Network structure and thermal properties of bioactive (SiO₂–CaO–Na₂O–P₂O₅) glasses

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ABSTRACT

Ca- and P-based bioactive glasses are excellent candidates for design and manufacture of biomaterials. Understanding the structure and physico-chemical–thermal behaviour of bioactive glasses is a fundamental step towards the design of a new generation of biocompatible materials. In this study, the structure of SiO₂–CaO–Na₂O glasses and its derivatives, obtained by substituting Na₂O with P₂O₅ and prepared by melt–quench technique, was studied with neutron and electron diffraction techniques combined with thermal analysis, high-resolution electron microscopy and X-ray photoelectron spectroscopy. Neutron and electron diffraction data were analysed with reverse Monte Carlo simulation and pair distribution function analysis, respectively. Bioactivity of P₂O₅ substituted glasses was also investigated and proven in vitro using simulated body fluid. Based on the structural analysis, it was found that Si and P atoms are in well-defined tetrahedral units with a bond distance of 1.60 Å for both Si–O and P–O bonds, although P exhibits a higher average coordination number than Si. With increasing phosphate content, tendentious changes in the glass behaviour were observed. Linear increase in T_g , supported by the changes in the average coordination numbers of Si and P, indicates strengthening of network structure with increasing P content and formation of P–O–Ca atomic linkages, which lead to Ca–P-rich atomic environments in the silicate network. These Ca–P-rich environments trap volatile elements and thus decrease the total weight loss during heating at higher P concentrations. In the case of the highest investigated P₂O₅ content (5 mol%), nanoscale structural inhomogeneity and the formation of Ca–P-rich clusters were also revealed by electron diffraction and atomic resolution imaging. This type of Ca–(Na)–P clustering has a key role in the behaviour of phosphate-substituted silicate glasses under physiological conditions.

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Introduction

Bioactive glasses are mostly silicate-based glasses which, besides exhibiting biocompatibility, are able to bond actively to host living tissue [1]. Their main practical advantages with respect to other bioactive or biocompatible materials like ceramics, bulk metallic glasses or other metallic materials are based on their metastable amorphous structure, which induces high reactivity under physiological conditions. At the same time, their composition, in contrast to metal-based implant materials, allows biomedical applications without additional coating.

Besides silicates, several glassy compositions based on B_2O_3 or P_2O_5 have been found suitable for different kinds of biomedical applications [2, 3]. Each compositional series has its advantage: the SiO_2 -based group comprises a wide range of glass formulations, the B_2O_3 -based glasses are characterized by higher reactivity than silicate materials, which leads to faster bioactive kinetics, and P_2O_5 -based systems are better resorbable materials under physiological conditions, and their dissolution rate can be tuned by changing their compositions [4]. Various concentrations of other oxides can be incorporated in the basic glass composition to enhance particular properties of the glassy material, like the CaO and Na_2O are useful to adjust the surface reactivity in biological environments.

However, common disadvantages of all compositions, namely poor load bearing performance and manufacturing difficulties, impede their widespread application in clinics. One way to overcome these disadvantages is the synthesis of glass–ceramics nanocomposite materials from bioactive glass as a starting material either by heat treatment or melt–quench technique [5]. As both bioactivity and the high temperature behaviour of glasses depend on composition and structure, the structure of bioactive glasses has been intensively investigated.

It has been established that bioactive silicate glasses are characterized by a network structure of SiO_4 polyhedra with some orthophosphate (PO_4) substitution [6]. Subsequently, molecular dynamics simulations [7] suggested that the distribution of the network modifier cation Ca^{2+} might not be homogeneous in the random network structure but has a strong affinity to the orthophosphates. Combined neutron and X-ray diffraction study of commercial

Bioglass[®] provided experimental evidence for the non-uniform distribution of Ca^{2+} in the network structure [8]. At the same time, nuclear magnetic resonance spectroscopy proved the existence of phosphate clusters up to six PO_4 tetrahedra units [9, 10]. These results indicate that local fluctuations in the atomic structure and composition comprise an inherent property of bioactive silicate glasses that has to be considered when thermal and mechanical properties or bioactive behaviour is explained.

This integrated bulk-to-nanoscale study is motivated by a better understanding of the connection between the nanostructure and thermal behaviour of bioactive silicate glasses. To achieve this goal, we measure and model the average network structure of a bioactive glass series in the compositional range of $SiO_2(45)CaO(25)Na_2O(30 - x)P_2O_5(x)$, where $x = 0, 1, 3, 5$, using neutron diffraction and reverse Monte Carlo simulations, and then study the nanoscale inhomogeneities by transmission electron microscopy methods and X-ray photoelectron spectroscopy. In parallel, thermal characterization is carried out as a function of composition. Finally, merging bulk and nanoscale structural data, interpretation of thermal behaviour is presented.

The requirements for synthetic bone substitute materials summarize the influence of the respective material towards the biocompatibility and bioactivity [11]. In the present work, the biological properties of studied materials were evaluated using in vitro settings.

Experimental details

Sample preparation

Glassy samples were prepared by melt–quench technique, melted under atmospheric conditions, at temperatures between 1100 and 1250 °C in Pt crucibles. The melted mixture has been kept at the melting temperature for 2 h, during which the melt was periodically homogenized by mechanical stirring. The melt was quenched by pouring it on a stainless steel plate. The nominal compositions of the investigated glassy specimens are summarized in Table 1. The raw materials used were all of p.a. grade, SiO_2 , P_2O_5 are the basic glass-forming oxides, while Na_2O and CaO both serve as network modifiers.

Neutron diffraction experiments

Neutron diffraction (ND) measurements were performed in a broad momentum transfer range, combining the data measured by the 2-axis PSD monochromatic neutron diffractometer ($\lambda_0 = 1.069 \text{ \AA}$; $Q = 0.45\text{--}9.8 \text{ \AA}^{-1}$) [12] at the 10 MW Budapest research reactor and by the 7C2 diffractometer at the LLB, Saclay ($\lambda_0 = 0.726 \text{ \AA}$; $Q = 0.52\text{--}19 \text{ \AA}^{-1}$) [13]. The powder specimens of about 3–5 g/each were filled in cylindrical V-sample holders of 8 and 6 mm diameter for the two experiments, respectively. The structure factors, $S(Q)$ s, were evaluated from the raw experimental data, using the programme packages available at the two facilities. As the statistics of the data is better for the PSD diffractometer at relatively low Q values (below $\sim 4 \text{ \AA}^{-1}$) and the statistics of 7C2 diffractometer data is much better above $8 \text{ \AA}^{-1}$, the $S(Q)$ data were combined by normalizing the data of the PSD diffractometer to that of the 7C2 diffractometer in the $4\text{--}8 \text{ \AA}^{-1}$ range by least squares method. The agreement of the corresponding $S(Q)$ values was within 1% in the overlapping Q -range. The combined values of the two spectra were used for further data treatment. (i.e. for $Q < 4 \text{ \AA}^{-1}$ only the PSD data and for $Q > 8 \text{ \AA}^{-1}$ only the 7C2 data were used.)

Electron microscopy and electron diffraction

For high-resolution transmission electron microscopy (HRTEM) and electron diffraction (ED), the sample was gently crushed under ethanol in an agate mortar, and a drop of the resulting suspension was deposited onto a lacey carbon-covered Cu grid (Ted Pella). HRTEM was carried out using a JEOL 3010 at 300 keV (LaB₆ cathode, 0.17 nm point-to-point resolution, UHR pole piece) equipped with GIF. Electron diffraction measurements were carried out in

nanobeam ED mode using a Philips CM20 (operating at 200 keV) and a JEOL 3010 (operating at 300 keV) TEMs, both with LaB₆ cathode. The diameter of the analysed area was $1.5 \text{ }\mu\text{m}$ and 25 nm for CM20 and JEOL 3010 microscopes, respectively. The applied camera length was 500 mm . Special care was taken to avoid background in nanobeam ED, by selecting appropriate areas for diffraction. The scattered intensity was recorded using Ditas Imaging Plates ($17.5 \text{ }\mu\text{m}$ pixel size) and Gatan Orius CCD ($7.4 \text{ }\mu\text{m}$ pixel size) for CM20 and JEOL3010 microscopes, respectively. The use of Imaging Plates allows to record linear response to the electron dose over six orders of magnitude, which is ideal for measuring scattered intensity by amorphous structures. In the case of CCD, the dynamic range was extended by merging together diffraction patterns taken with different exposure times using the Digital Micrograph script written by Bernhard Schaffer (Gatan). The diffraction measurement procedure was based on the protocol summarized for selected area ED mode [14], which ensured reproducibility of camera length within 0.5%. Camera length was calibrated for the applied lens currents using a self-supporting random nanocrystalline Al thin film.

Thermal characterization

DTA measurements were performed using a SETARAM 92-16.18 DTA equipment with a TGA-92 set-up under Ar atmosphere. The DTA was calibrated by melting of high-purity In, Zn and Al metals, and each DTA scan consisted of a controlled heating with $10 \text{ }^\circ\text{C/min}$ constant heating rate and a subsequent instantaneous uncontrolled cooling of the sample (with an approximate initial cooling rate of $> 50 \text{ }^\circ\text{C/min}$).

XRD

X-ray diffraction (XRD) measurements were performed using a Bruker AXS D8 Discover diffractometer equipped with Göbel mirror and a scintillation detector with Cu K α radiation. The X-ray beam dimensions were $1 \text{ mm} \times 5 \text{ mm}$, the 2θ step size was 0.02° , and the scan speed $0.1^\circ/\text{min}$. We used the Diffrac.EVA program and the ICDD PDF database for phase identification.

Table 1 Nominal composition in mole% of the studied glass samples

	SiO ₂	CaO	Na ₂ O	P ₂ O ₅
S45P0	45	25	30	0
S45P1	45	25	29	1
S42P3	45	25	27	3
S45P5	45	25	25	5

XPS

Approximately 1-cm-sized specimens were selected for XPS analysis under ultrahigh vacuum conditions (2×10^{-9} mbar). The specimens were exposed to 70 °C heat treatment for 48 h, which is the standard baking procedure of the applied vacuum system. The photoelectron spectra were obtained using X-ray radiation (Al anode with water cooling, 15 keV excitation). Constant energy resolution of 1.5 eV was provided by a special cylindrical mirror analyser with a retarding field (type DESA 150, Staib Instruments Ltd.). All spectra were recorded with 0.1 eV energy steps. The XPS measurement yielded information on the average surface composition of an area of ca. 5 mm diameter. Detected lines: O 1s (532 eV); Ca 2p (347 eV); C 1s (285 eV); Na Auger (497 eV); P 2s (189 eV); Si 2p (100 eV). Low concentration elements such as P were recorded with longer detection time to improve the statistics and hence the reliability of the quantification. Spectra were evaluated by applying the usual Shirley background subtraction, and compositions were calculated from peak areas assuming homogeneous model. Sensitivity factors were calculated from the reference area in Ref. [15]. Concentration versus depth curves (called depth profiles) were recorded by alternating ion sputtering (1 keV Ar ion beam) and XPS measurement.

Bioactivity tests

To test the bioactivity of the bulk glasses, samples were incubated in simulated body fluid (SBF) for 30 min, 3 h, 3 days, 7 days and 21 days at 37 °C and $p(\text{CO}_2) = 0.05$ atm (5%) as human serum is in equilibrium with such a partial pressure [16]. The SBF and the validation of the apatite-forming ability were done according to the procedure of Kokubo and Takadama [17]. After soaking, the samples were removed from the SBF, gently washed with deionized water and dried at room temperature. The surface morphology of the dried samples was explored using a LEO 1540XB scanning electron microscope (SEM).

Structural modelling

Structure factor calculation based on neutron diffraction

Neutron diffraction data were used to deduce average structural information on the different bioactive

glasses. The total structure factors, $S(Q)$, were obtained from the ND experiments with a good signal-to-noise ratio up to $Q_{\text{max}} = 19 \text{ \AA}^{-1}$. The diffraction experiments performed up to high Q values were important to obtain fine r -space resolution for the atomic distribution function analyses. Figure 1 shows the experimental ND $S(Q)$ data of the investigated samples. For the first sight, the experimental ND curves seem to be similar and only slight differences can be observed in the region of the low Q values near the first visible peak at $1.5\text{--}2.2 \text{ \AA}^{-1}$.

The visible differences in the shape of the ND spectra are mainly due to the different values of the weighting factors, w_{ij} , of the partial structure factors, $S_{ij}(Q)$, defined as:

$$S(Q) = \sum_{i,j}^k w_{ij} S_{ij}(Q) \quad (1)$$

$$w_{ij}^{\text{ND}} = \frac{c_i c_j b_i b_j}{\left[\sum_{i,j}^k c_i b_j \right]^2} \quad (2)$$

where c_i , c_j are the molar fractions of the components, b_i , b_j the coherent neutron scattering amplitudes, and k the number of elements in the sample. The neutron scattering amplitude of an element is constant in the entire Q -range [18]. Table 2 shows the corresponding weighting factors for the atomic pairs, w_{ij} . It can be seen that the Si–O, Ca–O, Na–O and O–O atom pairs have significant contributions in the ND experiment.

Reverse Monte Carlo modelling

The experimental structure factors, $S(Q)$, data have been simulated by the reverse Monte Carlo (RMC) method using the software package RMC++ [19].

Figure 1 Total structure factors (dotted line) together with RMC fits (solid line) for S45 series of samples: S45P0 (red), S45P1 (green), S45P3 (blue) and S45P5 (purple). The curves are shifted vertically for clarity.

Table 2 ND weighting factors of the partial interatomic correlations in the glasses

Atom pairs	Weighting factor, w_{ij}^{ND} (%)			
	S45P0	S45P1	S45P3	S45P5
Si–O	16.93	16.70	16.37	16.04
Ca–O	10.64	10.52	10.29	10.07
Na–O	19.69	18.86	17.16	15.50
P–O	–	0.92	2.69	4.43
O–O	38.05	38.70	39.90	40.99
Si–Si	1.89	1.80	1.69	1.58
Si–Ca	2.38	2.28	2.12	1.98
Si–Na	4.38	4.07	3.52	3.03
Si–P	–	0.21	0.56	0.87
Ca–Ca	0.75	0.71	0.66	0.62
Ca–Na	2.75	2.56	2.21	1.91
Ca–P	–	0.13	0.35	0.55
Na–Na	2.54	2.31	1.85	1.47
Na–P	–	0.22	0.59	0.85
P–P	–	0.01	0.04	0.11

RMC minimizes the squared difference between the experimental $S(Q)$ and the calculated one from a 3D atomic configuration. The RMC algorithm calculates the one-dimensional partial atomic pair correlation functions $g_{ij}(r)$, and they are inverse-Fourier-transformed to calculate the partial structure factors, $S_{ij}(Q)$:

$$S_{ij}(Q) = 1 + \frac{4\pi\rho_0}{Q} \int_0^{r_{\max}} r[g_{ij}(r) - 1] \sin Qr dr \quad (3)$$

where $r_{\max}$ is the half edge-length of the simulation box of the RMC calculation. The actual computer configuration is modified by moving the atoms randomly until the calculated $S(Q)$ agrees with the experimental data within the experimental error. Moves are only accepted if they are in accordance with certain constraints.

For the starting RMC model, a disordered atomic configuration was built up with a simulation box containing 10,000 atoms with density data 0.076, 0.0752, 0.0741 and 0.0714 atoms/Å^{−3} and $r_{\max}$ = 26.39, 26.52, 26.65 and 26.93 Å for the S45P0, S45P1, S45P3 and S45P5 glasses, respectively. In the RMC simulation procedure, two types of constraints were used, for the minimum interatomic distances between atom pairs (cut-off distances) to avoid unreasonable atom contacts and coordination constraints. For the starting configuration, we have used

the results based on the literature and our previous results for binary SiO₂–Na₂O [20] and CaO–P₂O₅ [21] glasses. We apply two types, a positive and a negative coordination constraint for the network former Si atoms. Based on the literature and our previous results [22–24], it is reasonable to suppose that silicon has a fourfold oxygen coordination as a positive constraint, and the lack of onefold and/or twofold oxygen coordination as negative constraints.

Structure factor calculation based on electron diffraction

Electron diffraction-based structural analysis was carried out parallel to the ND-based RMC simulations to obtain localized information on the glassy structure. As structural inhomogeneities are related to phosphate content [8–10], we focused these experiments for the S45P5 sample. Table 3 compares ND and ED weighting factors of the X–O (X: Si, Ca, Na, P, O) interatomic correlations for the S45P5 composition. In the case of electron scattering, a simple approach was used and the angular dependence of the scattering factor was neglected. Similar simplification was previously applied in the literature for X-ray scattering [25]. In Table 3, the ED weighting factors for zero scattering angle are listed. As it can be seen, cation–O contributions in the ED measurement are quite similar to those in ND measurement, implying that the reliability of these correlations and the derived first-neighbour distances will be similar as well. As the ED-based quantitative structural analysis of amorphous solids (e.g. the calculation of the partial correlation functions) has not yet been fully established in the literature, this statement supports the expectation that ED

Table 3 Comparison of the isotropic ND weighting factors w_{ij}^{ND} and the angle-dependent ED weighting factors for zero scattering angle w_{ij}^{ED} for the S45P5 composition

S45P5	w_{ij}^{ND} (%)	w_{ij}^{ED} (%)
Si–O	16	13.5
O–O	41	8.4
Ca–O	10	12.7
Na–O	15.5	12.2
P–O	4.5	2.8

The atomic scattering factors for electrons are for neutral atoms and based on the formula given by Peng et al. [26]

measurements on small volumes of bioactive glasses provide reliable structural data.

From Table 3, it is also seen that, while during ND experiment almost all of the overall scattering (ca. 90%) is from O–O and cation–O contribution, in the case of electron scattering this contribution comprises only 50% of the overall scattering, implying a significant cation–cation (mostly Si–Si) contribution for this composition, which carries structural information on the medium-range order (MRO).

ED patterns were acquired from different sample volumes in the S45P5 glass using 200 keV and 300 keV electrons and analysed subsequently with the Process Diffraction software [27]. Reduced interference functions were derived from ED measurements and compared to that calculated from ND experiments as shown in Fig. 2. The position of the first sharp diffraction peak at $2.2 \text{ \AA}^{-1}$ coincides, however, in the interference function of the 300 keV electron diffraction measurement; additional peaks appear as marked by arrows. At first glance, the 200 keV measurements appear to be better resolved at high Q values than the 300 keV one. This can be explained with the different experimental set-up: (1) during the 300 keV measurement, scattered intensity is gathered from a 25-nm-diameter area, while in the case of 200 keV the analysed volume is 60 times

larger (supposing the same sample thickness), which implies significant improvement in signal-to-noise ratio; and (2) in the case of 200 keV measurement the detection efficiency due to the application of Imaging Plates was higher [28].

Results and discussion

Thermal stability

Thermal analysis of the studied bioactive glasses was performed in linear heating experiments. Figure 3a shows the thermal signals exhibiting a glass transition and a single exothermic devitrification event followed by a multiple-stage melting for all the different glass compositions. Figure 3b indicates the weight loss curves measured during the same linear heating DTA scans. Characteristic temperatures of the different thermal processes, such as glass transition temperature (T_g), the peak temperature of the exothermic devitrification event (T_x), the melting temperature (T_m) and the peak temperature of the weight loss rate (TG peak), have been determined and are summarized in Table 4.

Fused silica glass crystallizes at high temperatures and has a T_g at about 1200°C due to their high-strength SiO_4 tetrahedron network [29]. It is well known that already trace amount of alkali elements, especially Na, reduces effectively the crystallization temperature of silica glass by breaking the network and promoting the rearrangement of the SiO_4 tetrahedra [30]. Therefore, it is not surprising that the T_g and T_x temperatures are substantially lower for the Ca- and Na-containing S45P0 sample than for fused silica. P is also a network-forming component, and the addition of low concentrations of phosphate to the glass induces a gradual increase in T_g and T_x . This is visible in Fig. 4, where with increasing phosphate content the glass transition temperature shifts to higher values from 516°C for S45P0 composition to 550°C for S45P5 composition [31]. This trend fits well with a linear function with $7\text{C/at\%}$ slope, which implies that the glass transition temperature is directly related to the amount of PO_4 tetrahedra in the network structure. Similarly, linear relationship was found between the T_g and the composition of miscible blends of phosphate glasses [32]. Above the glass transition temperature, the rigid structure of the glass transits into the viscous supercooled liquid state

Figure 2 Reduced interference functions from electron and neutron diffraction measurements. The position of the first sharp diffraction peaks (dashed line) coincides independently from the scattering experiment. Extra peaks on the 300 keV electron diffraction measurements with respect to the 200 keV experiment are indicated by arrows.

Figure 3 Thermal analysis of the glasses with the **a** artificially displaced thermal signals showing the glass transition (T_g), the exothermic devitrification event (T_x) and melting (T_m) and **b** the weight loss curves shifted to a common origin at 300 °C. The

Table 4 Characteristic temperatures of the thermally activated processes for the different bioactive glass compositions

Sample	T_g (°C)	T_x (°C)	T_m (°C)	TG peak (°C)
S45P0	516	662	1215	503
S45P1	527	689	1192	467
S45P3	540	754	1209	418
S45P5	550	690	1183	410

insets show the magnified TG(T) curve of the Si45P5 sample with the $T_{G_{start}}$ and $T_{G_{end}}$ temperatures and the corresponding derived smoothed weight loss rate curve with the $T_{G_{peak}}$ temperature.

in which thermal atomic movements can gradually transform it into the equilibrium crystalline state.

As shown in Fig. 4a, structural strengthening due to the PO_4 content increases also the stability of the supercooled liquid state, so that T_x is also increased gradually with the PO_4 content up to 3 mol% of phosphate concentration. However, SiO_2 and P_2O_5 have a large miscibility gap in crystalline state and, according to the phase diagram [33], at low

Figure 4 **a** The different characteristic temperatures as a function of the P concentration of the bioglass samples, where T_g is the inflection point of the glass transition temperature and T_x is the peak temperature of the exotherm crystallization event. $T_{TG_{start}}$,

$T_{TG_{peak}}$ and $T_{TG_{end}}$ are the start, peak and end temperatures of the weight loss process, respectively. **b** The weight loss as a function of the P concentration of the bioglass samples.

temperature only eutectic forms and practically no miscibility exists. At higher temperature, above cc. 1000 °C, in the liquid state phosphate is miscible in liquid silica. Presumably, this better miscibility prevails in the glassy state as well. The continuously increasing T_g indicates the increase in the cohesion in the glass structure with phosphate content. It is an unexpected behaviour, because the melting point of phosphate glasses is typically lower than that of silica glass. The same trend can be observed in the case of the T_x crystallization temperature up to 3% PO_4 content. Above this concentration, the phosphate component becomes saturated and phase separation is preferred. The phase separation in the supercooled liquid state is indicated by the drop of the T_x for S45P5 sample.

At the same time, the investigated glasses show another minor transition, namely a 0.02–0.25% weight loss during the heat treatment. This process also indicates the appearance of some mobility in the glass structure with the increasing temperature. For S45P0, the peak of the weight loss process coincides with the glass transition temperature, indicating a close relation between the two processes. The increase in phosphate content reduces the total weight loss and also the temperatures of the weight loss process. The large melting point difference between the silica and phosphate phases [32] indicates that the PO_4 -containing structure is less stable at elevated temperatures; thus, we anticipate that partial melting of the PO_4 -containing environments induces mobility in the glass structure. This process results in the lowering of weight loss temperature at higher phosphate concentration.

The decrease in total weight loss with phosphate content implies that the amount of volatile component is decreasing. Previous studies indicate the clustering of phosphate [9] and the non-uniform distribution of Ca^{2+} in the network structure [8]. We suppose that the volatile component becomes bonded by the formation of more stable $\text{Ca}(\text{Na?})$ -phosphate clusters in the glass. These clusters are able to trap the volatile component and thus remove it from the channels of the silica-dominated network structure, leading to the decrease in the total weight loss during heating.

Above 800 °C, the glasses transform into a crystalline glass-ceramic material, as indicated by the presence of crystalline phases in the XRD patterns of the heat-treated sample (Fig. 5). It is clearly seen that

one phase, the hexagonal sodium calcium silicate ($\text{Na}_6\text{Ca}_3\text{Si}_6\text{O}_{18}$, ICDD PDF Nr: 077-2189, B in Fig. 5), is present in all the samples. This phase was identified in the thermally treated Bioglass® above 600 °C as well [5]. Besides that, in sample S45P5, similarly to Bioglass® [5] the presence of orthorhombic beta sodium calcium phosphate silicate ($\text{Na}_2\text{Ca}_4(\text{PO}_4)_2\text{SiO}_4$, ICDD PDF Nr: 32-1053) can be observed. Decreasing the phosphorus content, in sample S45P3 this latter phase disappears, and only the hexagonal phase is present. Further decrease in the phosphorus content leads to the appearance of the lines of cubic sodium calcium silicate ($\text{Na}_{15.6}\text{Ca}_{3.84}(\text{Si}_{12}\text{O}_{36})$, ICDD PDF Nr: 75-1332, A in Fig. 5), as well as further lines in sample S45P1. These unidentified lines are denoted by arrows in Fig. 5. The diffractogram of sample S45P0 is fairly similar to that of S45P1 and shows the same tendency: the lines of the cubic phase and the unidentified lines are stronger, while the lines of the hexagonal phase are weaker.

Network structure from neutron diffraction and reverse Monte Carlo simulation

Several RMC runs have been completed by modifying the cut-off distances in such a way that the results of each run have been carefully checked to obtain reliable data for each partial pair correlation function (ppcf) and coordination number (CN) distributions.

Figure 5 XRD patterns of the different bioactive glasses after linear heat treatment up to 800 °C. The different devitrified crystalline phases are indicated as green sticks— $\text{Na}_{15.6}\text{Ca}_{3.84}(\text{Si}_{12}\text{O}_{36})$, ICDD PDF Nr: 75-1332, black sticks— $\text{Na}_6\text{Ca}_3\text{Si}_6\text{O}_{18}$, ICDD PDF Nr: 077-2189, and *— $\text{Na}_2\text{Ca}_4(\text{PO}_4)_2\text{SiO}_4$, ICDD PDF Nr: 32-1053. Arrows indicate unidentified peaks in the S45P0 and S45P1 samples.

Results for the most important partial pair correlation functions obtained from the RMC simulation are displayed in Fig. 6.

For Si–O, a covalent bond length at $1.60 \text{ \AA}$ was revealed for all studied glasses, showing an excellent agreement within limit of error (see Table 5). This is a somewhat shorter value than that in $v\text{-SiO}_2$ ($1.615 \text{ \AA}$) or in $70\text{SiO}_2\text{--}30\text{Na}_2\text{O}$ ($1.62 \text{ \AA}$) [20 and references therein]. The coordination number distribution shows that Si atoms are surrounded by four oxygen atoms. The actual average coordination numbers are 3.67, 3.78, 3.77 and 3.78 (± 0.15), where the coordination constraint was fulfilled by 83.1%, 91.7%, 90.9% and 91.2%, for the S45P0, S45P1, S45P3 and S45P5, respectively (see Fig. 7a).

For the Ca–O network, we have established two distinct first-neighbour distances at $2.30 \pm 0.05 \text{ \AA}$ and $2.55 \pm 0.05 \text{ \AA}$, in agreement with the high-resolution neutron diffraction study [21]. Taking into consideration the medium resolution of the present ND experiment, the agreement is reasonably reported for CaSiO_3 glasses [8, 24]. For the studied glassy compositions of the Ca–O average coordination number, distributions close to threefold coordinated oxygen atoms are obtained, that is 2.99, 2.68, 2.86 and $2.56 (\pm 0.15)$ atoms for the S45P0, S45P1, S45P3 and S45P5 compositions, respectively (see Fig. 7b).

The P–O first-neighbour distributions show a characteristic peak at $1.60 \pm 0.05 \text{ \AA}$ and a small second peak at $2.00 \pm 0.1 \text{ \AA}$, where the second peak intensity changes in the function of phosphorous concentration. The agreement is reasonably reported for CaP glasses [8, 21]. The P–O average coordination number varies as 3.97, 3.93 and 3.94 (± 0.05) atoms for the S45P1, S45P3 and S45P5, respectively (see Fig. 7c).

Unfortunately, $g_{\text{Na-O}}(r)$ and $g_{\text{O-O}}(r)$ overlap with each other; thus, the results have to be handled carefully. It can be established that for the S45P3 and S45P5 glasses the distributions are similar. In the case of S45P0 and S45P1, the O–O distribution shows a wide distribution with one peak. This indicates that the modifier Na ions prefer the neighbourhood of Si-oxide units, indicating that Na_2O acts as a modifier as it breaks up the silicate network, similarly to any alkali oxides, producing non-bridging oxygen atoms within the network. For Na–O, a double peak has been revealed at $2.27\text{--}2.35 \pm 0.03 \text{ \AA}$ and $2.62 \pm 0.03 \text{ \AA}$ for all samples [34, 35]. Two well-defined peaks have been obtained for the O–O at $2.30 \pm 0.03 \text{ \AA}$ and $2.65 \pm 0.04 \text{ \AA}$ [8, 22, 36]. Note that the overlapping character of Na–O and O–O distributions should be taken into account.

Figure 6 **a** Si–O, **b** Ca–O, **c** P–O and **d** O–O ppcf's for S45P0 (red), S45P1 (green), S45P3 (blue) and S45P5 (purple) glasses.

Table 5 Most important oxygen-linked atomic distance, r_{ij} (Å) obtained from RMC simulation

Sample	Interatomic distances, r_{ij} (Å)				
	Si–O	Ca–O	Na–O	P–O	O–O
S45P0	1.60 ± 0.01	$2.30/2.55 \pm 0.05$	$2.25/2.65 \pm 0.05$	–	2.52 ± 0.05
S45P1	1.60 ± 0.01	$2.30/2.60 \pm 0.05$	$2.25/2.60 \pm 0.05$	1.60 ± 0.05	2.55 ± 0.05
S45P3	1.60 ± 0.01	$2.30/2.55 \pm 0.05$	$2.25/2.55 \pm 0.05$	1.60 ± 0.05	$2.30/2.55 \pm 0.05$
S45P5	1.60 ± 0.01	$2.33/2.55 \pm 0.05$	$2.25/2.55 \pm 0.05$	1.60 ± 0.05	$2.30/2.56 \pm 0.05$

Figure 7 a Si–O, b Ca–O and c PO CN's distributions from RMC modelling: S45P0 (red), S45P1 (green), S45P3 (blue) and S45P5 (purple) glasses.

The RMC modelling provides information on the second coordination sphere. The shortest second-neighbour distances are obtained for the Si–Si and Si–P ppcf's with characteristic distributions, as it is illustrated in Fig. 8.

Si–Si correlation functions show distributions at $2.95/3.05 \pm 0.02$ Å, which is in good agreement with the literature data [20, 22] and supports the formation of well-defined SiO_4 units. In the case of S45P1 sample, the Si–P correlation functions consist of a double peak with distances at $2.85/3.10 \pm 0.05$ Å, these are melting to the one wider peak at 3.10 ± 0.05 Å for the S45P3 and S45P5 samples, and the P concentration dependence can be observed. The shortest second-neighbour distances obtained for Si–P as ~ 3 Å show a connection between the SiO_4 and PO_4 tetrahedral units, which indicates that in the

building of the basic glass network take parts the [4]Si–O–[4]P linkages.

We have calculated the three-particle bond angle distributions (BAD) using the final atomic configuration of the RMC simulation, plotted as the function of both $\cos(\theta)$ and θ , scale below and above, respectively, where θ represents the actual bond angle. Figure 9 shows the distributions for the network former atoms: Si–O–Si, O–Si–O, P–O–P, O–P–O, P–O–Si and O–O–O. For the Si–O–Si and O–Si–O, the peak positions are at $148^\circ \pm 3^\circ$ and $108^\circ \pm 3^\circ$, respectively, which are very close values to the ideal tetrahedral (Si–O–Si and O–Si–O at 149° and 109.5° [37]) configuration. O–Si–O bond angle distribution exhibits a pronounced shoulder at a lower value, at $91^\circ \pm 3^\circ$. The peaks of the bond angle distributions for P–O–P and O–P–O are very similar to Si–O–Si and O–Si–O

Figure 8 Second-neighbour partial atomic pair correlation functions obtained from the RMC modelling a Si–Si and b Si–P, where S45P0 (red), S45P1 (green), S45P3 (blue) and S45P5 (purple) glasses.

Figure 9 a Si–O–Si, b O–Si–O, c P–O–P, d O–P–O, e P–O–Si and f O–O–O BAD for S45P0 (red), S45P1 (green), S45P3 (blue) and S45P5 (purple) glasses.

distributions. Characteristic distribution of P–O–P bonding angles show peaks at $145^\circ \pm 5^\circ$. The broad distribution of O–P–O bond angles shows double peaks, the average angles being $107.5^\circ \pm 5^\circ$ and $92^\circ \pm 5^\circ$. These distributions suggest that fourfold P atoms are present. The O–P–O bond angle distributions are close to the O–Si–O distribution. These detailed features of Si–O–Si and P–O–P bond angle distributions are consistent with the obtained coordination numbers. The P–O–Si distribution shows a peak at $149^\circ \pm 5^\circ$ at lower phosphorous concentration. With increasing the P concentration appears a second peak at $135 \pm 3^\circ$, which became stronger with the increasing P concentration. The P–O–Si angle distribution is close to the Si–O–Si/P–O–P

distributions, in agreement with Tilocca et al. [7]. The O–O–O bond angle distribution shows peaks centred at $60^\circ \pm 2^\circ$.

The short-range order of the glassy network structure is determined by two parameters, the bond length and the oxygen–cation–oxygen bond angles. Si–O and P–O bond lengths, both $1.60 \text{ \AA}$, coincide for all compositions within the error of the measurement (Table 1) and bond angle distributions, specific of the silicate structure, fall fairly close to each other as well (Fig. 8). This implies similar average network structures for all compositions, in good agreement with the literature data [38, 39]. However, careful observation of the average coordination numbers allows us to make some considerations regarding the

changeability in the network structure. In the case of S45P0 glass, the average coordination number of Si is 3.67, in agreement with the literature data for soda-lime glasses [40], indicating the presence of non-bridging oxygen, i.e. Si–O–Ca- and Si–O–Na-type connections, which break up the network structure [41]. By adding phosphate to the system, the coordination number of Si slightly increases, but still remains below 4 (3.78, 3.77 and 3.78, for S45P1, S45P3 and S45P5, respectively), while that of P fairly coincides with the ideal value of the tetrahedral PO_4 units (3.97, 3.93 and 3.94 for S45P1, S45P3 and S45P5, respectively).

Similarly, different coordination numbers were found for the network formers Al and Si in $\text{Ca}_{x/2}\text{Al}_x\text{Si}_{1-x}\text{O}_2$ glasses [38] and explained by the presence of Si–O–Ca-type bonds, which reduces the coordination number of Si without creating vacancy in the network structure [42]. This way, two types of atomic environments are forming in Ca–Al–Si-oxide glasses, namely Si–O and Al–O tetrahedral, and the former one will promote the disintegration of the network structure by the non-bridging oxygen-type Si–O–Ca linkages.

In our case, silica-rich and phosphate-rich environments were deduced from thermal measurements. The linear increase in T_g with phosphate content indicates the strengthening of network structure, which is also reflected in the increase in the average coordination number of Si by ca. 3%. We

Figure 11 **a** Typical HRTEM image taken from the S45P5 glass indicates nanocrystalline domains in the glassy matrix. **b** Inverse Fourier transform of the area indicated by white box, which contains a nanocrystal embedded in the glassy matrix. **c** Lattice fringe periodicity of the nanocrystal is measured as 2.7 Å.

propose that this strengthening of the network structure relies on the removal of Ca (and probably Na) from the environment of Si by the phosphate clusters. In this way, Ca- and P-rich environments

Figure 10 **a** Total pair distribution functions from electron diffraction measurements, **b** low r range of the total pair distribution functions from electron diffraction measurements with the indicated first-neighbour distances determined by neutron-based RMC simulation.

form, which, as indicated by the coordination numbers of P, are well ordered, independently of the overall phosphate content of the glass. These Ca–P clusters are similar in bonding to the building blocks of crystalline Ca–phosphates which can be stable up to above 1000 °C. Thus, the increase in thermal stability reflected in the slopes of the T_g can be explained by the formation of P–O–Ca instead of non-bridging oxygen-type Si–O–Ca linkages. As phosphate traps Ca (and probably Na) by incorporating them into a more ordered, and thermally more stable structure,

the weight loss should seemingly decrease with phosphate content, which is in agreement with thermal data (Fig. 4b).

Nanostructure: ePDF analysis, HRTEM and XPS

As both thermal properties and RMC indicated nanoscale inhomogeneities in the network structure, an attempt was made to prove directly the presence of these inhomogeneities using local analytical

Figure 12 Low-magnification HRTEM of sample S45P5. **a** Image taken at the beginning of the analysis, **b** Fourier transform of the whole, ca. 150×150 nm area indicates the dominance of 8.1 Å, 5.2 Å and 3.4 Å periodicities which are in good agreement with $d(100)$, $d(101)$ and $d(200)$ lattice spacings of

apatite. **c** After a few minutes of exposure to the electron beam, the studied volume exhibits a significant structural rearrangement. **d** On the Fourier transform of **c** Miller indices of apatite are marked.

methods. Electron diffraction-based pair distribution function (ePDF) analysis was carried out on S45P5 sample. As this sample has the highest P_2O_5 content, structural deviations from the SiCaNa glasses, if there are any, are expected to be the most enhanced.

Figure 10 shows the total pair distribution functions of the ED measurements (ePDF). Comparing atomic distances derived from neutron-based RMC and ePDF, it can be concluded that the main peak positions are the same; however, smaller shift can be observed in the case of the 1.6 Å and 2.3 Å peaks. It has been proven for nanocrystalline materials that ePDF peak positions can be used for fingerprint phase identification [43]. Similarly, we made a set of measurements on amorphous silica, which indicated that peak position originating from atom pair frequencies on ePDF does not vary with experimental and evaluation parameters (Supplementary Material). Thus, we think that the ePDFs reflect real structural features and imply structural inhomogeneities on the nanometre scale.

Figure 11 shows a HRTEM image of the S45P5 sample. Lattice fringes of 2.7 Å periodicity are apparent, which originates from a ca. 5-nm-sized crystalline domain embedded in the amorphous matrix. Such crystalline nanodomains remain unrevealed during bulk neutron diffraction measurements, and their uneven distribution in the glass matrix can lead to the observed differences in the ePDFs.

Besides individual crystalline nanodomains like the one shown in Fig. 11, larger areas exhibiting nanocrystalline character have been also observed (Fig. 12a). The Fourier transform of the ca. 150×150 nm area (Fig. 12b) provides an overview of the distribution of spatial frequencies in the analysed sample volume. According to the intensity profile, 8.1 Å, 5.2 Å and 3.4 Å periodicities are dominant, which are in good agreement with $d(100)$, $d(101)$ and $d(200)$ lattice spacings of apatite. The studied area exhibited strong radiation sensitivity, and a significant structural rearrangement was observed after few minutes under the electron beam (Fig. 11c, d). The resulting structure is also nanocrystalline and, according to the Fourier transform (Fig. 11d), can be identified as apatite. Comparing the Fourier transforms before and after the structural rearrangement, it seems that the size of the crystalline domains not, only their number has increased.

As the crystalline (apatite-like) character has been enhanced under the electron beam, we cannot state steadily that the crystalline domains presented in Fig. 11a are inherent in the S45P5 glass structure. However, the fact that the structural rearrangement under the electron beam resulted in nanocrystalline apatite serves as an indirect proof of the chemical inhomogeneity of the glass structure, manifested in the formation of Ca- and P-rich environments. The sample volume analysed in Fig. 11 originally contained undoubtedly more Ca and P than silica, as proven by its ability to transform into nanocrystalline apatite. Sample volumes, which did not show this type of structural rearrangement, are supposed to build up by dominantly silica.

Surface properties, like morphology, surface area and surface chemistry, have prominent role in bioactivity. As the surface composition can deviate even significantly from the bulk composition, XPS measurements were applied to judge the potential bioactive behaviour of the glass samples. All the samples exhibited strong carbon signal due to surface contamination. Depth profile measurement of the highest-phosphate-containing S45P5 glass (Fig. 13) indicates that this carbon signal disappears at ca. 2 nm depth, and, in parallel, the concentration of Si increases. Interestingly, Na and P concentrations remain almost constant, irrespectively of the surface contamination. The detected P content in this S45P5 is 2.6 at% which corresponds to 9.2 mol% P_2O_5 . That is somewhat higher than the nominal 5 mol% of P_2O_5 . Since the information depth of XPS measurement is about 3 nm for these peaks, the far bulk composition is not reached by this technique. The increased P_2O_5

Figure 13 Elemental concentration down to ca. 15 nm depth calculated from XPS lines for S45P5 specimen.

Figure 14 SEM images at two different magnifications together with the EDS spectra of the reaction layer formed on the surface of the PO_4 -containing samples after 21 days of soaking in SBF prove

the apatite-forming ability. **a, b** S45P1 sample, **c, d** S45P3 sample, **e, f** S45P5 sample.

content in the studied 15-nm layer with respect to the expected bulk value can be attributed to the quenching procedure and anticipates good reactivity under physiological conditions.

Bioactivity

The bioactivity is generally described as the apatite-forming ability of the material on its surface after merging in SBF. Although there are several recipes

and procedures to test the bioactivity, in this study we followed the most frequently used protocol published by Kokubo and Takadama [17] completed with the criterion regarding the CO_2 partial pressure [16]. Figure 14 presents SEM images and EDS spectra of the well-developed reaction layer formed after 21 days of soaking in SBF.

On the surface of all three PO_4 -containing glasses, a phosphorus-containing reaction layer was formed already after 30-min soaking [44]. This reaction layer was not continuous, and its composition also

changed from place to place. Morphologically, similar layer was formed on the surface of the S45P0 sample as well; however, this layer was phosphorus free. As the SBF is supersaturated with respect to apatite, this observation is of key importance and supports that the reaction layer is indeed the product of the incipient ion exchange between SBF and glass and not heterogeneously precipitated phosphate phase on the surface of the glass.

Based on morphological and compositional criteria [17], the apatitic reaction layer on the surface of all three samples can be recognized. A detailed nanostructural analysis of the bioactive layer of the glass samples is a subject of another paper.

Conclusions

The structure of $\text{SiO}_2(45)\text{CaO}(25)\text{Na}_2\text{O}(30 - x)\text{P}_2\text{O}_5(x)$ ($x = 0, 1, 3, 5$) glasses has been studied using diffraction methods, RMC simulation and HRTEM and compared to the composition-dependent thermal properties.

Neutron diffraction-based RMC simulation revealed that the average Si–O and P–O network structures of the different glasses with Ca and Na modifiers are similar on the short-range scale, since both partial pair correlation functions and first neighbours nearly coincide for the different glasses within the error of the measurement. However, the differences observed in the coordination of the Si and P atoms indicate varying medium-range order for the different glass compositions.

Based on the tendentious change of thermal stability with increasing P content, we presume that weakly bounded Ca (and Na) was removed from the environment of Si in the silicate network by forming phosphate clusters which are more stable as they melt above 1000 °C in the bulk form. Thus, the enhanced thermal stability, reflected in the linear increase in the glass transition temperature with phosphate content, can be explained by the formation of these P–O–Ca linkages instead of non-bridging oxygen-type Si–O–Ca linkages. Therefore, Ca–P-rich clusters are similar in bonding to crystalline Ca-phosphates and may trap additional volatile cations, like Na, in agreement with the total weight loss of the glasses on thermal activation. The tendency for Na–P association in weakly bounded atomic environments was demonstrated by the Na- and P-rich surface

chemistry revealed by XPS, while, at the larger P content ($x = 5$), the formation of Ca–P-rich clusters as nanometre-range heterogeneities was observed in HRTEM. We propose that these atomic-scale heterogeneities have a key role in the behaviour of phosphate-doped bioactive glasses under physiological conditions.

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References

- [1] Jones JR (2013) Review of bioactive glass: from Hench to hybrids. *Acta Biomater* 9:4457–4486

- [2] Gerhardt LC, Boccaccini AR (2010) Bioactive glass and glass–ceramic scaffolds for bone tissue engineering. *Materials* 3:3867–3910
- [3] Baino F, Vitale-Brovarone C (2011) Three-dimensional glass-derived scaffolds for bone tissue engineering: current trends and forecasts for the future. *J Biomed Mater Res A* 97:514–535
- [4] Abou Neel EA, Pickup DM, Valappil SP, Newport RJ, Knowles JC (2009) Bioactive functional materials: a perspective on phosphate-based glasses. *J Mater Chem* 19:690–701
- [5] Lefebvre L, Chevalier J, Gremillard L, Zenati R, Thollet G, Bernache-Assolant D, Govin A (2007) Structural transformations of bioactive glass 45S5 with thermal treatments. *Acta Mater* 55:3305–3313
- [6] Elgayar I, Aliev AE, Boccaccini AR, Hill RG (2005) Structural analysis of bioactive glasses. *J Non-Cryst Solids* 351:173–183
- [7] Tilocca A, Cormack NA, Leeuw NH (2007) The structure of bioactive silicate glasses: new insight from molecular dynamics simulations. *Chem Mater* 19:95–103
- [8] FitzGerald V, Pickup DM, Greenspan D et al (2007) A neutron and X-ray diffraction study of Bioglass® with Reverse Monte Carlo modelling. *Adv Funct Mater* 17:3746–3753
- [9] Fayon F, Duée C, Poumeyrol T, Allix M, Massiot D (2013) Evidence of nanometric-sized phosphate clusters in bioactive glasses as revealed by solid-state ^{31}P NMR. *J Phys Chem C* 117:2283–2288
- [10] Lockyer MWG, Holland D, Dupree R (1995) NMR investigation of the structure of some bioactive and related glasses. *J Non-Cryst Solids* 188:207–219
- [11] Karadjin M, Essers Ch, Tsitlakidis S, Reible AM, Boccaccini AR, Westhauser F (2019) Biological properties of calcium phosphate bioactive glass composite bone substitutes: current experimental evidence. *Int J Mol Sci* 305:1–22
- [12] Sváb E, Gy Mészáros, Deák F (1996) Neutron powder diffractometer at the Budapest research reactor. *Mater Sci Forum* 228:247–252
- [13] Cuello GJ, Darpentignz J, Hennet L (2016) 7C2, the new neutron diffractometer for liquids and disordered materials at LLB. *J Phys Conf Ser* 746:012020
- [14] Kis VK, Dódony I, Lábár JL (2006) Amorphous and partly ordered structures in SiO_2 rich volcanic glasses. An ED study. *Eur J Miner* 18:745–752
- [15] Crist BV (ed) (2000) Handbook of monochromatic XPS spectra. Wiley, New York
- [16] Bohner M, Lemaitre J (2009) Can bioactivity be tested in vitro with SBF solution? *Biomaterials* 30:2175–2179
- [17] Kokubo T, Takadama H (2006) How useful is SBF in predicting in vivo bone bioactivity? *Biomaterials* 27:2907–2915
- [18] Hannon AC (2006) ISIS Disordered materials database. <http://www.isis2.isis.rl.ac.uk/Disordered/Database/DBMain.htm>
- [19] Gereben O, Jovari P, Temleitner L, Pusztai L (2007) A new version of the RMC⁺⁺ Reverse Monte Carlo programme, aimed at investigating the structure of covalent glasses. *J Optoelectron Adv Mater* 9:3021–3027
- [20] Fábrián M, Jóvári P, Sváb E, Gy Mészáros, Proffen T, Veress E (2007) Network structure of $0.7\text{SiO}_2\text{--}0.3\text{Na}_2\text{O}$ glass from neutron and x-ray diffraction and RMC modelling. *J Phys Condens Mater* 19:335209
- [21] Wetherall KM, Pickup DM, Newport RJ, Mountjoy G (2009) The structure of calcium metaphosphate glass obtained from X-ray and neutron diffraction and reverse Monte Carlo modelling. *J Phys Condens Mater* 21:035109
- [22] Fábrián M, Sváb E, Gy Mészáros, Zs Révay, Proffen T, Veress E (2007) Network structure of multi-component sodium borosilicate glasses by neutron diffraction. *J Non-Cryst Solids* 353:2084–2089
- [23] Vedishcheva NM, Shakhmatkin BA, Wright AC (2004) The structure of sodium borosilicate glasses: thermodynamic modelling vs. experiment. *J Non-Cryst Solids* 39:345–346
- [24] Mead RN, Mountjoy G (2005) The structure of CaSiO_3 glass and the modified random network model. *Phys Chem Glasses* 46:311–314
- [25] Kohara S, Suzuya K (2005) Intermediate-range order in vitreous SiO_2 and GeO_2 . *J Phys Condens Matter* 17:S77–S86
- [26] Peng LM, RenSL, Dudarev SL, Whelan MJ (1996) Robust parametrization of elastic and absorptive electron atomic scattering factors. *Acta Cryst A* 52:257–276
- [27] Lábár JL (2005) Consistent indexing of a (set of) SAED pattern(s) with the process diffraction program. *Ultramicroscopy* 103:237–249
- [28] Zuo JM (2000) Electron detection characteristics of a slow-scan CCD camera, imaging plates and film, and electron image restoration. *Microsc Res Tech* 49:245–268
- [29] Ojovan MI (2008) Viscosity and glass transition in amorphous oxides. *Adv Condens Mater Phys*. <https://doi.org/10.1155/2008/817829>
- [30] Fanderlik I (1991) Silica glass and its application. Glass science and technology, vol 11. Elsevier, Amsterdam. ISBN 0-444-98755-X
- [31] Mabrouk A, Bachar A, Atbir A, Follet C, Mercier C, Tricoteaux A, Leriche A, Hampshire S (2018) Mechanical properties, structure, bioactivity and cytotoxicity of bioactive Na–Ca–Si–P–O–(N) glasses. *J Mech Behav Biomed Mater* 86:284–293

- [32] Fulchiron R, Belyamani I, Otaigbe JU, Bounor-Legare V (2015) A simple method for tuning the glass transition process in inorganic phosphate glasses. *Sci Rep* 5:8369. <https://doi.org/10.1038/srep08369>
- [33] Rahman M, Hudon P, Jung I-H (2013) A coupled experimental study and thermodynamic modelling of the SiO_2 – P_2O_5 system. *Metal Mater Trans* 44B:837–852
- [34] Fabian M, Svab E, Proffen Th, Veress E (2008) Structure study of multi-component borosilicate glasses from high-Q neutron diffraction measurement and RMC modelling. *J Non-Cryst Solids* 354:3299–3307
- [35] Cormier L, Neuville DR (2004) Ca and Na environments in Na_2O – CaO – Al_2O_3 – SiO_2 glasses: influence of cation mixing and cation-network interactions. *Chem Geol* 213:103–113
- [36] Poulsen HF, Neuefeind J, Neumann HB, Schneider JR, Zeidler MD (1995) Amorphous silica studied by high energy X-ray diffraction. *J Non-Cryst Solids* 188:63–74
- [37] Floriano MA, Venezia AM, Deganello G, Svensson EC, Root JH (1994) The structure of pumice by neutron diffraction. *J Appl Cryst* 27:271–277
- [38] Petkov V, Billinge SJL, Shastri S, Himmel B (2000) Polyhedral units and network connectivity in calcium aluminosilicate glasses from high-energy X-ray diffraction. *Phys Rev Lett* 85:3436
- [39] Bouty O, Delaye JM, Beuneu B, Charpentier T (2001) Modelling borosilicate glasses of nuclear interest with the help of RMC, WAXS, neutron diffraction and ^{11}B NMR. *J Non-Cryst Solids* 401:27–31
- [40] Ha MT, Garofalini SH (2016) Local structure of network modifier to network former ions in soda-lime alumina-borosilicate glasses. *J Am Cer Soc* 14565:1–9
- [41] Yu Y, Renny M, Eden M (2018) Quantitative composition-bioactivity relationships of phosphosilicate glasses: bearings from the phosphorus content and network polymerization. *J Non-Cryst Solids* 502:106–117
- [42] Stebbins JF, Xu Z (1997) NMR evidence for excess non-bridging oxygen in an aluminosilicate glass. *Nature* 360:60–62
- [43] Gorelik TE, Schmidt MU, Kolb U, Billinge SLJ (2015) Total-scattering pair-distribution function of organic material from powder electron diffraction data. *Microsc Microanal* 2:459–471
- [44] Mahdi OS (2019) Bioactive glasses in dental applications (literature review). *J Univ Babylon Eng Sci* 27:207–2012

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