

# Tuning the translational freedom of DNA for high speed AFM

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**Received:** 13 August 2014

**Revised:** 02 December 2014

**Accepted:** 03 December 2014

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## KEYWORDS

high speed atomic force microscopy (HS-AFM), DNA, protein, bionanotechnology

## ABSTRACT

Direct observation is arguably the preferred way to investigate the interactions between two molecular complexes. With the development of high speed atomic force microscopy (AFM), it is becoming possible to observe directly DNA-protein interactions with relevant spatial and temporal resolutions. These interactions are of central importance to biology, bionanotechnology, and functional biologically inspired materials. As in all microscopy studies, sample preparation plays a central role in AFM observation and minimal perturbation of the sample is desired. Here, we demonstrate the ability to tune the interactions between DNA molecules and the surface to create an association strong enough to enable high-resolution AFM imaging while also providing sufficient translational freedom to allow the relevant protein-DNA interactions to take place. Furthermore, we describe a quantitative method for measuring DNA mobility, while also determining the individual forces contributing to DNA movement. We found that for a weak surface association, a significant contribution to the movement arises from the interaction of the AFM tip with the DNA. In combination, these methods enable the tuning of the surface translational freedom of DNA molecules to allow the direct study of a wide range of nucleo-protein interactions by high speed atomic force microscopy.

## 1 Introduction

DNA nanotechnology is a promising approach for the bottom-up construction of sophisticated nano-scale complexes. In combination with methods such as hierarchical assembly using location-specific arrangements of proteins upon structural DNA scaffolds [1–3],

it offers significant potential for the development of novel functional materials that are heterogeneously structured at the nano-scale. However, in order to exploit the potential of this technology, a solid understanding of the interactions that drive the bottom-up assembly of nano-scale structures has to be established.

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In recent years, a significant understanding of the complex interactions between proteins and nucleic acids *in vivo* has been developed. When attempting to utilize these interactions outside their native biological context, however, additional factors have to be taken into account. For example, the presence of solid surfaces leads to additional interactions between DNA and proteins, and the presence of unusual topological features in the DNA molecules, for instance branch-points such as those present in DNA origami [4], can have an impact on the interactions. For the full potential of these approaches to be exploited, it is important to understand in detail the relevant interactions in the context that they are to be employed. Arguably, direct observation using atomic force microscopy (AFM) would be the preferred way to study these dynamic protein-DNA interactions *in vitro* and in the proximity of solid surfaces. However, the dynamic nature of these processes poses significant challenges for AFM investigations and, until recently, time-course studies of such interactions were limited by the acquisition rate of the AFM.

The recent development of high speed atomic force microscopy (HS-AFM), and in particular HS-AFM in fluid, has allowed for the direct examination of discrete biological interactions and nano-scale self-assembly processes in physiological buffer at relevant spatial and temporal resolution [5]. This technology not only enables the confirmation of established hypotheses in biology, such as the hand-over-hand motion of myosin [6], but also has the potential to further the understanding of how protein complexes and nucleic acids interact, something that is critical to all forms of life [7–13]. HS-AFM can also be applied in the study of a wide range of biologically inspired materials.

HS-AFM work builds upon two decades of biological studies with conventional AFM [14] which, to-date, has achieved significant success on model systems such as RNA polymerase [15, 16], bacteriophage Lambda Cro protein [17], DNA photolyase [18], nucleosomes [19], and restriction enzymes [20]. HS-AFM may therefore have a central role to play in bionanotechnology and experimental biology, complementing current biochemical techniques and crystallography while elucidating fundamental biological processes.

The sample preparation procedure and its impact on the experiment is a key concern in all forms of microscopy. Here, AFM has distinct advantages over radiative-based alternatives, as it does not require the labeling or modification of delicate biological structures. However, AFM employs a physical probe and therefore requires the deposition of the sample on a solid support surface [14]. Muscovite mica surfaces are typically used as the substrate owing to their perfect cleavage along a <001> plane, yielding large atomically flat areas. Mica consists of layers of an aluminum phyllosilicate lattice ionically bonded through interstitial K<sup>+</sup> ions. Upon cleavage, these K<sup>+</sup> ions are highly mobile and are readily exchanged with divalent cation species at the solid–liquid interface [21]. This exchange results in a positive overcharging of the mica surface, which enables the deposition of molecules that hold a net negative charge, such as DNA [22].

The 2D confinement of the molecules inherently perturbs any biological interaction of interest. It is therefore necessary to mediate a surface adsorption that allows the retention of sufficient translational and rotational freedom while securely adhering the molecules against the instantaneous lateral forces imposed by the scanning probe. Additionally, it is necessary to maintain a suitable reduced physiological environment for biological activity to be retained. Previous studies employing methods to modify the mica surface chemically [23], using cyclic dielectric fields [24, 25] and cyclic buffer exchanges [10, 26, 27], have attempted to mitigate confinement effects by cycling the surface between a loose association—allowing reactions to proceed freely—and a tight association to enable high-resolution imaging. It has also been shown that modulation of surface voltage can be used to control adhesion forces [28] but this requires the use of metal electrodes as substrates and very low salt concentrations. Additionally, the use of DNA origami tiles as support structures to isolate the biological interactions being imaged from the surface has been demonstrated [29]. These alternative methods either put significant constraints on the experimental setup or do not provide the required functionality, and therefore pre-incubation of mica with divalent cations remains the common practice.

It is well established that upon cleavage of mica layers, the interstitial  $K^+$  ions are split between the two cleavage faces and tend to cluster. The resulting vacant sites are easily filled upon exposure to divalent cations. Transition metal cations such as  $Ni^{2+}$ ,  $Co^{2+}$ , and  $Zn^{2+}$  bind irreversibly to mica and have been demonstrated to displace residual  $K^+$  ions. They interact with the hydroxyl groups of mica cooperatively [22, 30], leading to phase-separated domains of positive surface charge [31]. Where transition metal cations are utilized, a strong adhesion between DNA and mica is achieved due to directional bonding of the d-orbitals of the divalent cation. Such deposited DNA molecules adopt a kinetically trapped form [31], sufficient for high-resolution imaging in aqueous buffer.

In contrast,  $Mg^{2+}$  cannot form directional bonds because it is continually exchanging with residual  $K^+$  and  $H^+$  ions on the mica surface and in the imaging buffer. As a consequence,  $Mg^{2+}$  only mediates a relatively weak and diffuse adhesion between DNA and the mica surface, allowing DNA molecules to adopt an equilibrated form [22, 31–33]. This complex spatial distribution has been rationalized by others [31, 33], where the phase-separated domains of ionic species are represented as an idealized polka dot pattern: An ionic patchwork of evenly distributed positively charged  $Ni^{2+}$  clusters interspersed across a mica surface undergoing dynamic exchanges between  $K^+$ ,  $H^+$ , and other cations such as  $Mg^{2+}$ .

Previous work has taken advantage of this difference in binding capacities by adjusting the ratio between different monovalent and monovalent-to-divalent ion concentrations in the deposition buffer to alter the surface adhesion of DNA in air [20, 34, 35].

Interestingly,  $Mg^{2+}$  is the primary co-factor for the majority of enzymes that manipulate all biological polyphosphates including ATP, DNA, and RNA [36]. The transient nature of  $Mg^{2+}$  association allows it to be utilized, in equilibrium, as both a surface binding agent and enzymatic co-factor. Typically, cellular  $Mg^{2+}$  ranges from 5–20 mM, where 95% is chelated with proteins and nucleic acids, primarily ATP [36]. However, a concentration below 10 mM is sufficient for most nucleo-protein interactions. In contrast,  $Ni^{2+}$  exhibits little to no physiological role in higher

organisms, enabling its use as a strong surface binding agent.

When employing the idealized polka dot representation, it is possible that pre-incubation of the mica surface with different concentrations of  $Ni^{2+}$  allows for control over the localized surface-DNA association. If the DNA molecules are now deposited in  $Mg^{2+}$  buffer,  $Ni^{2+}$  should act to restrain the translational freedom through a few specific anchor points while  $Mg^{2+}$  mediates a more global and distributed but weak association. Thus, the mobility of a DNA molecule is governed by the number of  $Ni^{2+}$  interactions and is controlled by the  $Ni^{2+}$  concentration and exposure time during surface pre-incubation.

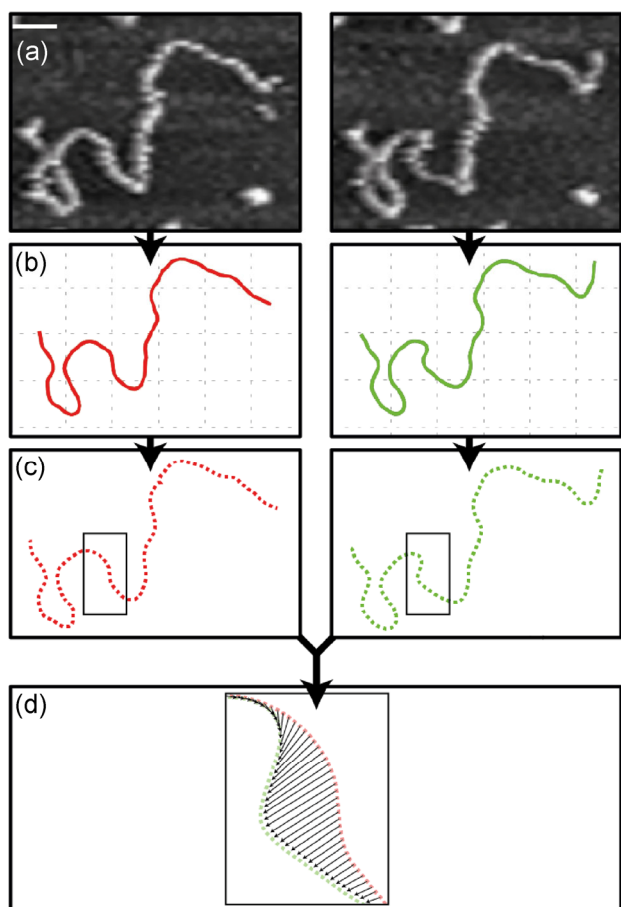
By modulating the concentration of  $Ni^{2+}$  for mica pre-treatment, we demonstrate the ability to control the surface translational freedom of DNA molecules while maintaining a fixed  $Mg^{2+}$  concentration within the imaging buffer, which can be tailored to optimize the relevant nucleo-protein interactions. This allows us to maintain a transient surface interaction of nucleic acids strong enough for imaging with HS-AFM under fluid, while simultaneously providing enough mobility of the DNA to allow the relevant nucleo-protein interactions to take place. We employ a novel methodology for quantifying DNA mobility and use it to demonstrate our ability to tune the surface interaction from tightly surface-tethered to highly mobile DNA.

## 2 Results and discussion

### 2.1 Quantifying the mobility of DNA molecules

In order to establish the methodology for quantifying the mobility of surface-immobilized DNA molecules, mica substrates were pre-incubated with 15 mM  $Ni^{2+}$ . Subsequently, 3.5-kbp DNA molecules were deposited in Tris-Mg buffer and imaged by AFM. A  $Ni^{2+}$  concentration of 15 mM was expected to provide strong surface adhesion, allowing contrasting small regions of chain mobility to be easily identified. Areas of  $1 \mu m^2$  of sample were continuously imaged in solution to observe the motion of the DNA molecules. For each sequence of AFM images, several representative DNA molecules were selected and processed using a

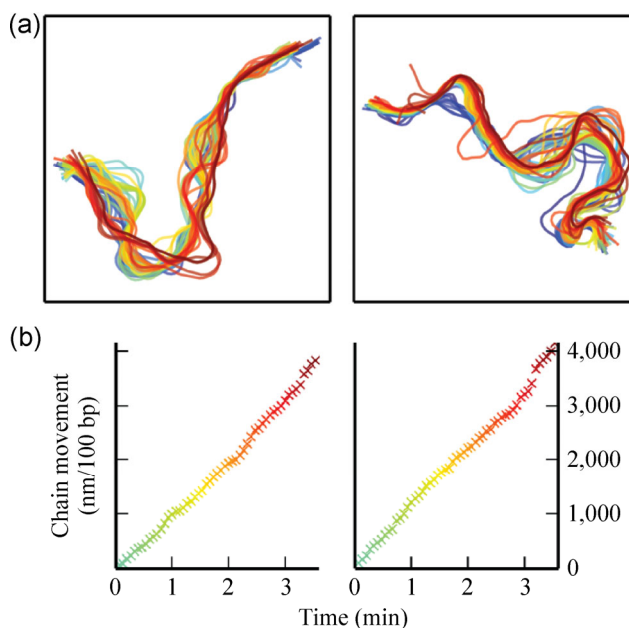
chain-fitting algorithm. A chain of co-ordinates was fitted to the height peaks in the AFM image, generating a vector representation of the molecule's conformation (Figs. 1(a) and 1(b)). This method eliminates the noise and image artifacts that arise during high-speed AFM imaging in liquid. Each selected DNA molecule was tracked sequentially through an image series, where fitting was repeated for sections of the chain that deviated from the previous image, allowing their motion to be quantified. Each chain was then divided into >100 equidistant points and a minimization algorithm was used to map corresponding points between successive frames in a time series, mitigating errors in imaging and fitting around the chain ends. The amount of motion for each pair of points could



**Figure 1** A schematic diagram depicting the chain fitting and evolution processing from the raw AFM images. (a) Sequential AFM images following a single DNA molecule. (b) Derived chain vectors. (c) Mapping of chain vectors into equidistant points. (d) Point mapping is indicated across a short section of the molecule; the relevant section of the molecule is indicated by the boxes in (c). The scale bar is 100 nm.

then be calculated, averaged, and normalized to yield movement velocities for individual DNA chains or sections of a chain (Figs. 1(c) and 1(d)).

To quantify the lateral motion of each DNA molecule over time, the movements of individual molecules were analyzed. Figure 2(a) shows the time-course of two representative DNA molecules over the course of an image sequence. The time evolution is represented by a color scale, with the darkest red line representing the final state and the lightest blue line the initial state. The total distance travelled by the DNA chain, normalized by the length of the DNA chain, was determined by summing up all the distances travelled by the equidistant points on the chain. The results for the two representative DNA molecules are shown as a function of time in Fig. 2(b). The movements were found to be linear in time and hence, from the graphs in Fig. 2(b), a velocity per unit of DNA in nanometers per 100 base pairs length per second ( $\text{nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$ ) was then derived as the characteristic quantity to



**Figure 2** (a) Sequential HS-AFM images of two representative 3.5-kbp DNA molecules over long time scales at  $\text{Ni}^{2+}$  surface pre-incubation concentrations of 15 mM. The time evolution of the DNA chain is represented by a color scale, with the lightest blue line representing the initial state and the darkest red line the final state. Under these binding conditions, DNA molecules have little mobility, as indicated by the tight overlap through subsequent frames. Panel (b) shows the chain movement per 100 bp for both DNA molecules, from which an average chain mobility of  $17 \text{ nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$  can be calculated.

measure lateral mobility (see movie S1 in Electronic Supplementary Material (ESM) for details). This detailed analysis of the lateral motion of DNA molecules reveals a number of intricacies in the surface interaction and the influence of the microscope probe on the sample.

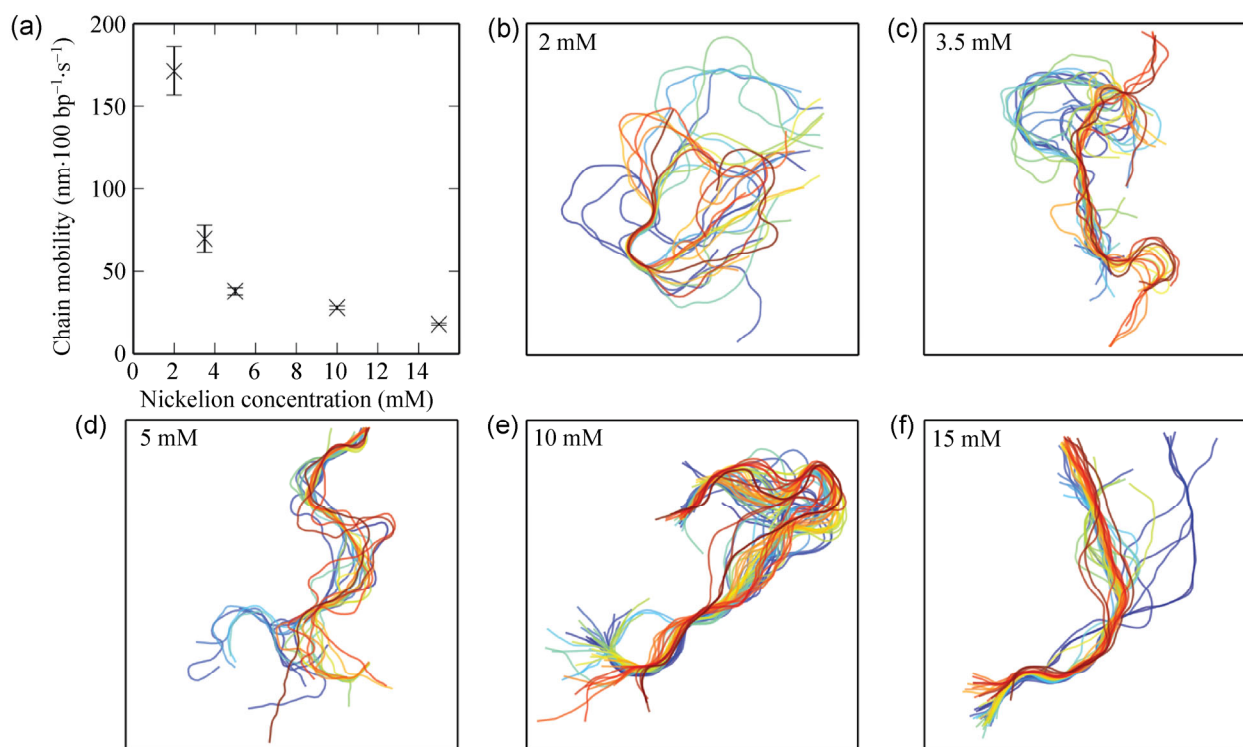
Analyzing the motion of DNA molecules is not a novel concept. A previous study has attempted the direct superposition of sequential images aligned to immobile parts of the molecule [37] or to a reference elsewhere in the frame [38]. Deriving additional details by analysis of vectorized molecules has also been undertaken through hand-tracing methods [39] in order to examine quantities such as elastic bending energies [40] and the influence of the AFM probe [11]. However, such studies lack detail due to the crude alignment and vector derivation methodologies, which yield mobility analyses based on single point mapping of center-of-mass or chain termini only. Consequently, these analyses lack the power to provide the understanding necessary to tune the translational

freedom of DNA and enable relevant nucleo-protein interactions to take place.

## 2.2 Tuning DNA surface mobility with Ni<sup>2+</sup> pre-incubation

To investigate whether the DNA mobility can be controlled via tuning the interaction of the surface-immobilized Ni<sup>2+</sup> ions by varying their density, the above approach was applied across a range of Ni<sup>2+</sup> concentrations from 1 mM to 15 mM (Fig. 3). Varying the ion concentration was chosen over increasing the incubation time, which may lead to unwanted crystallization of Ni-salts. A lower Ni<sup>2+</sup> concentration is expected to lead to a lower density of positively charged sites on the surface, providing fewer pinning points for a DNA molecule and allowing it more translational freedom.

Figure 3(a) shows the chain mobility as a function of Ni<sup>2+</sup> concentration. Each point on the graph represents an average across a number of DNA molecules and the error bars represent the standard deviation. It can



**Figure 3** (a) DNA molecule translational mobility (nm·100 bp<sup>-1</sup>·s<sup>-1</sup>) as a function of Ni<sup>2+</sup> surface pre-incubation concentration. A distinct decrease in mobility is associated with an increasing Ni<sup>2+</sup> concentration. Error bars indicate the standard deviation for each data point. Example chain vector evolution profiles for (b) 2 mM, (c) 3.5 mM, (d) 5 mM, (e) 10 mM, and (f) 15 mM Ni<sup>2+</sup> surface pre-incubation concentrations.

be seen that the DNA translational mobility increases significantly with decreasing  $\text{Ni}^{2+}$  concentration. Where the surface concentration of  $\text{Ni}^{2+}$  is at the highest level investigated, large regions of the chain remain stationary through many consecutive images in a series, indicating a very tight surface association (see Fig. 3(f) for an example). In contrast, below 5 mM, the surface  $\text{Ni}^{2+}$  becomes sufficiently sparse such that large stretches of the DNA chain show considerable movement over the duration of the experiment (Fig. 3(d)). This is also reflected in the chain mobility, which was calculated to be  $38 \pm 2 \text{ nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$  at 5 mM  $\text{Ni}^{2+}$ , with even larger degrees of freedom found for 3.5 and 2 mM  $\text{Ni}^{2+}$  ( $70 \pm 8 \text{ nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$  and  $171 \pm 15 \text{ nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$ , respectively). For the lowest  $\text{Ni}^{2+}$  concentration investigated (1 mM), a high velocity of motion was observed (see Movie S2 in ESM), which meant that a meaningful quantification of the mobility was not possible; hence, this concentration is not represented in the graph.

When a particular nucleo-protein interaction is to be observed, it is necessary to be able to image specific molecules continuously over the time course of the reaction. If the surface association is too weak, the DNA molecule may be able to move out of the frame and key events will inevitably be missed. Therefore, optimal binding conditions need to present weak surface associations without large overall translational movements of the DNA across the mica surface, while at the same time allowing individual segments of the DNA molecule to move relatively freely. We concluded from the data presented in Fig. 3 that for the 3.5-kbp DNA molecules used in this study, optimal conditions are achieved at around 5 mM  $\text{Ni}^{2+}$ , which results in optimal spatial resolution and chain flexibility, with a mobility of  $38 \pm 2 \text{ nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$ . This is proposed to be sufficient for imaging enzymatic interactions with minimal hindrance from the mica support surface, while the DNA molecules remain relatively immobile within a  $1 \mu\text{m}^2$  imaging area. As a proof-of-concept, we investigated the influence of different translational mobilities on the efficiency of restriction enzyme cleavage of surface-associated DNA. EcoRI was able to cleave DNA deposited on a 5 mM  $\text{Ni}^{2+}$  surface, allowing real-time imaging of individual cleavage events, while on 15 mM  $\text{Ni}^{2+}$  surfaces, the

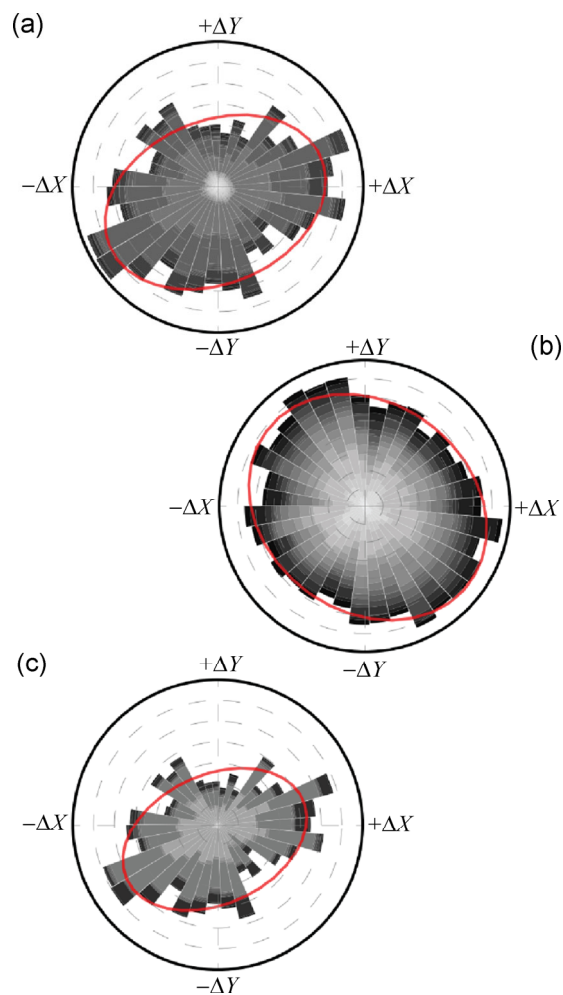
cleavage efficiency was minimal (see Figs. S1 and S2, Table S1 and Movie S3 in the ESM).

We note that while the values quoted here have been normalized with respect to the sequence length, the absolute size of the DNA molecule is of importance. The 3.5-kbp DNA molecules studied above were compared to shorter, 890-bp DNA molecules, which undergo large “worm-like” movements across the surface under comparable conditions (data not shown). Therefore, while the surface preparation can be tuned to produce the desired degree of nucleic acid association, it may be necessary to adjust conditions to account for the length and charge of the particular molecules of study.

### 2.3 Influence of the HS-AFM probe

AFM images are acquired through the monitoring of the interaction of a sharp solid tip with the surface-immobilized molecules. When imaging biological systems, the tip radius is generally of the same order of magnitude as the surface-immobilized molecules; hence, it can be expected that the interaction is significant. Furthermore, in the investigation reported here, the DNA molecules are deliberately only weakly associated with the surface, leading to increased impact from the tip-molecule interactions. Vectorization of the chain motion employed here enables behavioral analysis of individual segments of each DNA molecule and allows for the tip-DNA molecule interaction to be analyzed.

The direction of movement for each DNA chain segment is known and therefore a polar histogram of the magnitude of the movement versus the direction can be plotted for the whole dataset across all  $\text{Ni}^{2+}$  concentrations (Fig. 4(a)). A distinct preference for movements along a particular direction can be observed, and an anisotropy of 1.4 was obtained by fitting an ellipsoid to the data. Random thermal motion of the DNA molecule is not expected to lead to any directional preference. In contrast, the AFM tip is scanned back and forth very fast along one axis (the fast scan axis) and relatively slowly along the other axis. Therefore, the AFM tip-molecule interactions are expected to be predominately in the direction of the fast scan axis, and hence would lead to an anisotropic histogram.



**Figure 4** Polar histograms indicating the magnitude and directionality of chain movements (a) including all  $\text{Ni}^{2+}$  concentrations, (b) including only high  $\text{Ni}^{2+}$  concentrations (10 mM and 15 mM), and (c) including only low  $\text{Ni}^{2+}$  concentration (2 mM and 3.5 mM). The movements of all segments are binned according to the direction and weighted by the magnitude of the movement. The grey scale delineates the contributions of different DNA chains. The degree of the anisotropy of each histogram is indicated by the elliptical fit to the data (indicated by the red ellipsoid).

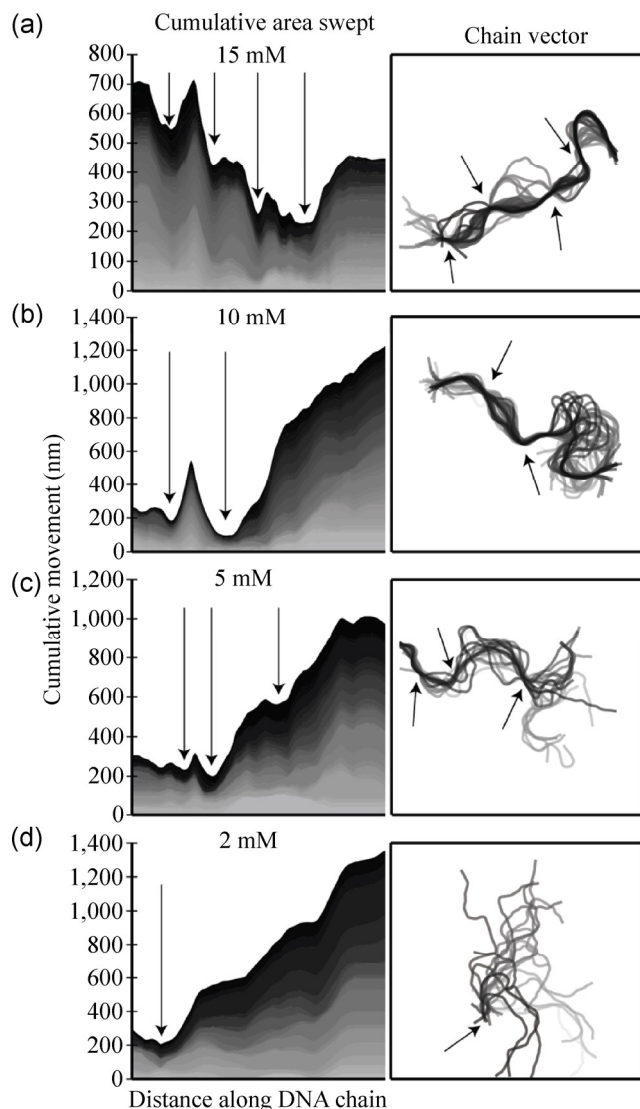
When examined more closely, it can be seen that the anisotropy arises mainly from highly mobile DNA molecules that appear on low  $\text{Ni}^{2+}$  sample preparations. Figure 4(b) shows the polar histogram of the magnitude of the movement versus the direction but only with  $\text{Ni}^{2+}$  concentrations of 10 mM and 15 mM included. An anisotropy of only 1.2 is obtained from the fit of the ellipsoid to the data. In contrast, when considering only the very weakly bound DNA molecules, which show significant lateral mobility (2 mM and 3.5 mM  $\text{Ni}^{2+}$ , Fig. 4(c)), the anisotropy is even more pronounced

than in Fig. 4(a) (anisotropy of 1.5), demonstrating that the anisotropy increases with increasing lateral mobility. Notably, the skew seen in the magnitude data is found to be in line with the image acquisition direction, suggesting that the AFM tip-DNA interaction contributes significantly to the observed motion of loosely bound DNA molecules. Conversely, higher  $\text{Ni}^{2+}$  preparations are characterized by smaller magnitude motions and are largely isotropic in nature. This would be consistent with molecules undergoing small conformational changes as a result of thermal fluctuations, notably constrained against large translational AFM tip-induced motions.

The lateral forces imparted by the AFM tip naturally perturb the sample of interest and may influence the nucleo-protein interaction. However, the ability to extract detailed information regarding the behavior of molecules during the imaging process may lead to a better understanding of the nature of the observed biological interactions.

#### 2.4 Identification of discrete surface anchor points

To consider the role of  $\text{Ni}^{2+}$  within our system, we adopted the idealized polka dot surface model discussed by others [30, 32]. It is reasonable to assume that the density of surface-associated  $\text{Ni}^{2+}$  ions increases with increasing  $\text{Ni}^{2+}$  concentration during incubation. It has previously been demonstrated that the distribution of  $\text{Ni}^{2+}$  on the surface is highly non-uniform [40] and lacks homogeneity [30]. However, it may be possible to gain further insight into the  $\text{Ni}^{2+}/\text{Mg}^{2+}$ -governed surface interactions by identifying regions of specific surface association by examining the motion of the DNA chains. When plotting the cumulative movement for each segment along individual DNA molecules (Fig. 5), a series of minima can be observed (indicated by arrows). Figure 5(a) shows the results for a representative DNA molecule immobilized on a 15 mM  $\text{Ni}^{2+}$  pre-incubated surface, and four distinct minima can be identified. The right hand panel shows the time evolution of the DNA molecule and in this representation, particular regions of the chain appear pinned to the surface, while other chain regions move large distances. The pinned, stationary positions coincide with the observed minima in movement and are again indicated by arrows.



**Figure 5** Area plots depicting the cumulative movement of chain segments for representative DNA chains for different  $\text{Ni}^{2+}$  concentrations (left panels). Distinct regions of the DNA molecule are seen to be anchored at particular locations (indicated by arrows). The density of minima increases with  $\text{Ni}^{2+}$  concentrations, suggesting that  $\text{Ni}^{2+}$  ions provide specific anchor points on the surface to increase DNA surface association. The grey scale indicates successive frames in a time series. The panels on the right show the chain evolution with the minima location indicated by arrows.

The number of such minima, and hence the number of stationary points, decreases with decreasing  $\text{Ni}^{2+}$  concentration (Figs. 5(b)–(d)). We note that all of the molecules imaged on surfaces pre-incubated with  $\geq 10$  mM  $\text{Ni}^{2+}$  and in excess of half of the molecules imaged on 5 mM  $\text{Ni}^{2+}$  surfaces show distinct pinning at one or more locations. Interestingly, in some cases minima disappear over the course of the imaging

sequence, while others appear in subsequent frames, suggesting that specific surface interactions break and re-form continuously. This behavior is more prominent with molecules imaged with  $\text{Ni}^{2+}$  concentrations of 5 mM or lower. Although a direct correlation with surface distributions of  $\text{Ni}^{2+}$  would be purely speculative without further in depth studies, the results together with previous findings on the distribution of  $\text{Ni}^{2+}$  ions [30, 40] suggest that positively charged  $\text{Ni}^{2+}$  domains act as anchor points for the negatively charged DNA chains, with the interstitial regions governed by weak  $\text{Mg}^{2+}$  associations, allowing for the desired mobility.

### 3 Conclusion

When attempting to observe biological processes *in vitro* with the HS-AFM, it is essential to ensure that the measurement only minimally perturbs the interactions of interest. For the investigation of nucleo-protein interactions, the DNA molecules have to be associated with the surface strongly enough to enable stable imaging over relevant timescales, while at the same time providing enough translational freedom to allow the proteins to interact with the DNA with minimal disturbances. A number of different approaches have been reported in the literature for controlling the surface association of DNA molecules. However, none of the existing methods offer the ability to mediate the surface interaction and thus the translational freedom of the DNA to enable large ranges of diverse investigations within the additional constraints of maintaining suitable reduced physiological conditions. Here, we demonstrated an approach to tune the surface interaction of DNA that fulfills these requirements. Both stable imaging and reaction conditions are orchestrated simultaneously without the need to perturb the system throughout the reaction time-course.

We have developed an analytical method for quantifying the mobility of DNA under different surface association conditions, and we showed that for physiological conditions, the interaction of the DNA with the mica surface could be tuned from tightly surface-associated to highly mobile. This approach, therefore, provides a highly flexible method to establish



conditions which enable the investigation of a large range of nucleo-protein interactions. The presented analytical approach allowed us to investigate the impact of the AFM tip interactions with the surface-associated DNA. We showed that the overall translational movement of the DNA is mostly isotropic for a stronger surface association, while increasing movement in the fast-scanning direction of the AFM tip is observed with decreasing strength of the surface association, indicating that the AFM tip-DNA molecule interaction contributes significantly to the overall movement.

The tools presented here confer the ability to orchestrate and evaluate discrete biological interactions for novel applications in experimental biology and bionanotechnology.

## 4 Experimental section

Reagents: Linear DNA (3.5 kbp) was amplified by PCR from a modified pGEM-T plasmid vector [41]. Linear DNA (890 bp) was amplified from lambda phage DNA. Magnesium-acetate, Tris-acetate, and nickel chloride, which were prepared as 100 mM stocks with a pH of 7.4, were all purchased from Sigma Aldrich, St Louis, USA.

### 4.1 HS-AFM sample preparation

Mica (Agar Scientific, USA) was freshly cleaved and pre-incubated with  $\text{NiCl}_2$  (20  $\mu\text{l}$ ) at concentrations ranging from 1 mM to 15 mM for 1 minute. Excess  $\text{NiCl}_2$  solution was removed and DNA solution (20  $\mu\text{l}$ ) was immediately applied to the mica surface and incubated for 5 minutes. Subsequently, the surface was partially de-wetted. All DNA samples were prepared using 10 mM Tris-acetate (pH 7.4), 10 mM Magnesium-acetate, and 3.5 kbp DNA (10 ng). Mica samples were re-immersed in Tris-Mg buffer (200  $\mu\text{l}$ ) for imaging, with a small volume (50  $\mu\text{l}$ ) applied directly to the AFM cantilever.

### 4.2 HS-AFM imaging in aqueous buffer

All samples were imaged with a Dimension FastScan using FastScan-DX probes (Bruker AXS, USA). All images were collected at a scan rate of 38 Hz and a

resolution of  $128 \times 128$  pixels. The drive amplitude and set point used were typically around 3 V and 200 mV, respectively, but adjusted for optimum resolution as needed.

Image analysis and chain fitting: AFM images were processed with a low-pass filter and a linear vector (chain) was fitted to the intensity peaks of the image using the ImageJ software (<http://rsbweb.nih.gov/ij/>) with the JFilament plugin [42]. Subsequently, the chains were split into >100 equidistant points and overlaid frame by frame (Fig. 1). Finally, the point-by-point differences between two sequential chains in a series were calculated and averaged to represent the chain movement in nm per 100 bp per second ( $\text{nm} \cdot 100 \text{ bp}^{-1} \cdot \text{s}^{-1}$ ). This process is discussed in more detail in the main text. The cumulative movement of individual segments along DNA molecules was calculated by adding up the distances travelled by the segments between time frames. The distribution of segments along the chains of individual time frames was chosen so that local minima in movement were aligned.

## Acknowledgements

This work was funded in part by the EPSRC Centre for Doctoral Training in Molecular Scale Engineering, and WELMEC, a Centre of Excellence in Medical Engineering funded by the Wellcome Trust and EPSRC, under grant number WT 088908/Z/09/Z. The authors would like to acknowledge Alexander Dulebo, Hartmut Stadler and Bruker AXS, Karlsruhe for their time and contribution to this work, and the equipment funding from the BBSRC.

**Electronic Supplementary Material:** A short movie depicting the chain fitting process through a set of sequential AFM images is supplied as a visual aid to the description given in the results and discussion section (Movie S1). A short movie depicting the surface mobility of 3.5 kbp DNA fragments as a function of surface-immobilized  $\text{Ni}^{2+}$  concentration is supplied in support of Fig. 3 (Movie S2).

Additionally, AFM images showing cleavage of DNA strands by the EcoRI enzyme (Figs. S1 and S2), statistical analysis of the cleavage efficiency (Table S1),

and a short movie showing a single cleavage event (Movie S3) are provided.

This information is available in the online version of this article at <http://dx.doi.org/10.1007/s12274-014-0681-y>.

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