adjuvant radiotherapy should be considered for patients with adverse pathologic findings at prostatectomy (i.e., seminal vesicle invasion, positive surgical margins, or EPE) and salvage radiotherapy for patients with PSA or local recurrence after prostatectomy [77]. Hence, the application of mpMRI in the pre-therapeutic setting can support the interdisciplinary confirmation of individualized concepts for patients with locally advanced PCa [78].

Clinical decision support systems for diagnosis of prostate cancer

Clinical Decision Support Systems (CDSS) offer patient-specific advice based on guideline recommendations to enhance the process of decision-making by physicians and other healthcare practitioners, improve safety, and facilitate evidence-based practice. A multifactorial decision support system (mDSS) describes a tool which improves the clinical decision-making process by utilizing clinical inputs for an individual patient to generate case-specific therapy advice [79].

Different decision support systems can be applied in PCa diagnostics to enhance early tumor detection, reduce overdiagnosis, and avoid unnecessary testing. These systems utilize several parameters including imaging, clinical, and biological features to improve detection and risk classification of PCa in a minimally invasive way, thereby maximizing individual treatment. mDSS for diagnostic interventions aim to detect, diagnose, or classify PCa using various methods. Several prediction tools are currently used in clinics to support PCa diagnostics including analysis of potential LN involvement, organ confinement, seminal vesicle involvement, and extracapsular extension as well as the risk of failure after treatment [79].

Sadoughi et al. [80] trained an artificial neural network on laboratory results to conduct particle swarm optimization supporting the distinction between localized PCa and benign hyperplasia of the prostate. Van Leeuwen et al. [81] developed a nomogram that includes many parameters, e.g., PI-RADS-score, age, PSA, DRE findings, prostate volume, and prior biopsy results. The model performed with an AUC of 0.864 on an external validation set enabling the proposal of an optimal strategy to reduce the number of biopsies needed while minimizing the risk of underdiagnosis. A study conducted by Lee et al. [82] was designed to support the use of a biopsy by predicting initial biopsy outcomes through different models based on TRUS findings and clinical parameters, including age and PSA. Comparing multiple logistic regression analysis, artificial neural networks, and support vector machines (SVM), AUC values of 0.768, 0.778, and 0.847 could be achieved, respectively [79, 82].

Due to the application of various MRI sequences in mpMRI, the correct and consistent interpretation of multiparametric image data is still challenging. An automated decision support system that conducts image segmentation, feature extraction, and classification enables a computer-aided diagnosis by which a systematic and objective approach for PCa diagnosis and staging can be achieved [83].

As a comparison between MRI and biopsy results, Chan et al. generated statistical maps based on SVM and Fisher linear discriminant (FLD) analysis on calculated ADC, PD, and T2 maps from T2w and DWI performed at 1.5 T with TRUS-guided biopsy results. Additionally, Vos et al. used T2w and parametric DCE-MRI maps at 3.0 T validated with whole-mount sections to develop a CAD (Computer-Aided Design) system based on SVM [83].

Another study performed to introduce a new method of decision support systems for detecting and localizing PCa in the PZ is described by Shah et al. [83]. They used SVM to train their model on pathological regions of MRI scans of patients who underwent prostatectomy with the aim of diagnosing PCa as well as locating it specifically on MRI scans by modeling voxel specific risk analyses. Sensitivity and specificity of the model with optimized SVM parameters were both 90%. The generated cancer probability maps can support the localization of tumors and facilitate planning of targeted biopsies and focal therapies [83].

Outlook: workflow automation and artificial intelligence in radiology

Within healthcare systems, AI will prospectively become a major driver of many applications, including medical diagnostics and imaging, risk management, and hospital management. AI enables the recognition of complex patterns in image data resulting in an automated quantitative assessment. Therefore, more accurate and standardized image assessment is possible when AI is integrated into the clinical workflow as a tool to assist physicians in their daily routine. The primary trigger for the implementation of AI in medical imaging has been the desire for greater efficacy and efficiency in clinical processes [84].

AI methods are often based on machine learning algorithms. Machine learning involves engineered features that are defined by human experts and interpreted in terms of mathematical equations and can thus be quantified by computer programs. These features are used as inputs to machine learning models, which are trained to classify diseases, thereby supporting clinical decision-making [84]. Machine learning will generate novel algorithms which partly automate several aspects of the radiological workflow including image analysis, interpretation, and report creation to optimize decision support and therapy planning in the long term.

To achieve this, a workflow integration of quantitative imaging biomarkers detected by AI, radiomics, or structured reporting data is required. Implementing results of quantitative image analysis and image-based measures directly into the radiological report avoids redundant processes and allows to prepopulate radiological reports based on algorithm findings which ensures time-efficient reporting. Prior studies addressing the detection of quantitative imaging biomarkers clearly show an advantage of semi- or fully automated methods of data extraction for outcome prediction [85, 86], the refinement of software tools for importing biomarker data into structured reports [87, 88], the development of tools to facilitate longitudinal imaging biomarker tracking [89], and the integration of these tools into existing radiological information systems [90]. More recent studies show that quantitative imaging biomarkers using radiomics-based analysis and guideline-driven reporting via PI-RADS can assess tumor aggressiveness and that a combination of clinical factors (such as PSA density), structured reporting (according to PI-RADS) and radiomics analysis even leads to a superior prediction of prostate cancer presence and aggressiveness [65]. Although sufficient scientific evidence is available for a range of radiomics and AI-based studies to enhance tumor characterization and outcome prediction, quantitative image parameters and semantic data from structured reports are nowadays insufficiently incorporated into clinical decision-making processes since the availability of structured reporting software tools as a platform for AI-integration in daily clinical routine is limited. For the widespread dissemination and increasing implementation of practical AI applications in medical diagnostics, huge amounts of data have to be prepared in a structured way and the analyzed models have to be trained continuously [91]. Currently, the dependence of AI on well-curated datasets and large amounts of medical data constitutes a major limitation in the development and advancement of AI algorithms. While in some cases, such as for photographic images, crowdsourcing can be utilized to label and curate a dataset, medical datasets need to be classified by trained personnel to ensure that defined quality criteria are met. Data protection requirements also constrain the development of AI tools and increases both costs and time needed [84].

To overcome these limitations, semi- or fully automated segmentation algorithms have been developed in an effort to curate datasets and prime them for subsequent use with novel AI algorithms. So far, these segmentation algorithms still require human readers for post-hoc verification of the segmentation results, limiting their benefits during the curation process [92]. Combining synoptic reporting and subsequent integration of findings from automated segmentation may overcome these limitations.

Besides, ethical concerns arise when AI is deployed in medicine. AI tools utilize large amounts of sensitive patient

data during development and consequent application. To ensure adequate safety, secure connections are required both within medical institutions and to AI systems. So far, major effort has been expended to improve data sharing with minimal safety concerns. For instance, by training AI models with encrypted datasets and sharing the AI models without their input data, AI algorithms can be used without distributing patient data between institutions. ‘Cryptonets’ further increase privacy, since these deep learning networks are not only trained on encrypted datasets but also provide encrypted predictions which can only be decrypted by the designated institution holding the decryption key [84]. Nonetheless, these solutions are still in their initial development phase and need further advancements before they can be brought into operation in daily routine [60].

Conclusions

Currently, mpMRI is the leading pre-therapeutic imaging modality for the assessment of local tumor extent of PCa and superior to other imaging methods such as TRUS. Structured reporting of PCa is based on the revised PI-RADS classification (v2.1, 2019) which includes modifications in the diagnostic criteria for tumors in the TZ on T2w, a clear distinction between typical and atypical nodules in the TZ, a revision of the sector map, and clinical indications for the utilization of bpMRI over mpMRI. A workflow integration of radiological results through guideline-driven, software-based structured reporting tools and advanced image analysis using radiomics leads to the optimization of diagnostic processes. This may facilitate the implementation of AI-based applications that enable the recognition of complex patterns in image data, resulting in an automated quantitative assessment. Synoptic reporting depicts the most advanced form of structured reporting, since it incorporates discrete fields and fully analyzable data based on radiological ontologies, which increase the reproducibility, completeness, and quality of report data for subsequent analyses building the foundation to standardize and automate the radiological workflow.

Author contributions All coauthors contributed substantially to the success of our research article. SM-B, TH, DN and WS are (part-time) employees of Smart Reporting GmbH (Munich, Germany), KY, PW and MFF are medical students or medical consultants of Smart Reporting GmbH (Munich, Germany) and MFR and SOS are members of the scientific advisory board of Smart Reporting GmbH (Munich, Germany). However, no commercial software or product-related applications have been tested in the study as this is a review article. The research is not financially supported by industry. Academic radiologists (DN, TH, MFF, SOS, MFR) had full control over the academic considerations and outline of the clinical relevance of topics discussed in this research article. There are no other potential conflicts of interests.

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Declarations

Conflict of interest Sanas Mir-Bashiri (S.M-B): COI: Employee of Smart Reporting GmbH, Germany. Kaneschka Yaqubi (K.Y.): Department of Clinical Neurobiology, German Cancer Research Center (DKFZ), COI: Working student of Smart Reporting GmbH, Germany. Piotr Woźnicki (P.W.): Experimental Radiation Oncology Group, University of Heidelberg, Germany; COI: Working student of Smart Reporting GmbH, Germany. Niklas Westhoff (N.W.): Department of Urology, University Medical Center Mannheim, Mannheim, Germany; COI: None. Jost von Hardenberg (J.H.): Department of Urology, University Medical Center Mannheim, Mannheim, Germany; COI: None. Thomas Huber (T.H.): Department of Radiology and Nuclear Medicine, University Medical Center Mannheim, Germany; COI: Part-time employee of Smart Reporting GmbH, Germany. Matthias F. Froelich (M.F.F.): Department of Radiology and Nuclear Medicine, University Medical Center Mannheim, Germany; COI: Medical Consultant of Smart Reporting GmbH, Germany. Wieland Sommer (W.S.): Department of Radiology, University Hospital Munich, Germany; COI: CEO of Smart Reporting GmbH, Germany. Maximilian F. Reiser (M.F.R.): Department of Radiology, University Hospital Munich, Germany; COI: Member of scientific advisory board of Smart Reporting GmbH, Germany. Stefan O. Schoenberg (S.O.S.): Department of Radiology and Nuclear Medicine, University Medical Center Mannheim, Germany; COI: Member of scientific advisory board of Smart Reporting GmbH, Germany. Dominik Nörenberg (D.D.): Department of Radiology and Nuclear Medicine, University Medical Center Mannheim, Germany; COI: Part-time employee of Smart Reporting GmbH, Germany.

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