

# DSC examination of cartilage damage of patients undergoing shoulder replacement

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#### Abstract

Shoulder replacement is a viable surgical treatment for comminuted proximal humerus fractures and shoulder osteoarthritis. Proper evaluation of hyaline cartilage is essential for the right choice of prosthesis; however, there are only a limited number of studies available investigating the cartilage of glenohumeral joint of patients undergoing shoulder replacement. We hypothesized that differential scanning calorimetry (DSC) could determine the grade of cartilage damage in patients undergoing reversed shoulder replacement, providing insights into the structural changes of the human cartilage samples. Sample of hyaline cartilage of glenohumeral joint was harvested during reversed shoulder replacement of orthopaedic and trauma patients. Thermal parameters were measured using DSC, and radiological examination of glenohumeral joint was also done prior to surgery. We have found that changes in thermal characteristics and DSC scans clearly indicate the severity of osteoarthritis and cartilage damage. The denaturation temperature range and the half-width of the heat flow curves were significantly wider in the orthopaedic samples compared to the control and traumatic ones. The calorimetric enthalpy ( $\Delta H_{cal}$ ) exhibited significant differences in both pathologic samples, compared to the control. The melting temperatures ( $T_m$ ) show that structural change caused by orthopaedic condition is greater than the effect of traumatic. Therefore, differential scanning calorimetry could help to determine the grade of cartilage damage in orthopaedic and trauma patients undergoing reversed shoulder replacement.

Keywords DSC · Cartilage · Shoulder · Osteoarthritis · Fracture · Reversed shoulder replacement

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## Introduction

Shoulder replacement is a viable surgical treatment for comminuted proximal humerus fractures and shoulder osteoarthritis [1–3]. Generally, severe glenohumeral osteoarthritis requires total shoulder replacement and hemiarthroplasties are used only in selected cases. Meanwhile, in the case of rotator insufficiencies and rotator cuff tear arthropathies, reversed shoulder replacement is the primary choice [4]. In the case of comminuted 3- and 4-part proximal humerus fractures, hemiarthroplasty could be an applicable alternative to osteosynthesis [5]; however, reversed shoulder arthroplasty should be preferred in elderly patients or with preexisting rotator cuff damages and arthropathies [6].

Details about the condition of cartilage, osteoporosis, inflammation and rotator cuff damage could help to select the right type of implant [7–9]. Accordingly, Toma T. et al. investigated the histopathological changes of humerus head in cuff tear arthropathy (CTA) compared to osteoarthritis (OA) and found that the cartilage layer in CTA was thicker, compared to OA [10].

DSC has been found a relevant method in the examination of joint and cartilage diseases [11–13]. For instance, Naumov et al. utilized DSC in the investigation of hyaline cartilage of the fractured human femoral head [14]. DSC has also been successfully used in the examination of degenerative shoulder conditions [15] and spine diseases [16]. Furthermore, Patczai et al. demonstrated that duration of cryopreservation could interfere with the morphology of human cartilage samples [17].

While the knowledge of the condition of the joint surface is crucial for determination of the right type of prosthesis, there are only a limited number of studies available in the literature, investigating the cartilage of glenohumeral joint of patients undergoing shoulder replacement.

Therefore, we hypothesized that DSC could determine the grade of cartilage damage in orthopaedic and trauma patients undergoing reversed shoulder replacement. We also hypothesized that DSC examination could provide further details about the structural changes of the examined cartilage samples.

#### **Materials and methods**

#### Sample collection

The  $5 \times 5 \times 2.5$  mm sized sample of the hyaline cartilage of the removed humerus head from the estimated glenohumeral contact area (GCA) was harvested during reversed shoulder replacement [18], Additionally, a cylindrical (5 mm in diameter) part of the glenoid was collected during preparation of the glenoidal component of the prosthesis. Then, samples were properly stored for further measurements, as described in details elsewhere [11, 13]. The hyaline cartilage samples-three from different medical stages-were obtained patients who underwent reversed shoulder replacement: 1) due to acute trauma (4-part dislocated or Neer Type VI proximal humerus fractures (samples A2-4) and 2) due to rotator cuff tear arthropathy (samples B1 and B2). The control sample (originally labelled as A1) was collected from a young patient with dislocated 4-part proximal humerus fracture and was considered macroscopically as a healthy cartilage. This finding was confirmed by histological examination. All of these samples were considered as waste from the point of surgery.

All procedures followed were in accordance with the ethical standards of the responsible Regional and Institutional Research Ethics Committee and with the Helsinki Declaration of 1975, as revised in 2008.

# Clinical and radiological evaluation of rotator cuff damage

Based on patient history and results of the physical examination on case of rotator cuff arthropathy (RCA) patients, an individual score system was applied to assess the potential level of rotator cuff and cartilage damage. Samples of RCA of trauma origin were also macroscopically assessed, looking for signs of rotator cuff injury and cartilage injury (grade 0–5). The rotator cuff tendon damage was scored with Hamada classification [19]; for evaluation of primary arthropathies and cartilage damage, Walch [20] and Outerbridge classifications [21] were used, respectively. Radiological analysis of conventional X-rays, CT and MRI images was performed by using Siemens Syngo.via software (Siemens Healthineers Global).

#### **Histological processing**

The cartilage samples were fixed in 4% formaldehyde for at least 2 days. After fixation, two representative sections from each sample were cut. Then, the tissues were dehydrated and embedded in paraffin according to the standard histopathological processing and 4- $\mu$ m-thick sections were cut by microtome. The slides were stained with hematoxylin–eosin.

#### **DSC investigations**

Before the measurements, the stored samples were washed three times in normal saline and remained in a sterile isotonic saline on 4 °C till starting the calorimetric examinations (max. half an hour). The measurements were made by a SETARAM Micro DSC-II calorimeter between 0 and 100 °C with a heating rate of 0.3 K min<sup>-1</sup>. Conventional closed Hastelloy batch vessels (V=1 mL) were used for the experiment to perform the thermal denaturation. Samples' masses were in the case of healthy control between in mgs: 157–172. In the case of orthopaedic samples the masses varied in group B1: 55-72, for B2: 80-90 mg. In the case of traumatic samples, it was in the range of 56-66 for A2, 8-11 for A3 and 40-60 mg for A4 patients. Normal saline was used as a reference. With the help of a two-point setting, SETARAM peak integration calorimetric enthalpy  $(\Delta H_{cal})$ was calculated from the area under the heat absorption curve and then the other thermal parameters (denaturation or melting temperature  $(T_m)$ , range of denaturation  $(\Delta T)$ , half width of transition  $(T_{1/2})$  and calorimetric enthalpy data of samples) were compared. Because of the relatively small sample mass, the raw scans were smoothed and baseline correction was made by Origin 6.0.

(a)

#### **Data evaluation**

The average of three measurements for all case was calculated, and the average curves were plotted. Because of the small number of samples, standard deviation was not calculated.

#### Results

#### **Radiological and histological evaluation**

Radiological evaluation of rotator cuff tendon damage and glenohumeral arthritis was performed based on the available conventional X-rays, CT and MRI scans (Figs. 1a–d, 2a–c). Table 1 shows the results of radiological assessment of orthopaedic and trauma shoulders (4-part or Neer Type VI dislocated proximal humerus fractures).

According to the Walch classification, grade 'D' in the case of sample B2 indicates a very severe arthritis with anterior humeral head subluxation and level 'A1' in the case of sample A3 means a well-centred humeral head with only minor erosions. Based on MRI scans, Outerbridge 'grade 2' of sample B1 means blister-like swelling/fraying of articular cartilage extending to surface, a moderately damaged cartilage. The Hamada classification indicates the progression of rotator cuff tear arthropathies (from 1 to 5). Of the trauma samples, A3 was graded as '4b' and orthopaedic samples B1



**Fig. 1** Rotator cuff tear arthropathy. (**a**) Conventional X-ray, (**b**) MRI—T1-weighted, axial plane (**c**) MRI—PD (proton density) fat saturated, axial plane (**c**) MRI—PD (proton density), coronal plane, (**d**) MRI—MRI—PD (proton density), fat saturation, coronal plane



Fig. 2 Rheumatoid arthritis. (a) Conventional X-ray, (b) CT-scan, axial plane, (c) CT-scan, coronal plane

and B2 were graded as '4A' and '5', respectively, demonstrating a worse prognosis of arthropathy for the orthopaedic patients.

The macroscopic findings were scored based on the observation of the surgeon during samples collection. We have found that in the case of the orthopaedic samples, the cartilage was in markedly worse condition, compared to the trauma samples.

It is important to note that most of the classifications found in the literature are applied only for degenerative conditions, not for trauma cases. In the case of healthy, control hyaline cartilage samples, histological examination confirmed the absence of pathologic findings (Fig. 3a).

# Thermal denaturation of orthopaedic and trauma samples

The average curves for orthopaedic and trauma samples are shown in Fig. 4 and in Fig. 5, respectively. The shape and run of scans, as well as the thermal data of Table 2 can

 Table 1
 Evaluation of glenohumeral arthritis and rotator cuff damage of trauma and orthopaedic shoulders, based on radiological and macroscopic findings

|             | Classification |             |        |             |  |
|-------------|----------------|-------------|--------|-------------|--|
|             | Walch          | Outerbridge | Hamada | Macroscopic |  |
| Orthopaedic |                |             |        |             |  |
| B1          | _              | 2           | 4a     | 4           |  |
| B2          | D              | _           | 5      | 5           |  |
| Trauma      |                |             |        |             |  |
| A2          | -              | _           | -      | 3           |  |
| A3          | A1             | -           | 4b     | 2           |  |
| A4          | _              | -           | -      | 2–3         |  |
|             |                |             |        |             |  |



Fig. 3 Histological section from healthy hyaline cartilage. Hematoxylin–eosin staining, magnification is 10X



Fig. 4 The average scans of control, B1 and B2 orthopaedic samples of different stages of hyaline cartilage damage

prove the structural changes caused by the actual orthopaedic stage.

Our main observation regarding the origin of the samples and the consequence of the disease is that the denaturation temperature range and the half-width of the heat flow curves are significantly wider in the orthopaedic samples compared to the control and traumatic samples (see Figs. 4, 5 and Table 2). These facts show the thermal consequence of the less cooperativity among the different structural domains of the orthopaedic cartilage.



**Fig. 5** Thermal denaturation of different traumatic cartilages. The average scans of control, A2–A4 samples of trauma patients with different stages of hyaline cartilage damage

The calorimetric enthalpy exhibited also significant differences in both samples referring to the control. Because we have no biochemical background to separate the different compounds of cartilage, it would be difficult to interpret the 'big jumps' in B1 and B2, compared to the control. The melting temperatures ( $T_m$ ) show that structural change caused by disease (B2) is greater than in the case of a traumatic impact.

### Discussion

Despite recently published protocols and guidelines [22–25], there is still a need for studies to analyze the biochemical background of rotator cuff degeneration and hyaline cartilage damage. These data could provide more details to the surgeon about the expected grade of arthritis, especially under circumstances when MRI examination is not available.

In this study, we have demonstrated that changes in the thermal parameters of human cartilage samples could determine the grade of osteoarthritis. We have also found clear differences, comparing DSC scans of trauma and orthopaedic patients.

Based on the DSC curve shapes and thermal characteristics of samples with different origins, we have found that the structural changes caused by degenerative diseases (osteoarthritis, rheumatoid arthritis or rotator cuff tear arthropathy) are greater than changes observed in trauma patients. The structural damage detected in trauma patients could be either due to a preexisting condition or the effect of the trauma itself.

It is known that the human hyaline cartilage consists of three zones (superficial, transitional and deep zone);

| Sample             | Thermodynamic        | Thermodynamic parameters     |                 |                                   |  |  |  |
|--------------------|----------------------|------------------------------|-----------------|-----------------------------------|--|--|--|
|                    | $\Delta T/^{\circ}C$ | $T_{1/2}/^{\circ}\mathrm{C}$ | $T_{\rm m}$ /°C | $\Delta H_{\rm cal}/{ m Jg}^{-1}$ |  |  |  |
| Orthopaedic carti  | lage                 |                              |                 |                                   |  |  |  |
| Control            | 19.0                 | 7.9                          | 56.5            | 0.62                              |  |  |  |
| B1                 | 27.1                 | 17.6                         | 56.0            | 1.84                              |  |  |  |
| B2                 | 20.0                 | 10.5                         | 50.0            | 1.04                              |  |  |  |
| Traumatic cartilag | ge                   |                              |                 |                                   |  |  |  |
| Control            | 19.0                 | 7.9                          | 56.5            | 0.62                              |  |  |  |
| A2                 | 17.1                 | 4.3                          | 61.1            | 0.41                              |  |  |  |
| A3                 | 15.0                 | 8.9                          | 58.9            | 1.07                              |  |  |  |
| A4                 | 14.6                 | 5.0                          | 58.9            | 1.09                              |  |  |  |

**Table 2** Thermal characteristics of orthopaedic and traumatic cartilage samples. Data are averages of three samples. Symbols:  $\Delta T$  denaturation temperature range,  $T_{1/2}$  half width at the highest heat flow,  $T_{\rm m}$ 

the melting temperature and  $\Delta H_{cal}$  is the calorimetric enthalpy normalized on the wet mass of the samples

each zone has different function and consistency [26]. Interestingly, we have found that the thermal denaturation scans of certain samples exhibited 'jumps' that can be an interference of one of the components of the different zones. Separation of the different layers of the cartilage is beyond the scope of our current study; however, it might worth further investigations.

In comparison, Naumov et al. investigated the effect of time elapsed from the fracture of femoral neck on thermal parameters. They demonstrated differences in both melting temperature and thermal enthalpy, comparing control, fresh fractures and different stages of avascular necrosis (control, fresh fractures:  $T_{\rm m} = 68.2 \,^{\circ}\text{C}$ ,  $\Delta H_{\rm cal} = 2.87 \,\text{J g}^{-1}$ , avascular necrosis:  $T_{\rm m} = 70.7 \,^{\circ}\text{C}$ ,  $\Delta H_{\rm cal} = 3.61 \,\text{J g}^{-1}$ ). It supports the notion that human hyaline cartilage suffers significant structural changes in the case of inadequate blood supply, such as avascular femoral head necrosis [14].

Potential limitation of the study is the relatively low number of cases in which radiological scoring was available, based on CT/MRI scans. It highlights the problem that most of the classification either utilizes MRI or evaluates only orthopaedic cases, i.e. RCA or OA shoulders, but not traumas. Meanwhile, the proper assessment of hyaline cartilage is essential in the decision-making process and surgical planning, especially in trauma cases.

Another limitation of this study is that only the average values were calculated instead of standard deviation and error of means (because of the low number of patients). However, considering the excellent reproducibility of the measurements, we believe that DSC produces marked differences, therefore a useful examination method in the assessment of cartilage damage of patients undergoing shoulder replacement.

### Conclusions

Differential scanning calorimetry could help to determine the grade of cartilage damage in orthopaedic and trauma patients undergoing reversed shoulder replacement.

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Authors' contributions Dr. András Bata was involved in sample collection and handling, data analysis and manuscript writing. Dr. László G Nöt was involved in operations, sample collection and handling, data analysis and manuscript writing. Dr. János Cifra was involved in histological examination. Dr. Hajnalka Szabó was involved in radiological evaluation. Prof. Dr. Dénes Lőrinczy is corresponding author and principal investigator and was involved in DSC experiments, data analysis and manuscript writing.

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Availability of data and material There are no additional available data to upload.

#### **Compliance with ethical standards**

**Conflict of interest** The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

**Consent to participate** Consent from patients to participate in the study has been obtained.

**Consent for publication** Copyright form has been uploaded with the manuscript.

**Ethical approval** All procedures followed were approved in accordance with the ethical standards of the responsible committee on human experimentation (institutional and national) and with the revised Helsinki Declaration of 1975.

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