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Peptide therapeutics and assemblies for cancer immunotherapy

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ABSTRACT Immunotherapy has been considered as one of the most promising strategies for protection against cancer cells due to the tremendous advantages arising from host immune defense. However, establishing versatile strategies with high biosafety and the capability for efficient modulation of immune responses remains challenging. The structural features resembling native proteins of peptides bestow their great potential to address these challenges *via* either directly eliciting immune responses or improving the efficacy of therapeutics. This review summarizes the progress of cancer immunotherapy achieved based on the strategies utilizing short peptides as therapeutic agents or peptide assemblies as delivery scaffolds, beyond long sequences like proteins and polypeptides. Starting from a brief introduction of cancer immunotherapy, we outline the peptide sequences in terms of their specific functions including immune checkpoint blockades, vaccine antigens and adjuvants. We particularly highlight peptide-based nanomaterials as scaffolds for targeting delivery or co-delivery of multiple therapeutics to enhance immunogenicity. The extraordinary therapeutic efficacy of the limited examples covered here demonstrates the great potency of the peptide-based strategies in modulating immune responses, thus potentially facilitating the clinical translation of cancer immunotherapy in the future.

Keywords: cancer immunotherapy, peptides, self-assembly, checkpoint blockades, combinatorial immunotherapy

INTRODUCTION

Cancers are one of main life-threatening diseases and their therapy suffers from the challenges in sufficient treatments, despite the progress made in conventional strategies including surgical resection, chemotherapy, and radiation therapy [1,2]. As an alternative approach, im-

muno-therapy has attracted broad attention over the past few decades due to its advantages in curative efficacy and lowered side effect arising from drug off-target [3,4]. In contrast to directly attack cancer cells, immunotherapy elicits host natural immune responses and thereby killing cancer cells. Since the first marketed immunotherapy for hairy cell leukaemia, a variety of cancer vaccines have been developed and applied in cancer immunotherapy [5]. Recently, the breakthrough of cancer immunotherapy has been achieved based on the new strategies provoking immune responses *via* targeting different immune cells [6]. In principle, the immune system consists of innate immune system and adaptive immune systems dependent on the involved immune cells, including macrophages, monocytes, neutrophils, and dendritic cells in innate immune system, and T or B lymphocytes in adaptive immune system. On the basis of the mechanism for immune activation, therapeutic agents targeting different immune responses could be classified into cancer vaccines, immune adjuvants, cytokines, checkpoint blockades, and engineered T cells, among other emerging categories. Currently checkpoint blockade immunotherapy [7,8] and adoptive immunotherapy using engineering T-cells [9] are two promising strategies used in clinical trials. The checkpoints of the programmed cell death 1 (PD-1) and its ligand PD-L1 or cytotoxic T lymphocytes antigen 4 (CTLA-4) are two conventional targeting sites for the blockades including antibodies or small molecular drugs. Adoptive transfer of engineered T cells like chimeric antigen receptors T (CAR T) cells to replace natural T cell receptors also allows for directly eliciting immune responses [10–13]. Despite the great curative potential, the failure of many clinical trials arising from low immunogenicity and serious adverse side

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effect such as cytokine release syndrome significantly hampers its further development. Hence, new therapeutic agents for efficiently modulating immune responses and novel delivery scaffolds for reducing adverse effect such as autoimmune side effect are demanded.

Peptides, consisting of amino acids analogue to native proteins, have been broadly utilized in development of drugs and biomaterials for tissue regeneration and drug delivery [14–16]. Due to the potential capability derived from native proteins or mimicking structural features of protein substrates, peptide sequences might exhibit the propensity to associate with foreign pathogens or cancer cells and serves as peptide therapeutics. For examples, inspired by the innate immune responses arising from antimicrobial peptides, antimicrobial agents have been developed by rational design of peptide sequences with broad spectrum antibiotics to defend bacteria and fungi [17,18]. Compared to large protein antibodies, short peptide therapeutics exhibit several remarkable advantages in administration and tumor accumulation. The shortened sequences of peptides are readily synthesized and also potentially benefit the penetration into solid tumor tissues. The structure of short peptides can also be precisely tuned to prevent any allergies or autoimmune reactions arising from drug contaminants. The therapeutic efficacy of short peptides does not require stable global conformational analogue to protein antibodies, which is critical for the curative efficacy of antibodies and leads to challenges in administration of protein antibodies. In addition, modulating the noncovalent interactions of peptide therapeutics allows for promotion of peptide self-assembly into nanomedicines, which usually show controllable pharmacokinetics. On the other hand, nanostructures formed by peptides possess specific features when serving as delivery platforms compared to polymeric systems. While the natural component of peptides renders their excellent cytocompatibility, rational design of peptides allows for precisely tailoring their association, thus creating nanostructures with controllable morphologies and subsequently developing functional biomaterials for disease diagnosis and therapy [19,20]. Peptide assemblies responsive to tumor micro-environment, particularly responsive to the biomarkers, are ideal scaffolds for efficient tumor imaging [21–23] and targeting delivery [24,25] and have been broadly utilized in conventional cancer therapy [26–28]. Combining these advantages with the potential transmembrane capability, peptides possess great potential in cancer immunotherapy serving as either therapeutics or delivery scaffolds [29–31].

Thus far, synthetic short peptides and their assemblies have been employed in different classes of cancer immunotherapy (Fig. 1) [32,33]. Peptide epitopes derived from the domains within native proteins are potentially capable of interacting with receptors present in innate or adaptive immune cells or cancer cells, thus endowing their therapeutic functions to modulate host immune system [34,35]. In addition, molecular evolution technology allows for *de novo* design of peptides targeting the receptors participating in suppression or activation of immune system, leading to an alternative approach to discovery of peptide immune therapeutics. Thus far, a considerable number of short peptides serving as the checkpoint blockades [36,37], cancer vaccines [38,39] and adjuvants [40] have been developed. On the other hand, peptide assemblies have been broadly utilized as nano-carriers in targeting delivery of immune therapeutic agents ranging from large objects like cells and antibodies to small drugs into tumor sites [41,42]. Based on the morphological transition of peptide assemblies, peptide nanocarriers can also increase the circulation time of therapeutics [43–45]. Recently, peptide assemblies have attracted specific attention in the combinatory conventional therapeutic and immunotherapy approaches [46–50], due to their versatility for co-loading multiple cargoes. Despite the great potential of peptides in cancer immunotherapy, the progress of peptide-based strategies has not been summarized yet.

This review summarizes the strategies of peptide-based

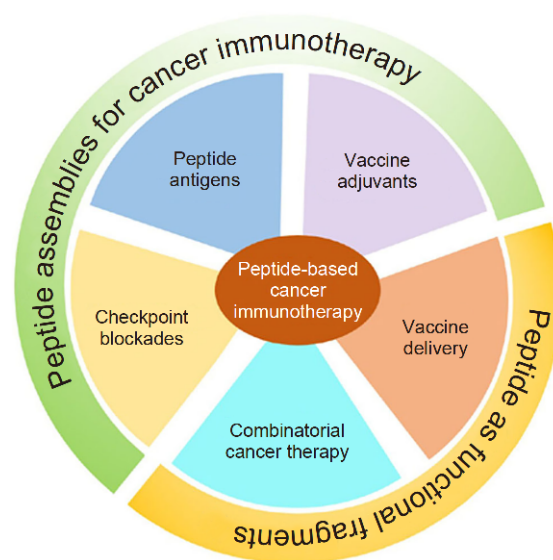


Figure 1 Applications of peptide epitopes or peptide assemblies in cancer immunotherapy ranging from directly serving as therapeutics or as delivery systems for therapeutics.

cancer immunotherapy in terms of the functions of peptides in therapeutic processes. We initially outline peptide-based immunotherapy utilizing peptides as immune therapeutics. Subsequently, the applications of peptide nanostructures as delivery scaffolds for therapeutic agents will be introduced. We particularly highlight the synergistic immunotherapy or the combinatorial immunotherapy involving conventional chemotherapy and photodynamic therapy. It is worth noting that this review only covers the cancer immunotherapy utilizing short peptides as therapeutics or delivery scaffolds, beyond those strategies involving long sequences like proteins and polypeptides. In addition, immunotherapeutic peptides have emerged a couple of decades ago and a considerable number of therapeutic peptides for distinct modalities and cancers have been developed thus far. To precisely illustrate the covered references, the immunotherapeutic peptides summarized in this manuscript are confined as those mostly discovered within the past decade, and also the peptide delivery platforms are created recently for the burgeoning immunotherapeutic modalities such as checkpoint blockades and combinatorial immunotherapy. On the basis of the sophisticated properties of peptides, summarizing the strategies of peptide-based cancer immunotherapy allows for over-viewing the current status of the applications of peptides in immunotherapy and potentially stimulating the development of new strategies to improve the curative efficacy, thus potentially facilitating the clinical translation of cancer immunotherapy in the future.

PEPTIDE CHECKPOINT BLOCKADES

Immune checkpoints are referred to as the negative regulators present in the immune system to maintain homeostasis and prevent autoimmunity from attacking cells indiscriminately [51]. However, immune checkpoint mechanisms can be also activated in cancer cells to inhibit the nascent antitumor immune responses and thus leading to the escape and growth of cancer cells [52,53]. Inhibition of the immune checkpoints allows for blocking the immune evasion of cancer cells and stimulation of the activity of the immune cells such as cytotoxic T cells to protect against cancer cells, which has been considered as a promising and effective strategy for cancer immunotherapy [54]. In principle, the primary inhibitory receptors expressed by activated T cells include PD-1 [55], CTLA-4 [56], lymphocyte-activation gene 3 (LAG-3) [57–59], T-cell immunoglobulin 3 (TIM-3) [60–62], and T cell-immunoglobulin and ITIM domain (TIGIT) [63–65]. Hence these receptors serving as targeting

immune checkpoints allow for development of inhibitors for activating immune responses, as represented by PD-1 and CTLA-4 broadly used in current preclinical studies and clinical trials (Fig. 2) [63].

CTLA-4 is a transmembrane glycoprotein highly expressed on regulatory or activated T cells [66]. CTLA-4 exhibits a high degree of homology with the costimulatory molecule receptor (CD28) on the surface of T cells and enables to bind with B7 proteins, i.e. CD80 (B7-1) and CD 86 (B7-2), with an associating affinity approximately 20-fold greater than CD 28 (Fig. 2). This allows CTLA-4 to outcompete CD28 for B7 binding and thus preventing release of CD28-B7 costimulatory signals and inhibiting T cell activation [67–69]. Current research indicates that CTLA-4 inhibits T cell immune responses potentially through either signaling or non-signaling pathways. The signaling pathway suggests that CTLA-4 activates the phosphatases to dephosphorylate the signals for T cell receptors (TCR). The non-signaling pathway indicates that CTLA-4 potentially captures and removes CD80 and CD86 proteins from the membrane of antigen presenting cells (APC) through the transendocytosis process, thus attenuating CD28 activation [70,71]. PD-1 is another immune checkpoint belonging to the extended B7/CD28 family and highly expressed in activated T cells, B cells, natural killer cells, dendritic cells, and tumor-associated macrophages [72]. PD-1 protein consists of an extracellular domain, a transmembrane domain, and an intracellular domain. In contrast to CTLA-4 affecting naïve T-cells, PD-1 is conventionally expressed on mature T cells and regulates effector T cell activity within the tumor microenvironment (Fig. 2) [73]. The ligands for PD-1 including PD-L1 (B7-H1 or CD 274) and PD-L2 (B7-DC or CD 273) are expressed by APCs and tumor cells [74,75]. Binding PD-1 with its ligands leads to inactivation of T cell kinase and dephosphorylation of TCR signals, thus ultimately reducing production of inflammatory cytokines and regulating T cell activity [76,77]. Therefore, blocking the PD-1/PD-L1 pathway maintains the activity of tumor-specific T cells and allows the immune system to re-identify and attack tumor cells, thereby preventing immune evasion of tumor cells.

Thus far, while the common CTLA-4 checkpoint inhibitors are antibodies, the explicit sequences of PD-1 and PD-L1 and their complex structures inspire rational design of short biomimetic peptides with the capability to outcompete the PD-1 and PD-L1 association (Table 1). Despite the achievement of monoclonal antibodies as PD-1/PD-L1 checkpoint inhibitors in clinical trials, the problems of antibodies including poor penetrance through

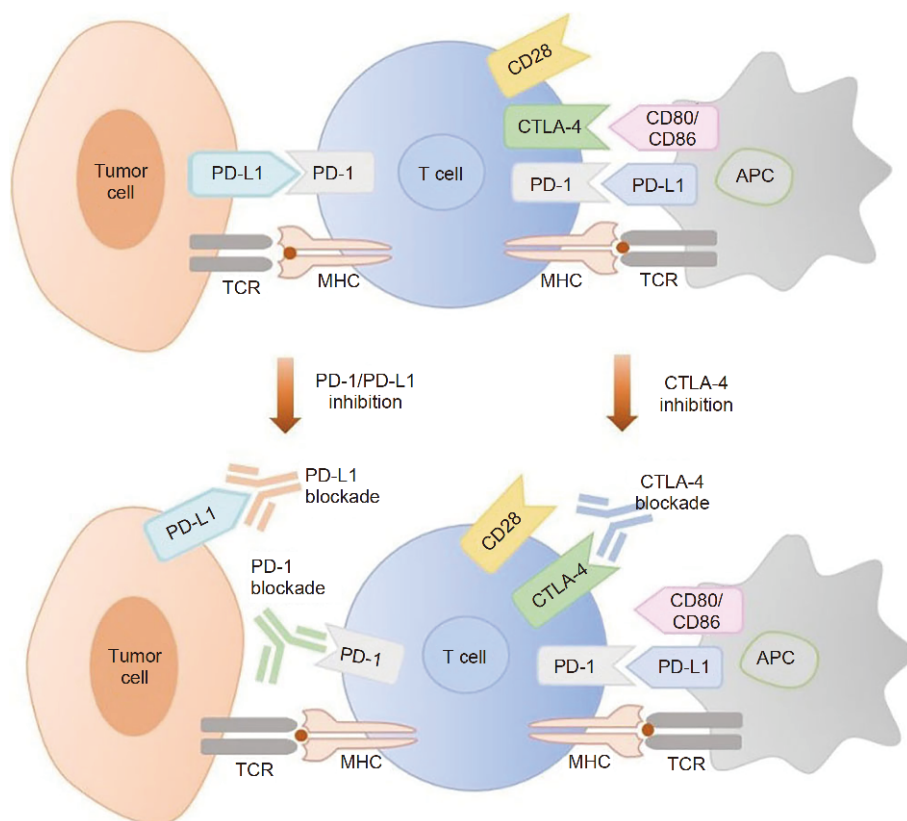


Figure 2 Schematic illustration of the mechanism of immunotherapy based on inhibition of either the cytotoxic T-lymphocyte-associated antigen 4 (CTLA-4)-mediated immune checkpoint or the programmed cell death protein 1 (PD-1) and its ligand PD-L1 checkpoint.

solid-tumor tissues, low stability, high production cost, limited administration approaches, and less controllable pharmacokinetics significantly hamper the clinical translation [78,79]. In addition, antibody inhibitors show limited capability to activate cytotoxic immune responses through natural killer cells and macrophages. Peptides or other small organic molecules serving as the PD-1/PD-L1 checkpoint blockades are alternative drugs to address these problems of monoclonal antibodies. Considering the extraordinary biocompatibility and easy synthesis of short peptides, peptide-based PD-1/PD-L1 inhibitors have attracted broad attention in cancer immunotherapy. This section primarily covers the development of peptide PD-1/PD-L1 inhibitors and summarizes the available sequences in both clinical and preclinical trials.

One of the pioneering peptide PD-1/PD-L1 inhibitors is AUNP-12 that was discovered by Aurigene Discovery Technologies and Laboratories Pierre Fabre with a pharmacokinetic advantage compared to antibody inhibitors, on the basis of the non-linear combination of the 7- to 30-mer domains within human and murine PD-1

extracellular domain [80]. In preclinical studies, AUNP-12 showed the remarkable capability in inhibition of growth of multiple tumors including B16F10 mouse melanoma cells and mouse breast 4T1 cancer cells. *In vivo* studies demonstrated that mediating interferon- γ (IFN- γ) production is the potential signal pathway for AUNP-12 inhibitory activity. The studies of the structure-activity relationship of AUNP-12 revealed that either deletion of the C-terminal eight residues or acylation of the N-terminal serine residues led to loss of the inhibitory activity, whereas the activity was retained by removal of the branched domain or acylation of the C-terminal lysine residue. A short peptidomimetic compound of AUNP-12 peptide was also discovered and exhibits an even better activity in cancer immunotherapy compared to AUNP-12. Following this study, a series of peptidomimetic PD-1/PD-L1 inhibitors have been developed by Aurigene based on this concept.

In addition, Chang *et al.* [81] developed the first proteolysis-resistant D-peptide PD-1/PD-L1 interaction antagonist (^DPPA-1, NYSKPTDRQYHF) on the basis of

Table 1 Peptide therapeutics in cancer immunotherapy

Therapeutics	Name	Peptide sequences	Pathway	Ref.
PD-1/PD-L1 blockades	AUNP-12	(SNTSESF) ₂ KFRVTQ -LAPKQIKE-NH ₂	PD-1	[80]
	^D PPA-1	NYSKPTDRQYHF	PD-L1	[81]
	^D PPA-2	KHAHHTHNLRLP	PD-L1	[81]
	HAC-I	HVIHEGTVVI	PD-L1	[82]
	HAC-V	HVVHEGTVVI	PD-L1	[82]
	TPP-1	SGQYASYHCWC -WRDPGRSGGSK	PD-L1	[83]
	PDLong1	FMTYWHLN -AFTVTVPKDL	PD-L1	[84]
	Peptide-57	Cyclic[F(NMe)ANPHLSWSW (NMe)[NLe](NMe)[NLe]R(Scc)]G	PD-L1	[85]
	Peptide-71	Cyclic[F(NMe)F(NMe)[NLe](Sar) DV(NMe)FY(Sar)WYL(Scc)]G	PD-L1	[85]
	Peptide-99	Cyclic[FLIVIRDRVFR(Scc)]G	PD-L1	[85]
Peptide antigens	OVA ₂₅₇₋₂₆₄	SIINFEKL	CD8 ⁺ T cell	[86]
	OVA ₂₅₃₋₂₆₆	EQLESIINFEKLTE	CD8 ⁺ T cell	[87]
	OVA ₃₂₃₋₃₃₉	ISQAVHAA -HAEINEAGR	CD8 ⁺ T cell	[88]
	NY-ESO-1	SLLMWITQV	CD8 ⁺ T cell	[89]
	MAGE-A3	FLWGPRALV	CD8 ⁺ T cell	[90]
	Tyrosinase ₁₋₉	MLLAVLYCL	CD8 ⁺ T cell	[91]
	Tyrosinase ₃₆₈₋₃₇₆	YMDGTMSQV	CD8 ⁺ T cell	[91]
	MART-1 ₂₆₋₃₅	EAAGIGILTV	CD8 ⁺ T cell	[92]
	gp100 ₂₈₀₋₂₈₈	YLEPGPVTA	CD8 ⁺ T cell	[93]
	gp100 ₂₀₉₋₂₁₇	IMDQVPFSV	CD8 ⁺ T cell	[94]
	HGP100	KVPRNQDWL	CD8 ⁺ T cell	[95]
	TRP2	SVYDFVWVW	CD8 ⁺ T cell	[96]
	Survivin-2B ₈₀₋₈₈	AYACNTSTL	CD8 ⁺ T cell	[97]
	E75	KIFGSLAFL	CD8 ⁺ T cell	[98]
	WT1Pep427	RSDELVRHH -NMHQRNMTKL	CD4 ⁺ T cell	[99]
	E7 ₁₁₋₂₀	YMLDLQPETT	CD8 ⁺ T cell	[100]
	E7 ₈₆₋₉₃	TLGIVCPI	CD8 ⁺ T cell	[101]
	E7 ₄₃₋₅₇	GQAEPDRAHYNIVTF	CD4 ⁺ , CD8 ⁺ T cell	[102]
	E7 ₄₉₋₅₇	RAHYNIVTF	CD8 ⁺ T cell	[103]
	E7 ₄₈₋₅₄	PDRAHYNI	CD4 ⁺ T cell	[104]
OFA 2	ALCNTDSPL	CD4 ⁺ , CD8 ⁺ T cell	[105]	
Vaccine adjuvants	Q11	QQKFQFQFEQQ	-	[106]
	KFE8	FKFEFKFE	-	[107]
	Hydrogel	Nap-G ^D F ^D F ^D Y ^D	-	[108]
	Hydrogel	Nap-G ^D F ^D F ^D Y ^D K	-	[109]
Hydrogel	G ^D F ^D F ^D Y	-	[110]	

mirror-image phage display technology. Mirror-image phage display technology allows for screening D-clones for binding L-targets by using a chemical synthesized D-

peptide bait. Starting from the immunoglobulin-like variable (Ig-V) domain, the authors designed a D-version of the folded IgV domain (^DIgV^{PD-L1} 9) serving as the bait

peptide in mirror-image phage display. Screening a duodecimal peptide library displayed on M13 phage allowed the authors to select two D-sequences (^DPPA 1: NYSKPTDRQYHF, ^DPPA 2: KHAHHTHNLRLP) with the highest frequency. Surface plasmon resonance spectroscopy estimated the binding constants (K_D) of ^DPPA 1 and ^DPPA 2 with human PD-1 to be 0.51 and 1.13 $\mu\text{mol L}^{-1}$, respectively. Flow cytometry experiments showed that ^DPPA 1 exhibited an advanced capability for inhibiting PD-1/PD-L1 interaction compared to ^DPPA 2. *In vivo* experiments revealed the inhibition of the growth of CT26 cells implanted in 36 Balb/c mice by the ^DPPA 1 administration potentially due to the activation of the antitumor immune system. Therefore, the anti-hydrolysis D-peptide has the potency as a small molecular drug for cancer immunotherapy, which has been currently utilized in many preclinical studies.

On the basis of the yeast-surface display technology, Maute *et al.* [82] developed competitive peptide antagonists, i.e., HAC-I (HVIHEGTVVI) and HAC-V (HVVHEGTVVI), with a high affinity with PD-L1 using a two-library strategy. In this approach, the first generation library derived from the domain of human PD-1 at the interacting interface with PD-L1 allowed for identification of mutational residues governing the high affinity, whereas the second generation library determined the optimal combination of the residues. As a consequence, two sequences of HAC peptides that are merely different with an isoleucine or valine residue at position 41 were produced, and the resulting HAC sequences enable to bind with PD-L1 with a K_D value of approximately 100 pmol L^{-1} . Therapeutic studies showed that the HAC peptides possessed the ability to treat both small and large tumors. In particular, radiolabeling the HAC peptides led to positron emission tomography imaging of the presence of PD-L1 in tumors, thus allowing for direct immune diagnostics.

Based on an alternating random and focused library screening strategy of bacterial surface display technology, Zhu and coworkers [83] discovered a targeting PD-L1 peptide (TPP-1, SGQYASYHCWCWRDPGRSGGSK) with a high associating affinity with PD-L1 and the capability to inhibit the PD-1/PD-L1 interaction. Both *in vitro* and *in vivo* assays revealed that treatment of tumors with TPP-1 activates T cells and elicited immune responses, thus demonstrating the inhibitory potency in cancer immunotherapy. Andersen and coworkers [84] designed and synthesized a T cell epitope derived from PD-L1, termed as PDLong-1 (FMITYWHLL-NAFTVTVPKDL), which contains a PD-L1-derived

CD8⁺ T cell epitope (PDL1₁₅₋₂₃, LLNAFTVTV). The authors found that co-stimulation of dendritic cell (DC)-based vaccination with PDLong-1 led to significant increase of the number of T cells. This finding demonstrates that reactivation of PD-L1 associated T cells potentially allows for direct modulation of DC vaccination immunogenicity. In addition, starting from the macrocyclic peptide PD-L1 inhibitors developed by Bristol-Myers Squibb, Magiera-Mularz *et al.* [85] investigated the affinities of three macrocyclic peptides, i.e., peptide-57, peptide-71, and peptide-99, binding with PD-L1. The authors found that all the three macrocyclic peptides inhibited the PD-1/PD-L1 interaction and their affinities with PD-L1 were estimated in an order of peptide-71 > peptide-57 > peptide-99. These limited examples demonstrate that peptides are burgeoning checking point blockades with great potency in modulating the immune system. Combining peptide inhibitors with the peptide nanocarriers leads to a promising strategy towards cancer immunotherapy with low side effect.

PEPTIDE-BASED CANCER VACCINES

As another representative method of immunotherapy, cancer vaccines target activation of host immune system protecting against cancer cells by using tumor cell-associated antigens. Due to the antigen-specific immune responses and long-term immune memory, cancer vaccines exhibit great potential in cancer immunotherapy. Vaccination probably is the most classical immunotherapy approach and has been utilized broadly through ancient to modern medicine [111]. In conventional cancer vaccines, tumor cell-associated antigens collected from different types of cancer cells are used to stimulate the immune cells like B-cells and T-cells. During vaccination, the injected vaccines can be up-taken by antigen-presenting cells through either endocytosis initiated by binding with Toll-like receptors (TLR) or phagocytosis directly (Fig. 3) [112]. Within the APC cells, the up-taken antigens were degraded into short peptides based on proteasome-mediated processes. Displaying the resulting peptides on the APC cell surface *via* association with major histocompatibility complex (MHC) class I or II receptors leads to activation of immune responses. In the case of the MHC class I pathway, association of antigens with MHC and T cell receptors (TCR) results in production of CD8⁺ cells eliciting cellular immune responses involving cytotoxic T-lymphocyte (CTL) cells [113]. However binding antigens with the MHC class II receptors activates the T-helper cells that further cause production of B cells for humoral immunity or CTL cells

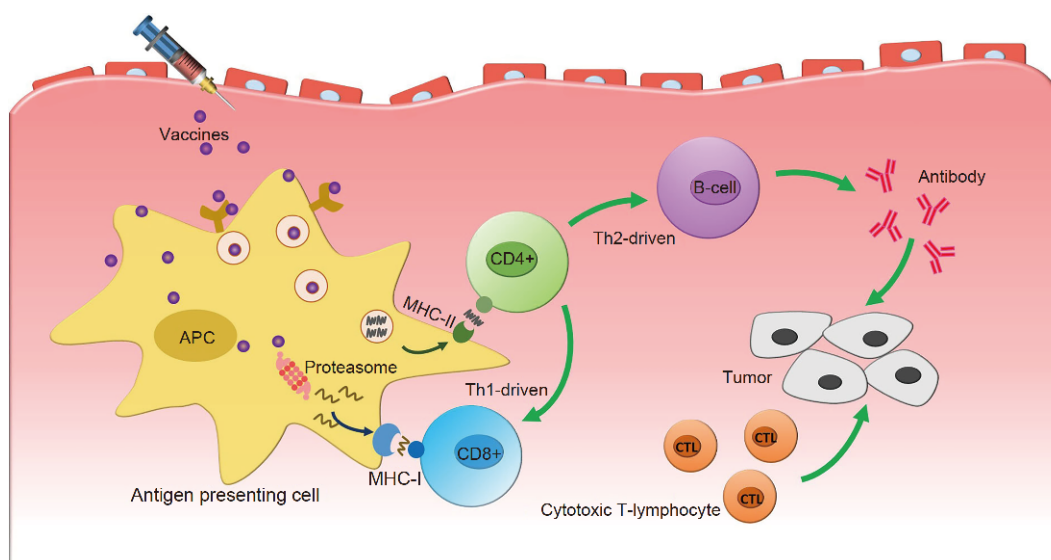


Figure 3 Schematic representation of immune response pathways for vaccines. Vaccines are up-taken by antigen-presenting cells (APCs) through either endocytosis initiated by binding with Toll-like receptors (TLR) or phagocytosis directly. Degradation of vaccines into short peptides allows for displaying on the surface of APCs *via* association with major histocompatibility complex (MHC) class I or II receptors.

for cellular immunity [114,115]. Traditional cancer vaccines are attenuated organisms or viruses and the subunits of active proteins isolated from viruses. Despite the success in some cancer treatments, traditional vaccination therapy remains challenging primarily arising from contaminant-associated immune risks, poor stability of antigens, difficulties in production and transportation to lymph nodes, and the off-targeting-induced undesired autoimmunity, among others [116].

Peptide antigens

Recently, short peptides with minimal antigenic epitopes to bind with targeting receptors have been developed as alternative vaccines due to their precise structures and facile production [117,118]. Sufficient affinity of antigens for the TLR or MHC receptors is crucial for promoting the production of $CD4^+$ or $CD8^+$ T cells for immune responses. Due to the limited immunogenicity of short peptide antigens, utilization of peptide adjuvants to assist the activation of the immune response of peptide antigens is a typical strategy and indeed a bunch of peptide adjuvants have been developed thus far. This section briefly summarizes peptide vaccines including design of peptide antigens involving sequences less than 20 amino acids. Due to the long period of peptide vaccine research, the more detailed reviews of peptide vaccines were referred to elsewhere [111,112].

On the basis of the revealed sequences of native pro-

teins within organism or virus vaccines, the subunits of these proteins inspire the design of short peptides as potential antigens to induce remarkable and long-term immunity against viruses (Table 1). Dependent on the stimulating pathways, the designed peptide antigens associated with MHC class I receptors towards activation of $CD8^+$ T cells typically consist of 8–10 amino acids, whereas the antigens loaded by MHC class II receptors and $CD4^+$ T cells usually possess 13–18 amino acids, though there is no strict limitation on the peptide length [117]. Due to the heterogeneity of the MHC receptors of individual patients, immune tolerance to peptide antigens has been observed in clinical trials. Combining the targeting delivery with the assistance of peptide adjuvants in immune responses renders peptides antigens still promising in cancer immunotherapy [119]. Here we summarize peptide antigens mostly developed within the past decade with an emphasis on the originality of peptides and the underlying immunogenicity mechanism.

Peptide vaccines have been broadly utilized in melanoma immunotherapy [120]. Most melanoma peptide antigens are derived from melanocyte differentiation proteins such as tyrosinase, MART-1 (Melan-A), and glycoprotein 100 (gp100) [121], and predominately promote the production of CTLs for immunity. For instance, tyrosinase, which is the rate-limiting enzyme in melanin synthesis, contains two immunogenic peptides, i.e., tyrosinase_{1–9} and tyrosinase_{368–376} [91]. The tyrosinase_{368–376}

domain with the replacement of asparagine residue at position 3 with aspartic acid was proved to exhibit the extraordinary immunogenicity. The original MART-1_{26–35} domain [92,122] was employed as antigens in clinical trials to treat melanoma patients as well. In addition, the domain of gp100_{280–288} within protein gp100 [93] that is expressed by both melanoma and healthy melanocytes caused immunogenicity for a large proportion of patients, despite a low amount of CTL production. Combining a vaccine-restricted domain gp100_{209–217} with an immune activator interleukin-2 (IL-2) improved the immune response against cancer cells. A hydrophilic epitope HGP100_{25–33} and a hydrophobic epitope within tyrosine-related protein 2 (TRP2_{180–188}) are two alternative melanoma-derived antigens. Guo *et al.* [95] created a nanovaccine formulation by integrating nanoparticles composed of poly(D,L-lactide-co-glycolide) functionalized with antigen HGP100 and adjuvant monophosphoryl lipid with liposomes coated with mannose. Mirkin and coworkers [123] attached antigen HGP100 peptide to immune-stimulatory spherical nucleic acid for vaccine development. Wakabayashi *et al.* [96] utilized a solid-in-oil nanodispersion as nanocarriers for the co-delivery of antigen TRP-2 peptide modified with three lysine residues (KKKGSVYDFFVWL) and adjuvant Resiquimod (R-848). This system exhibited the great capability in inhibiting melanoma growth and suppressing lung metastasis in tumor-bearing mice. Antigens HGP100 and TRP2 were also simultaneously co-encapsulated into hollow mesoporous silica nanoparticles, which was efficient in stimulating dendritic cells (DC) and their maturation and further secreting tumor necrosis factor- α (TNF- α), IFN- γ , IL-12 and IL-4 for promoting immunity [124].

Epitopes derived from ovalbumin have been widely used as peptide antigens including OVA_{257–264}, OVA_{253–266}, OVA_{250–264}, and OVA_{323–339}, and conventionally activate CD8⁺ cytotoxic T cell immune responses. Utilization of the nanocapsules composed of 60 nonviral E2 subunits of pyruvate dehydrogenase, Wang and coworkers [86] developed a viral-mimicking vaccine scaffold encapsulating antigen OVA_{257–264} and oligonucleotide adjuvant cytosine-guanine motif (CpG). This multifunctional vaccine platform showed synergistically spatiotemporal delivery of therapeutic agents to DCs and thus enhancing CD8⁺ T cell production and immune activation. In addition, elongating OVA_{257–264} epitope to CCYSIINFEKL with two thiol groups allowed for *in situ* preparation of fluorescent antigen-gold nanoclusters (peptide-AuNCs), which displayed enhanced immune-

stimulatory capability [125]. The immunity was further improved by co-loading CpG adjuvant on the AUNC surfaces. Furthermore, Zhang and coworkers [88] created ultra-small biocompatible nanovaccines functionalized with scavenger receptor class B1 targeting mature DCs, which efficiently delivered peptide antigens including OVA_{257–264}, OVA_{323–339}, and HGP100_{25–33} to lymph nodes.

Membrane-binding glycoprotein mucin 1 (MUC1) that plays a critical role in protection of epithelial surfaces and signaling transduction is typically overexpressed with glycosylation mutation in many cancers such as breast and pancreas cancers or myelomas and lymphomas, thus rendering MUC1 immunogenic [126]. This phenomenon inspires the design of peptide antigens capable of inducing MUC1-associated cytotoxic T lymphocyte responses. MUC1 is a type I transmembrane glycoprotein featured with an extracellular domain consisting of a variable number of 20-amino acid repeat sequences (PDTRPAPGSTAPPAHGVTSA) and a high glycosylation level on serine and threonine residues within each tandem repeat. Hence, MUC1-related peptide antigens can be designed based on glycosylation of MUC1 epitopes. For example, Huang *et al.* [127] designed and synthesized several vaccine candidates *via* conjugating HGVTSA PDTRPAPGSTAPPA sequence with glycosylated threonine residues at position 9 or 16 to an assembling domain Q11. These B cell epitope-containing vaccines elicited significant cytotoxic T cell immune responses activated by type I T-helper cells. In addition, Zhao and coworkers [128] also designed MUC1-related antitumor vaccines based on covalently connecting antigen candidate glycopeptide tandem repeat TSAPDTRPAP with an assembling sequence Nap-G^DF^DF^DY^DK.

In addition to the broadly used melanocyte mutated proteins, ovalbumin, and MUC1, some other immunogenic proteins have also been employed to design peptide vaccines. For instance, an epitope E75 derived from HER2/neu, which is a proto-oncogene expressed in many epithelial cancers, was designed and utilized in breast cancer treatments [98]. A WT1 Pep427 originated from Wilm's tumor protein (WT1) was also discovered as immunogenic antigens and was covalently conjugated with single-wall carbon nanotubes to induce rapid specific IgG responses [99]. New York esophageal squamous cell carcinoma-1 (NY-ESO-1) [89] is an immunogenic cancer testis antigen highly expressed in many human cancers (melanoma, breast cancer) and capable of inducing T cell-associated immunity. Gazzinelli and coworkers [129] connected antigen NY-ESO-1 and adjuvant CpG DNA to carbon nanotubes (CNT) and developed a

new anti-cancer vaccine platform. Wang and coworkers [90] employed E2 viral-like capsules to simultaneously encapsulate antigens NY-ESO-1 and HLA-A2 to overcome the low immunogenicity of individual antigens. In addition, the epitopes derived from human papillomavirus (HPV) including HPV16 E7₁₁₋₂₀ [100,101], E7₈₆₋₉₃ [101], E7₄₃₋₅₇ [102,103,130], E7₄₉₋₅₇ [101,103,131], and E7₄₈₋₅₄ [103,104], or from oncofetal antigen including OFA 1, OFA 2, and OFA 3 [105], have been utilized as antigens for cancer immunotherapy. Extending from these examples, new-generation peptide antigens such as multivalent or multifunctional peptide antigens, peptide cocktail antigens, hybrid peptide antigens, as well as personalized peptide antigens (neoantigens) have attracted broad attention in clinical trials and show great potency for cancer therapy.

Peptide vaccine adjuvants

Design of vaccine antigens from short peptides benefits from their defined structures and selective targets within the immune system. However, immunogenicity caused by peptide antigens is still insufficient and requires the presence of vaccine adjuvants. On the basis of the deep understanding of anti-tumor immune responses, vaccine adjuvants have been widely used to augment immune responses during vaccination. Despite utilization of many adjuvants like aluminium salts for peptide im-

munotherapy thus far, currently available adjuvants including oil emulsions, virosomes, and TLR ligands still suffer from their structural heterogeneity and resulting difficulties in mechanism understanding and administration [132,133]. Recently, peptide assemblies have been developed as homogenous peptide antigens predominantly due to the capability in displaying multivalent antigens on the surface of peptide assemblies.

The pioneer work of peptide vaccine adjuvants was reported by the Collier group [106], in which the authors attached antigen OVA₃₂₃₋₃₃₉ to a domain Q11 (QQKFQFQFEQQ) able to undergo self-assembly into well-defined nanofibrils, leading to peptide OVA-Q11 that assembled into well-defined nanofibers under mild condition (Fig. 4). Treating C57BL/6 mice with peptide OVA-Q11 resulted in significant increase of the population of IgG titers in serum, thus enhancing the immunogenicity. This enhanced immunogenicity of OVA-Q11 was potentially attributed to the multivalent surface display of the epitope on the fibrils. More detailed studies revealed the lack of cytokine responses and an elevated IgM response induced by OVA-Q11, indicative of an immunogenic mechanism independent on T cell response. The Q11 domain was also used to connect MUC1-derived epitopes with varied glycosylated threonine residues to develop self-adjuncting antigens from nanofibrils with B cell epitopes displayed on their surface.

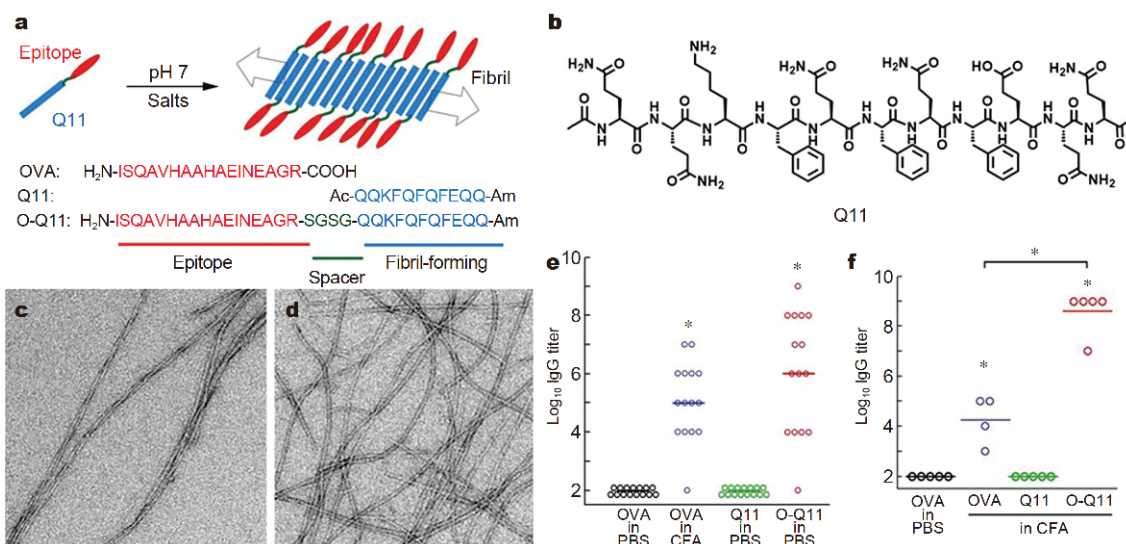


Figure 4 Peptide assemblies as vaccine adjuvants. (a) Schematic illustration of formation of antigen-displaying peptide nanofibrils and the design of sequences consisting of antigen OVA₃₂₃₋₃₃₉ and assembling domain Q11. (b) Chemical structures of Q11. TEM images of nanofibrils formed by peptide Q11 (c) and O-Q11 (d). (e) Expression of IgG induced by fibrillized Q11 domains compared to traditional complete Freund's adjuvant (CFA). (f) Improved secretion of IgG titers induced by OVA, Q11, and O-Q11 in the presence of CFA. **p*<0.01. Reproduced with permission from Ref. [106]. Copyright 2010, National Academy of Sciences.

Alternative to Q11 domain, Collier and coworkers [107] also connected antigen OVA_{323–339} to a assembling sequence KFE8 (FKFEFKFE), leading to OVA-KFE8 that formed nanofibrils and activated strong antibody responses analogue to OVA-Q11. Furthermore, Rudra and coworkers [134] changed the natural D-amino acids to L-amino acids in Q11 domain and investigated the enantiomeric effect of nanofibrils on immune response of OVA epitopes. On the basis of characterization of enantiomeric nanofibrils, the authors discovered that compared to the L-counterparts, nanofibrils composed of D-amino acid sequences enhanced antibody responses and prolonged antigen-presentation in mice, suggestive of the advanced performance of D-peptides in vaccination and also the stereochemistry-associated biomaterials in modulation of the immune system. These results demonstrate that utilization of peptide assemblies as homogenous peptide vaccine adjuvant allows for facilitation of vaccination.

In addition to peptide assemblies, Yang and coworkers [135] created hydrogels composed of peptide assemblies to develop vaccine adjuvants, which might simplify vaccine administration and improve the biosafety of adjuvants (Fig. 5). The authors investigated the enantiomeric effect of the resulting hydrogels on vaccination by synthesizing the peptide gelators consisting of either D- or L-amino acids, i.e., Nap-GFFpY-OMe and Nap-G^DF^DF^DpY-OMe, which underwent hydrogelation

promoted by alkaline phosphatase (ALP)-induced dephosphorylation. Co-assembling of the gelators with OVA protein maintained the hydrogelating behavior, implying the efficient up-taking of OVA within the hydrogels. *In vivo* studies revealed that both the two enantiomeric hydrogel adjuvants effectively caused production of immune antibody and secretion of cytokines, due to the enhanced cellular uptake of antigens, accumulation of antigen at lymph nodes, maturation of dendritic cells, and formation of germinal centers. In particular, the authors found that the D-peptide hydrogels possessed a better performance in accumulating OVA and preventing tumor growth, compared to the L-counterpart hydrogels.

To further avoid the difficulty in preparing vaccine adjuvants caused by enzymatic hydrolysis, the authors developed hydrogel adjuvants directly from enantiomeric peptide gelators Nap-GFFY and Nap-G^DF^DF^DY [108]. The thixotropic feature of the resulting hydrogels allowed for efficient encapsulation of antigen OVA. In addition, the hydrogels also encapsulated X-ray attenuated tumor cells serving as antigen therapeutics to suppress tumor growth and prolong the survival of tumor-bearing mice through the CD8⁺ T cell activation pathway. Analogue to the enzyme-instructed hydrogelation, Nap-G^DF^DF^DY hydrogels exhibited advanced capability in activation of immune response compared to the L-peptide hydrogels. On the basis of the concept of hydrogel adjuvants, a series

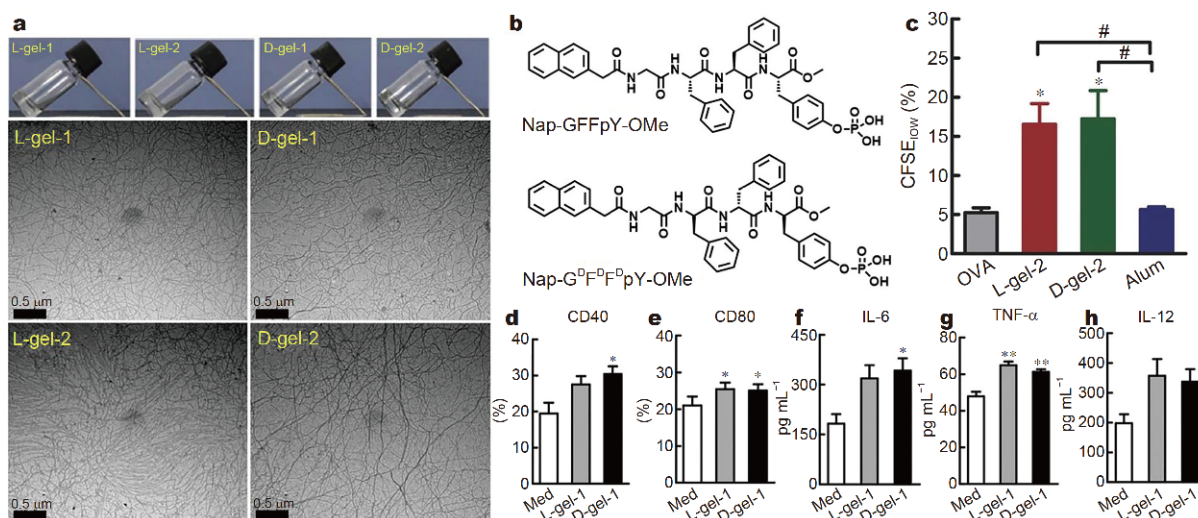


Figure 5 Peptide hydrogels as vaccine adjuvants. (a) Optical and TEM images of hydrogels prepared by phosphatase-induced hydrolysis of Nap-GFFpY-OMe and Nap-G^DF^DF^DpY-OMe in the absence (L-gel-1, D-gel-1) or presence (L-gel-2, D-gel-2) of antigen OVA. (b) Chemical structures of Nap-GFFpY-OMe and Nap-G^DF^DF^DpY-OMe. (c) The numbers of germinal centers and B-cell follicles induced by different vaccines. (d–h) Production of CD40 (d) and CD86 (e) based on maturation of bone marrow dendritic cells and expression of cytokine IL-6 (f), TNF-α (g), and IL-12 (h) treated with medium (Med) or L-/D-gel vaccines. **p*<0.05. Reproduced with permission from Ref. [135]. Copyright 2016, John Wiley and Sons.

of peptide gelators derived from the Nap-GFFY or Nap-G^DF^DF^DY^D sequences have been developed for vaccine adjuvants. For example, tailing Nap-G^DF^DF^DY^D with either a positively or negatively charged residue at C-terminus led to Nap-G^DF^DF^DY^DK and Nap-G^DF^DF^DY^DE [109]. When encapsulating OVA protein, the hydrogels composed of the positively charged peptides displayed the better capability in inducing immune responses compared to the negatively charged one, potentially attributed to the efficient encapsulation of OVA. In another example, the authors replaced naphthalene unit with non-steroidal anti-inflammatory drugs at the N-terminus of G^DF^DF^DY^D, resulting in several drug-modified vaccine adjuvants [110]. Combining the anti-inflammatory property of drugs, the hydrogels up-taking OVA showed the extraordinary capability in elimination of tumor in mice. Alternative to OVA protein, incorporation of MUC1 epitopes into Nap-G^DF^DF^DY^DK sequence allows for enhancement of the immunogenicity of antigen MUC1 [128].

PEPTIDE ASSEMBLIES IN CANCER IMMUNOTHERAPY

Despite their success in immune activation in some preclinical studies and clinical trials, peptide immune therapeutics still suffer from the low immunogenicity in clinical trials. In principle, shortening the sequences of native proteins to partial epitopes significantly weakens the affinity of peptides to corresponding targeting receptors, and also increases the possibility of the enzymatic degradation of short peptides, which further lowers the circulation life-time and accumulation of peptides around lymph nodes. In addition to these drawbacks, the heterogeneity of APC cells of patients further leads to the challenge in effective immunogenicity of peptide therapeutics. Based on these considerations, exploration of additional functions of peptides in cancer immunotherapy becomes essential.

Self-assembly of peptides into well-defined nanostructures with morphologies ranging from nanoparticles [136], nanofibers [137], nanoribbons [138], nanotubes [139], to hierarchical networks, driven by noncovalent interactions including hydrophobic interactions, hydrogen bonding interactions, and π - π stacking interactions, has great potency to address these issues. Basically, the resulting nanostructures are ideal platforms to deliver and display peptide therapeutics due to their unique structural properties such as biocompatibility and biodegradability [132,140]. Incorporation of peptide therapeutics into peptide nanostructures allows for prolonging the circu-

lation of therapeutics and increasing the affinity with targeting receptors arising from multivalent effect. In addition, the passive or active targeting capability of peptide nanostructures facilitates the accumulation of therapeutics at tumor sites. These advantages of peptide assemblies give rise to the great potential of peptide-based biomaterials as vaccine adjuvants for enhancement of antigen immune responses or the platforms for delivery of immunotherapeutic agents. This section covers cancer immunotherapy using peptide assemblies in cancer vaccination including vaccine adjuvants or delivery systems of immune therapeutics including genes, vaccines, antigens, checkpoint blockades, or their combinatorial drugs with conventional cancer therapeutics.

Peptide assemblies in vaccination delivery

Despite the great potential of cancer vaccines in humoral and cellular immune responses, many clinical trials of vaccination still suffer from the low immunogenicity. This potentially results from several reasons, such as immunosuppression, poor T cell infiltration, and low production of T cell. Development of novel delivery scaffolds able to target antigen-presenting cells and facilitate antigen production allows for improvement of the immunogenicity, thus potentially leading to positive clinical performance. Compared to conventional biomaterials, the precisely customizable properties of peptide assemblies render their great potential for serving as delivery systems for cancer vaccines. Extending from the conventional functions of peptide assemblies as delivery platforms, modulating the aggregating features of peptide therapeutics also allows for establishment of self-delivering systems, termed as drug amphiphiles [141]. In addition to the succeeded advantages of peptide delivery systems, assemblies of drug amphiphiles increase the density of antigens on the surface of platforms and also eliminate the content of useless components in drug formulation, thus lowering the biosafety, decreasing production cost, and simplifying drug administration. Combining the traditional strategy with the burgeoning approaches, it is promising to develop peptide delivery system for cancer vaccines to improve their immunogenicity.

In the case of drug amphiphiles, Tirrell and coworkers [87] developed the pioneering work of antigen amphiphiles by attaching two palmitic chains to a cytotoxic T-cell epitope from ovalbumin, i.e., OVA₂₅₃₋₂₆₆ (SIINFEKL), leading to antigen amphiphile DiC16-OVA (Fig. 6). Self-assembly of DiC16-OVA amphiphiles led to formation of cylindrical micelles with a diameter of approximately

8 nm and a length distribution mainly ranging from 200 to 500 nm. The resulting cylindrical micelles consisted of a hydrophobic core composed of alkyl tails and a hydrophilic surface displaying antigen epitopes. Under physiological condition, the antigen micelles are stable with a lifetime over hours, which is beneficial for transportation and accumulation of antigen to lymph nodes. Cellular assays showed that incubation of cells in the presence of diC16-OVA assemblies did not lead to stimulation of DC cells for immune response. *In vivo* studies showed that treatment of tumor-bearing mice induced suppression of tumor growth and prolonging the survival of mice through activation of cytotoxic T-cell immune response. This concept demonstrated that self-assembly of antigen amphiphiles into nanostructures is an efficient strategy for antigen delivery and development of self-adjuvanting antigen systems.

In addition to delivering single cancer vaccines, peptide assemblies were utilized to transport multiple antigens with tunable dose ratios. For this purpose, Collier and

coworkers [142] developed a strategy for creation of peptide nanofibrils able to integrate multiple proteins while maintaining their independent conformation and bioactivity (Fig. 7). The proteins were fused with a tag sequence MALKVELEKLKSELVVLHSELHKLKSEL, termed as β Tail that undergoes a slow conformational transition from an α -helix to a β -sheet in solution. Simultaneously dissolving the β Tail fusion protein, i.e., β Tail-GFP, with peptide Q11 that rapidly assembles into nanofibers led to efficient integration of fusion proteins into nanofibers. The dose of the integrated proteins within nanofibers was precisely tuned based on the concentration of proteins in solution. This method was applied to integrate different proteins, i.e., β Tail-GFP and β Tail-cutinase, into nanofibers with a controllable molar ration, in which individual protein-associated antibody titers were induced. Combining the adjuvanticity of single fusion protein with the capability for precisely integrating multiple proteins, a tailorable multi-antigen vaccine scaffold with controllable antigenic dominance based on

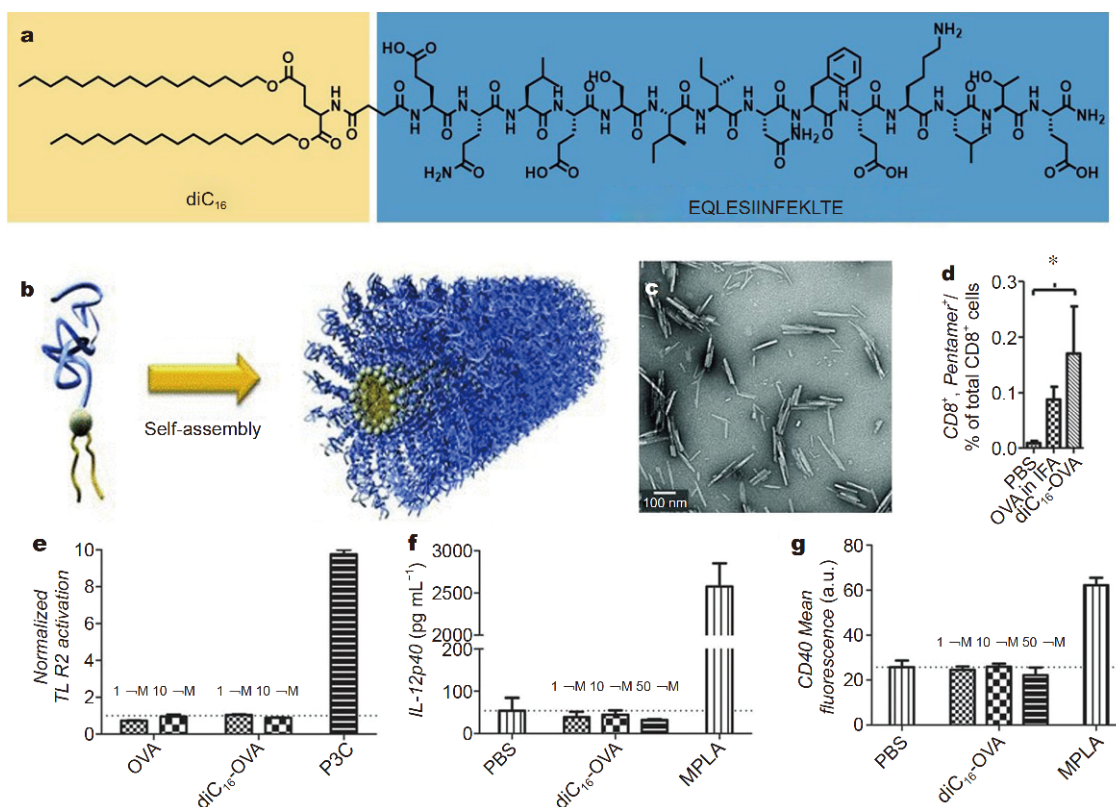


Figure 6 Self-assembled antigen amphiphiles. (a) Chemical structure of peptide amphiphile diC₁₆-OVA composed of OVA₂₅₃₋₂₆₆ and two palmitic tails. Schematic representation of self-assembly of diC₁₆-OVA into cylindrical micelles (b) and their TEM image (c). (d) Production of CD8⁺ cells induced by different treatments. **p*<0.05. Expression of cytokine TLR2 in transfected HEK cells (e), IL-12p40 in DC cells (f), and CD40 in DC cells (g) induced by various treatments. Reproduced with permission from Ref. [87]. Copyright 2012, John Wiley and Sons.

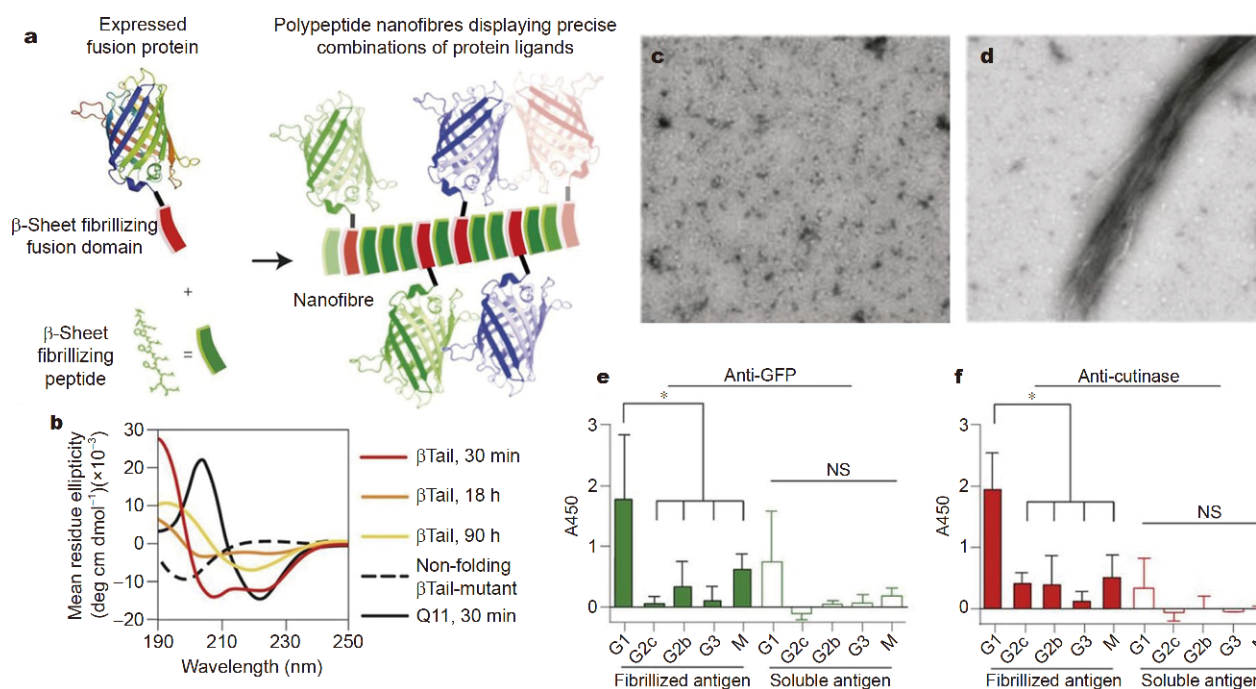


Figure 7 Supramolecular nanomaterials with integrated multiple proteins. (a) Schematic illustration of integration of multiple engineered fusion proteins with a β Tail domain into Q11 nanofibers. (b) CD spectra of peptide β Tail at different aging times, indicative of the conformational transition from α -helix to β -sheet, as well as CD spectra of Q11 and β Tail-mutant. TEM images of self-assemblies of peptide β Tail before (c) and after (d) the conformational transition. (e) Antibody polarization towards IgG1 in mice immunized with proteins GFP and cutinase co-fibrillized nanofibers, which is consistent with that immunized with individual protein. Reproduced with permission from Ref. [142]. Copyright 2014, Nature Publishing Group.

the dose of each antigen and the booster formulation was established. The multi-antigen vaccine platforms exhibit advantages of simultaneous immunity against different pathogens and high affinity for single pathogen, thus leading to great potential in cancer vaccination.

Peptide assemblies in combinatorial immunotherapy

Due to the complicated underlying mechanism for host immune operation as well as the phenotypic heterogeneity of individuals, modulating immune responses by single immune therapeutic approach is insufficient in most cases, thus leading to low immunogenicity and limiting the applications of cancer immunotherapy in clinical trials. Simultaneously integrating different therapeutics in immunotherapy has been considered to be efficient for enhancing immune responses through various pathways [143–145]. In addition, the relative long period for immune responses compared with the instant treating effect in conventional therapies such as chemotherapy and phototherapy and the usual cycle involving repetitive formulation administration for immune responses further limit the clinical application of cancer immunotherapy to the patients under the late stage of

cancers. Combining conventional therapy of tumors with immunotherapy enhances the immune responses and has synergistic effects for curative metastatic cancer treatment [146,147]. Therefore, to efficiently prolong the survival of patients, combinatorial treatments involving both conventional therapies and immunotherapy have been also developed. Due to their intrinsic capability for both covalently and non-covalently up-taking cargoes, peptide assemblies have been broadly utilized in combinatorial immunotherapies. This section covers the progress in utilization of peptide assemblies as platforms for co-delivery of multiple therapeutics towards combinatorial immunotherapy achieved recently. It is worth noting that the approaches of co-administrated immunotherapy or using administration booster [38], rather than the co-delivery strategy, will not be discussed here. In addition, the strategies using polypeptides as delivery vehicles [50] will also not be covered due to the focus on the self-assembly of peptides.

Combinatorial immunotherapy

Peptide nanostructures or hydrogels composed of peptide assemblies enable to encapsulate many immune ther-

apeutics ranging from large cargoes like immunogenic cells and antibodies, to small objects like peptides and small synthetic drugs. In particular, the hydrogelating behavior of peptide assemblies simplifies the preparation of injectable formulation and increases the maintenance of therapeutics at tumor sites during administration. In addition, peptide assemblies could be manipulated under the stimuli associated with cancer biomarkers or tumor microenvironment, thus potentially allowing for spatial and temporal on-demand release of therapeutics. Hence, utilization of peptide assemblies to co-deliver multiple immune therapeutics exhibits the great potential for enhancing immune responses in cancer immunotherapy. Here we summarize several most recent examples using peptide assemblies to co-deliver therapeutics for multiple immunotherapy.

Based on the co-delivering strategies, peptide assemblies were used to co-deliver short peptide antigens and small drug inhibitors. Nie and coworkers [148] created a peptide assembling nanoparticles based on co-assembly of an amphiphilic peptide containing with a 3-diethylaminopropyl isothiocyanate (DEAP) segment, a domain PLGLAG cleavable by matrix metalloproteinase-2 (MMP-2), and a short D-peptide antagonist (^DPPA-1), with a drug NLG919 as the inhibitor for indoleamine 2,3-dioxygenase (IDO) that is an immunosuppressive enzyme due

to its capability to hydrolyze L-tryptophan to L-kynurenine (Fig. 8). The mild acidic microenvironment induced the structural swelling of the resulting nanoparticles termed as NLG919@DEAP-^DPPA-1 due to decrease of the hydrophobicity of DEAP moieties arising from their protonation, thus facilitating the MMP-2 cleavage of PLGLAG domain and collapse of the nanoparticles and thereby release of up-loaded cargoes. Overexpression of MMP-2 by tumor cells allows for spatial release of antagonist ^DPPA-1 and drug NLG919, which target PD-L1 and IDO, respectively, around tumor sites. Flow cytometric analysis revealed that the cleaved LAG^DPPA-1 domain exhibited strong associating affinity with PD-L1 despite the addition of the three N-terminal residues. Under the mild acidic condition and in the presence of MMP-2, inhibition of IDO expression induced by treatment of NLG919@DEAP-^DPPA-1 is comparable to free NLG919. Treating melanoma-bearing mice with NLG919@DEAP-^DPPA-1 increased the level of tumor-infiltrated CTL and thereby efficiently inhibiting tumor growth.

Extending from small therapeutic molecules, peptide assemblies have been employed to co-deliver immune cell vaccines with other therapeutics. In this context, Li and coworkers [149] developed a personalized cancer vaccine (PVAX) *via* simultaneously encapsulating attenuated tu-

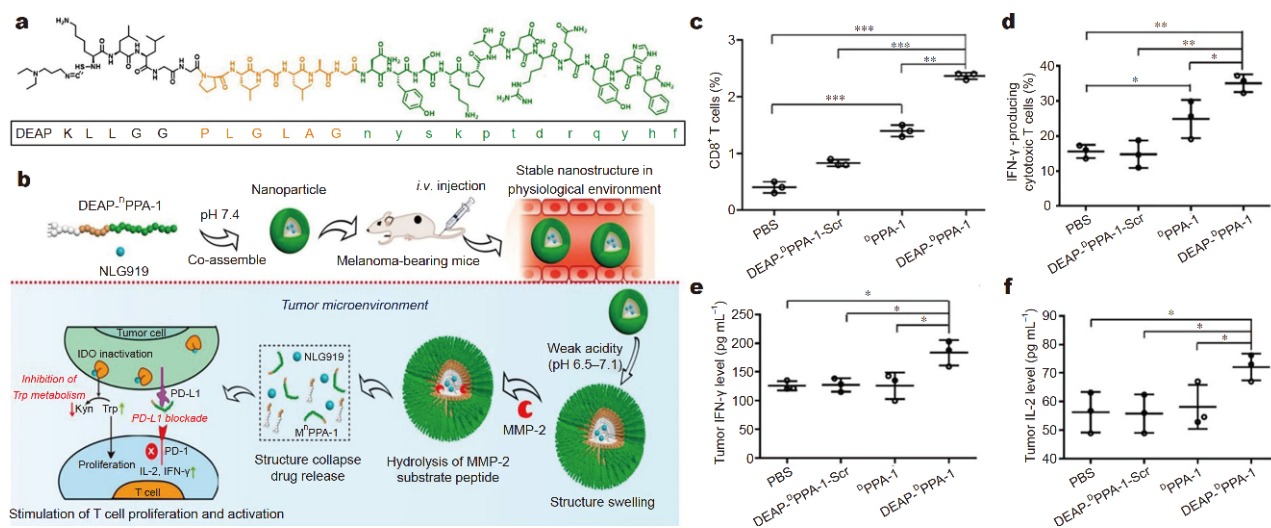


Figure 8 Sequentially responsive peptide assemblies for combinatorial anti-PD-L1 and anti-IDO immunotherapy. (a) Chemical structure of DEAP-^DPPA-1 consisting of a MMP-2-cleavable fragment PLGLAG as a linker to form the hydrophobic domain and a D-peptide antagonist ^DPPA-1. (b) Schematic illustration therapeutic mechanism of NLG919@DEAP-^DPPA-1 nanoparticles created from assembly of DEAP-^DPPA-1 and encapsulation of IDO inhibitor NLG919. Production of CD8⁺ T cells (c) and IFN-γ-producing cytotoxic T cells (d) induced by immunization of NLG919@DEAP-^DPPA-1 nanoparticles in tumors after treated on day 12. Expression of cytokines IFN-γ (e) and IL-2 (f) in mice estimated by ELISA in extracts of isolated tumors 12 days after treatment termination. **p*<0.05, ***p*<0.01, ****p*<0.001. Reproduced with permission from Ref. [148]. Copyright 2018, American Chemical Society.

mor cells and checkpoint blockades within peptide hydrogels, leading to FK@IQ-4T1 vaccine (Fig. 9). The attenuated tumor cell was collected from mouse 4T1 breast tumor xenografts and cultured in a Fcγ2b fixation and permeabilization buffer prior to hydrogel encapsulation. A small drug, i.e., JQ1, was employed as the inhibitor for bromodomain and extraterminal protein BRD4, which caused immune tolerance by controlling intratumoral expression of PD-L1. The peptide hydrogels were prepared from one sequence Fmoc-KCRGDK (FK) containing with two Fmoc groups on the N-terminal lysine residue to induce self-assembly of peptides and stabilize the hydrogels involving π, π -stacking interactions, whereas the RGD segment facilitates tumor-targeting delivery of therapeutics. To promote release of therapeutics, a fluorescent dye ICG exhibiting high photothermal conversion efficiency was co-loaded to promote the release of 4T1 and JQ1 based on the morphological transition of peptide assemblies induced by the hyperthermia effect upon exposure to laser irradiation. Combined flow cytometric and enzyme-linked immunosorbent assays revealed that FK@IQ-4T1 vaccines promoted *in vivo* and *in vitro* DC maturation, elicited $CD8^+$ CTL immune responses and blocked the PD-1/PD-L1 association *via* suppressing BRD4 activation. *In vivo* experiments further demonstrated the capability of PVAX vaccine in prevention of postsurgical tumor recurrence

and metastasis *via* eliciting memory immune responses, indicative of a robust cancer vaccine for postsurgical immunotherapy.

In addition, using peptide hydrogels as delivery vehicles, Yang *et al* [150] created a vaccine nodule *via* simultaneously encapsulating exogenous DC cell, OVA antigen, and anti-PD-1 antibody into RADA16 peptide hydrogels (Fig. 10). Peptide RADA16 is an alternating hydrophobic and hydrophilic sequence and has been demonstrated as an efficient hydrogelator to form robust peptide hydrogels [14]. Encapsulation of DC cells within the hydrogels allows for maintaining the cell viability of DC cells, prolonging their duration time at injection site, and facilitating their transportation to lymph nodes. Combination of DC cells and antigens elicits both exogenous and innate DC-associated immune responses, thus amplifying the antigen-specific T cell immunity. Additional encapsulation of anti-PD-1 antibodies into the hydrogels boosted the proliferation or infiltration of intratumoral $CD8^+$ T cells by preventing the down-regulation of MHC I induced by PD-1/PD-L1 association. While, both *in vivo* and *in vitro* experiments confirmed the maturation of DC cells and stimulation of antigen-specific effector T cells induced by Gel-DC-OVA vaccine; treating mice with Gel-DC-OVA+anti-PD-1 prolonged the survival of tumor-bearing animal and inhibited the growth of tumor significantly. The extraordinary im-

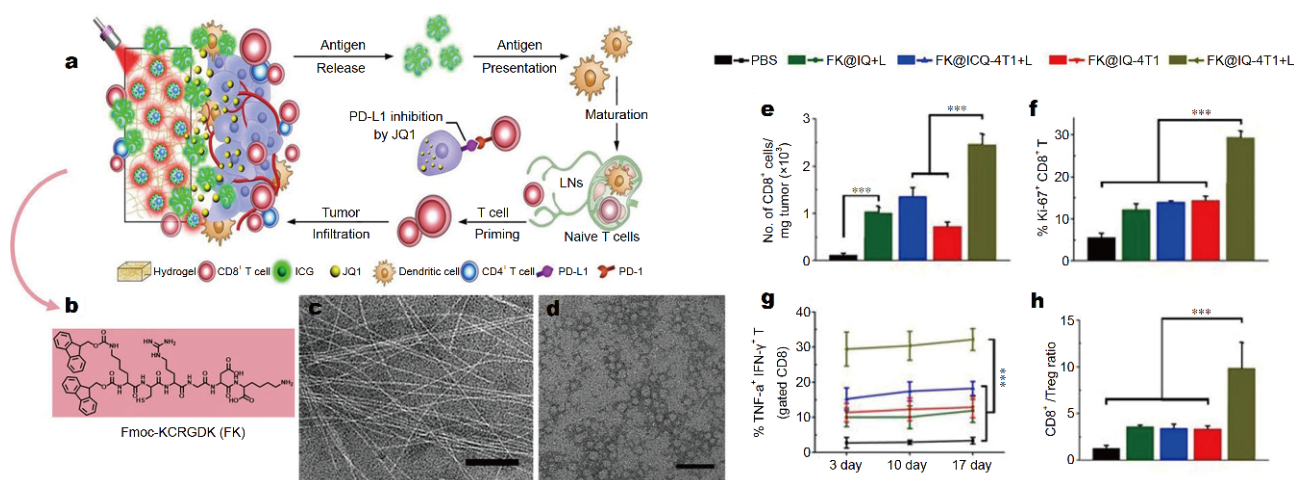


Figure 9 Peptide hydrogels for combinatorial tumor cell antigen and anti-PD-L1 immunotherapy. (a) Schematic representation of the personalized cancer vaccine (PVAX) for postsurgical immunotherapy *via* simultaneously encapsulating attenuated tumor cells and checkpoint blockades within peptide hydrogels. (b) Chemical structure of Fmoc-KCRGDK (FK) peptide. TEM image of the assemblies of peptide FK after incubation at (c) 37°C or (d) 70°C, respectively. Scale bar: 100 nm in (c) and 50 nm in (d). Tumor infiltration (e) and proliferation activity (f) of $CD8^+$ T cells in the recurrent tumors on 10 day after first treatment. (g) Frequency of $TNF-\alpha^+/IFN-\gamma^+ CD8^+$ T cells in the recurrent tumor 3 days after first treatment. (h) Ratios of $CD8^+$ T cells to Tregs in the recurrent tumor 10 days after the first treatment. *** $p < 0.01$. Data represent mean \pm s.d. ($n = 3$). Reproduced under the terms of the Creative Commons 4.0 license. [149] Copyright 2018, Nature Publishing Group.

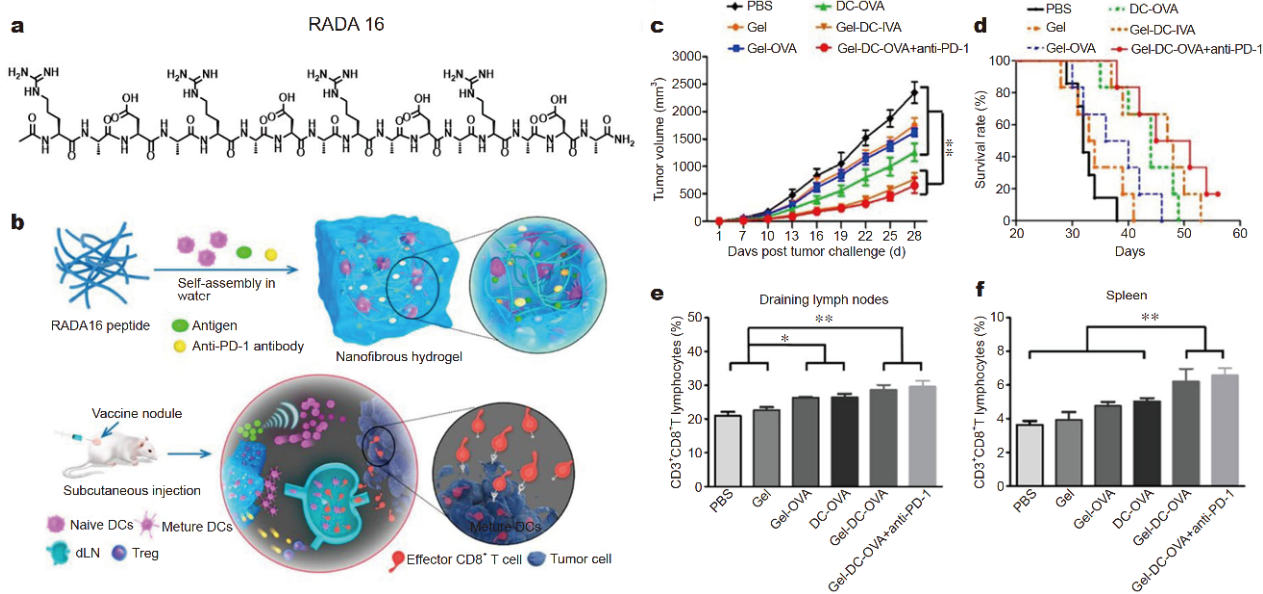


Figure 10 Peptide hydrogels for combinatorial DC-based vaccines and anti-PD-1 immunotherapy. (a) Sequence of peptide RADA. (b) Proposed mechanism of the vaccine nodule composed of RADA hydrogels, encapsulated exogenous DCs, tumor antigen, and anti-PD-1 antibody. (c) Average tumor volumes ($n = 5$) and (d) survival curves ($n = 5$) of mice after treated with vaccine nodule. Day 0 means the first day of tumor inoculation. $**p < 0.01$. (e) The ratios of $CD3^+CD8^+$ T cells in the dLNs and (f) in the spleen of vaccinated mice day 28 after tumor challenge ($n = 6$). $*p < 0.05$, $**p < 0.01$. Reproduced with permission from Ref. [150]. Copyright 2018, American Chemical Society.

munogenicity induced by Gel-DC-OVA+anti-PD-1 was attributed to infiltration of $CD8^+$ T cell into lymph nodes and suppression of intratumoral Treg cells.

Combinatorial conventional therapy and immunotherapy

In addition to combination of different immune therapeutics, peptide assemblies showed the great potential of co-delivery of therapeutics for both conventional treatments and immunotherapy. For example, both photodynamic therapy and chemotherapy are efficient for inhibiting growth of primary tumors, and also potentially causes immunogenic cell death, which is beneficial for immune responses to enhance antitumor immunity. Therefore, a combination of conventional therapy with immunotherapy exhibits the synergistic therapeutic effect, thus attracting broad attention in preclinical studies. In this context, Song *et al* [151] reported nanoparticles composed of a chimeric peptide, termed as PpIX-1MT, for combinatorial photodynamic therapy and immunotherapy (Fig. 11). Peptide PpIX-1MT consists of a hydrophobic segment including a palmitic tail and photosensitizer PpIX, and a hydrophilic part including a short PEG chain connecting to an immune checkpoint inhibitor 1-methyltryptophan (1MT) through a caspase-3-cleavable DEVD linker. Under the physiological con-

dition, peptide PpIX-1MT aggregated into nanoparticles with an average diameter of approximately 128.5 nm primarily driven by hydrophobic interactions, which targeted tumor cells based on the enhanced permeability and retention effect. Following the apoptosis of cancer cells induced by reactive oxygen species (ROS) produced by photosensitizer PpIX, the induced expression of caspase-3 cleaved the DEVD sequences and thereby releasing 1MT molecules, which is an IDO inhibitor to prevent the down-regulation of CTL cells and immunosuppression arising from Treg cells. Flow cytometric assay confirmed the immunogenic cell death caused by photodynamic therapy based on the cell-surface exposure of calreticulin, as well as activation of $CD8^+$ T cell immune responses. *In vivo* studies revealed that combining the cancer cell apoptosis and the immune activation promoted by photodynamic therapy with the enhanced immune response arising from inhibition of IDO allows for eradication of primary tumor and lung metastasis. Insight into the underlying mechanism demonstrated that the inhibition of primary tumor growth was attributed to photodynamic therapy, whereas the activated $CD8^+$ T cell immune responses eradicated the lung metastasis, thus establishing a cascaded synergistic therapeutic strategy.

In addition, Zhang's laboratory further developed the

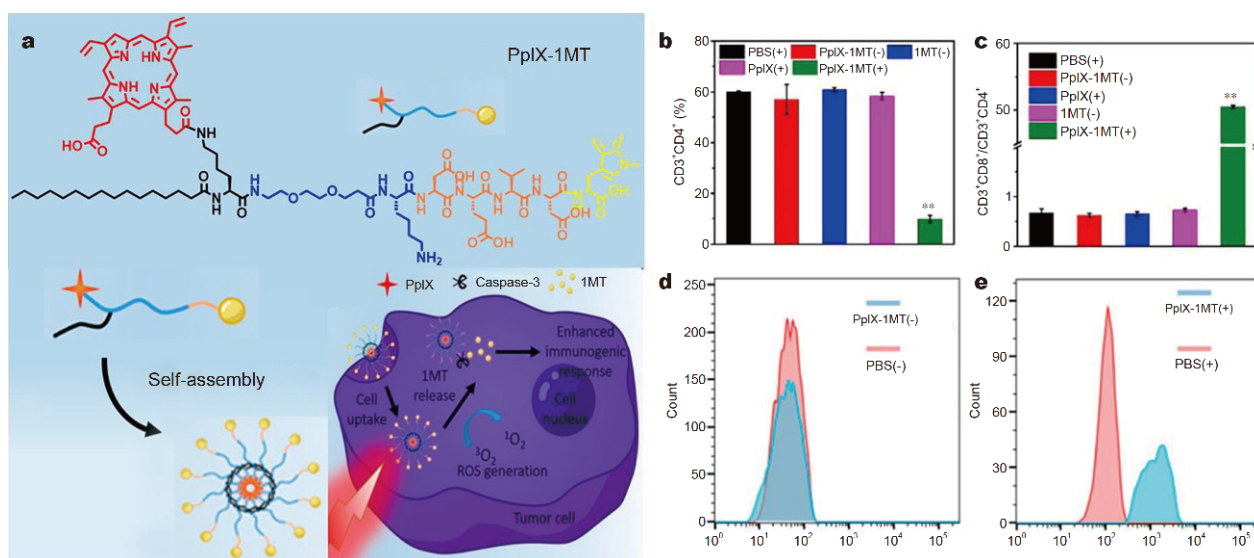


Figure 11 Combinatorial photodynamic therapy and anti-IDO immunotherapy. (a) Chemical structure of peptide PpIX-1MT and schematic illustration of self-assembly of PpIX-1MT into nanoparticles for combinational photodynamic therapy and immunotherapy. Ratio of CD4⁺ T cells to CD3⁺ lymphocytes (b) or CD3⁺CD8⁺ T cells to CD3⁺CD4⁺ T cells (c) in mice immunized in different strategies. Flow cytometry analysis of CRT exposure on the CT26 cell surface after incubation with PBS or PpIX-1MT without (d) or with (e) irradiation. Reproduced with permission from Ref. [151]. Copyright 2018, American Chemical Society.

combinatorial chemotherapy and immunotherapy for treatment of glioblastoma based on simultaneous delivery of chemotherapeutic doxorubicin (DOX) and immune checkpoint inhibitor 1MT into orthotopic glioma (Fig. 12) [152]. The co-delivering system, termed as DOX@MSN-SS-iRGD&1MT, was composed of mesoporous silica nanoparticles (MSN) loaded with drug DOX and displaying immune checkpoint blockade 1MT and tumor cell targeting epitope iRGD on the surface. While the DOX-loaded MSNs were capped by β -CDs *via* disulfide bonds, the surface displaying moieties were non-covalently attached through β -CD-adamantane association. Connecting inhibitor 1MT and adamantine *via* a DEVD domain allows for release of the inhibitor upon exposure to caspase-3, whereas release of DOX from MSNs was promoted by removal of β -CD caused by reduction of disulfide bonds by GSH. *In vitro* experiments revealed that treating glioma with DOX@MSN-SS-iRGD&1MT induced apoptosis of glioma cells and elicited antitumor immune responses. *In vivo* studies demonstrated the capability of DOX@MSN-SS-iRGD&1MT for penetrating blood brain barrier and spatially delivering and releasing DOX and 1MT at tumor sites. The synergistic therapeutic of chemotherapy and immunotherapy elicited the CTL immune responses and suppressed the activation of Treg cells, thus eventually leading to prolonged survival of glioma tumor-bearing

mice and inhibition of the growth of tumors.

SUMMARY AND OUTLOOK

Cancer immunotherapy is promising for tumor treatment due to its advantages in eliciting host immune responses to protect against local cancer cells and potentially inducing long-term immune memory to prevent cancer recurrence and metastasis. This review summarized peptide-based strategies for cancer immunotherapy in terms of the therapeutic functions of peptides or peptide assemblies and their mechanism for modulating immune responses. Due to the extraordinary biocompatibility of peptides and their protein-derived structural features, while short peptides have been utilized as therapeutics such as checkpoint blockades, antigens, and vaccine adjuvants, peptide assemblies showed advanced capability in targeting delivery or co-delivery of therapeutics in a controllable manner. Thus far many preclinical studies found the remarkable capability of peptide-based therapeutics for modulation of immune responses and inhibition of tumor growth, demonstrating the great potential of peptide-based immunotherapy in clinical trials.

Despite the progress achieved over the past decade, clinical applications of peptide-based cancer immunotherapy are still challenging and only limited examples have been approved. The primary challenge is the

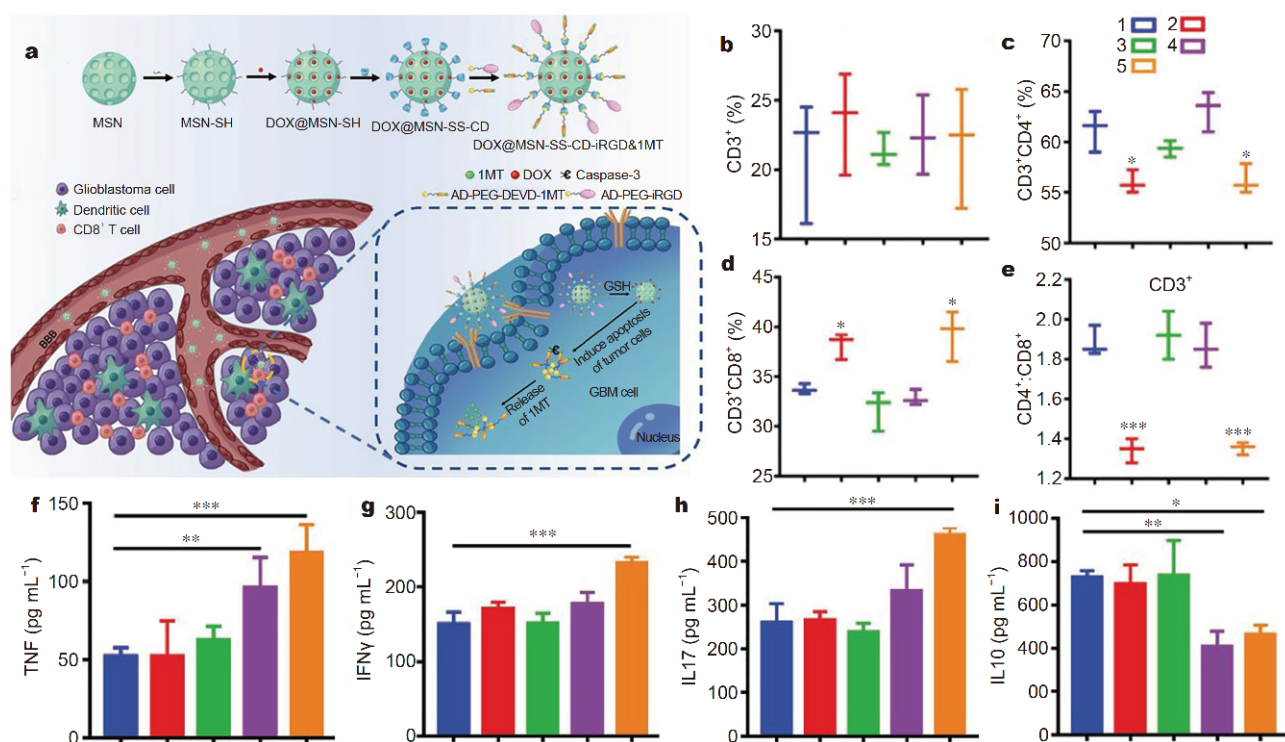


Figure 12 Combinatorial chemotherapy and anti-IDO immunotherapy. (a) Preparation of DOX@MSN-SS-iRGD&1MT and schematic illustration of DOX@MSN-SS-iRGD&1MT for eliciting antitumor immunity against glioblastoma and loading DOX for chemotherapy. (b–e) Immune responses induced by DOX@MSN-SS-iRGD&1MT *in vitro*: production of CD3⁺ T cells (b) or cytotoxic CD3⁺ CD8⁺ T cells (c) or CD3⁺ CD4⁺ T cells (d); (e) Ratio of CD3⁺ CD4⁺ T cells to CD3⁺ CD8⁺ T cells. **p*<0.05 and ****p*<0.001. (f–i) Expression of immune cytokines in orthotopic glioma tissue: (f) TNF; (g) IFN γ ; (h) IL17; and (i) IL10, in brain glioma tissue detected by ELISA. **p*<0.05, ***p*<0.01, and ****p*<0.001. From (b) to (i), 1: PBS; 2: free DOX with 1MT; 3: DOX@MSN-SS-CD; 4: DOX@MSN-SS-iRGD; and 5: DOX@MSN-SS-iRGD&1MT). Reproduced with permission from Ref. [152]. Copyright 2018, John Wiley and Sons.

relative low immunogenicity in most cases, which is attributed to many aspects [153]. Compared to large proteins as antibodies or vaccines, epitopes derived from proteins usually exhibit low selective affinity to specific targets. In addition, this association could be potentially further lowered by the phenotypic heterogeneity of targets or receptors in individuals. Another significant challenge of peptide-based immunotherapy lies in administration safety on the basis of observation of remarkable side effect and syndromes in preclinical trials. These side effect and syndromes could arise from the poor biocompatibility of therapeutics or delivery systems, off-target delivery of therapeutics, and resulting autoimmunity, among others. Although the efficacy of targeting release of therapeutics has been improved by utilizing peptide delivery systems, quantitative release of cargoes at tumor sites remains challenging [154].

Considering the aforementioned challenges, development of therapeutics with high immunogenicity and formulation with acceptable administration safety will be

the prospective developing direction of peptide-based immunotherapy. Regarding the development of new therapeutics, design of multivalent peptide checkpoint blockades, antigens, and neantigens [155] is a versatile strategy to improve the affinity of therapeutics with target substrates, thereby potentially leading to high immune responses [156]. The immunogenicity would be potentially improved by creating new delivery systems that enable to increase the infiltration and accumulation of activated T cells at lymph nodes or integrate multiple immune therapeutics with synergistic effect. In particular, establishment of multi-biomarker-controlled release of drugs and incorporation of multiple target-guiding epitopes into delivery systems likely prevent off-targeting release of therapeutics. In addition, self-assembly of drug amphiphiles based on phase collapse has also been developed as a new strategy for drug delivery, in which few useless species exist in formulations, thus perhaps improving vehicle safety. Combining the thoughts together, peptide-based cancer immunotherapy is a promising

strategy for cancer treatment in the future.

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Author contributions Li M prepared the manuscript under the guidance of Yu Z. Li M and Zhao X designed and prepared the figures. Yu Z and Dai J revised the manuscript. All authors contributed to the general discussion and revision of the manuscript.

Conflict of interest The authors declare no conflict of interest.



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多肽药物及组装体在癌症免疫治疗中的应用

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摘要 基于通过激活宿主天然免疫应答杀死癌症细胞的优势, 免疫治疗有望成为癌症治疗的新方法. 与传统治疗方法相比, 免疫治疗能够诱导长期的免疫记忆以预防癌症复发和转移, 具有更广谱的抗癌效果以及较小的副作用. 然而建立具有高生物安全性和免疫应答能力的策略仍然具有挑战性. 由于其与天然蛋白质类似的结构特征, 多肽分子有望通过直接引发免疫应答或改善药物递送效果来解决这些挑战. 本文总结了过去十年内发现的利用短肽分子作为免疫治疗药物或递送平台的癌症免疫疗法. 从简要介绍癌症免疫治疗开始, 我们概述了多肽分子的特定药物功能, 包括免疫检查点抑制剂、疫苗抗原和佐剂. 随后着重介绍了基于多肽纳米结构作为递送平台, 用于药物靶向递送或多种药物共同递送以增强免疫原性的进展. 最后对基于多肽的癌症免疫治疗面临的挑战以及未来的发展趋势进行了展望.