

Influence of particle size of nano zinc oxide on the controlled delivery of Amoxicillin

L. Palanikumar · S. Ramasamy · G. Hariharan ·
C. Balachandran

Received: 10 May 2012 / Accepted: 15 June 2012 / Published online: 5 July 2012
© The Author(s) 2012. This article is published with open access at Springerlink.com

Abstract A great effort has been exerted to develop drug carriers aiming at satisfying the requirements, such as safety, greater efficiency, predictable therapeutic response, and prolonged release period. The present study aims at developing the use of zinc oxide nanoparticles as a carrier as a function of particle size for amoxicillin drug delivery system. The amoxicillin-loaded zinc oxide nanoparticles have a good antibacterial activity against infectious Gram-positive and Gram-negative bacteria. Zinc oxide nanoparticles have been prepared by wet chemical precipitation method varying the pH values. Particle size and morphology of the as-prepared ZnO powders are characterized by X-ray diffraction, Fourier transform infrared spectroscopy and transmission electron microscope. Drug loading, in vitro drug release and antibacterial activity have been analyzed. Maximum zone of inhibition is observed for *Staphylococcus epidermis*. The results show that inhibitory efficacy of drug-loaded ZnO nanoparticles is very much dependent on its chosen concentration, drug loading, and size.

Keywords Amoxicillin · ZnO nanoparticles ·
Controlled release · Antibacterial activity

L. Palanikumar · S. Ramasamy (✉)
Crystal Growth Centre, Anna University,
Chennai 600025, India
e-mail: sinna_ramasamy@yahoo.com

G. Hariharan
Institute for Ocean Management, Anna University,
Chennai 600025, India

C. Balachandran
Division of Microbiology, Entomology Research Institute,
Loyola College, Chennai 600034, India

Introduction

Over the past few years, local delivery systems have attracted much attention due to their efficacy to improve the ingrowth and regeneration of bones and teeth (Kim et al. 2004). Drugs, such as antibiotics, anti-tumors, and growth factors, have been administered to the defect regions to induce therapeutic effects (Di Silvio and Bonfield 1999). A great deal of effort has been exerted to develop drug carriers, in the form of foams, films, and microspheres, aiming at satisfying the requirements, such as safety, greater efficiency, predictable therapeutic response and prolonged release period (Gautier et al. 2001). Due to the large surface-to-volume ratio the nanoparticles are very useful for attaching drug molecules and other compounds (De Jong and Borm 2008). Nanoscale devices, smaller than 50 nm, can easily enter most cells and circulate through the body through blood vessels (Courrier et al. 2002). The advances in micro and nano-fabrication technology have enhanced the tools available to create clinically important therapeutic applications (Lu and Chen 2004).

Controlled drug delivery is the technology by which the drugs can be released at a predetermined rate for a long period of time in the blood stream or delivered at the target site (Kamaly et al. 2012). Unlike the traditional oral, intravenous drug delivery methods whereby the drug is distributed to both healthy and diseased tissue, in controlled local drug delivery high concentration of drug is achieved at the infected site. This leads to increase in therapeutic index and therapeutic efficacy and abridged side effects to other organs (Melville et al. 2008; Noel et al. 2008). Drug stability, optimized drug absorption, treatment continuation in natural phase improvement in pharmacokinetic characteristics of drug can be achieved by localized

drug delivery (Smola et al. 2008). In controlled drug delivery system, the carrier plays a vital role since they incorporate the drug, retain it, and release it progressively with time. So, properties such as (1) drug incorporation and release, (2) formulation stability and shelf life, (3) biocompatibility, (4) bio-distribution, and (5) functionality must be analyzed thoroughly when choosing a carrier for delivery of drugs. The drug release from any carrier depends upon solubility of drugs, microstructure of carrier, degradation of carrier, and the bond between the drug and carrier (De Jong and Borm 2008). The application of nanotechnology to medical applications, commonly referred to as “nanomedicine”, seeks to deliver a new set of tools, devices and therapies for treatment of human disease (Rasmussen et al. 2010). The potential use of zinc oxide (ZnO) and other metal oxide nanoparticles in biomedical and cancer applications is gaining attention in the scientific and medical communities, largely due to the physical and chemical properties of these nanomaterials (Rasmussen et al. 2010). ZnO is one of the five zinc compounds which are currently recognized as safe for nutrients by the US Food and Drug Administration (21CFR182.8991). ZnO nanoparticles (NPs) are widely used in many consumer products like cosmetics, toothpaste, textiles, and skin lotions (Ng et al. 2010).

Amoxicillin trihydrate is a semi synthetic antibiotic with a broad spectrum of bactericidal activity against many Gram-positive and Gram-negative, aerobic and anaerobic microorganisms. It does not resist destruction by β -lactamases; therefore, it is not effective against β -lactamase-producing bacteria. Chemically, it is d(-)-a-amino-p-// hydroxybenzyl penicillin trihydrate. Amoxicillin is an excellent agent to treat otitis media, bacterial sinusitis, and bacterial exacerbations of bronchitis, acute lower-urinary-tract infections, gonorrhoea, and typhoid (Khuroo et al. 2008). *Staphylococcus aureus* and *Staphylococcus epidermidis* are natural inhabitants of human and animal skin, but it can sometimes cause infections that affect many organs (Bhunia 2008). *S. aureus* is one among the most important pathogens that cause bone and joint infections, soft tissue and overwhelming sepsis and express many surface adhesions that promote attachment to plasma and extra cellular matrix (ECM) proteins of the host cell (Venkatasubbu et al. 2011). The pathogenic bacteria *Klebsiella pneumonia* and *Enterobacter aerogenes* are the major causative agents of noso-comial infections (Saonum et al. 2008). Serotype paratyphi B var. L (+) tartrate (+) causes a typical *Salmonella gastroenteritis* instead of enteric fever (Prager et al. 2003).

In the present work different sizes of zinc oxide were synthesized in nano form and characterized. Amoxicillin was loaded to these ZnO nanoparticles. The various parameters for drug loading were optimized. The drug

loading percentage, stirring time and the influence of drug release profile on these parameters were analyzed. The interaction between nanoparticles and drug was analyzed. Antibacterial response of drug-loaded nanoparticles against infectious Gram-positive and Gram-negative microbes was investigated.

Materials and methods

Synthesis and characterization of ZnO nanoparticles

Zinc oxide nanoparticles were synthesized with a slight modification suggested by Wu et al. (2006) from aqueous solutions of zinc nitrate ($\text{Zn}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$) (purchased from Fischer Chemicals, Mumbai, India; Purity 96 %) and hexamethyltetramine (HMT) ($\text{C}_6\text{H}_{12}\text{N}_4$) (purchased from Qualigens Chemicals, Mumbai, India; Purity 99 %). The two chemicals were mixed separately with milli-Q water to a concentration of 0.05 M for the ($\text{Zn}(\text{NO}_3)_2$) solution and 1.5 M for the HMT solution. The separate solutions were stirred for 30 min each and then mixed with 130 rpm stirring. The solutions were adjusted to the desired pH (5.0, 6.0 and 7.2) and heated to 80 °C for 45 min. The product was collected by centrifugation (Compufuge, Model CPR 32, Remi Electrotechnik Limited, Thane, India). The ammonium hydroxide solution (one normality solution) was added to pH 5.0 synthesized solutions to enhance the formation of ZnO at 80 °C (Wu et al. 2006).

Particle characterization

Powder X-ray Diffraction (XRD, Seifert, JSO-DE BYE-FLEX 2002, Germany) was used to identify the crystalline phase composition and purity. The phase was found to be hexagonal and no impurity peaks were found. The morphology and grain size of the ZnO were observed by TECNAI G^2 Model T-30 S-twin high-resolution transmission electron microscopy (HRTEM). The quality of the ZnO NPs was analyzed by FTIR (FTIR, Perkin Elmer Spectrum One). The size distributions were performed in a dilute aqueous nanoparticle suspension at pH 7.0 with particle size analyzer (Malvern S particle size analyzer).

Drug loading

In order to load the drug into ZnO nanoparticles, amoxicillin trihydrate was dissolved in 100 ml of distilled water at different concentrations (1, 3, 5 and 10 %). 1 g of different sizes of ZnO nanoparticles was added to all the three drug solutions and stirred using magnetic stirrer at 600 rpm for various time periods (30, 60 and 120 min) at room temperature. Then the solution was left undisturbed

overnight. The suspension was then centrifuged at 5,000 rpm for 5 min and the supernatant and precipitate were separated. The amount of loaded drug was determined by finding the difference in amoxicillin concentration in the aqueous solution before and after drug loading. Percentage of drug loading was calculated using the following equation:

$$\text{Percentage of drug loading} = [(A - B)/A] \times 100$$

where A and B represent the initial and final drug concentration of the aqueous drug solution (Hamblett et al. 2004; Venkatasubbu et al. 2011). The attachment of amoxicillin with ZnO nanoparticles was analyzed by FTIR (FTIR, Perkin Elmer Spectrum One).

In vitro drug release studies

In order to determine the drug release profile, 100 mg of the drug loaded ZnO nanoparticles was introduced into a screw-capped (100 ml) glass bottle containing 50 ml of phosphate-buffered saline (PBS) medium at 37 °C and pH 7.4 under sterile condition. In vitro drug release study was done for a period of 650 h. 5 ml samples were withdrawn by a pipette and centrifuged at 5,000 rpm and replaced immediately with 5 ml of fresh PBS medium, which was accounted for when calculating the amount released. Amoxicillin concentration in the supernatant was measured spectrophotometrically at a wavelength of 230 nm. The pH in the media at different intervals was estimated. The experiments were repeated thrice.

Antimicrobial assay

The antibacterial assay of drug-loaded ZnO nanoparticles with different sizes was tested by disc-diffusion method (Jayaseelan et al. 2012). The following bacteria were used for the experiments: *Salmonella* paratyphi-B, *Klebsiella pneumoniae* MTCC 109, *Bacillus subtilis* MTCC 441, *Enterobacter aerogenes* MTCC 111 and *Staphylococcus epidermidis* MTCC 3615. The reference cultures were obtained from Institute of Microbial Technology (IMTECH), Chandigarh, India-160 036. Petri plates were prepared with 20 ml of sterile Mueller–Hinton agar (MHA) (Himedia, Mumbai). The test cultures were swabbed on the top of the solidified media and allowed to dry at room temperature for 10 min. The suspension of drug loaded nanoparticles (in milli-Q water) was used to prepare 50, 100 and 200 $\mu\text{g ml}^{-1}$ added to each well separately (8 mm diameter). Amoxicillin trihydrate (25 $\mu\text{g}/\text{disc}$; purchased from Himedia Chemicals Ltd., Mumbai, India) was used as positive control. The plates were incubated for 24 h at 37 °C. Zones of inhibition were recorded in millimeters by repeating the experiment thrice for each concentration.

Statistical analysis

Experiments were repeated thrice and results were presented as means and standard deviations from the three replicates. Drug release, pH buffer data, and antimicrobial assay were evaluated by one-way analysis of variance (ANOVA) in combination with Tukey's multiple comparison tests. A significance level of $P < 0.05$ was considered statistically significant.

Results and discussion

The present study employed a low-temperature synthesis method to prepare ZnO NPs. Zinc nitrate and HMT solutions were mixed at 80 °C for 45 min at different pH. After precipitation of ZnO, the pH value was found to be 8.2. The XRD pattern of synthesized ZnO nanoparticles demonstrated that the nano ZnO to be crystalline in nature, and the diffraction peaks matched very well with hexagonal zincite phase of ZnO (Fig. 1). The diffraction pattern and inter-planar spacing closely matched those in the standard diffraction pattern of ZnO (powder diffraction file ICDD 36-1451: $a = 3.249 \text{ \AA}$ and $c = 5.206 \text{ \AA}$). The XRD peaks show (100), (002), (101), (102), (110), (103), (200), and (201) reflection lines of hexagonal zincite phase of ZnO particles. No characteristic peaks of any impurities were found suggesting good-quality ZnO nano powders. The particle size based on broadening has been analyzed by Scherrer formula, modified forms of Williamson-Hall analysis, and size-strain plot method. The crystalline size can be calculated using the following equation:

$$(d_{hkl}\beta_{hkl} \cos \theta)^2 = K/D(d_{hkl}^2\beta_{hkl} \cos \theta) + (\varepsilon/2)^2$$

where K is the constant that depends on the shape of the particles. The particle size has been determined from the slope of linearly fitted data. The root of the y intercept gives the strain (Zak et al. 2011).

The functional or composition quality of the synthesized product has been analyzed by the FTIR spectroscopy. Figure 2 shows the FTIR spectrum acquired in the range of 400–4,000 cm^{-1} . The band at 535 cm^{-1} corresponds to the stretching vibration of Zn–O bond. The broad absorption bands in the range 3,900–2,350 cm^{-1} and 1,637 cm^{-1} correspond to the presence of the surface hydroxyl groups (Sharma et al. 2009). C–OH stretching (1,387 cm^{-1}) is detected from the FT-IR spectrum (Song et al. 2008). The band at 1,387 cm^{-1} corresponds to the CH₂ deformation, and absorption bands at 1,235–1,125 cm^{-1} are responsible for CN stretch. 998 cm^{-1} and 897 cm^{-1} correspond to CH₂ rock (Bernstein et al. 1994). The TEM image of pure ZnO nanoparticles is presented in Fig. 3. The insert Fig. 3 is particle size distribution as measured by dynamic light

Fig. 1 XRD Pattern of ZnO prepared at different pH. **a** As-prepared, **b** pH 6.0, **c** pH 5.0

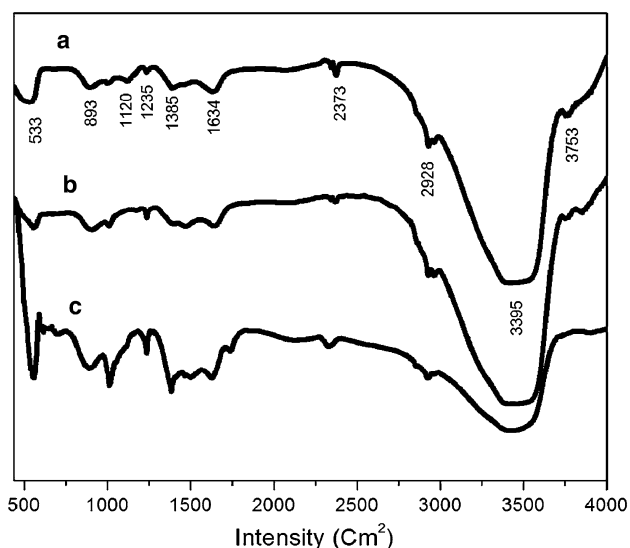
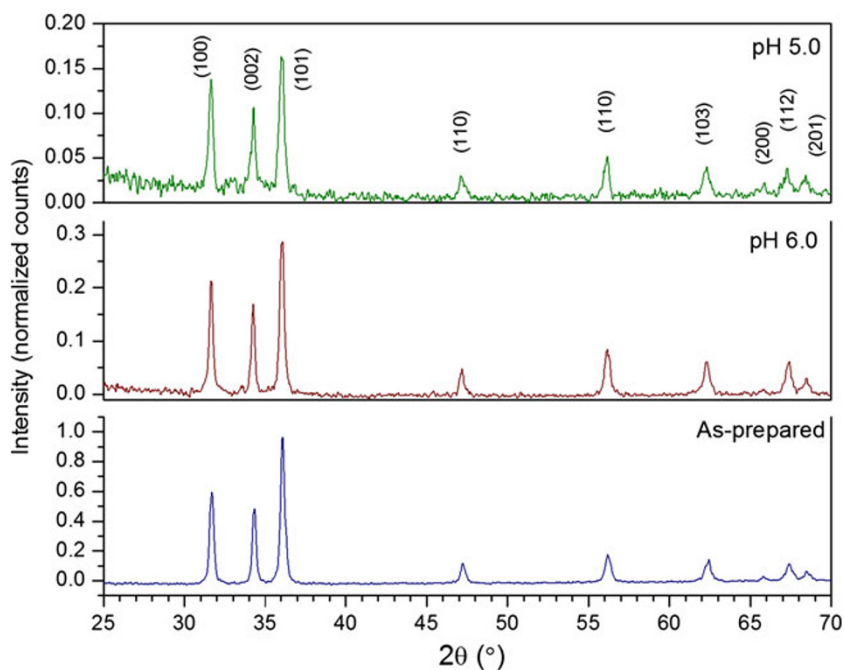


Fig. 2 FTIR spectrum of as-prepared ZnO nanoparticles. **a** As-prepared, **b** pH 6.0, **c** pH 5.0

scattering (DLS). The TEM images confirm the formation of hexagonal structure of ZnO and are in agreement with the XRD results. The particle size of the ZnO prepared at different pH are 38 ± 2 , 25 ± 4 and 15 ± 4 nm in as-prepared, pH 6.0 and 5.0 respectively.

The structure of the amoxicillin-loaded ZnO nanoparticles analyzed using FTIR spectroscopy is shown in Fig. 4. Characteristics bands of both ZnO and amoxicillin are observed for all ZnO/drug samples. The ZnO nanoparticles loaded with drug represent mixed bands typical of ZnO

nanoparticles, where $3,900\text{--}2,375\text{ cm}^{-1}$ corresponds to the presence of the surface hydroxyl groups and amoxicillin major peaks observed at $3,359\text{ cm}^{-1}$ (amide NH and phenol OH stretch), $2,971$ and $2,375\text{ cm}^{-1}$ benzene ring CH stretch, $1,583\text{ cm}^{-1}$ benzene ring C=C stretch, $1,398\text{ cm}^{-1}$ (NH bend CB stretch combination band and NH^{3+} symmetric deformation (Kumar et al. 2011)). The peaks observed between $1,573$ and 739 cm^{-1} in amoxicillin-loaded ZnO nanoparticles comply with peak of ZnO and amoxicillin trihydrate and indicate that the amoxicillin is compatible with ZnO.

Drug loading

The drug loading efficiency of ZnO nanoparticles has been examined as described previously. It is dependent on the concentration of drug, size of nanoparticles and the ratio of drug and ZnO NPs. The drug loading percentage increases with increase in these parameters. It increases and becomes constant at a particular level. The variation in drug loading with change in drug concentration is shown in Table 1. For 1 and 3 % drug concentration, the drug loading is 60 and 80 % and it increases to 90 % at 5 and 10 % drug concentration and remains to be 90 % for both these concentrations for 15 nm size ZnO. The drug loading is 87 % for 5 and 10 % drug concentration in 25 and 38 nm ZnO NPs. The variation in drug loading with change in stirring time is given in Table 2. With 1 and 3 % drug concentration and stirring at 30 min, the drug loading is found to be 37 and 49 % and it increases to 62 and 79 % at 5 % and 10 % drug concentration for 15 nm ZnO NPs. Maximum drug

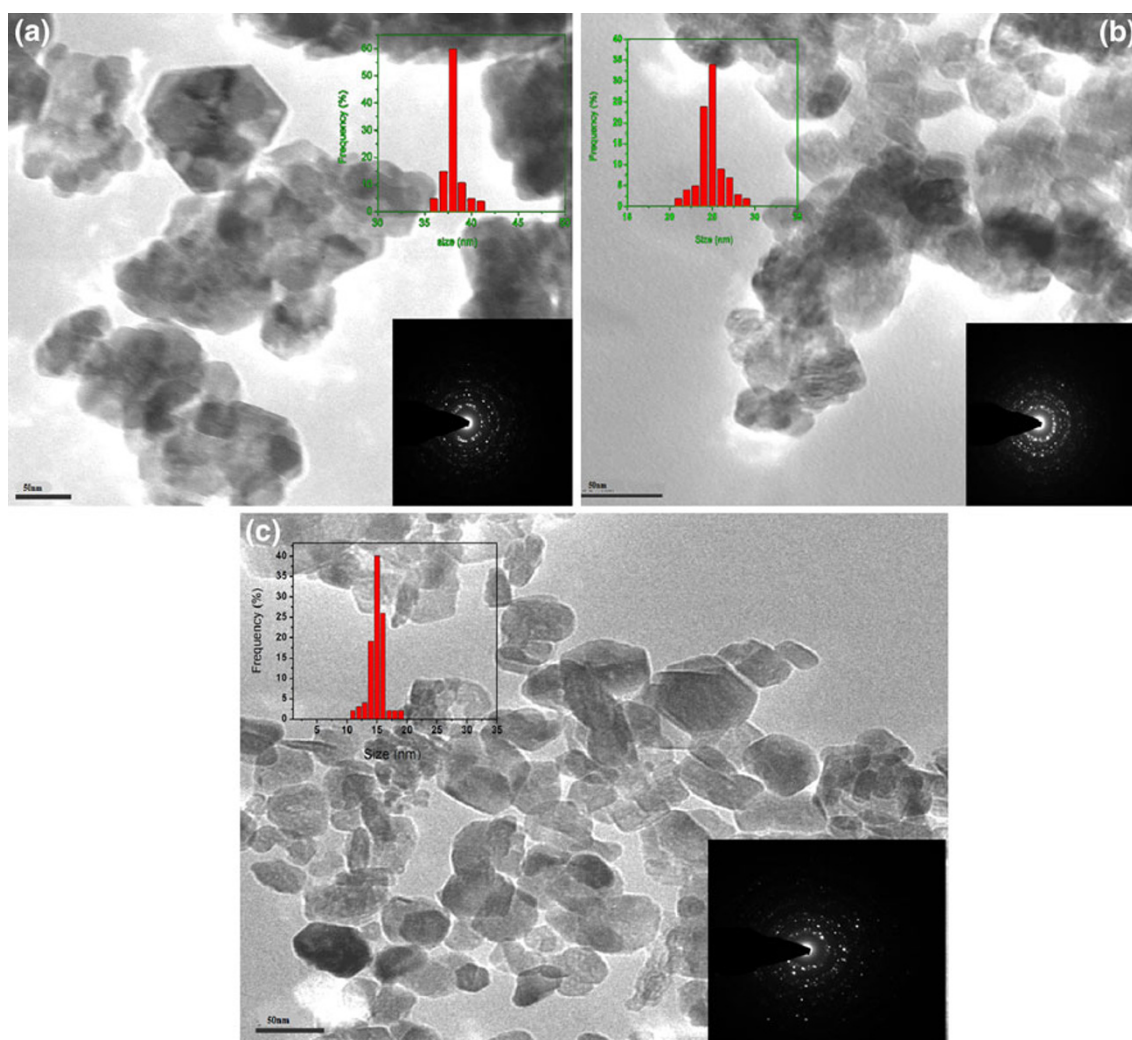


Fig. 3 TEM images of ZnO nanoparticles prepared at different pH (*inset picture* describes particle distribution and size in aqueous suspension). **a** As prepared, **b** pH 6.0, **c** pH 5.0

loading is obtained at 60 and 120 min and then it becomes constant for all the three different sizes of nanoparticles.

In vitro drug release

Many carrier systems are used for the controlled delivery of amoxicillin. Polyethyleneglycol-coated polycyanoacrylate nanoparticles loaded with amoxicillin have been used for phagocytic uptake (Fontana et al. 2001). The study reports the release profile of amoxicillin at different pH 7.4, 4.0 and 1.1 in comparison with urease. This work reports the release studies at pH 7.4 and in human plasma evidences that the amoxicillin release occurs with a biphasic profile with an initially rapid followed by zero-order kinetics. Nanoparticles incorporated in pH-sensitive hydrogels as amoxicillin delivery for eradication of *Helicobacter pylori* (Chang et al. 2010). The results of drug releasing in vitro study clearly indicate that the amount of

amoxicillin released from nanoparticles incorporated in hydrogels in pH 1.2 is relatively low (14 %), compared with that from only nanoparticles (50 %). The sustained release of amoxicillin from chitosan tablets was investigated by Sahasathian et al. (2007). These authors have shown that chitosan with the particle size less than 75 μm is able to provide a significantly improved sustained release profile of amoxicillin compared with release profile of a commercial capsule. Amoxicillin release kinetics of gamma-irradiated chitosan/pHEMA membranes have shown that the amount of drug release is dependent on membrane network crosslinking due composition, radiation and membrane thickness (Casimiro et al. 2007).

In this work, amoxicillin has been loaded on ZnO to investigate the efficacy of the drug delivery system. The different drug release profiles are illustrated in Fig. 5. The estimated percentages of drug released in 648 h are found to be 60, 80, and 90 % from 1, 3, 5, and 10 % drug-loaded

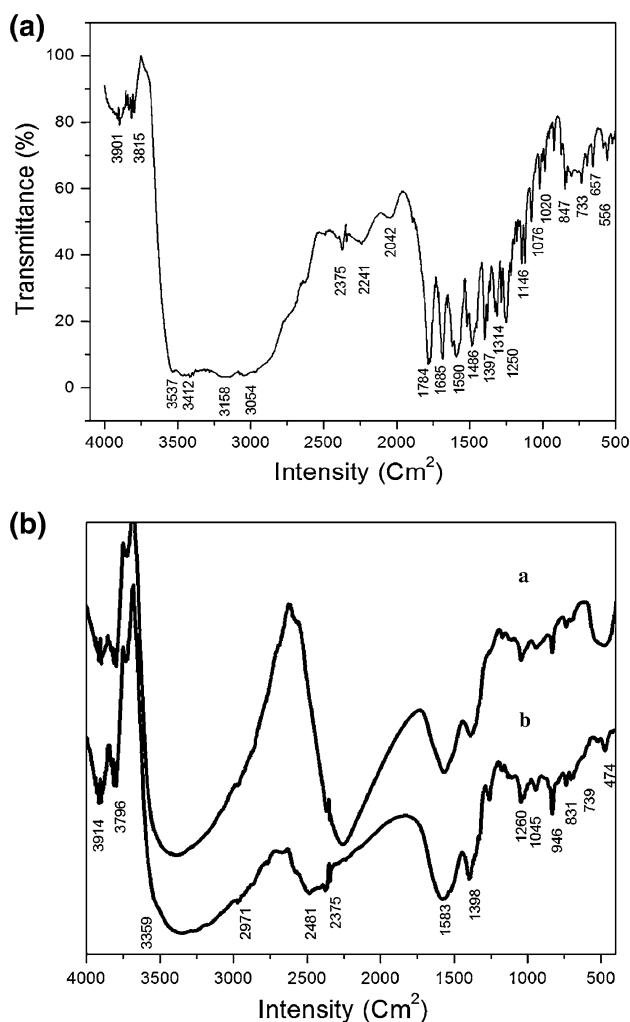


Fig. 4 FTIR Spectrum of drug loaded nanoparticles. **a** FTIR spectrum of amoxicillin, **b** FTIR spectrum of drug loaded 15 nm ZnO NPs at *a* 1:3 ratio and *b* 1:5 ratio

Table 1 Drug loading percentage with various concentrations

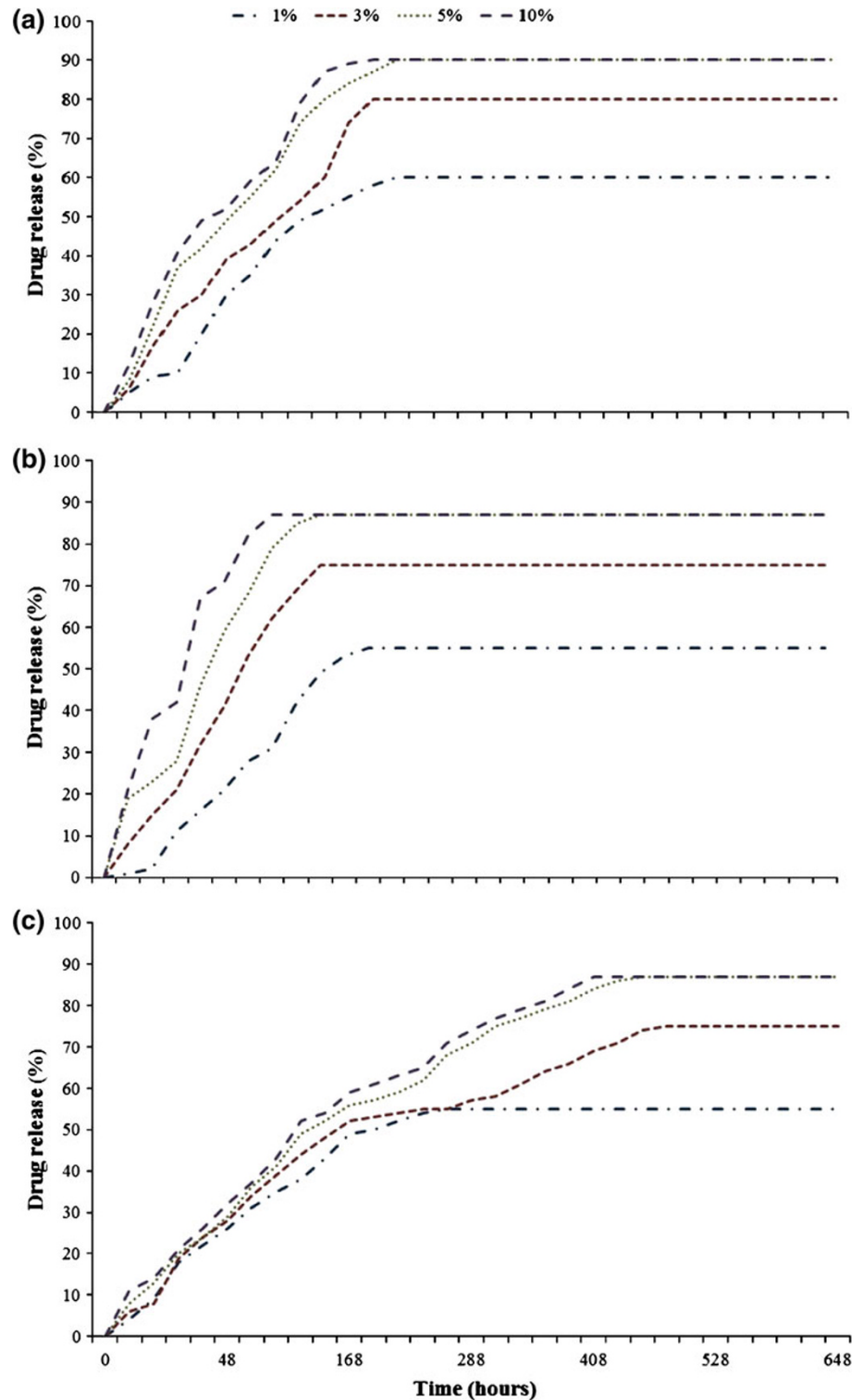
Drug concentration (%)	Drug loading
15 nm ZnO NPs	
1	60
3	80
5	90
10	90
25 nm ZnO NPs	
1	55
3	75
5	87
10	87
38 nm ZnO NPs	
1	55
3	75
5	87
10	87

Table 2 Drug loading percentage with different stirring time

Drug concentration (%)	Stirring time (min)	Drug loading
15 nm ZnO NPs		
1	30	37
	60	60
	120	60
3	30	49
	60	80
	120	80
5	30	62
	60	90
	120	90
10	30	79
	60	90
	120	90
25 nm ZnO NPs		
1	30	31
	60	55
	120	55
3	30	34
	60	75
	120	75
5	30	45
	60	87
	120	87
10	30	54
	60	87
	120	87
38 nm ZnO NPs		
1	30	27
	60	55
	120	55
3	30	30
	60	75
	120	75
5	30	36
	60	87
	120	87
10	30	46
	60	87
	120	87

samples, respectively. The drug release increases gradually over a period of time. This shows that the drug is released in a controlled manner. The amount of drug released in 24 h of time is well above the minimum inhibition concentration of amoxicillin which is up to $25 \mu\text{g ml}^{-1}$ for infectious pathogens. Such an observed release profile will provide a rapid delivery of drug to give antibacterial effects at the infected site and a sustained release to aid long-term

Fig. 5 Drug release profile in
a Amoxicillin loaded on
 15 nm ZnO nanoparticles,
b Amoxicillin loaded on
 25 nm ZnO nanoparticles,
c Amoxicillin loaded on 38 nm
 ZnO nanoparticles



healing and avoid the toxic and adverse systemic effects caused by high concentration of antibiotics. The release of drug from ZnO NPs exhibits a two stage release mechanisms. The drug release is high during the initial time and then it reduces and becomes stable. Amoxicillin release during the initial burst stage is due to adsorption of drug

molecules that are located on the surface of the particles (Fontana et al. 2001). These particles do not strongly interact with the ZnO NPs. During the in vitro drug release analysis, the ZnO absorbs the surrounding fluids into the nanoparticles. This leads to the dissolution and exclusion of the loaded amoxicillin. The smaller the particles, the more

Fig. 6 Antimicrobial activity of amoxicillin-loaded ZnO nanoparticles in **a** gram-positive bacteria, **b** Gram-negative bacteria. * $P < 0.05$ statistically significant when compared with control

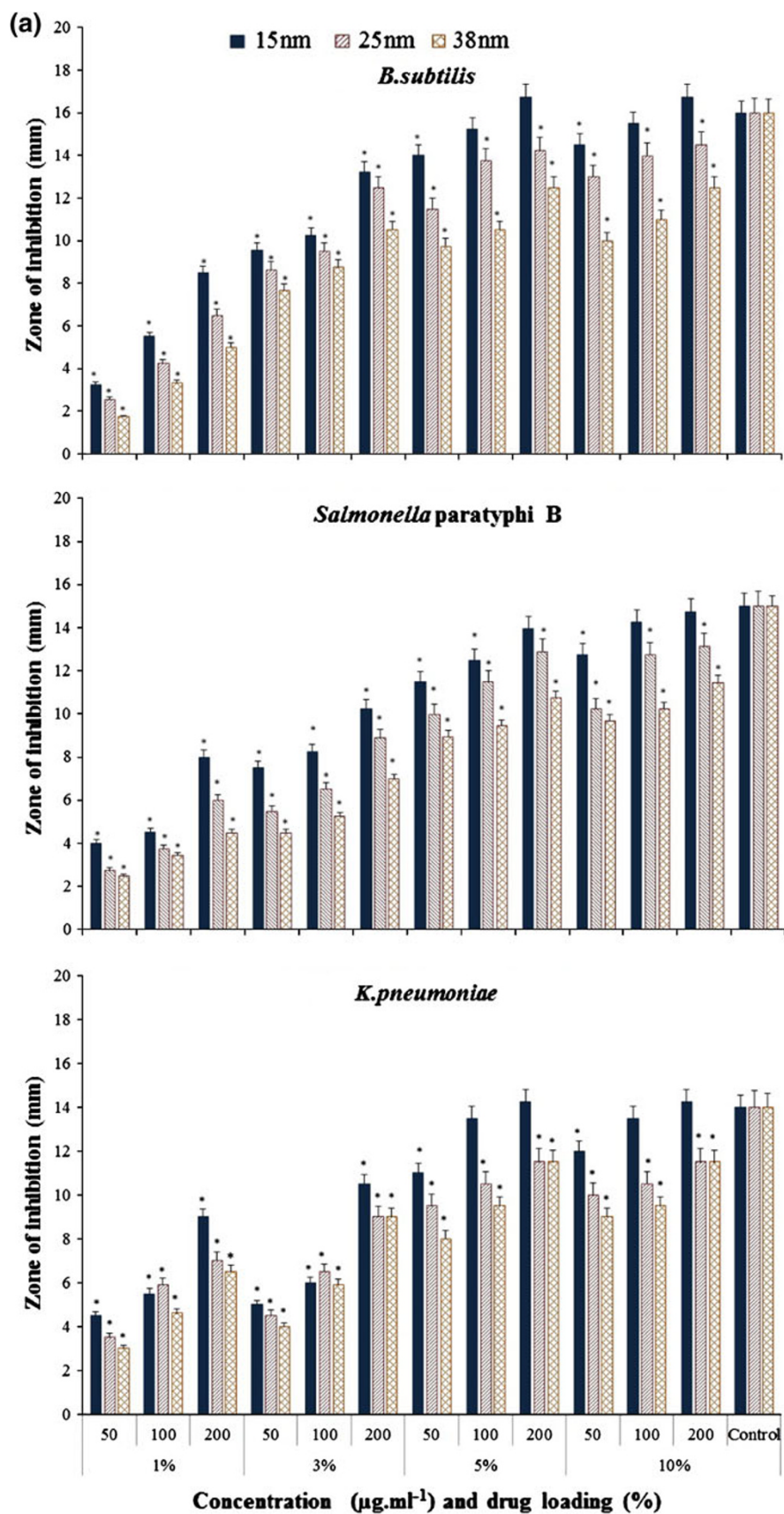
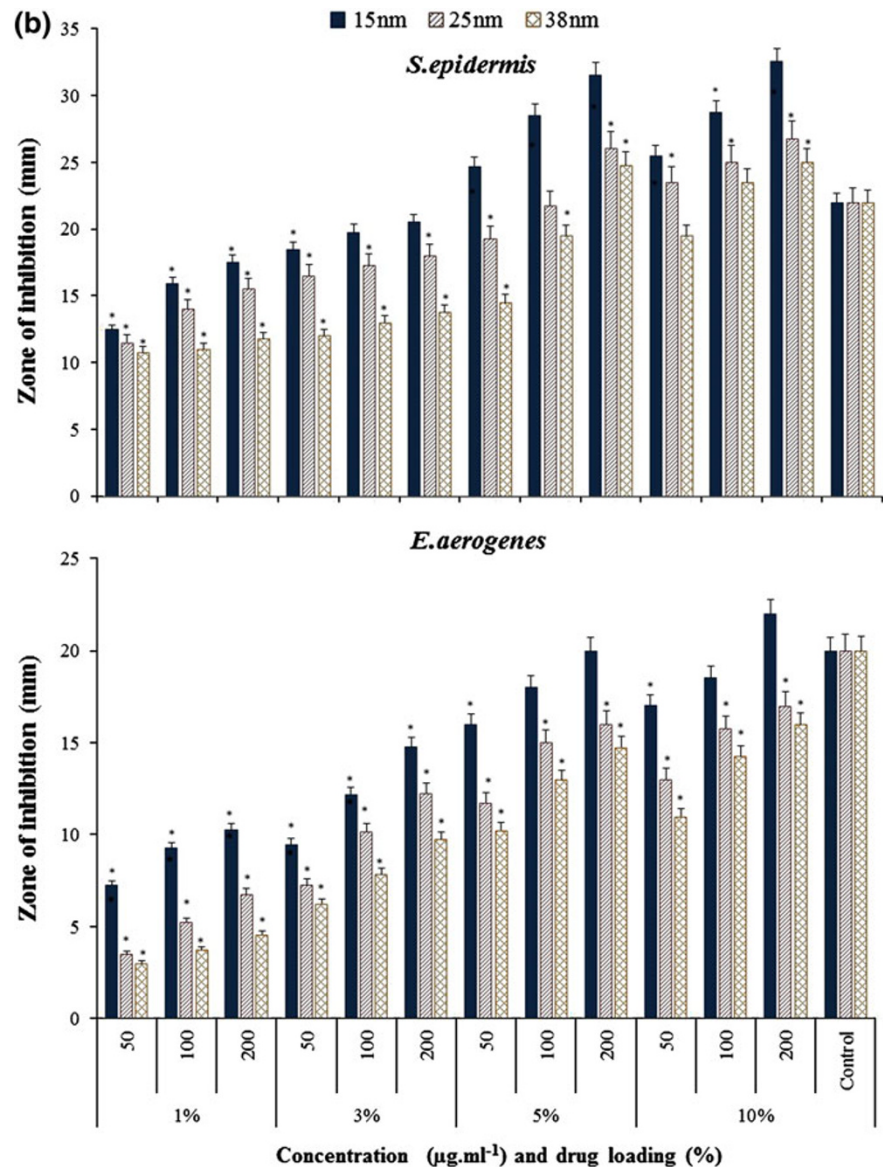


Fig. 6 continued



the exposure of amoxicillin to the fluid. When the loosely adsorbed drug has almost completely desorbed, the drug release becomes slow. The slow release of amoxicillin is due to the incorporation of the drug ZnO NPs.

Antibacterial activity

The re-emergence of infectious diseases poses a serious threat to public health. The increasing rate of the appearance of antibiotic-resistant strains in a short period of time within both Gram-positive and Gram-negative microorganisms is a major public health concern (Jones et al. 2008). Alternative therapeutics to control and prevent the spread of infections in both community and hospital environments are required (Sharma et al. 2009). The results of antibacterial activity of different sizes of drug-loaded ZnO NPs are

shown in Fig. 6a and b. The zone of inhibition (in mm) reflects magnitude of susceptibility of the microorganism. The strains susceptible to nanoparticles exhibit larger zone of inhibition, whereas resistant strains exhibit smaller one. Significant difference between each concentration has been compared. Maximum zone of inhibition has been observed for *S. epidermis*. Increase in drug loading concentration significantly ($P < 0.05$) increases the zone of inhibition from 1 to 3 % drug concentration. Insignificant differences between zones of inhibition are observed for 5 and 10 % drug concentration. Highest zones of inhibition are observed for drug-loaded 15 nm ZnO NPs.

The antibacterial activity of ZnO NPs from the present results suggests that ZnO nanoparticles may play differential response to various tested microorganisms. This may be consistent with the prediction that *S. epidermis* can

metabolize Zn^{2+} as an oligo element (Roselli et al. 2003). Similarly, metal-ion homeostasis is important for bacterial life because of their involvement in the regulation of a wide array of metabolic functions asco-enzymes, cofactors, and catalysts, and as structural stabilizers of enzymes and DNA-binding proteins (Padmavathy and Vijayaraghavan 2003). However, excess metal or metal ions are toxic for bacterial cells. Therefore, certain bacteria have developed mechanisms to regulate the influx and efflux processes to maintain the steady intracellular concentration of metal ions, including the Zn^{2+} ion (Gaballa et al. 2002). The higher antibacterial activity of drug loaded ZnO nanoparticles in *S. epidermis* may involve the production of reactive oxygen species (ROS) and the deposition on the surface or accumulation in the cytoplasm of the cells as observed in earlier studies for *S. aureus* (Raghupathi et al. 2011). The results obtained in our study indicate that the inhibitory efficacy of drug-loaded ZnO nanoparticles is very much dependent on its chosen concentration, drug loading, and size which are similar to other related findings (Yin et al. 2010; Wahab et al. 2010).

Amoxicillin trihydrate is currently marketed as tablets (floating tablets) of 250 and 500 mg. The long-term administration of amoxicillin trihydrate is required against *Streptococcal pharyngitis* (<http://www.healthystock.net/drugs/amoxicillin.shtml>).

The presently available conventional therapy is associated with a number of drawbacks such as highly variable absorption and low bioavailability after oral administration (Bhosale et al. 2011). Furthermore, with increase in dose, there is decrease in bioavailability. Maximal therapeutic efficacy needs to be coupled with minimal toxicity, a goal which can be achieved by formulating drugs with nanoparticles (Horwitz et al. 2010).

Conclusion

A drug delivery system with different sizes of ZnO NPs has been developed to treat against infectious bacteria. ZnO NPs can be used as drug delivery system for the controlled delivery of amoxicillin. The antimicrobial property increases with increase in the drug loading and becomes stable at 5 and 10 % drug loading. The drug loading depends on the size of nanoparticles, concentrations of drug, and stirring time. The drug loading increases with increase in stirring time and drug concentration. The drug release profile from all three sizes of ZnO NPs shows a controlled release. The antibacterial investigations of amoxicillin loaded on nano ZnO with particle sizes of 15, 25, and 38 nm have been carried out. The bacteria investigated in this work are Gram positive and Gram negative and it is found that the antibacterial activity of amoxicillin

loaded on nano ZnO is insignificant for *E. aerogenes* and *K. pneumoniae*.

Acknowledgments Prof. Dr. S. Ramasamy, CSIR Emeritus Scientist and Dr. L. Palanikumar, CSIR-RA acknowledge the financial support given to them to carry-out this work under CSIR Emeritus Scientist Scheme number 21(0174)/08/EMR-II dated 28-04-2008. The authors thank National Centre for Nanoscience and Technology, University of Madras, Chennai, India, for providing HRTEM facilities. The authors thank the Reviewers for their constructive comments.

Open Access This article is distributed under the terms of the Creative Commons Attribution License which permits any use, distribution, and reproduction in any medium, provided the original author(s) and the source are credited.

References

- Bernstein MP, Sandford SA, Allamandola LJ, Chang S (1994) Infrared spectrum of matrix-isolated hexamethylenetetramine in Ar and H₂O at cryogenic temperatures. *J Phys Chem* 98:12206–12210
- Bhosale UV, Kusum DV, Jain N (2011) Formulation and optimization of mucoadhesive nanodrug delivery system of acyclovir. *J Young Pharm* 3:275–283
- Bhunja AK (ed) (2008) Food borne microbial pathogens: mechanisms and pathogenesis. Springer LLC, New York
- Casimiro MH, Gil MH, Leal P (2007) Drug release assays from new chitosan/pHEMA membranes obtained by gamma irradiation. *Nucl Instrum Methods Phys Res B* 265:406–409
- Chang CH, Lin YH, Hsu YM, Yeh CL, Chen YS, Chen YC, Chiou SF, Wang CC (2010) Nanoparticles incorporated in pH-sensitive hydrogels as amoxicillin delivery for eradication of *Helicobacter pylori*. *Biomacromolecules* 11:133–142
- Courrier HM, Butz N, Vandamme TF (2002) Pulmonary drug delivery systems: recent developments and prospects. *Crit Rev Ther Drug Carrier Syst* 19:425–498
- De Jong WH, Borm PJA (2008) Drug delivery and nanoparticles: applications and hazards. *Int J Nanomed* 3:133–149
- Di Silvio L, Bonfield W (1999) Biodegradable drug delivery system for the treatment of bone infection and repair. *J Mater Sci Mater Med* 10:653–658
- Fontana G, Licciardi M, Mansueto S, Schillaci D, Giammona G (2001) Amoxicillin-loaded polyethylcyanoacrylate nanoparticles: influence of PEG coating on the particle size, drug release rate and phagocytic uptake. *Biomaterials* 22:2857–2865
- Gaballa A, Wang T, Ye RW, Helmann JD (2002) Functional analysis of the *Bacillus subtilis* Zur regul-Ion. *J Bacteriol* 184:6508–6514
- Gautier H, Daculsi G, Merle C (2001) Association of vancomycin and calcium phosphate by dynamic compaction: in vitro characterization and microbiological activity. *Biomaterials* 22:2481–2487
- Hamblett KJ, Senter PD, Chace DF et al (2004) Effects of drug loading on the antitumor activity of a monoclonal antibody drug conjugate. *Clin Cancer Res* 10:7063–7070
- Horwitz E, Kagan L, Chamisha Y, Gati I, Hoffman A, Friedman M, Lavy E (2010) Novel gastroretentive controlled-release drug delivery system for amoxicillin therapy in veterinary medicine. *J Vet Pharmacol Ther* 34:487–493
- Jayaseelan C, Abdul Rahuman A, Vishnu Kirithi A, Marimuthu S, Santhoshkumar T, Bagavan A, Gaurav K, Karthik L, Bhaskara Rao KV (2012) Novel microbial route to synthesize ZnO nanoparticles using *Aeromonas hydrophila* and their activity

- against pathogenic bacteria and fungi. *Spectrochim Acta Part A* 90:78–84
- Jones N, Ray B, Ranjit KT, Manna AC (2008) Antibacterial activity of ZnO nanoparticle suspensions on a broad spectrum of microorganisms. *FEMS Microbiol Lett* 279:71–76
- Kamaly N, Xiao Z, Valencia PM, Radovic-Moreno AF, Farokhzad OC (2012) Targeted polymeric therapeutic nanoparticles: design, development and clinical translation. *Chem Soc Rev* 41:2971–3010
- Khuroo AH, Monif T, Verma PRP, Gurule S (2008) Comparison of effect of fasting and of five different diets on the bioavailability of single oral dose of amoxicillin 500 mg capsule. *Clin Res Reg Aff* 25:73–86
- Kim HW, Knowles JC, Kim HE (2004) Hydroxyapatite/poly(ϵ -caprolactone) composite coatings on hydroxyapatite porous bone scaffold for drug delivery. *Biomaterials* 25:1279–1287
- Kumar DA, Dharmendra S, Jhansee M, Shrikant N, Pandey SP (2011) Development and characterization of chitosan nanoparticles loaded with amoxicillin. *Int Res J Phar* 2:145–511
- Lu Y, Chen SC (2004) Micro and nano-fabrication of biodegradable polymers for drug delivery. *Adv Drug Del Rev* 56:1621–1633
- Melville AJ, Rodriguez-Lorenzo LM, Forsythe JS (2008) Effects of calcinations temperature on the drug delivery behavior of ibuprofen from hydroxyapatite powders. *J Mater Sci Mater Med* 19:1187–1195
- Ng CT, Li JJ, Bay BH, Yung LYL (2010) Current studies into the genotoxic nanomaterials. *J Nucleic Acids* 12
- Noel SP, Courtney H, Bumgardner JD, Haggard WO (2008) Chitosan films potential drug delivery systems for antibiotics. *Clin Orthop Related Res* 466:1377–1382
- Padmavathy N, Vijayaraghavan R (2003) Enhanced bioactivity of ZnO nanoparticles—an antimicrobial study. *Sci Technol Adv Mater* 9:035004
- Prager R, Rabsch W, Streckel W, Voigt W, Tietze E, Tschape H (2003) Molecular properties of *Salmonella enterica* serotype paratyphi B distinguish between its systemic and its enteric pathovars. *J Clin Microbiol* 41:4270–4278
- Raghupathi KR, Koodali RT, Manna AC (2011) Size-dependent bacterial growth inhibition and mechanism of antibacterial activity of zinc oxide nanoparticles. *Langmuir* 27:4020–4028
- Rasmussen JW, Martinez E, Louka P, Wingett DG (2010) Zinc oxide nanoparticles for selective destruction of tumor cells and potential for drug delivery applications. *Expert Opin Drug Deliv* 7:1063–1077
- Roselli M, Finamore A, Garaguso I, Britti MS, Mengheri E (2003) Zinc oxide protects cultured enterocytes from the damage induced by *E. coli*. *J Nutr* 133:4077–4082
- Sahasathian T, Kerdcholpetch T, Chanweroch A, Praphairaksit N, Suwonjandee N, Muangsin N (2007) Sustained release of amoxicillin from chitosan tablets. *Arch Pharm Res* 30:526–531
- Saonum P, Hiransuthikul N, Suankratay C, Malathum K, Dancha-Ivijitr S (2008) Risk factors for noso-comial infections caused by extended spectrum β -lactamase producing *Escherichia coli* or *Klebsiella pneumonia* in Thailand. *Asian Biomed* 2:485–491
- Sharma PK, Pandey AC, Zolnierkiewicz G, Guskos N, Rudowicz C (2009) Relationship between oxygen defects and the photoluminescence property of ZnO nanoparticles: a spectroscopic view. *J Appl Phys* 106:094314
- Smola M, Vandamme T, Sokolowski A (2008) Nanocarriers as pulmonary drug delivery systems to treat and to diagnose respiratory and non-respiratory diseases. *Int J Nanomed* 3:1–19
- Song R, Liu Y, He L (2008) Synthesis and characterization of mercaptoacetic acid-modified ZnO nanoparticles. *Sol Stat Sci* 10:1563–1567
- Venkatasubbu GD, Ramasamy S, Ramakrishnan V, Kumar J (2011) Nanocrystalline hydroxyapatite and zinc-doped hydroxyapatite as carrier material for controlled delivery of ciprofloxacin. *3 Biotech* 1:173–186
- Wahab R, Kim YS, Mishra A, Yun SI, Shin HS (2010) Formation of ZnO micro-flowers prepared via solution process and their antibacterial activity. *Nanoscale Res Lett* 5:1675–1681
- Wu PF, Pike J, Zhang F, Chan SW (2006) Low-temperature synthesis of zinc oxide nanoparticles. *Int J Appl Ceram Technol* 3:272–278
- Yin H, Casey PS, McCall M, Fenech M (2010) Effects of surface chemistry on cytotoxicity, genotoxicity and the generation of reactive oxygen species induced by ZnO nanoparticles. *Langmuir* 26:15399–15408
- Zak AK, AbdMajid WH, Abrishami ME, Yousefi R (2011) X-ray analysis of ZnO nanoparticles by Williamson–Hall and size-strain plot methods. *Sol Stat Sci* 13:251–256