



# Diabetic retinopathy detection using supervised and unsupervised deep learning: a review study

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## Abstract

The severe progression of Diabetes Mellitus (DM) stands out as one of the most significant concerns for healthcare officials worldwide. Diabetic Retinopathy (DR) is a common complication associated with diabetes, particularly affecting individuals between the ages of 18 and 65. As per the findings of the International Diabetes Federation (IDF) report, 35–60% of individuals suffering from DR possess a diabetes history. DR emerges as a leading cause of worldwide visual impairment. Due to the absence of ophthalmologists worldwide, insufficient health resources, and healthcare services, patients cannot get timely eye screening services. Automated computer-aided detection of DR provides a wide range of potential benefits. In contrast to traditional observer-driven techniques, automatic detection allows for a more objective analysis of numerous images in a shorter time. Moreover, Unsupervised Learning (UL) holds a high potential for image classification in healthcare, particularly regarding explainability and interpretability. Many studies on the detection of DR with both supervised and unsupervised Deep Learning (DL) methodologies are available. Surprisingly, none of the reviews presented thus far have highlighted the potential benefits of both supervised and unsupervised DL methods in Medical Imaging for the detection of DR. After a rigorous selection process, 103 articles were retrieved from four diverse and well-known databases (Web of Science, Scopus, ScienceDirect, and IEEE). This review provides a comprehensive summary of both supervised and unsupervised DL methods applied in DR detection, explaining the significant benefits of both techniques and covering aspects such as datasets, pre-processing, segmentation techniques, and supervised and unsupervised DL methods for detection. The insights from this review will aid academics and researchers in medical imaging to make informed decisions and choose the best practices for DR detection.

**Keywords** DR detection · Diabetic Retinopathy review · Unsupervised deep learning · Supervised learning

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## Abbreviations

|               |  |
|---------------|--|
| <b>ACC</b>    | Accuracy   |
| <b>AMD</b>    | Age-related macular degeneration                           |
| <b>ANN</b>    | Artificial Neural Network                                  |
| <b>ARIA</b>   | Automated Retinal Image Analysis                           |
| <b>AUC</b>    | Area under the ROC curve                                   |
| <b>BPNN</b>   | Back Propagation Neural networks                           |
| <b>BPDFHE</b> | Brightness preserving dynamic fuzzy histogram equalization |
| <b>CE</b>     | Contrast Enhancement                                       |
| <b>CLAHE</b>  | Contrast limited adaptive histogram equalization           |
| <b>CNN</b>    | Convolutional Neural Network                               |
| <b>CS</b>     | Convergence State  |
| <b>CT</b>     | Computed Tomography  |
| <b>DA</b>     | Data Augmentation  |
| <b>DBN</b>    | Deep Belief Network  |
| <b>DEC</b>    | Deep Embedded Clustering                                   |
| <b>DM</b>     | Diabetes Mellitus  |
| <b>DHAC</b>   | Distributed hierarchical agglomerative clustering          |
| <b>DL</b>     | Deep Learning  |
| <b>DNN</b>    | Deep Neural Network  |
| <b>DR</b>     | Diabetic Retinopathy                                       |
| <b>FAZ</b>    | Foveal Avascular Zone                                      |
| <b>FAZID</b>  | Foveal Avascular Zone Image Database                       |
| <b>FIRE</b>   | Fundus Image Registration dataset                          |
| <b>FNN</b>    | Feed Forward Neural Network                                |
| <b>FoV</b>    | Field of View  |
| <b>FPPI</b>   | False Positive per Image                                   |
| <b>GAN</b>    | Generative adversarial network                             |
| <b>HAC</b>    | Hierarchical Agglomerative Clustering                      |
| <b>HM</b>     | Hemorrhages  |
| <b>IDF</b>    | International Diabetes Federation                          |
| <b>IEEE</b>   | Institute of Electrical and Electronics Engineers          |
| <b>IDRID</b>  | Indian diabetic retinopathy Image dataset                  |
| <b>KCM</b>    | K-Means Clustering with MapReduce                          |
| <b>MAs</b>    | Microaneurysms   |
| <b>MIL</b>    | Multiple Instance Learning                                 |
| <b>ML</b>     | Machine Learning   |
| <b>NPDR</b>   | Non-Proliferative Diabetic Retinopathy                     |
| <b>MLP</b>    | Multilayer Perceptron                                      |
| <b>MRI</b>    | Magnetic Image Resonance                                   |
| <b>MSE</b>    | Mean Square Error  |
| <b>OD</b>     | Optic Disc   |
| <b>PDF</b>    | Probability density function                               |
| <b>PDR</b>    | Proliferative Diabetic Retinopathy                         |
| <b>PPV</b>    | Positive predictive value                                  |
| <b>RAUNet</b> | Residual-Attention UNet                                    |
| <b>RNN</b>    | Recurrent Neural Network                                   |
| <b>RMSE</b>   | Root Mean Square Error                                     |
| <b>ROC</b>    | Retinopathy Open Challenge                                 |

|            |                           |
|------------|---------------------------|
| <b>SL</b>  | Supervised Learning       |
| <b>SN</b>  | Sensitivity               |
| <b>SP</b>  | Specificity               |
| <b>SVM</b> | Support Vector Machine    |
| <b>UL</b>  | Unsupervised Learning     |
| <b>WHO</b> | World Health Organization |

## 1 Introduction

The medical decision support system aids doctors in analyzing patients' health records, encompassing various decisions. Moreover, experience and knowledge play crucial roles in their decision-making processes. Most computer-assisted diagnostic systems are built upon conventional Machine Learning (ML) techniques that depend on relevant data representation for their performance. These systems necessitate substantial domain expertise and meticulous manual engineering. There is a considerable need for manual efforts in traditional ML algorithms to extract hidden features. Deep Learning (DL) can be viewed as an emerging and latest development in this direction, aiming to broaden the scope of conventional ML.

Furthermore, the DL algorithm operates on the automatic representation of data, which is considered a vital advantage in the technique of DL models. However, it requires extensive training and a large, well-annotated dataset to enhance the model's performance. Supervised DL algorithms play a crucial role in predictive analysis, demonstrating the substantial potential and providing solutions for various issues (Raheja et al., 2021). Conversely, Unsupervised DL algorithms have the potential to identify multiple hidden patterns in healthcare data (Raza and Singh 2021). UL diverges from supervised methods by operating without labeled training data.

UL plays a crucial role in exploratory data analysis, delving into patterns and structures within data without the guidance of labeled outcomes. The challenge lies in evaluating the outcomes of UL methods due to the absence of a universally accepted mechanism for cross-validation or validation on independent datasets. Unlike SL, where predictive models can be assessed by predicting responses on unseen data, UL operates where the accurate answers are unknown (James et al. 2000). This inherent nature of unsupervised problems makes validating or cross-valid results challenging, emphasizing the need to understand the data better and carefully interpret the discovered patterns. Despite the absence of a straightforward validation process, UL remains a powerful tool for uncovering hidden insights and relationships within datasets (James et al. 2000).

Notably, UL, exemplified by clustering techniques, brings several advantages. It facilitates exploratory analysis, which proves valuable in scenarios where the nature of the data is not fully understood. UL methods alleviate the dependency on extensive labeled datasets (An et al. 2022), which is particularly beneficial in the medical field where expert annotation is time-consuming. Moreover, UL excels in handling complex and high-dimensional data structures, providing insights into intricate relationships within medical imaging data. Its effectiveness in anomaly detection and generalization to new, unseen data further enhances its utility for early disease detection and adaptability to diverse patient cases.

While acknowledging noteworthy advantages, challenges in parameter tuning and interpretation of learned representations are vital. Choosing between supervised and unsupervised approaches depends on dataset characteristics and the medical imaging

problem's nature, requiring thorough evaluation for optimal model performance (A. Kumar et al. 2019).

The clustering algorithm, in particular, tends to group dissimilar elements based on their attributes without the need for supervision or labeled data (Chakradar et al., 2021). This method arranges data based on the discovery of knowledge. Deep clustering techniques represent a fusion of clustering and deep learning algorithms. The superior performance of DEC (Deep Embedded Clustering) techniques compared to UL methods is attributed to their effective clustering capabilities. The ability of clustering algorithms to combine feature learning with cluster assignment introduces new possibilities, overcoming challenges related to labeling in SL approaches (Enguehard et al., 2019).

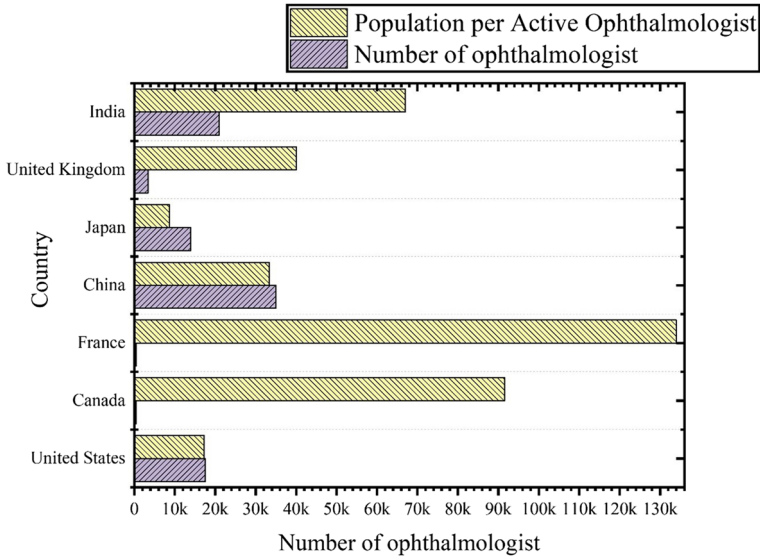
According to the International Council of Ophthalmologists (data on ophthalmologists worldwide, n.d.), the data highlights the urgent need for ophthalmologists, as shown in Fig. 1. The global epidemic of diabetes intensifies this need, a primary cause of Diabetic Retinopathy (DR), with an estimated 780 million people facing diabetes by 2045, as shown in Fig. 2. Additionally, it is projected that 35% of these individuals are expected to suffer from DR (H. Sun et al. 2022). Furthermore, it is projected that 86 million individuals (11%) will have severe sight-threatening retinopathy by 2045.

DR is commonly identified through the Early Treatment Diabetic Retinopathy Study (ETDRS) scale, which assesses the severity of the condition. This scale is widely accepted and used for clinical research and in the management of DR (Singer et al. 2024). The classification is based on the findings from color fundus photographs of the retina. The ETDRS scale categorizes DR into the following stages.

|   |   |
|---|---|
| No retinopathy (Level 10)                   | There are no signs of DR in the retina  |
| Mild non-proliferative DR (NPDR) (Level 20) | Microaneurysms (minor swelling in the retina's blood vessels) are present, but there is no evidence of more severe changes  |
| Moderate NPDR (Level 35)                    | In addition to microaneurysms, there are more severe retinal changes, such as hemorrhages and hard exudates (yellow deposits in the retina)                           |
| Severe NPDR (Level 47)                      | More significant retinal changes are observed, including more hemorrhages and more widespread retinal damage  |
| Proliferative DR (PDR) (Level 53)           | In the most advanced stage of DR., New blood vessels grow abnormally in the retina, and there is an increased risk of severe vision loss due to bleeding and scarring |

The severity scale helps guide treatment decisions and determine the need for intervention. Timely identification and effective handling of DR are essential in preventing the risk of vision impairment.

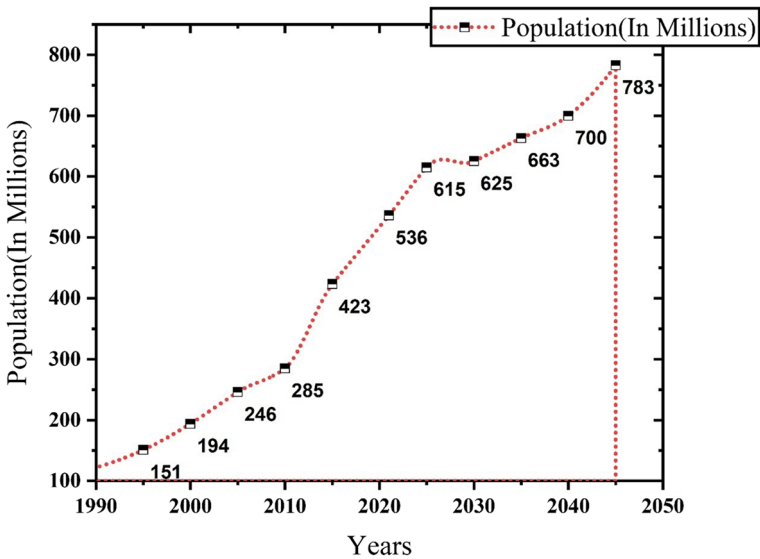
Therefore, the demand for effective healthcare solutions, such as advanced unsupervised algorithms for early DR detection, becomes increasingly imperative (Alhussein et al., 2020; IDF). This intersection of rising DR prevalence and the scarcity of ophthalmologists underscores the importance of innovative approaches, like those integrating DL and UL algorithms, to address the challenges DR poses on a global scale (Ishtiaq et al. 2020). DR is caused by Diabetes Mellitus (DM) when the retina's blood vessels are blocked, leading to fluids leaking into the macula and blocking vision (Johnson et al., 2018). Similarly, to increase blood flow into the retina and overcome the blockage, new blood cells form over the surface of the fragile retina, leading to further fluid leakage and vision impairment. Therefore, DR can be mainly categorized into two classes, as mentioned below and shown in Fig. 3. The severity of DR, characterized by lesions and stages detailed in Table 1,



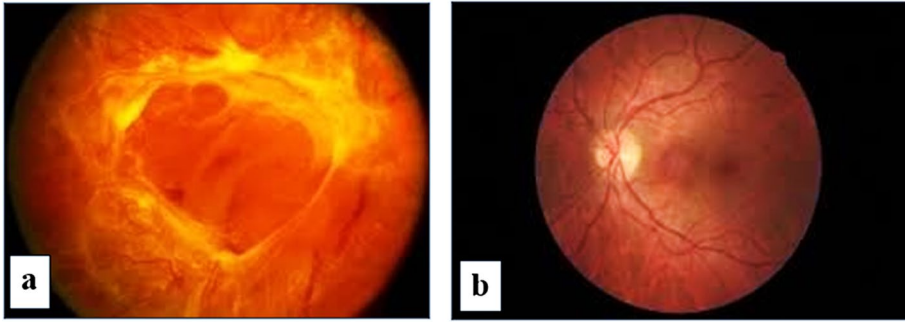
**Fig. 1** Number of ophthalmologists per country (Albo et al. 2023; Association of American Medical Colleges 2023; Buchan et al. 2024)

emphasizes the pressing need for timely diagnosis, aligning with the scarcity of ophthalmologists globally.

1. Non-Proliferative Diabetic Retinopathy



**Fig. 2** Estimations of the global prevalence of Diabetes (2000–2045) (Saeedi et al. 2019; H. Sun et al. 2022; WHO 2023)



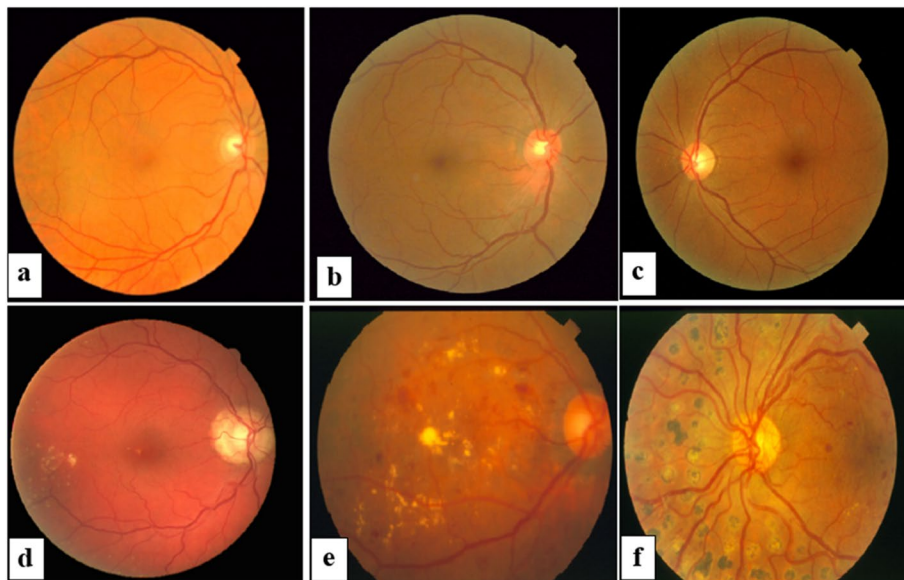
**Fig. 3** Samples of Proliferative Diabetic Retinopathy and Non-Proliferative Diabetic Retinopathy Fundus Images (a) Proliferative Diabetic Retinopathy Fundus Image (b) Non-Proliferative Diabetic Retinopathy Fundus Image (Niemeijer et al., 2010)

**Table 1** Severity Level of DR and Lesions

| Severity Level of DR and Lesions Associated |   |
|---|---|
| DR Severity Level                           | Lesions   |
| No DR                                       | Lesions are not Present   |
| Mild NPDR                                   | Only MAs found  |
| Moderate NPDR                               | MAs were found, but DR is not severe  |
| Severe NPDR                                 | Any conditions stated here: <ul style="list-style-type: none"> <li>• Four retinal quadrants may have twenty intraretinal hemorrhages or more</li> <li>• More than two retinal quadrants with venous beading</li> <li>• Visible intraretinal microvascular anomalies in more than one quadrant</li> <li>• PDR symptoms absent</li> </ul> |
| Proliferative DR                            | Any conditions mentioned here: <ul style="list-style-type: none"> <li>• Vitreous/pre-retinal Haemorrhages</li> <li>• Neovascularization</li> </ul>  |

## 2. Proliferative Diabetic Retinopathy

Approximately 75% of individuals with DR are located in developing nations, emphasizing a deficiency in access to both diagnosis and treatment (Maritim et al., 2003). According to official statistics from the World Health Organization (WHO) (Broadbent et al., 2021) and the IDF, DR is considered a complex and widely spread eye disease (Sun et al. 2022). It can be observed that DR is one of the most common reasons for sightlessness among adults and the working-age population in developed countries. Therefore, substantial efforts have been made in previous years to mitigate the impact of DR and assist in its analysis by developing tools for early diagnosis. DR can be categorized into diverse stages, as shown in Fig. 4. Artificial Intelligence (AI) provides insights into the data for better DR classification and is widely used as a medical



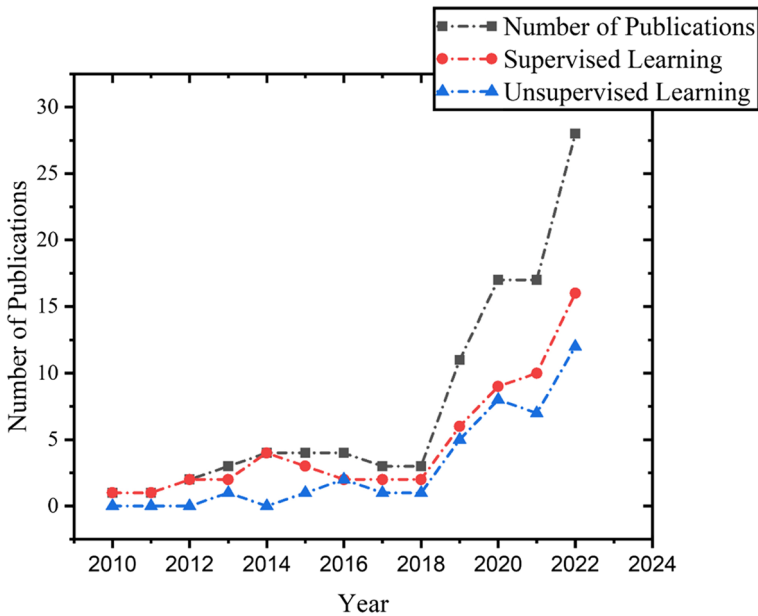
**Fig. 4** Stages of DR (a) Without DR (Normal) (b) Early stage of DR (c) Minor NPDR (d) Moderate NPDR (e) Severe NPDR (f) PDR and Neovascularization (Ishtiaq et al. 2020; Ishtiaq et al. 2020; Ishtiaq et al. 2020; Ishtiaq et al. 2020; Nagpal et al. 2021a)

imaging method. It can potentially mitigate the workload of ophthalmologists, thereby reducing the associated burden (Mansour, 2018).

The early detection of DR can be achieved through the automated AI approach, including supervised and unsupervised ML approaches. The pros and cons of these approaches are also discussed, with several articles published on both SL and UL methods for DR detection, as depicted in Fig. 5. The SL algorithm has been a prevailing trend for quite a long time, while the potential of the unsupervised algorithm is yet to be fully explored (Nath and Dandapat 2012; Saeed et al. 2021). Several researchers have applied both methods for early DR detection. Consequently, this review paper examines the current supervised and unsupervised methods utilized for the early diagnosis of diabetes. The paper seeks to categorize the diverse functional models of both SL and UL. Furthermore, the article demonstrates the comparability between the effectiveness of both methods on different dimensionalities of DR data.

The primary objectives of this review study include:

1. The literature review initially focused on keywords associated with SL methods and then explored UL methods from 2018 to 2023.
2. The proposed review identifies publicly available and functional datasets for a comprehensive study on DR classification.
3. The review explores the widely used SL techniques for DR detection, encompassing features and classification methods.
4. The review examines the widely used UL techniques for DR detection, detailing features and classification methods.
5. The proposed review work conducted a comparative analysis of Unsupervised and Supervised methods for DR classification.



**Fig. 5** Number of Publications Selected for the Study in the DR Domain Using Unsupervised and Supervised Learning, Extracted from Web of Science, Science Direct, Scopus, and IEEE Xplore Databases (2010–2023)

The remaining paper is arranged sequentially. The second section outlines the Article Selection Criteria for this review paper and details the methods employed for article extraction. The third section presents a systematic and categorical review of DR Detection using supervised and unsupervised approaches, which encompasses the functional datasets, image processing, blood vessel segmentation, and optic disk segmentation techniques for DR classification. The fourth section engages in the discussion and critical analysis of the study. The fifth section addresses open challenges in DR classification, focusing on the potential of SL and UL. The paper concludes in the sixth section with future discussions.

## 2 Article selection criteria

Figure 6 provides a visual representation of the detailed process used to select publications, outlining the identification of review targets. It is crucial to emphasize that this study deviates from the systematic review category, although it employs a similar methodological approach.

The selection criteria for the 103 articles were meticulously crafted, incorporating both inclusion and exclusion criteria. Inclusion criteria focused on articles relevant to the study of SL and UL methods in DR detection, unsupervised or supervised methods for segmentation, pre-processing, or feature extraction. Exclusion criteria ensured the exclusion of articles not directly related to the targeted research area. Therefore, the publication period spanned from 2010 to 2023, capturing a comprehensive range of literature. The search process encompassed four diverse well-known databases, including Scopus, Science Direct,



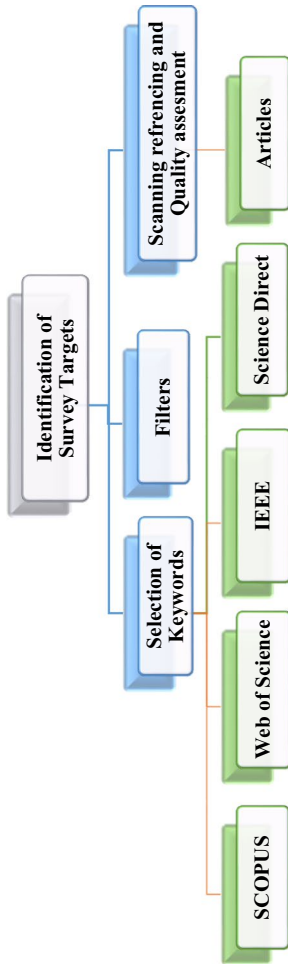


Fig. 6 Selection process for choosing the article

Web of Science, and IEEE, to ensure a thorough exploration of available literature on the subject. This rigorous selection process aimed to gather a representative and comprehensive set of articles for robust analysis in the review.

The keyword selection is made with the primary objective across four databases. Three diverse groups of keywords are formulated using a combination of search queries, as shown in Table 2. The prepared keyword search uses four databases: Scopus, Science Direct, Web of Science, and IEEE. Five filters, namely query-based, year-based, technique-based, article-based, abstract, and keywords-based filters, are applied for selecting primary work throughout these datasets. Moreover, the filters are applied to extract 23 documents from Scopus, 28 from Science Direct, 26 from Web of Science, and 26 from IEEE to detect DR using SL and UL techniques. Figure 7 shows the filters applied to extract the research and review papers for the extensive literature review.

The first filter is applied to four databases, retrieving 1306 articles, including the research and review work on DR detection using unsupervised and supervised DL. Furthermore, the second filter (year-based) limits the selected articles to 761. The articles were chosen between the time duration of 2010 and 2023. The third filter selects the review and research articles among all papers, including only core conference papers for the review. Based on all these parameters, 525 articles were chosen among 761 papers. Furthermore, the fourth and fifth filters were applied to retrieve the 103 articles for review.

**Filter 1** targets the formulated keywords for the selection of primary studies.

**Filter 2** deals with the publication year, which is taken between 2010 to 2023.

**Filter 3** considers the primary work's article title, keywords, and abstract selection.

**Filter 4** targets the techniques for SL and UL to select related articles.

**Filter 5** considers the abstract and keywords like diabetic retinopathy, DR detection, and DR prediction using SL and UL methods to select relevant articles.

The filters are applied to four databases and distributed among them, as shown in Table 3. Four presumed databases (Web of Science, Scopus, ScienceDirect, IEEE) are used to select the number of quality publications for the review work. In all these 90 articles, authors have applied unsupervised or supervised methods for segmentation, DR detection, pre-processing, or feature extraction. 224, 601, 434, and 47 articles (DR detection using supervised or unsupervised methods) are retrieved from Web of Science, Scopus, ScienceDirect, and IEEE databases using the query-based filter. Moving forward, filter two retrieves 142, 349, 237, and 36 manuscripts for all four databases from 2010 to 2023.

Furthermore, Filter Three retrieves only review and research articles related to specified topics and collects 84, 263, 145, and 33 articles, respectively. After applying the fourth filter, 43, 52, 82, and 26 manuscripts are retrieved. Finally, Filter 5 narrows the articles based on abstract and keyword-based searches and provides 26, 23, 28, and 26 manuscripts for further analysis, as shown in Fig. 8.

### 3 Review of diabetic retinopathy detection

Retinal abnormalities are considered vital and significant public health issues, with numerous cases prevalent in developing countries. These abnormalities can be categorized as systemic and non-systemic retinal abnormalities. Systemic retinal abnormalities can potentially affect multiple organs throughout the body, spreading from one point to

**Table 2** Formulated Keywords

| Group One  | Group two   | Group three  |
|--|---|--|
| Diabetic Retinopathy or DR Detection or Diabetes 2 or Retinal Disease or Retinal Disorder or DR or DR prediction or Diabetic eye disease | Feature extraction or, image normalization, or Image processing, or Image analysis, or Fundus image features, or Fundus Image classification, or Image segmentation | Supervised learning or Unsupervised learning or GANs or Clustering technique or Deep Embedded Clustering (DEC) or Deep Unsupervised Learning |

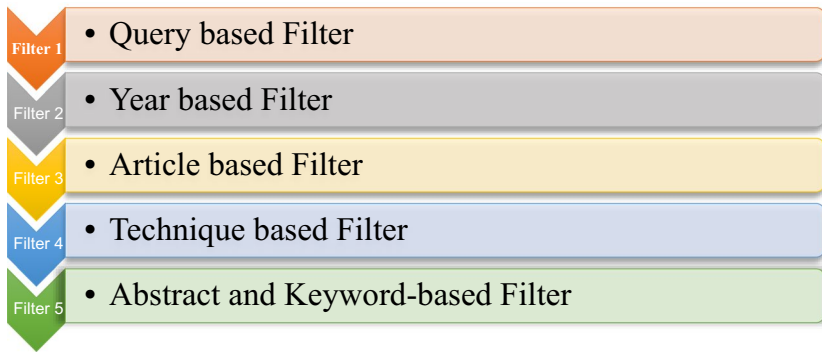


Fig. 7 Filter for selection criteria of articles

Table 3 Distribution of selected articles among databases

| Databases      | Filter 1 | Filter 2 | Filter 3 | Filter 4 | Filter 5 |
|----------------|----------|----------|----------|----------|----------|
| Web of Science | 224      | 142      | 84       | 43       | 26       |
| Scopus         | 601      | 349      | 263      | 52       | 23       |
| ScienceDirect  | 434      | 237      | 145      | 82       | 28       |
| IEEE           | 47       | 36       | 33       | 26       | 26       |
| Total          | 1306     | 764      | 525      | 203      | 103      |

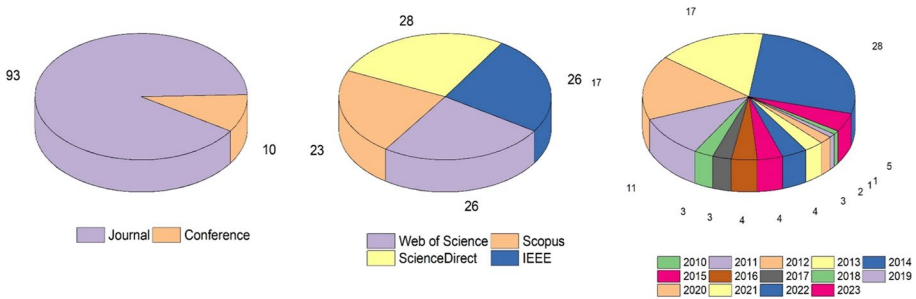


Fig. 8 Number of publications selected for review

the entire body(Madhusudhan et al. 2011). In contrast, non-systemic abnormalities only reside in the retina and originate through ocular manifestations (WHO 2023). Among various retinal abnormalities, diabetes can be considered a significant one. Diabetes can have a severe impact on different organs of the body, leading to problems such as cardiovascular disease and physical disability. Additionally, prolonged diabetes, accounting for 15% of all occurrences of blindness, is considered the leading cause of vision loss. The IDF states that the prevalence of diabetes is rising daily, affecting 451 million people worldwide, and is expected to impact 693 million people by 2045 (Cho et al., 2018).

The image acquisition system has significantly improved in recent years, as the disease detection and interpretation of results depend primarily on image quality.

Therefore, magnetic resonance imaging (MRI) has enhanced the image acquisition and reconstruction process. The interpretation of extracted details from these images remains a crucial challenge, requiring expert knowledge to extract helpful information from numerous images. Automated medical image analysis methods have the potential to enhance interpretation and accurate prediction (Hervella et al., 2020). Moreover, it can reduce the burden on ophthalmologists. Automated DR classification can be achieved with ML/ DL techniques. However, DL methods have recently been observed to outperform most ML results, facilitating automated feature extraction and the interpretation of medical image information (Poonguzhali Elangovan 2022). Furthermore, these advantages make DL algorithms more suitable and widely accepted for medical image analysis (Chen et al., 2022). DL algorithms can be divided into supervised and unsupervised for medical imaging classification.

Most research (Anas Bilal et al. 2023; Anas Bilal et al. 2022c) has predominantly utilized supervised methods for the analysis of medical images, specifically for DR classification, and these algorithms have demonstrated human-level performance in most cases (Miotto et al., 2017). However, these systems have shown significant promise in advancing medical imaging and the healthcare sector over the last few years. Nevertheless, SL techniques require labeled or annotated data for model training, and preparing the model with labeled data proves beneficial for real-time applications. However, labeling that data requires manual effort (Alanazi, 2022). On the other hand, UL algorithms are highly suitable for medical domain applications to explore new possibilities (Chen & Yu, 2017; Anas Bilal et al. 2021a, b, c; Anas Bilal et al. 2022a, b, c). In general, biases are inherent in a specific set of rules that limit the ability of SL methods to discover other possibilities. Moreover, in cases of unavailable labeled data, there is a need for extra effort, manual work, and time for marking the data in the SL process. No existing work is available to discuss the utilization of supervised and unsupervised learning methodologies for diagnosing DR. Additionally, there is a lack of discussion on the preferred approach for detecting DR based on existing research.

This section reviews 103 selected articles, examining supervised and unsupervised deep learning methods for DR detection. The review covers 1) dataset characteristics, 2) pre-processing techniques, 3) DR detection modalities, 4) methods employed, comparative analyses, and 5) advantages, disadvantages, and issues associated with both approaches.

### 3.1 Functional datasets for DR detection

Multiple public and external datasets for detecting DR, comprising a diverse array of fundus images, are readily available. Some researchers have utilized open-access datasets in diverse studies, while others have employed primary ones. Dai et al. (Dai et al. 2021) utilized a comprehensive dataset comprising 466,627 fundus images from 121,342 diabetic patients. The authors evaluated both primary and secondary datasets, encompassing a cumulative total of 261,326 fundus images. Similarly, Yang et al. (Yehui Yang et al. 2017) utilized a publicly available DR dataset obtained from the Kaggle repository, which includes 22,795 images divided into training and testing sets. The author employed 800 fundus photos for testing the model and 21,995 for grading and detecting eye abnormalities.

Table 4 presents the dataset details for DR used in selected articles and other DR-related works focusing on detecting microaneurysms (MAs), hard exudates (HM), exudates, or DR screening. The table includes the names of the datasets and the corresponding publication years. Several researchers (Anas Bilal et al. 2021a, b, c; Anas Bilal et al. 2022a, b, c) have

**Table 4** Details of Datasets

| S. No | Dataset Name   | Capturing device   | Number of Images  | Motivation   | Availability link   | Public/ External   | SL | UL |
|-------|--|--|---|--|---|--------------------|----|----|
| 1     | (ROC 2007; Budak et al. 2017; Chudzik et al. 2018)         | CR5-45NM, Topcon NW100 and NW10 camera   | A total number of 100 Images (50 for training and 50 for testing)                     | Computer-aided detection and diagnosis (CAD) of DR | <a href="http://webeye.ophth.uowa.edu/ROC/">http://webeye.ophth.uowa.edu/ROC/</a>   | Publicly Available | ✗  | ✓  |
| 2     | E-ophtha (2020; Fraz et al. 2017; Kusakuniran et al. 2018) | OPHDIAT e-ophtha-MA and e-ophtha-EX  | 47 images with exudates and 148 with MAs or small HM 35 and 233 images with no lesion | scientific research and DR Lesion detection        | <a href="https://www.adcis.net/en/third-party/e-ophtha/">https://www.adcis.net/en/third-party/e-ophtha/</a>                     | Publicly Available | ✓  | ✓  |
| 3     | Kaggle EyePACS Dataset (2016)                              | –  | A total of 88,702, from which 35,426 were for training and 53,576 for testing         | DR Lesion Detection                                | <a href="https://www.kaggle.com/c/diabetic-retinopathy-detection">https://www.kaggle.com/c/diabetic-retinopathy-detection</a>   | Publicly Available | ✓  | ✓  |
| 4     | DRIVE (2004)   | Canon CR5 non-mydiatric 3CCD camera along with the 45-degree field of view (FoV) | Total of 40 images (20 for training and 20 for testing)                               | DR Lesion Detection                                | <a href="https://docs.activeloop.ai/datasets/drive-dataset">https://docs.activeloop.ai/datasets/drive-dataset</a>               | Publicly Available | ✓  | ✗  |
| 5     | STARE (Structure Analysis of Retina, 2020)                 | Topcon TRV 50 camera with a 35-degree FoV  | A total of 400 fundus images  | Exudates and HM detection                          | <a href="https://www.kaggle.com/datasets/vidheeshma/stare-dataset">https://www.kaggle.com/datasets/vidheeshma/stare-dataset</a> | Publicly Available | ✓  | ✓  |
| 6     | DIARETDB0 (2020)   | Digital Fundus Camera with a 50-degree FoV                                       | A total of 130 images with 20 standards and 110 with DR sign                          | DR Lesions Detection                               | <a href="https://www.it.lut.fi/projects/imageret/diaretdb0/">https://www.it.lut.fi/projects/imageret/diaretdb0/</a>             | Publicly Available | ✓  | ✓  |
| 7     | DIARETDB1 (2020)   | Digital Fundus Camera with a 50-degree FoV                                       | A total of 89 images with five standards and 84 with moderate to severe DR sign       | DR Detection                                       | <a href="https://www.it.lut.fi/projects/imageret/diaretdb1/">https://www.it.lut.fi/projects/imageret/diaretdb1/</a>             | Publicly Available | ✓  | ✗  |
| 8     | Messidor (2020)  | 3CCD camera Topcon TRC NW6 non-mydiatric fundus camera                           | 1200 images (400 without pupil dilation and 400 with pupil dilation)                  | DR Lesion detection                                | <a href="https://www.adcis.net/en/third-party/messidor/">https://www.adcis.net/en/third-party/messidor/</a>                     | Publicly Available | ✓  | ✓  |

**Table 4** (continued)

| S. No | Dataset Name                                  | Capturing device  | Number of Images   | Motivation  | Availability link   | Public/ External   | SL | UL |
|-------|---|---|--|---|---|--------------------|----|----|
| 9     | Messidor-2 (2019)                             | Topcon TRC NW6 fundus camera  | 874 examinations (Total of 1748 images)  | DR Lesion detection                                     | <a href="https://www.adcis.net/en/third-party/messidor2/">https://www.adcis.net/en/third-party/messidor2/</a>   | Publicly Available | ✓  | ✓  |
| 10    | DriDB (2020)                                  | Zeiss VISCUCAM 200 Camera   | Total of 50 fundus Images  | DR Lesion detection                                     | <a href="https://pg.fer.hr/fgp/resources/image_data_base#">https://pg.fer.hr/fgp/resources/image_data_base#</a>   | Publicly Available | ✓  | ✓  |
| 11    | DR1(X, Li et al. 2018; Naqvi et al. 2015)     | TRX 50X mydriatic camera with a 50-degree FoV                                     | A total of 234 images  | DR Lesion detection                                     | <a href="https://recod.ai/code-data/#retinopathy">https://recod.ai/code-data/#retinopathy</a>   | Publicly Available | ✓  | ✓  |
| 12    | DR2 (Naqvi et al. 2015)                       | TRX NW8 mydriatic camera with a 50-degree FoV                                     | Total of 530 images  | DR Lesion detection                                     | <a href="https://recod.ai/code-data/#retinopathy">https://recod.ai/code-data/#retinopathy</a>   | Publicly Available | ✓  | ✓  |
| 13    | ARIA (Automated retinal image analysis, 2006) | Zeiss FF450+ fundus camera with a 50-degree FoV                                   | A total number of 143 color fundus images (92 DR-related, 61 standards, and 92 AMD images) | DR Detection and age-related macular degeneration (AMD) | <a href="http://www.damianjfmell.com/?page_id=276">http://www.damianjfmell.com/?page_id=276</a>   | Publicly Available | ✓  | ✓  |
| 14    | (Foveal Avascular Zone Image Database, 2020)  | -   | Total of 304 retinal fundus images (107 Diabetic, 109 myopic, and 88 Normal images)        | Screening of DR and refractive state of the eye         | <a href="https://www.openicpsr.org/openicpsr/project/117543/version/V2/view">https://www.openicpsr.org/openicpsr/project/117543/version/V2/view</a>                     | Publicly Available | ✓  | ✓  |
| 15    | CHASE-DB1 Retinal Image dataset               | Nidek NM-200-D with a 30-degree View of the field having a resolution of 1280×960 | Total 28 retinal fundus images of 14 children's eyes                                       | Retinal Vessel segmentation                             | <a href="https://www.idiap.ch/software/bob/docs/bob/bob.db.chasedb1/master/index.html">https://www.idiap.ch/software/bob/docs/bob/bob.db.chasedb1/master/index.html</a> | Publicly Available | ✓  | ✓  |

Table 4 (continued)

| S. No | Dataset Name   | Capturing device                                      | Number of Images   | Motivation  | Availability link  | Public/ External   | SL | UL |
|-------|--|---|--|---|--|--------------------|----|----|
| 16    | Tianjin Medical University Metabolic Diseases Hospital dataset (Z. Xiao et al. 2015) | Retinal fundus Camera                                 | Customized dataset with a total of 144 images  | Severity analysis of NPDR Detection   | The dataset is not made public by the authors. Although fundus images from the hospital can be accessed upon a reasonable request to <genglei@tjpu.edu.cn> | Exclusive          | ✓  | ✗  |
| 17    | Moorfields Eye Hospital datasets (Su Wang et al. 2017)                               | –   | 21,536 fundus images were collected on different nationalities at Moorfields Eye Hospital London | DR screening and MAs Detection  | The dataset is not made public by the authors  | Exclusive          | ✓  | ✓  |
| 18    | CLEOPATRA (Tan et al. 2017)  | Topcon NW6, Topcon TRC, Zeiss FF450                   | A total number of 298 images from 15 national healthcare center patients                         | Early DR detection and macular edema, Segmentation of MAs, exudates, and HM | A dataset is not made public by the authors. Can be requested at <Hfujita-799@acm.org>   | Exclusive          | ✓  | ✓  |
| 19    | Jichi Medical University dataset, 2015 (Takahashi et al. 2017)                       | AFC-230 and non-mydratric camera with a 45-degree FoV | Total 9939 posterior pole eye fundus images of 2740 diabetic patients                            | Lesion detection and DR Screening   | A dataset is not made public by the authors  | Exclusive          | ✓  | ✓  |
| 20    | Singapore National DR Screening dataset (Ting et al. 2017)                           | –   | Total 197,085 diabetic fundus images   | Actual DR lesion detection, diabetic macular edema                          | The dataset is not made public by the authors  | Exclusive          | ✓  | ✓  |
| 21    | ViCAVR Database  | Topcon non-mydratric camera                           | Total 58 fundus image with 768 × 584 resolution  | Vessel and its type (artery/vein) detection at a diverse radius from OD     | <a href="http://www.varpa.es/research/ophtalmology.html#vicavr">http://www.varpa.es/research/ophtalmology.html#vicavr</a>                                  | Publicly Available | ✓  | ✓  |



**Table 4** (continued)

| S. No | Dataset Name                                  | Capturing device   | Number of Images  | Motivation   | Availability link   | Public/ External   | SL | UL |
|-------|---|--|---|--|---|--------------------|----|----|
| 22    | IDRID   | Kowa fundus camera with a 50-degree FoV                        | Total 516 fundus color images with 4288×2848 resolution   | DR Screening, Detection of Lesions   | <a href="https://ieee-dataport.org/open-access/indian-diabetic-retinopathy-image-dataset-idrid">https://ieee-dataport.org/open-access/indian-diabetic-retinopathy-image-dataset-idrid</a> | Publicly Available | ✓  | ✓  |
| 23    | FIRE (Fundus Image Registration dataset,2017) | Nidek AFC-210 fundus camera with 45 Fields of View             | 129 retinal images are collected from 39 patients with 134 image pairs and 2912×2912 resolution   | DR Detection, Dark and light lesion detection  | <a href="https://projects.ics.forth.gr/cvrl/fire/">https://projects.ics.forth.gr/cvrl/fire/</a>   | Publicly Available | ✓  | ✗  |
| 24    | RODR (Longitudinal DR Dataset)                | Topcon TRC-NW65 fundus camera                                  | A total of 4-filed repeated 1120 fundus images with a 45-degree FoV from 70 patients  | Screening of DR, detection of lesions  | <a href="http://www.rodrep.com/longitudinal-diabetic-retinopathy-screening-description.html">http://www.rodrep.com/longitudinal-diabetic-retinopathy-screening-description.html</a>       | Publicly Available | ✗  | ✓  |
| 25    | RIM-ONE (Fumero et al. 2011)                  | Nidek AFC-210 with Canon EOS 5D Mark II body (21.1 megapixels) | A total of 169 images, from which 118 are standard eye images,12 contain early glaucoma signs, 28 are moderate and deep glaucoma, and 11 are related to Ocular hypertension (OHT) | Optic Nerve detection, DR Screening  | <a href="https://www.idiap.ch/software/bob/docs/bob/bob.db.rimoner3/stable/guide.html">https://www.idiap.ch/software/bob/docs/bob/bob.db.rimoner3/stable/guide.html</a>                   | Exclusive          | ✓  | ✓  |
| 26    | FGADR (Y. Zhou et al. 2021)                   | -  | A total of fine-grained 2,842 images, with 1,842 having pixel-level diabetic retinopathy (DR)-related lesion annotations and 1,000 featuring image-level labels                   | Segmentation of DR lesion, DR grading, and Transfer learning for ocular multi-disease identification | <a href="https://csyizhou.github.io/FGADR/">https://csyizhou.github.io/FGADR/</a> (dataset is available upon reasonable request from the corresponding author.)                           | Exclusive          | ✓  | ✗  |

Table 4 (continued)

| S. No | Dataset Name           | Capturing device | Number of Images               | Motivation   | Availability link   | Public/<br>External | SL | UL |
|-------|------------------------|------------------|--------------------------------|--|---|---------------------|----|----|
| 27    | OCTA-500 (Mingchao Li) | –                | OCTA imaging from 500 subjects | The largest and most comprehensive OCTA dataset includes OCTA imaging with two fields of view (FOVs), rich images, and annotations | <a href="https://iee-dataport.org/open-access/octa-500">https://iee-dataport.org/open-access/octa-500</a> | Publicly Available  | ✓  | ✓  |

employed diverse publicly available or open-access datasets for DR detection. However, it is noteworthy that some investigators (Grzybowski et al. 2020) have utilized exclusive datasets with limited accessibility. Moreover, extensive datasets have been compiled from various colleges or hospitals employing different camera settings (Lim et al. 2022). Consequently, Table 4 also provides information about exclusive datasets and the specific camera settings used in the respective studies.

The comprehensive dataset details outlined in Table 4, including the number of fundus images, training/testing sizes, and availability links for open-access databases, specify that the open-access datasets like ROC (Retinopathy Open Challenge), E-ophta, Messidor1 and 2, STARE, DIARETDB0, DIARETDB1, among others, have become standard in the field. As highlighted, researchers have explored these datasets with varied objectives, ranging from lesion detection and DR screening to identifying specific features such as HM, MAs, or exudates (Nagpal et al. 2021b). The last column of the table provides insights into the application of datasets for SL and UL. Further insights into dataset characteristics and specialties are represented in Fig. 9.

Various datasets are available for DR detection, chosen based on the nature of the algorithms employed. In the work by Zhou et al. (Zhou et al. 2017a, b), unsupervised classification was applied to the ROC dataset for detecting DR using retinal fundus images. The ROC dataset comprises 100 images, partitioned into 50 for training and 50 for testing. Notably, a ground truth table is available exclusively for the training subset, necessitating the utilization of 37 fundus images for training and 13 for testing. The openly accessible nature of the ROC dataset facilitates its adoption by researchers in their research work. Another study by Hong Tan (Tan et al. 2017) employed the CLEOPATRA dataset, a large dataset designed explicitly for automated detecting exudates, MAs, and HM. (Bala & Vijayachitra, 2014). This dataset is divided into 149 photos for testing and 149 for training. The proposed model showcased notable performance, achieving sensitivities of 87.56% for detecting exudates and 75.67% for identifying dark lesions on the CLEOPATRA dataset.

The e-ophta dataset combines 82 images from E-ophta EX and 381 from E-ophta MA. As per the literature review (Shuangling Wang et al. 2015, Orlando et al., 2018),

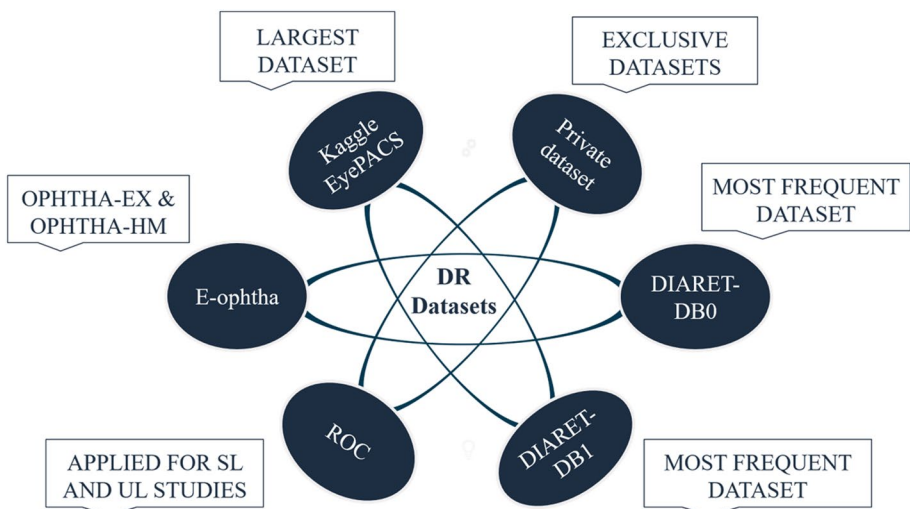


Fig. 9 DR Dataset and Characteristics

exudates are traditionally identified in retinal images using older methods, while MAs are primarily detected automatically through more advanced techniques. Yu and Xiao utilized a CNN model to automatically identify exudates using the e-ophtha dataset (Shuangling Wang et al. 2015).

Furthermore, Orlando and Prokofyeva (Orlando et al., 2018) utilized the E-ophtha MA dataset along with two other databases, DIARETDB1 and Messidor, for automated detection of MAs and red lesions. Emphasizing the importance of open-access datasets, Kaggle EyePACS emerges as the largest publicly available eye fundus dataset for automatic DR detection. Accessible through EyePACS, this dataset serves as a valuable resource, providing an open platform for accessing and sharing retinal fundus images. The Kaggle EyePACS dataset encompasses approximately 5 million retinal fundus images, featuring a diverse population and varying degrees of DR. With a vast collection of images representing different retinas worldwide, this dataset is a robust resource for training DL algorithms. Researchers globally leverage this dataset, prompting EyePACS and the California Health Care Foundation to collaborate on a Kaggle competition, aiming for improved outcomes in DR detection using the Kaggle dataset.

Nevertheless, it is imperative to underscore that the Kaggle dataset exhibits an imbalanced class distribution, with a significantly higher number of images labeled as “no DR” than other categories. Hence, Xu Feng (D. Xiao et al. 2017a, b) collected a subset of medical images derived from the Kaggle EyePACS dataset for early prediction and detection of DR utilizing a Convolutional Neural Network (CNN). The authors specifically concentrated on 800 eyeballs within the Kaggle dataset, allocating 200 for model testing in the proposed study. Furthermore, Xu Feng (D. Xiao et al. 2017a, b) curated a subset of medical images from Kaggle EyePACS for early DR prediction using a CNN. The study focused on 800 eyes, reserving 200 for dedicated model testing.

Furthermore, DIARETDB1 and DIARETDB0 have gained prominence as frequently employed datasets in numerous studies focusing on the detection of DR, particularly notable since 2020. Somasundaram & Alli (2017) and Xu et al. (2017) have explored the combination of DIARETDB1 and DIARETDB0 for DR detection. However, DIARETDB1 and DIARETDB0 display inherent imbalance. Specifically, among the images, there are 89 with five standards, 84 featuring DR signs, and 130 comprising 20 measures, with 110 images depicting DR signs.

Additionally, various exclusive datasets mentioned in Table 4 are accessible upon request through the respective authorities. These datasets play a significant role in DR detection, including the Tianjin Medical University Metabolic Diseases Hospital dataset, RIM-ONE, RoDR, FIRE, CLEOPATRA, Jichi Medical University dataset, Moorfields Eye Hospital datasets, IDRID, FAZ, SGHS Hospital, Singapore National DR Screening Program, Lotus Eye Care Hospital Coimbatore, Department of Ophthalmology, Kasturba Medical College, ViCAVR Database, IDRID Dataset, and Manipal, India (KMCM). Considering the imbalances in most datasets and the necessity to align image dimensions with the model’s requirements, image preprocessing becomes imperative. The subsequent section provides a comprehensive review of techniques applied to fundus images to augment the models’ performance.

### 3.2 Pre-processing techniques

Pre-processing techniques are vital in standardizing and enhancing data quality in image processing. In medical imaging, these methods, including normalization and

spatial transformations, ensure consistency and enable accurate diagnostic analysis. Image smoothing, noise reduction, and alignment contribute to refining medical images and improving clarity for precise evaluations. Medical image pre-processing utilizes 3-dimensional medical images obtained from Magnetic Resonance Imaging (MRI) or Computed Tomography (CT) to improve the overall quality of the image, which is achieved through various operations such as noise removal, contrast enhancement (CE), and edge detection. The pre-processed image enhances visualization for the network by making the image brighter and more precise and considering the Field of View (FoV). Multiple image processing techniques are available to enhance image quality. In this context, the authors have illustrated contrast enhancement (CE), green channel extraction, illumination correction, noise removal, and histogram equalization.

1. **Contrast Enhancement:** These techniques aim to modify images' relative brightness and darkness, improving their quality and visibility, as shown in Fig. 10. Contrast and tone adjustments in the image are achieved by mapping grey levels to new pixels through a grey-level transform. Grayscale images can undergo CE using suitable techniques. Local CE techniques, or histogram-based contrast techniques, distribute brightness evenly across the entire image. This approach enhances the darker portions of the image without over-exposing the brighter regions (Joshi & Karule, 2018).

Local contrast techniques become relevant due to the potential degradation of photograph quality by histogram equalization, which tends to over-enhance specific areas. This over-enhancement can result in information loss in the image's over-enhanced and darker parts. Several other equalization techniques aim to improve contrast and illumination for the further analysis and enhancement of small details in the image. Among these techniques, CLAHE (Contrast Limited Adaptive Histogram Equalization) is a popular choice in biomedical image processing. CLAHE is considered efficient in producing a precise pattern that is more visible, making it a valuable tool in this domain (Yamuna & Maheswari, 2013).

2. **Illumination Correction:** The objective of the illumination correction technique is to eliminate uneven illumination in the image, which may arise from factors like vignetting or the orientation of the image surface, as shown in Fig. 11. Illumination correction can be implemented through prospective correction and retrospective correction methods.

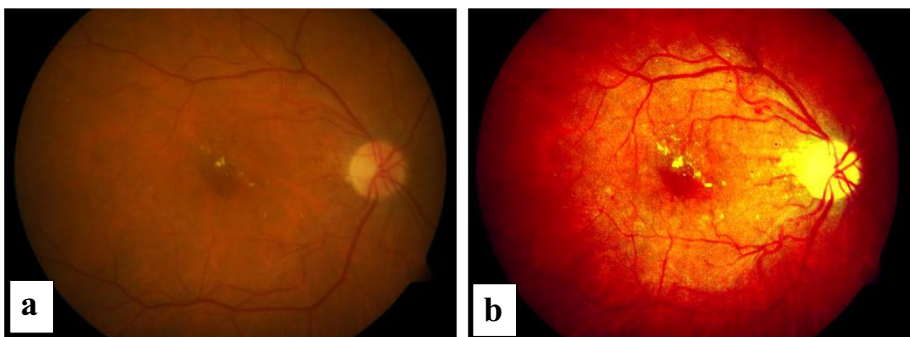
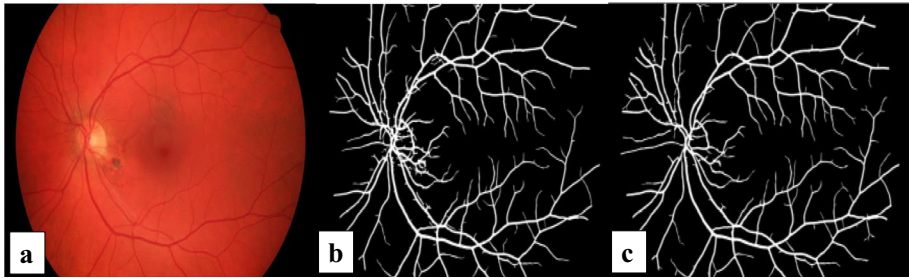


Fig. 10 Contrast enhancement (a) Original image (b) Image corrected using contrast enhancement



**Fig. 11** Illumination correction (a) original image (b) blood vessel segmentation without illumination correction pre-processing (c) blood vessel segmentation with illumination correction pre-processing

This technique primarily focuses on background correction to ensure a more even illumination across the image.

3. **Contrast Stretching:** This technique improves image quality and contrast by expanding the intensity value range, commonly known as contrast stretching or normalization. Through this adjustment, the pixels of the image are modified to ensure that the features become visible within the displayable range (Dissopa et al. in 2021).
4. **Noise Removal:** The images obtained from MRI or CT scans exhibit blurriness in their unprocessed state, characterized by hazy and blurry pixels commonly called blurred noise (Aurangzeb et al., 2021). Various types of noise, such as salt and pepper, Poisson, Gaussian, and speckle, may be present in medical images. Different filters can be applied according to the nature of the noise to enhance the image quality, as outlined in Table 5.
  - o **4.1. Gaussian Noise:**—Due to the regularity of the probability density function (PDF) associated with this type of noise, gaussian noise is also known as the gaussian distribution (Patidar et al., 2010). The Gaussian random variable ( $k$ ) PDF can be represented using Eq. (1).

$$P(k) = \left( \frac{1}{\sigma\sqrt{2\pi}} \right) e^{-(k-\mu)^2/2\sigma^2} \tag{1}$$

$k$ = grey level,  $\mu$ = means of an average value of  $k$ ,  $\sigma$ = standard deviation

- o **4.2. Impulse (salt and pepper) Noise:**—This noise can arise from sudden and shape changes in the image signal. Therefore, this type of noise is considered to be signal-dependent, and it is multiplied by the image values (Al-amri et al., 2010). The PDF is represented by Eq. (2).

**Table 5** Details of Noise and filter

|                       |                                     |
|-----------------------|-------------------------------------|
| Noise Type            | Best Applicable filter              |
| Poisson Noise         | Mean Filter                         |
| Gaussian Noise        | Gaussian Filter or Bilateral Filter |
| Salt and Pepper Noise | Median Filter                       |
| Speckle Noise         | Weiner Filter                       |

$$p(z) = \begin{cases} p_a & z = a \\ p_b & z = b \\ 0 & \text{otherwise} \end{cases} \quad (2)$$

a and b represent the grey levels. If b is measured as higher than a level, b is depicted as a light spot in the image, while level a is represented as a dark spot.

- o **4.3. Poisson Noise:**—Photon noise can be considered synonymous with Poisson noise. Poisson, or photon noise, occurs when the sensor does not receive sufficient photons to provide statistical information (Al-amri et al., 2010).
- o **4.4. Speckle Noise:**—The speckle noise can also be presented using Eq. (3).

$$k = lm + n * lm \quad (3)$$

k is referred to as speckle noise distribution, and lm as an input image. The uniform noise signal(N) comprises the mean O and variance V. (Al-amri et al., 2010). The cause of this noise is the lucid processing of data spread across numerous distributed locations.

- o **4.5. Uniform Noise:**—The pixels of the image appear quantized to various effective pixels for some reason. This issue results in uniform noise following a uniform distribution. The PDF of the uniform distribution is represented using Eq. (4).

$$P(z) = \begin{cases} \frac{1}{b-a} & \text{if } a \leq z \leq b \\ 0 & \text{otherwise} \end{cases} \quad (4)$$

5. **Clipping and Thresholding:** Image Clipping is a specific case of contrast stretching (Alhussein et al., 2020), and thresholding is regarded as an image segmentation technique where the image pixels are modified to acquire pixel values rapidly. In thresholding, the grayscale or color image is converted to binary, i.e., 0 or 1.
6. **Histogram Equalization:** An image's histogram illustrates the occurrence of each grey level. Histogram equalization involves redistributing the image's grey levels to achieve a uniform histogram (Mishra et al., 2020). Specific grey-level ranges are emphasized through histogram matching or histogram specification.

Retinal fundus images undergo pre-processing using the abovementioned techniques (Fig. 12) and additional existing algorithms to enhance image quality to aid diagnosis. Various researchers (Mumtaz et al. 2018; Zhou et al. 2017a, b; Vega et al. 2015) have applied diverse techniques in their studies, reflecting the summary of pre-processing methods employed in the selected articles for review.

The inherent low contrast of the image poses challenges in identifying the blood vessels' network and detecting the progression of DR. Consequently, CE is employed to improve image contrast by extracting the green channel of the retinal fundus image. The pre-processing comprises CE, brightness preserving dynamic fuzzy histogram equalization (BPDFH), and decorrelation stretching. BPDFHE introduces a few additional steps to restore image quality by implementing the CE technique (Joshi & Karule, 2018). Illumination correction is typically performed after applying the CE technique to enhance the

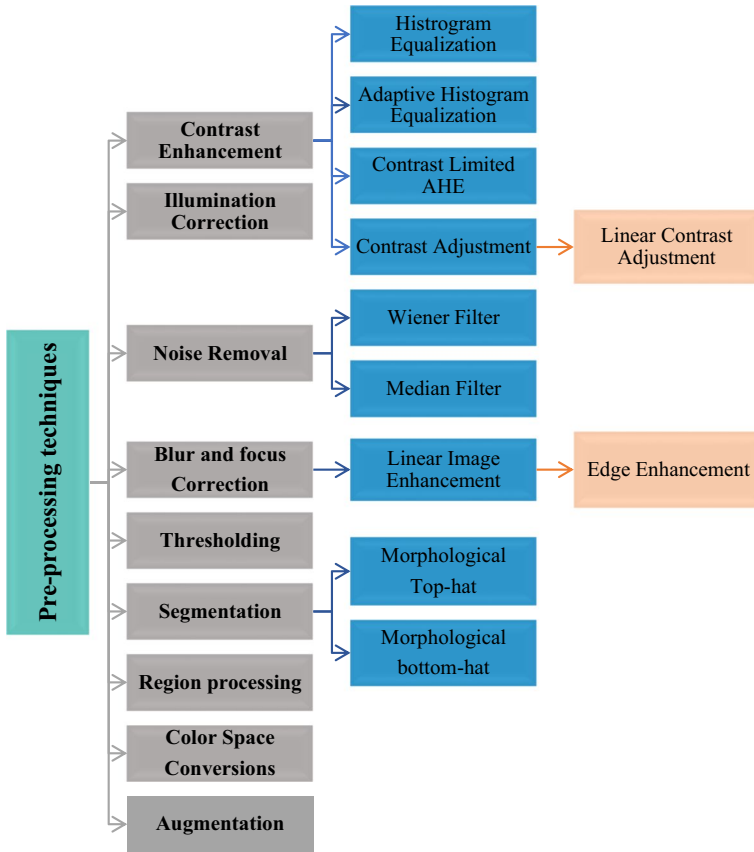


Fig. 12 Image pre-processing techniques for medical images

image’s luminosity. Another issue, known as "vignette," leads to reduced brightness along the image boundary. Illumination equalization is applied to address this problem, and the CLAHE method is utilized to reduce noise (Joshi & Karule, 2018).

Gaussian filtering provides an alternative method to enhance the image’s smoothness and eliminate unnecessary noise. The image is resized and adjusted in resolution to meet the required standards. The optic disc (OD) removal and masking are necessary for accurate DR lesion diagnosis. In most studies, the green channel is often extracted primarily for further processing. Zhou et al. (Zhou et al. 2017a, b) precisely select the green channel through pre-processing to detect MAs. However, augmentation techniques have proven helpful in addressing the class imbalance within the dataset (Mookiah et al., 2021). Various image rotation, flipping, and mirroring methods generate synthetic images for the minority class. Augmentation involves processes such as mirroring, contrast scaling, and rotation. According to Meindert Niemeijer et al. (Niemeijer et al., 2010), authors employed augmentation by rotating images from 0 to 360 degrees and translating them by distances ranging from -10 to 10 pixels.

Additionally, scaling from 85 to 115% was applied to synthesize the minority class in the DiaretDB1 dataset. Moreover, Storath and Weinmann (Storath & Weinmann, 2018)



proposed a fast-filtering algorithm for denoising images using unit circle values based on arc distance median. The proposed median filter is robust, preserves values, and maintains edges, making it the most widely employed filtering tool for smoothing real-valued data.

The authors (Dissopa et al., 2021) conducted a comparative study on pre-processing techniques for CE and illumination correction in DR retinal images. The authors scrutinized dividing methods using median and quotient methods employing homomorphic filtering. The authors also explored CLAHE and the polynomial grey level transformation operator to enhance CE in fundus images. Dissopa et al. (Dissopa et al., 2021) concluded that the division method employing median filtering is the most successful technique for estimating the background in the red component based on visual and statistical evaluations. Nevertheless, (Satpathy et al., 2016) compared various filters, including the box filter, Gabor filter, median filter, and Gaussian filter, for filtering medical images. Their survey revealed that the median filter produced better outcomes, as evidenced by the estimated peak signal-to-noise ratio (PSNR) values for Gaussian noise.

Moreover, (Satpathy et al., 2016) compared various filters, including the box filter, Gabor filter, median filter, and Gaussian filter, to filter medical images. Based on the estimated PSNR values for Gaussian noise, the survey revealed that the median filter exhibited superior outcomes. Several studies from selected articles have applied diverse pre-processing techniques to enhance their results. Table 6 presents the research objectives along with the corresponding pre-processing methods and their achieved performance. The techniques are denoted as T1 to T6.

### 3.3 Diagnostic modalities for DR detection

DR can be evaluated through diverse imaging modalities, each offering distinct insights into the disease. Fundus photography provides a broad, two-dimensional perspective facilitating the identification of tumors and hemorrhages. Optical Coherence Tomography (OCT) delivers high-resolution cross-sectional views of retinal layers, aiding in detecting structural changes and fluid accumulation. The non-invasive Optical Coherence Tomography Angiography (OCTA) technique produces detailed vascular maps crucial for assessing microvascular alterations by visualizing blood flow in the retinal and choroidal vasculature, as shown in Fig. 13.

OCT presents a robust capability for producing high-resolution cross-sectional images, enabling early detection of microstructural changes characteristic of DR while also allowing for precise quantitative measurements of retinal thickness and morphology. Specifically, the introduction of 3D OCT enhances these capabilities further. By capturing volumetric data, 3D OCT provides a more comprehensive assessment of retinal structures, facilitating the detection of subtle changes and offering improved visualization compared to traditional 2D OCT scans. However, despite its advantages, OCT has its drawbacks, including its higher cost, longer imaging acquisition times, and the need for specialized equipment and expertise. On the other hand, fundus imaging provides a wide-field view of the retina, offering a comprehensive assessment of retinal abnormalities associated with DR. Fundus images are relatively cost-effective, quick to capture, and widely available in most eye care settings. However, they lack the detailed structural information and quantitative measurements that OCT, mainly 3D OCT, offers.

The application of 3D OCT is advisable when necessitating structural visualization, quantitative analyses, and precise monitoring of disease progression in diabetic retinopathy. The volumetric data provided by 3D OCT allows for more accurate assessments of

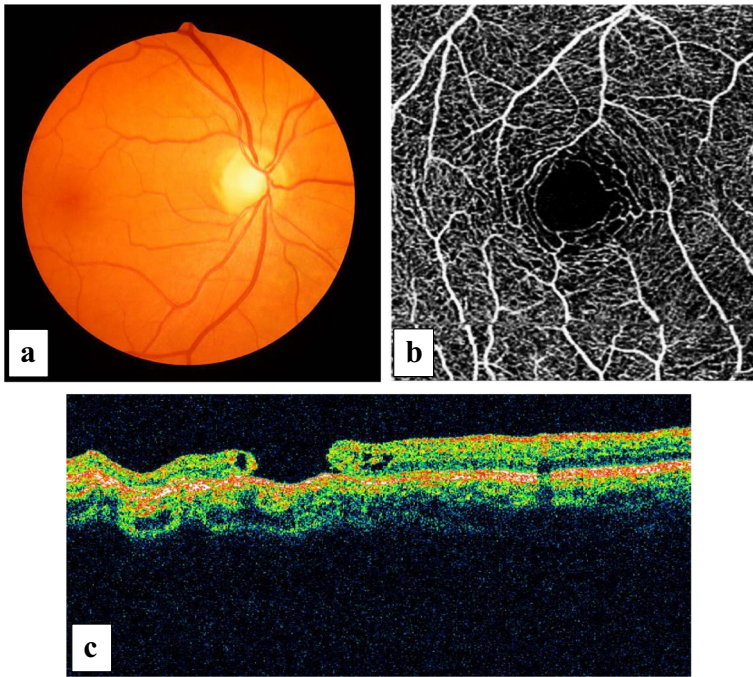
**Table 6** Pre-processing techniques

| Objective                          | T <sub>1</sub> | T <sub>2</sub> | T <sub>3</sub> | T <sub>4</sub> | T <sub>5</sub> | T <sub>6</sub> | T <sub>7</sub> | T <sub>8</sub> | T <sub>9</sub> | T <sub>10</sub> | Result   | Ref No                    |
|------------------------------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|-----------------|--|---------------------------|
| Detection of retinal hemorrhages   | ✓              | ✗              | ✗              | ✓              | ✓              | ✓              | ✗              | ✗              | ✗              | ✗               | SN-89%<br>SP-87%<br>ACC-89%                            | (Mumtaz et al. 2018)      |
| Automated MA's detection using UL  | ✓              | ✗              | ✗              | ✓              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗               | SN- 48%<br>FPPI-43.13                                  | (W. Zhou et al. 2017a, b) |
| Automated MA detection             | ✓              | ✗              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗              | ✓               | Average SN-<br>0.285                                   | (W. Zhou et al. 2017a, b) |
| Retinal vessel extraction          | ✓              | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗               | SN-94%<br>SP-96%<br>ACC-94%                            | (Vega et al. 2015)        |
| Exudates Detection                 | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗               | SN-74%<br>ACC-91.92%                                   | (D. Xiao et al. 2017a, b) |
| Grading of DR and lesion detection | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✗              | ✓              | ✗               | AUC-95.9   | (Yehui Yang et al. 2017)  |
| DR fundus image classification     | ✓              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✓               | SN-86.03%<br>SP-97.11%<br>AUC-98.34<br>ACC-92.01%      | (X. Li et al. 2018)       |
| DR detection using fundus image    | ✗              | ✓              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✗               | SN-95%<br>SP-30%<br>ACC-75%                            | (Pratt et al. 2016)       |
| Automated detection of DR          | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✗               | ACC- 94.5%   | (Xu et al. 2017)          |
| Retinal vessel segmentation        | ✓              | ✓              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗              | ✗               | Precision-84.9%<br>SP-98.01%<br>ACC-95.3%<br>AUC-97.44 | (Franklin and Rajan 2014) |
| Automated NPDR screening           | ✓              | ✗              | ✗              | ✓              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗               | SN-100%<br>SP-89%<br>ACC-94%                           | (Z. Xiao et al. 2017a, b) |
| Retinal HM detection               | ✗              | ✗              | ✗              | ✗              | ✓              | ✓              | ✗              | ✓              | ✗              | ✗               | SN-91.9%<br>SP-85.6%                                   | (D. Xiao et al. 2017a, b) |

**Table 6** (continued)

| Objective                                       | T <sub>1</sub> | T <sub>2</sub> | T <sub>3</sub> | T <sub>4</sub> | T <sub>5</sub> | T <sub>6</sub> | T <sub>7</sub> | T <sub>8</sub> | T <sub>9</sub> | T <sub>10</sub> | Result  | Ref No                                 |
|---|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|----------------|-----------------|---|--|
| Hierarchical blood vessel segmentation          | ✗              | ✗              | ✗              | ✗              | ✓              | ✗              | ✓              | ✓              | ✗              | ✗               | SN-81.7%<br>SP-97.3%<br>ACC-97.6%<br>AUC-94.7%                            | (Shuangling Wang et al. 2015)          |
| Retinal Exudate detection and classification    | ✗              | ✗              | ✓              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗              | ✓               | SN-98.6%<br>SP-94.8%<br>ACC-96.7%<br>PPV-94.9                             | (Omar et al. 2016)                     |
| DR Exudate detection and classification         | ✗              | ✗              | ✗              | ✗              | ✓              | ✓              | ✗              | ✗              | ✗              | ✗               | SN-93.8%<br>SP-100%<br>ACC-96%  | (Vanithamani and Renee Christina 2018) |
| HM detection using color fundus image           | ✓              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✓               | AUC-97.2  | (Van Grinsven et al. 2016)             |
| Bright Lesion extraction                        | ✓              | ✗              | ✗              | ✓              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗               | ACC: -<br>Training set-90.9%<br>Testing set-91.0%<br>Validation set-89.3% | (Hantůsková et al. 2013)               |
| Exudate detection and classification of DR      | ✗              | ✗              | ✗              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗               | SN-78.9%<br>SP-100%<br>ACC-86%  | (Mateen et al. 2020)                   |
| OD, fovea, and retinal vasculature segmentation | ✗              | ✓              | ✗              | ✗              | ✓              | ✗              | ✗              | ✗              | ✗              | ✗               | Average ACC-92.68%  | (Tan et al. 2017)                      |

\*T<sub>1</sub>-Contrast Enhancement, T<sub>2</sub>-Normalization, T<sub>3</sub>-Illumination Correction, T<sub>4</sub>- Thresholding, T<sub>5</sub>- Green Band Extraction, T<sub>6</sub>-OD and Blood Vessel Segmentation extraction, T<sub>7</sub>-Gaussian/median Filter, T<sub>8</sub>-Histogram Equalization, T<sub>9</sub>- Data Augmentation (DA) T<sub>10</sub>-foV extraction

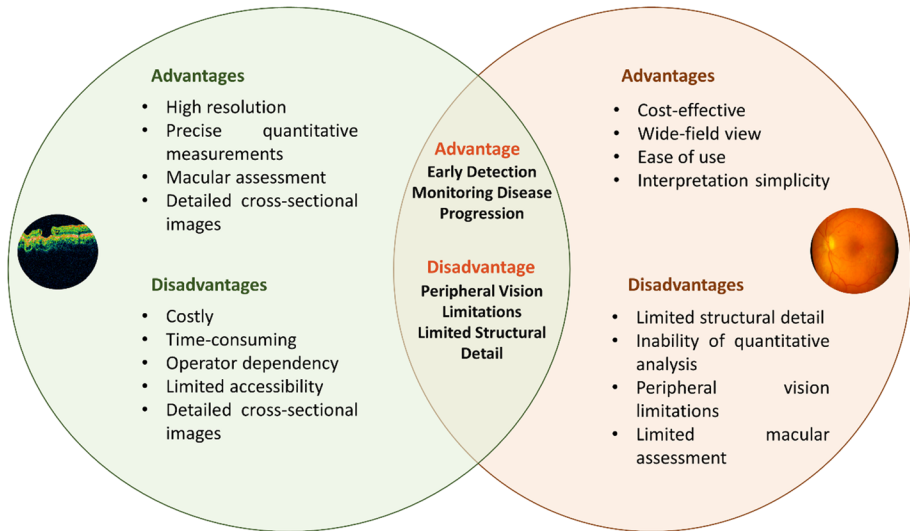


**Fig. 13** DR Diagnostic Modalities **a)** Fundus Images of the normal eye with optic disk and blood vessel **b)** An OCT Angiogram of a healthy eye reveals intricate macular microvasculature, showcasing the foveal avascular zone at its center (Pichi et al. 2017) **c)** A full-thickness macular hole is evident in the Time-domain OCT scan (Salchow et al. 2006)

retinal thickness and morphology changes over time. In contrast, fundus imaging may be used when prioritizing cost-effectiveness, accessibility, and ease of implementation, particularly in settings constrained by resources or when evaluating peripheral retinal changes in diabetic populations. Figure 14 illustrates some of the different and common advantages and disadvantages of OCT and fundus modalities for DR detection.

Recognizing the significance of each modality in DR diagnosis, researchers (Elsharkawy et al. 2022; Pichi et al. 2017; Z. Sun et al. 2021) have explored the implementation of OCT and OCTA for detecting DR. Elsharkawy et al. (Elsharkawy et al. 2022) proposed a system for automatic segmentation of retinal layers in 3D OCT scans using prior share knowledge, texture feature, and a Markov-Gibbs random field model for DR diagnosis. Cumulative distribution function descriptors represent image-derived features, feeding into an artificial neural network for layer-wise classification. The proposed approach achieves an impressive accuracy of 96.88%. Additionally, Zang et al. (Zang et al. 2022) conducted a study involving 456 OCT and OCTA volumes obtained from 50 healthy individuals and 305 patients with diabetes. A framework trained on volumetric OCT and OCTA achieved a high AUC of  $0.96 \pm 0.01$  for referable DR (rDR) and  $0.92 \pm 0.02$  for vision-threatening DR.

Another retrospective study (Sandhu et al. 2020) was conducted at an academic medical center in the United States to collect demographic and health data using OCT and OCTA modalities. Applying ML to OCT and OCTA features, combined with clinical data, achieved an accuracy of 92%, sensitivity of 95%, specificity of 98%, and an AUC



**Fig. 14** Advantages and disadvantages of OCT and fundus images for DR detection

of 0.92 for NPDR classification, compared to clinical grading. Another study (Ahmed Sharafeldeen et al. 2023) focuses on a computer-aided diagnostic system for DR using 3D OCT features, computing thickness and first-order reflectivity per retinal layer. Classification is achieved by backpropagation neural networks, demonstrating performance with  $94.74\% \pm 5.55\%$  accuracy in tenfold cross-validation on 188 cases.

Moreover, the segmentation of retinal OCT layers is done in different studies to precisely quantify retinal thickness and identify specific pathological changes associated with DR (Galdran et al., 2022; Hao et al. 2021). Segmentation techniques in OCT imaging can precisely detect and measure the retinal nerve fiber layer (RNFL), ganglion cell layer (GCL), inner plexiform layer (IPL), and inner nuclear layer (INL), all of which are frequently impacted by DR. Despite the implementation of 2D segmentation algorithms, they fail to fully leverage contextual information and exhibit inconsistencies when applied to 3D applications. (Wang et al., 2023). In their work, (Wang et al., 2023) introduced a novel graph pyramid structure incorporating construction elements derived from graph theory alongside a segmentation network employing 3D convolution. The authors introduced a segmentation network employing 3D convolution and a novel graph pyramid structure with graph-inspired building blocks. They collected and manually corrected a large OCT segmentation dataset comprising normal and diseased cases. Their proposed method notably reduced segmentation errors from 38.47% to 11.43%. Another study (Galdran et al., 2022) highlighted that retinal vessel segmentation remains challenging, notably when test images differ significantly from training data, suggesting domain adaptation techniques are needed. The study demonstrates that a simplified version of a standard U-Net achieves comparable performance to more intricate techniques with significantly fewer parameters. Additionally, a cascaded extension (W-Net) achieves outstanding results on various datasets using substantially fewer learnable weights than previous methods (Galdran et al., 2022).

Moreover, a novel method is proposed for the segmentation of retinal blood vessels to address the challenge of low accuracy encountered during the removal of small blood vessels from retinal images (Hao et al. 2021). The method integrates local and global

enhancement techniques alongside a multi-scale linear detector, combining a multi-scale linear detector with local and global enhancement techniques. The response functions at different scales are fused to obtain the final retinal vascular structure. Experimental results on the STARE and DRIVE databases demonstrate high segmentation accuracy, with average vascular accuracy rates of 96.62% and 96.45% and average true positive rates of 75.52% and 83.07%, respectively. This approach yields improved blood vessel segmentation results, indicating its potential for enhancing the accuracy of OCT image segmentation (Hao et al. 2021).

Similarly, segmentation is also significant in fundus imaging for DR diagnosis. In fundus images, Automated segmentation algorithms can assist clinicians in identifying and quantifying these DR-related features, providing valuable information for disease staging and monitoring (Li et al. 2022). Additionally, segmentation techniques can help differentiate between different lesions, such as distinguishing between hard and soft exudates or identifying the presence of clinically significant macular edema (Saranya et al., 2022). This level of detail enables more accurate diagnosis and personalized treatment planning for patients with DR. Additional studies on DR detection utilizing OCT and OCTA are summarized in Table 7.

Each modality carries unique significance, contributing to improved DR detection based on the scenario and data availability. While OCT and OCTA have demonstrated promising results in recent years, excelling in retinal layer segmentation and neovascularisation detection, fundus images are widely accessible and abundant. They are extensively used for diagnosis and training deep learning models for DR detection. Table 8 provides a detailed overview of the appropriate DR modalities and their applications, offering comprehensive insights into their utilization.

### 3.4 Blood vessels segmentation methods

Among the structural components of the retina, there exists a variation in the lengths and widths of the retinal blood vessels. The initial stage in acquiring diagnostic data for the early detection of various retinal disorders involves precisely segmenting blood vessels. Consequently, multiple techniques for detecting and segmenting retinal blood vessels have been presented recently, as discussed in Table 9.

### 3.5 Retinal optic disc detection methods

An essential step in establishing systems for the automated diagnosis of various ocular illnesses involves the detection of OD. Chaudhuri et al. (Chaudhuri et al. 1989) introduced a novel template-based method for segmenting the OD from digital retinal images. Following the Circular Hough Transform, this method utilized edge detection and morphological approaches to approximate the circular OD boundary. Subsequently, the retinal vasculature is sectioned, and the vessel positions are processed to filter, highlighting the features of the vessels near the OD. Authors (Staal et al. 2004) proposed a new method for extracting ODs and exudates with adjustable and stable thresholds in another approach. Soares et al. (Soares et al. 2006) also tested a novel computerized segmentation approach for stereo-color images within the glaucoma series dimension. Moreover, Mendonça and Campilho (Mendonça and Campilho 2006) employed a two-step technique to identify the border of the OD for accurate boundary recognition.

**Table 7** Recent work on DR detection using different diagnostic Modalities

| Method   | Diagnostic Modality    | Dataset  | Result  | Ref No                            |
|--|------------------------|--|---|-----------------------------------|
| novel tetragonal local octa pattern, Extreme learning machine  | OCTA                   | Kaggle-DR, DRIVE, Review-DB, STARE   | Kaggle-DR(ACC)-99.6%<br>DRIVE(ACC)-99.96%<br>STARE(ACC)-99.95%<br>STARE(ACC)-98.94% | (Nazir et al. 2019)               |
| End-to-end deep CNN  | OCTA                   | A total of 240 images, consisting of 40 images for each stage of the DR        | ACC- 91–98%<br>SP-94–99%<br>SN-86–97%   | (Ryu et al. 2021)                 |
| backpropagation neural networks  | OCT                    | dataset comprised 188 cases, with 100 classified as normal and 88 as having DR | ACC-96.81%  | (Ahmed Sharafelddeen et al. 2023) |
| Graph-cut method, edge detection, adjacency matrices computation, and vertical gradient generation   | OCT                    | 8 Normal OCT Retinal images and 5 DR-affected OCT images                       | Retinal layer segmentation (thickness- $45.3 \pm 1.07$ )                            | (Sakthi Sree Devi et al. 2021)    |
| Markov-Gibbs random field (MGRF) and grey-level co-occurrence matrix (GLCM), support vector machine with linear kernel, backpropagation neural network | OCT B-Scans            | 130 patients, with two scans for both eyes (i.e., 260 OCT images),             | ACC- 97.69%<br>SP- 96.15%<br>SN-99.23%<br>F1-97.66%                                 | (A. Sharafelddeen et al. 2021)    |
| Multimodal OCTA and Fundus images dataset  | OCTA and fundus Images | 76 people, wherein 111 are OCTA images, and 111 are color fundus images        | 72(Mild DR)<br>59(Moderate DR)<br>4(Mild DR)<br>1(No DR)                            | (Bidwai et al. 2024)              |
| Deep Learning System   | OCT                    | 200 OCT images, augmented to 800 images  | ACC- 97.7 ± 0.5% improvement  | (Haggag et al. 2022)              |

Table 7 (continued)

| Method   | Diagnostic Modality | Dataset  | Result   | Ref No               |
|--|---------------------|--|--|----------------------|
| 3D segmentation approach using an adaptive patient-specific retinal atlas and appearance model | 3D OCT              | OCT scans from 50 patients with normal and pathological conditions | Dice Similarity Coefficient (DSC): $88.6 \pm 2.8$ ,<br>bidirectional modified Hausdorff Distance (HD): $3.3 \pm 4.0$<br>Unsigned Mean Surface Position Error (MSPE): $0.3 \pm 0.1$ ,<br>Average Volume Difference (AVD): $5.8 \pm 2.4$ | (Sleman et al. 2021) |
| OCTA-500 dataset creation and multi-object segmentation task (CAVF)                            | 3D OCTA             | OCTA imaging from 500 subjects                                     | The largest and most comprehensive OCTA dataset includes OCTA imaging with two FOVs, rich images, and annotations  | (Hao et al. 2021)    |



**Table 8** Comparative Analysis of DR Modalities

| Aspect                                      | Fundus Images                                | OCT  | OCTA  |
|---|--|--|---|
| <b>Image Type</b>                           | 2D Retinal Photographs                       | Cross-Sectional Imaging  | Vascular Network Imaging                            |
| <b>Structural Information</b>               | Provides Retinal Structure                   | High-Resolution Cross-Sections                                     | Blood Vessel Visualization                          |
| <b>Depth of Visualization</b>               | Surface Level                                | Multiple Retinal Layers  | Retinal and Choroidal Vascular Networks             |
| <b>Vascular Information</b>                 | Limited                                      | Limited  | Detailed Visualization of Blood Vessels             |
| <b>Lesion Detection</b>                     | ✓  | ✓  | ✓   |
| <b>Macular Assessment</b>                   | ✓  | ✓  | ✓   |
| <b>Choroidal Assessment</b>                 | Limited                                      | Moderate   | Low (limited visualization)                         |
| <b>Detection of MAs</b>                     | High   | High   | Limited   |
| <b>Visualization of Retinal Layers</b>      | High   | High   | Limited   |
| <b>Assessment of Retinal Thickness</b>      | Limited                                      | Low (structural information)                                       | High  |
| <b>Identification of Neovascularization</b> | Low  | Moderate   | Moderate  |
| <b>Ease of Image Interpretation</b>         | Moderate                                     | Moderate   | Moderate  |
| <b>Advantages</b>                           |  |  |   |
| <b>Structural Visualization</b>             | Offers a wide-field view of the retina       | Provides detailed cross-sectional images                           | Visualizes retinal and choroidal vasculature        |
| <b>Early Detection</b>                      | Helpful in identifying retinal abnormalities | Detects microstructural changes                                    | Identifies early microvascular abnormalities        |
| <b>Quantitative Measurements</b>            | Limited quantitative data                    | Allows precise measurements of retinal thickness and morphology    | Quantifies retinal and choroidal blood flow         |
| <b>Macular Assessment</b>                   | Limited in assessing macular abnormalities   | Helpful in assessing macular abnormalities                         | Provides a detailed assessment of macular perfusion |
| <b>Depth Visualization</b>                  | Lacks depth information beyond surface       | Offers depth-resolved imaging                                      | Enables visualization of different retinal layers   |
| <b>Limitations</b>                          |  |  |   |
| <b>Cost</b>                                 | It is less costly to acquire fundus images   | more expensive to perform  | It may be costlier than traditional OCT             |
| <b>Time-consuming</b>                       | quicker to capture fundus images             | It may require longer acquisition and analysis time                | Longer imaging acquisition times                    |
| <b>Operator Dependency</b>                  | Relatively straightforward interpretation    | Interpretation may vary depending on the expertise of the operator | Interpretation may require specialized training     |

**Table 8** (continued)

| Aspect              | Fundus Images                              | OCT   | OCTA  |
|---------------------|--|---|---|
| Accessibility       | Widely available in most eye care settings | Requires specialized equipment and expertise  | Requires specialized equipment and expertise  |
| Patient Cooperation | Generally easier for patients to undergo   | Requires stable fixation for accurate imaging | Requires stable fixation for accurate imaging |

**Table 9** Review of Blood Vessels Segmentation Methods

| Applied Methods   | Performance Metrics  | Advantages  | Limitations   | Ref No                       |
|---|--|---|---|------------------------------|
| Gaussian function and two-dimensional Matched filter  | —  | Conserves the connectivity between blood vessels                                    | There are no objective parameters were applied for the evaluation<br>Tested the algorithm with only two images  | (Chaudhuri et al. 1989)      |
| Threshold probing Method<br>Matched filter using Gaussian function                            | True Positive Rate -75.00%   | Keeps the blood vessels' continuity   | Applied on one parameter for the evaluation purpose<br>Unable to segment the diverse width of blood vessels<br>The high error rate in pathological images             | (Hoover 2000)                |
| KNN classifier using feature set<br>Ridge detection   | ACC- 87.00%  | Works satisfactorily for healthy images   | Blood vessels are segmented excessively<br>DRIVE database is used only for validation<br>Loss of blood vascular connection  | (Staal et al. 2004)          |
| Bayesian classifier<br>Feature vector composed of two-dimensional Gabor wavelet responses     | ACC- 94.66%  | Provide better results on the DRIVE database<br>Keeps the blood vessels' continuity | Keeps the blood vessels continuity and provides incorrect detection measures due to noise<br>Incorrect identification of lesions and OD as blood vessel               | (Soares et al. 2006)         |
| Directional differential operator<br>Iterative region growing method<br>Multiscale morphology | ACC-94.52% (DRIVE)<br>False Positive Rate—23.60 (DRIVE)<br>ACC- 94.40% (STARE)<br>True Positive Rate- 69.96 (STARE)<br>False Positive Rate—27.00 (STARE) | Detects the vessel center line candidates   | Unable to find the thin blood vessel segments due to under-segmentation<br>Needs to improve the separation of bright lesions from vessel structures for better result | (Mendonça and Campilho 2006) |

Table 9 (continued)

| Applied Methods   | Performance Metrics  | Advantages  | Limitations   | Ref No                    |
|---|--|---|---|---------------------------|
| Line operators<br>SVM based classifier                            | ACC—95.62% (DRIVE)<br>ACC—95.82% (STARE)   | Computationally simple<br>Detects branching points accurately   | More number of false positives around the OD<br>Substantial interference of blood vessels with lesions<br>Loss of weak vessels through segmentation | (Ricci and Perfetti 2007) |
| Multi perceptron neural network (MLP)<br>CLAHE for pre-processing | ACC—80.70%<br>SN—60.70%<br>SP—97.30%   | Provide better outcomes on healthy retinal fundus images  | Poor performance with pathological images<br>Need to test more databases other than the DRIVE database  | (Franklin and Rajan 2014) |
| GAN combined with Dense U-net using Inception module and MLP      | area under the PR curve (AUC-PR) -90.58<br>area under the ROC curve (AUC-ROC) -97.72 | Shows significant performance for automatic retinal vessel segmentation<br>The method can be applied to two-dimensional fundus blood vessel images and three-dimensional medical data | the hyperparameter adjustment for the proposed method could be improved<br>Information loss on micro-objects  | (X. Guo et al. 2020)      |
| Multi-scale global attention network<br>Dense Attention U-Net     | AUC- 98.08<br>F1-Score > 82%<br>ACC-96.2%  | Effective context feature representation<br>Facilitate feature fusion and acquire fusion features for thin blood vessels  | Tested with small-scale datasets  | (Gao et al. 2023)         |
| Context Spatial U-Net   | F1-Score-85.16%<br>ACC-97.02%<br>AUC-98.25   | Facilitate two-channel encoders to capture both spatial and context information   | The computational complexity is still high  | (Hussain et al. 2022)     |

**Table 9** (continued)

| Applied Methods  | Performance Metrics                               | Advantages  | Limitations  | Ref No                |
|--|---|---|--|-----------------------|
| Deep residual network with over-parameterized convolutional layers | ACC- 0.9672 ± 0.0027<br>F1-Score- 0.8236 ± 0.0161 | provides nonlinear fusion pooling to avoid information loss<br>Implementing an effective multi-scale feature expression helps mitigate the insufficient processing problem associated with local context features | Can be improved for multi-task learning scheme for better segmentation results | (B. Wang et al. 2021) |

The iterative component analysis is employed, followed by the iterative thresholding procedure to establish the approximate location of the OD center. This integrated approach provides a starting point for determining its precise boundaries. Finally, the accurate border of the OD is determined using an implicit active contour model based on a geometric model. Geometric models differ from parametric models because they are less dependent on the image gradient and less sensitive to the initial contour's placement. Consequently, they can be more effectively applied to objects with weak borders, such as the OD (Mendonça and Campilho 2006).

Furthermore, several approaches with disc restrictions using the OD and cup borders are available (Ricci and Perfetti 2007). A deformable representation of regional statistics is utilized to detect the borderline of ODs with manifestations in color space and the expected cup regularity. A habitual OD parameterization system evaluates the regions derived from monocular retinal pictures (Franklin and Rajan 2014). However, it is essential to note that this evaluation does not offer a method for identifying eye conditions.

Youssif et al. (Youssif et al. 2008) applied a precise method for OD segmentation, detecting the OD's image dissimilarity and round shape through spherical conversion. However, the proposed method struggled with separating the diagonally detected OD border for an extended period. In another approach, Meindert Niemeijer et al. (Niemeijer et al., 2009) proposed a novel template-based method for OD segmentation using digital fundus retinal images. This method utilizes the circular hough transform, employing morphological and border identification strategies to obtain a rough estimate of the spherical OD boundary. However, it requires additional pixels positioned inside the OD as a starting point.

Furthermore, Welfer et al. proposed an algorithm based on analytical methods (Welfer et al. 2010) capable of identifying red and bright lesions without pre-processing to detect DR-related abnormalities in fundus pictures. Authors introduced a feature extraction technique (Khaing et al. 2022) that captures the universal distinctiveness of fundus images and distinguishes standard images. However, the method's performance is not evaluated with a large set of databases. The summary of OD detection methods is presented in Table 10.

### 3.6 Supervised and unsupervised model for DR detection

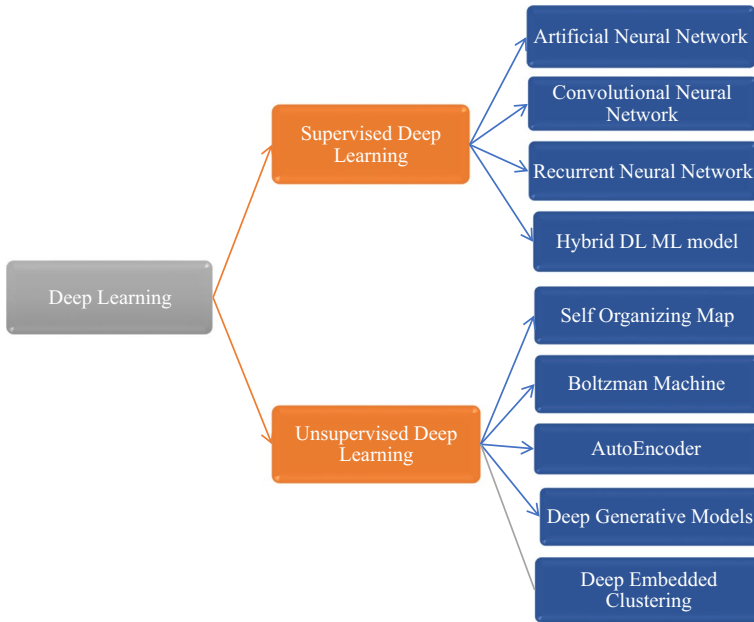
Handling vast data is a significant challenge for many enterprises and established sectors. The complexity of analyzing this information is formidable. To address this challenge, ML techniques, particularly DL algorithms, are crucial in advancing contemporary technologies and enabling in-depth analysis. SL demonstrates high potential and can solve many problems, with labeled data guiding the algorithm's training. Conversely, UL algorithms hold great promise for extracting hidden patterns from unlabelled data, providing insights into complex relationships within the dataset. Figure 15 illustrates the categorization of SL and UL methods.

#### 3.6.1 Using supervised deep learning

Supervised DL algorithms offer the advantage of creating models from unstructured labeled data. DL has demonstrated promising results in various natural language comprehension tasks, such as subject categorization, medical picture analysis, sentiment analysis, question answering, and language translation (Alyoubi et al. 2020). With its deep architecture, DL can address substantially more complex AI problems. DL

**Table 10** Review of Retinal OD Detection Methods

| Applied Method  | Number of Retinal Images   | OD location ACC (%)  | Ref No                        |
|---|--|--|-------------------------------|
| Matched filter using blood vessel orientation   | 81   | ACC- 98.77%<br>ACC- 100%   | (Youssif et al. 2008)         |
| The regression-based neural network method  | 250  | ACC—99.20%   | (Staal et al. 2004)           |
| Template-based method   | 61 (DIARETDB1)   | ACC—100%   | (Kauppi and Kälviäinen 2008)  |
| Point distribution model  | 500 (Normal)<br>100 (Unhealthy)  | ACC—98.40%<br>ACC—94.00%   | (Niemeijer et al. 2008)       |
| A hybrid snake model-based method   | 89 (DIARETDB1)<br>40 (DRIVE)   | ACC—97.75%   | (Welfer et al. 2010)          |
| A fully automatic hybrid method for OD localization, a smartphone-based approach                                | Three mobile cameras dataset,<br>Four datasets from standardized equipment | ACC—98%<br>Precision—92.64%<br>Recall—82.38%   | (Khaing et al. 2022)          |
| Combination of ML and computer vision algorithm for OD identification   | -  | ACC-99.71% SN-98.44%<br>0.41% improvement for OD extraction and eliminate the OD with 1.25 times faster  | (Rupanagudi et al. 2021)      |
| Mask Region-Convolutional Neural Network (R-CNN), MS R-CNN, CARAFE, Cascade Mask R-CNN, GCNet, SOLO, Point_Rend | REFUGE and G1020 datasets  | F1-Score (CARAFE)—96.3%<br>F1-Score (Cascade Mask R-CNN)—96.3%<br>F1-Score (SOLO)—91.6%<br>F1-Score (GCNet)—95.7%<br>F1-Score (Mask R-CNN)—96.3%<br>F1-Score (MS R-CNN)—96.3%<br>F1-Score (Point_Rend)—96.9% | (Alfonso-Francia et al. 2022) |
| convolutional autoencoder and pre-trained autoencoder network   | DRISHTI GS1 and RIM-ONE  | Dice Score Coefficient (DRISHTI GS1)—96.7%<br>Dice Score Coefficient (RIM-ONE)—90.2%   | (L. Zhang and Lim 2020)       |
| Particle Swarm Optimization (PSO)-enhanced ensemble deep neural networks  | Messidor   | ACC on Messidor (350 × 350) - 90.5%<br>ACC on Messidor (224 × 224)—95.93%  | (Bengani et al. 2021)         |



**Fig. 15** Categorization of Supervised and Unsupervised DL

employs methods like autoencoders, DBN, CNN, and RNN for feature representation. Supervised DL methods have outperformed traditional ML algorithms in the analysis of medical images (Table 11).

Consequently, several automated and computer-assisted systems have been developed for identifying DR, including Artificial Neural Networks (ANN), CNN, Recurrent Neural Networks (RNN), and hybrid models, as summarized in Table 12. Moreover, Within the realm of supervised deep learning approaches, the widespread success of Transformers in natural language processing has prompted numerous researchers (Huang et al. 2022; Lian and Liu 2024; Nazih et al. 2023; Yaoming Yang et al. 2024) to investigate their suitability in clinical applications, particularly in recognizing various ophthalmic diseases. Table 12 provides insights into recent studies on DR detection using vision transformers.

**Artificial neural network** Early detection of DR is critical as it is directly related to vision loss. For many patients, it is challenging and exhausting for medical experts to give the whole emphasise on the diagnosis of DR as well as to provide proper medical treatment. On the other hand, if DR is not detected early, the medical treatments are also more expensive for the patients in their later stages. Therefore, early diagnosis of DR is very much essential. An increasing variety of complex real-world issues have been tackled with ANNs. (Dutta et al. 2018). These neural networks have a significant advantage in solving complex problems for conventional technologies(Anas Bilal et al. 2022a, b, c). ANN is a networked collection of artificial neurons that processes information using a mathematical or computational model. ANNs mimic the human brain's information processing, learning from examples and detecting complex features in data sets. ANNs, with their nonlinear, distributed structure, operate without explicit instructions, making them effective for feature extraction and DR classification (Williamson et al. 1996).



**Table 11** Overview of Lesion Detection Methods using CNN and Variant

| Authors                           | Methodology  | Technique  | Detected Lesions                                   |
|-----------------------------------|--|--|--|
| (W. Zhou et al. 2017a, b)         | Unattended Classification Method based on sparse PCA     | Smoothing, CLAHE, Gaussian correlation coefficients  | MAs  |
| (Mazlan et al. 2020)              | Multilevel threshold and MLP                             | Green channel conversion, background elimination, CE, Multilevel thresholding, binarization, morphological close, Deep CNN | MAs  |
| (Wisaeng and Sa-Ngiamvibool 2019) | Mean shift algorithm                                     | Color normalization, noise removal, CE, OD localization, mean shift, and mathematical morphology algorithms                | Exudates   |
| (Pei et al., 2019)                | Enhanced Multi-feature Fusion Network (MFN)              | Multiple feature extraction, CNN, EMFN   | Hard Exudates                                      |
| (Zhou et al. 2017a, b)            | Multi-pixel classification with superpixels              | Multi-channel intensity features, contextual features, fisher discriminant analysis classifier                             | Multi-pixel classification images with superpixels |
| (Hatanaka et al. 2018)            | Segmentation ANFIS and MRG                               | Color channel separation, grey level run-length matrix MRG classified by ANFIS   | Retinal HM   |
| (Makarov et al., 2021)            | Artificial Neural network Fuzzy Inference System (ANFIS) | color channel separation, grey level run-length matrix, ANFIS, SVM   | HM   |

**Table 12** Supervised DL Methods for DR Detection

| Year | Applied Algorithm  | Applied Dataset                                | Performance   | Ref No                    |
|------|--|--|---|---------------------------|
| 2018 | SVM, Random Forest   | DIARETDB0                                      | ACC-85.23%<br>SN-93%<br>Kappa-0.67%   | (Sarwinda et al. 2019)    |
| 2018 | CLAE and CNN   | DIARETDB1                                      | ACC-87.6%<br>and 83.9%  | (Khojasteh et al. 2018)   |
| 2018 | Multiple Instance Learning (MIL) Framework   | MESSIDOR<br>DIARETDB0                          | AUC-90%<br>AUC (DB0)-93%  | (Costa et al. 2018)       |
| 2018 | Back Propagation Neural networks (BPNN), Deep Neural Network (DNN), and CNN                      | DIARETDB1<br>MESSIDOR                          | AUC (DB1)-96%<br>ACC (BNN)-62.7%<br>ACC (DNN)-89.6%   | (Dutta et al. 2018)       |
| 2018 | Image Processing and Linear SVM  | DIARETDB1                                      | ACC (CNN)-76.4%<br>SN-96%<br>SP-92%   | (S. Kumar and Kumar 2018) |
| 2018 | Image analysis technique and semi-supervised ML technique  | Real-time Images dataset                       | Image analysis technique<br>SN- 94%<br>SP-93%<br>Semi-supervised ML technique<br>SN-89%<br>SP-88% | (Zeng et al. 2019)        |
| 2019 | Siamese-like CNN architecture  | EyePACS  | Kappa Score-0.829   | (Zeng et al. 2019)        |
| 2019 | An ensemble of five deep CNN networks: Inceptionv3, Dense121, Resnet-50, Dense-169, and Xception | Kaggle dataset                                 | ACC-80.8%<br>Precision-63.8%<br>Recall-51.5%<br>SP-86.7%<br>F-Score-53.7%                         | (Qummar et al. 2019)      |
| 2020 | Circular bilateral Gabor filtering and local gradient analysis                                   | Retinopathy Online Challenge (ROC) database    | ACC-96%<br>SP- 53.9%  | (X. Zhang et al. 2020)    |
| 2020 | Image processing and Random sampling Boosting (RUS Boost) classifier                             | ROC database, e-ophtha, and SCREEN-DR database | F-Score-0.471, 0.510, 0.536<br>AUC-0.484, 0.575, 0.682  | (Melo et al. 2020)        |
| 2021 | SVM Classifier with statistical feature selection and ensemble CNN                               | IDRID dataset                                  | ACC - 90.01%<br>Min cross-entropy loss - 0.29   | (Bhardwaj et al. 2021)    |

**Table 12** (continued)

| Year | Applied Algorithm   | Applied Dataset  | Performance   | Ref No                     |
|------|---|--|---|----------------------------|
| 2022 | Gray scale and morphological feature-based segmentation with Residual-Attention Unet (RAUNet)                                 | Beijing Tongren manually labeled the dataset (528 labeled images)<br>OJADDR dataset (532 images) [Tao Li] Messidor dataset | Mean segmentation ACC is increased by 7%<br>RAUNET (weakly supervised) – 77.14<br>RAUNET (Fully supervised) – 70.61   | (Y. Li et al. 2022)        |
| 2022 | RTNet: Relation Transformer Network (Self-attention transformer, cross-attention transformer)                                 | DRIVE, STARE, DDR and IDRiD dataset  | AUC of Precision and Recall (AUC_PR: Hard Exudates)- 0.863<br>ROC-0.993<br>AUR_PR: Haemorrhages)-0.657<br>ROC-0.953<br>AUR_PR: Soft Exudates)-0.596<br>ROC-0.948<br>AUR_PR: Microaneurysm)-0.407<br>ROC-0.948 | (Huang et al. 2022)        |
| 2023 | vision transformer-based deep learning pipeline, vision transformer with different data balancing techniques                  | FGADR dataset  | ACC-82.5%<br>AUC-96.4%<br>F1-82.5%<br>Balanced ACC-82.6%<br>SP-95.6%  | (Nazih et al. 2023)        |
| 2024 | convolutional neural network-vision transformer (Classification)<br>Inception-Resnet-v2 backbone network (feature extraction) | ImageNet ISLVR2012 (Pre-training)<br>RFMiD dataset (fine tuning)<br>APTOS2019, Messidor dataset                            | ACC-95.3%<br>AUC-97.1%<br>S-96.6%<br>SP-94.2%   | (Lian and Liu 2024)        |
| 2024 | Vision Transformer, Transformer model with multiple instance learning and Global Instance Computing Block                     | APTOS dataset and Messidor-1 dataset   | APTOS<br>ACC- 85.6%<br>AUC- 95.6%<br>Messidor-1<br>ACC- 93.1%<br>AUC- 97.2%   | (Yaoming Yang et al. 2024) |

**Convolutional neural network (CNN)** CNN, a type of neural network, extracts higher representations of image content, featuring input, hidden, and output layers for image and video recognition. Comprising convolutional, pooling, and fully connected layers, CNN utilizes activation functions and dropout layers for effective processing, requiring less pre-processing than other machine or DL techniques (Mazlan et al. 2020). Table 11 discusses various studies on retinal lesion detection using CNN and its variants, presenting the information in a more structured form.

**Feed forward and recurrent neural network** Neural networks, including Feed Forward Neural Network (FNN) and RNN, vary in architecture. FNNs (Chakraborty et al. 2020) process information unidirectionally through layers, while RNNs use feedback loops, enabling real-time and time-series data analysis (W. Zhang et al. 2019). RNNs stand out for their memory.

**Hybrid ML-DL model** Several hybrid or ensemble models have been employed in DR screening to enhance model performance. This section discusses how ML techniques can be integrated as a layer within DL models to improve performance further. Various applied methods in this context are explored here.

S. Qummar et al. (Qummar et al. 2019) introduced an ensemble DL model for DR screening, utilizing five deep CNN models—Inceptionv3, Dense-121, Resnet-50, Dense-169, and Xception. Trained on the Kaggle dataset, the model detects various DR stages, achieving an early-stage detection accuracy of 80.8%. The ensemble method exhibits precision, specificity SP, recall, and F-scores of 63.8%, 86.7%, 51.5%, and 53.7%, respectively, addressing the challenge of manual DR screening by experts. Furthermore, Gupta et al. (Gupta et al. 2022) introduced a cost-effective smartphone-based DR detection technique, addressing the limitations of fundus cameras. Their hybrid method, integrating artificial neural networks (ANN) and deep convolutional neural networks (DCNN) within the social sky-driver (SSD), optimizes weight values for enhanced DR screening performance. The proposed system, tested on APTOS-2019-Blindness-Detection and EyePACS datasets, outperforms state-of-the-art algorithms, demonstrating promising results in smartphone-based DR detection.

Continuing the exploration of a hybrid method for DR detection, (Sreng et al., 2015) employ contrast and color illumination methods for pre-processing, followed by detecting fovea and red features. Lesions with blood vessels are identified, noise is eliminated, and HM is automatically detected. (Seoud et al., 2014) propose a method using CE and green histogram for image pre-processing, employing morphological flooding. Feature extraction involves various characteristics, and a random forest classifier achieves automated classification of both MAs and HM in fundus images.

Furthermore, (Khaing et al. 2022) present a fully automatic hybrid method with a smartphone-based approach, utilizing mobile cameras and standardized equipment datasets. The technique employs the exclusion method for analyzing vessel structure and integrates the active contour method with the hierarchical level set method (HLM) for OD segmentation. Achieving 98% OD localization accuracy for mobile camera datasets, the proposed method demonstrates impressive average precision and recall of 92.64% and 82.38%, outperforming state-of-the-art algorithms in OD segmentation performance.

### 3.6.2 Unsupervised DL methods

UL presents many undiscovered opportunities, mainly through clustering techniques that organize anonymous data into meaningful structures. These methods leverage knowledge discovery to autonomously group data without supervision. Deep clustering methods, such as the DEC algorithm introduced by (Ren et al., 2019), combine the strengths of DL and clustering, showcasing enhanced clustering capabilities. (Enguehard et al., 2019) Further emphasize DEC's potential, highlighting its ability to fill gaps left by supervised methods. Several algorithms have significantly influenced the fundamental processes of DEC. Additional UL algorithms for DR detection and lesion segmentation are detailed in Table 13.

**Autoencoder** Autoencoders, a type of FNN, represent both inputs and outputs as identical, trained for unsupervised representation learning. They comprise encoder, code, and decoder components. Autoencoders compress input into a latent feature space and reconstruct the output. Autoencoders fall under UL, operating without explicit data labels, and despite generating their labels, they are classified as Semi-SL techniques.

**Clustering with deep learning** The DEC algorithm is a hybrid approach that merges clustering and DL functionalities, yielding superior outcomes compared to UL processes. Through cluster assignment and feature learning, DEC algorithms unlock additional opportunities and bridge the gap typically addressed by SL methods.

**Autoencoder based DEC** The autoencoder with DEC can be implemented using a feature space to transform actual data into latent space features. The pre-training and fine-tuning operations are influenced during the training phase of the autoencoder. The clustering algorithm determines initial parameters such as convergence criteria and cluster centers during pre-training. These parameters are utilized in different sequences during fine-tuning (Kampffmeyer et al., 2019). DEC efficiently utilizes autoencoders for data reconstruction, and the DL network, such as CNN, is employed to study low-dimensional properties. The DEC implementation involves two stages: initialization of the autoencoder and pre-processing of the data in the first stage and optimization of parameters using an iterative technique and auxiliary target distribution computation in the second stage.

In the second stage, a gradient loss function is applied to calculate backpropagation, considering the t-distribution's degree of freedom ( $\alpha = 1$ ). After achieving the clustering score (CS), the algorithm progresses to find the cluster centers. The Kullback–Leibler (KL) loss is employed to calculate clustering and reconstruction losses. The clustering loss  $L_c$  is based on the calculated gradient loss function. During the reconstruction, the loss  $L_R$  is determined by the DNN. The learning parameters are then updated using these losses, forming the training network for subsequent sessions. As a Stacked Autoencoder (SAE), DEC simultaneously implements clustering and DL methods for effective UL processes. The architecture of autoencoder-based DEC is shown in Fig. 16.

**Clustering** UL plays a pivotal role in clustering, aiming to derive meaningful connections between data points with minimal supervision. Clustering, categorized into supervised, unsupervised, and semi-supervised types (Fig. 17), serves crucial practical purposes across applications such as information retrieval, text mining, web analysis, spatial databases, and medical diagnosis. Examining parameters in clustering algorithms involves considerations of clustering goals, types of data items, and data accessibility. Noteworthy clustering

**Table 13** Review of Supervised and Unsupervised DR Detection Methods

| Problem Addressed  | Dataset  | Results  | Methods   | Insight/Remark  | Ref No               |
|--|--|--|---|---|----------------------|
| Modern DL techniques in supervised, self-supervised, and vision transformers are reviewed and analyzed in this work    | Survey for DL Techniques   | According to various studies, the average accuracy is 91%                                    | supervised, self-supervised, and vision transformers  | After the screening, a subjective diagnosis must be made, often a drawn-out process subject to ophthalmologists.  | (Atwany et al. 2022) |
| This paper presents a new smartphone-based DR detection technique  | APTOS-2019-Blindness-Detection and EyePACS datasets                  | Visual representation of Segmented Lesions from EyePACS and APTOS dataset                    | Green channel conversion, CLAHE CNN and Life Choice-based optimizer                                   | The classification stage may be enlarged using enhanced ML and DL methods with different optimization algorithms to accomplish the maximum detection rate | (Gupta et al. 2022)  |
| To precisely detect OD using a smartphone-based, fully automatic hybrid approach                                       | Mobile cameras dataset and four datasets from standardized equipment | ACC—98% (OD localization for mobile camera datasets)<br>Recall—82.38%<br>Precision—92.64%    | hybrid method for OD localization (HLM)<br>Otsu's method, circle Hough transform, and decision tree   | Due to under-segmentation, thin blood vessel segments are missed  | (Khaing et al. 2022) |
| This article thoroughly analyses the most recent research on unsupervised DNN-based medical image registration methods | -  | Techniques, statistical analysis from different viewpoints, novelties, and future directions | Unsupervised deep neural network-based Image registration techniques/<br>Comprehensive Scoping Review | More research is required on the future combination of supervised and unsupervised methods  | (Abbasi et al. 2022) |

**Table 13** (continued)

| Problem Addressed   | Dataset  | Results   | Methods  | Insight/Remark   | Ref No                   |
|---|--|---|--|--|--------------------------|
| Health indicators are majorly based on feature extraction, and manual feature extraction can be done with domain knowledge; thus, the author proposed an unsupervised feature learning-based method | After experimenting on a DAHENG VMC850 CNC machining center, Authors obtained 4000 sample data points with a structure of 2560 × 1 × 8 | Relative similarity measure—90.5%<br>Trendability—96.92%  | multiscale convolutional autoencoder network (backbone and three encoder-decoder sections)   | some vessel segments are under-segmented   | (L. Guo et al. 2022)     |
| A combination of ML and computer vision algorithms for OD identification is proposed  | A total of 256 images were selected (165 training, 91 testing)   | There is an improvement of 0.41% for OD extraction, and algorithms run 1.25 times faster to eliminate OD<br>ACC-99.71%<br>SN-98.44% | The green component is extracted, the mean is found, and the threshold is calculated. Afterward, segmentation is done, and morphologic closing is performed to get the final output images | The system was created using the single-ethnic cohort  | (Rupanagudi et al. 2021) |
| The proposed method combines segmentation and pre-processing to detect MAs, retinal blood vessels, and backgrounds  | 100 photos from the e-ophtha project   | An accuracy of 92.28% surpasses that of SVM   | Multilevel thresholding, H-maxima, MLP, and morphological operations   | MAs are placed too close to blood vessels and might be segmented as blood vascular tissue                          | (Mazlan et al. 2020)     |
| Different automated computer vision methods are presented for DR detection  | Kaggle2 dataset with 35,126 (3888 × 2951) colour fundus Images   | Recall—97%<br>Precision—84%<br>F1-Score—90%   | Deep CNN models (Resnet50, Inceptionv3, Xception, Dense121, Dense169)  | The specific model can be implemented for particular stages, and an ensemble approach can further enhance accuracy | (Qummar et al. 2019)     |

**Table 13** (continued)

| Problem Addressed   | Dataset   | Results  | Methods  | Insight/Remark  | Ref No                            |
|---|---|--|--|---|-----------------------------------|
| The author explains the comprehensive review of the methods of subclinical DR biomarkers and how they may be applied for routine clinical use for the early detection of DR | -   | All research suggests that the indications in the initial phases of retinopathy may advance even without apparent clinical manifestations of retinopathy | All the studies related to subclinical DR biomarkers are reviewed  | The safety and efficiency of this approach in humans could be examined for clinical studies   | (Safi et al. 2018)                |
| The study aims to address the need for an effective MAs detector by proposing an approach that integrates three existing detectors to enhance prediction accuracy           | DIARETDB1 and ROC databases   | SN of 84% of False Positive rate 8.0 per image is recorded<br>The proposed method learns the parameters automatically                                    | Gabor filter, Hessian matrix, double-ring filter, three-layer perceptron, and a two-step DCNN                              | The network architecture could be made more efficient, and a post-processing technique could be added to enhance the method further | (Hatanaka et al. 2018)            |
| The novel technique employs a morphological mean shift algorithm to identify exudate lesions in color retinal pictures  | The training dataset consists of 72,214 pixels from 28 segmented abnormal images representing exudates and 77,422 from 28 segmented standard images representing non-exudates | ACC—98.40%,<br>SN—98.13%<br>SP—98.35%  | retinal picture normalization, CE, noise removal, and coarse segmentation approach   | Consultation with experts persists for small exudate regions, posing a significant challenge  | (Wisaeng and Sa-Ngiamvibool 2019) |
| A higher segmentation ability by employing Skeletonization and a Fuzzy Entropy approach is proposed to segment blood vessels  | STARE and DRIVE database (442 images of the retina)   | Accuracy—95% with a variation rate of 0.8%<br>Kappa coefficient—0.7<br>P-value—0.0451  | A three-step approach is applied, consisting of Wiener's filter, adaptive filtering, fuzzy entropy, and skeleton algorithm | Retina vessel 3D modeling can be created using image processing methods for real-time applications,                                 | (Rezaee et al. 2017)              |



**Table 13** (continued)

| Problem Addressed   | Dataset   | Results  | Methods   | Insight/Remark  | Ref No                    |
|---|---|--|---|---|---------------------------|
| A method for segmenting retinal vessels is provided. The segmentation process classifies each pixel of the fundus picture as a vessel or a non-vessel | DRIVE (768 × 584 pixels and 8 bits per color channel) dataset                               | The DRIVE dataset tests the model's performance, showing a 95% accuracy rate   | MLP neural network and Backpropagation algorithm  | Testing the results on datasets beyond DRIVE is imperative to establish the model's generalizability                  | (Franklin and Rajan 2014) |
| The automatic segmentation of the OD using a novel adaptive method based on mathematical morphology is proposed                                       | DRIVE and DIARETDB, two open-access datasets, were used to evaluate the suggested technique | DRIVE, mean of 41.47%, and OD placement with 100% images<br>DIARETDB1, mean overlap of 43.65% covering 97.75% of the fundus images | RMIN operator for background segmentation,<br>Novel adaptive morphological approach for foreground segmentation | Better accuracy can be achieved for detecting other crucial retinal structures, such as the fovea and the OD boundary | (Welfer et al. 2010)      |
| The approach combines image intensity and local vessel geometry to determine the correct positions in the fundus image                                | The performance is evaluated and recorded on 250 digital fundus images                      | The fovea and OD performance measurements were 99.2% and 96.4%, respectively   | KNN regressor   | The identical low contrast similarly restricts fovea detection  | (Niemeijer et al. 2008)   |

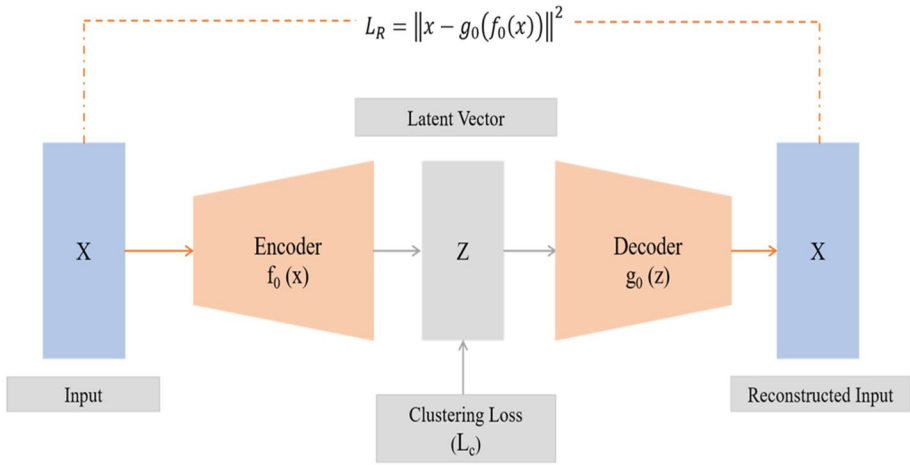


Fig. 16 Autoencoder-based DEC

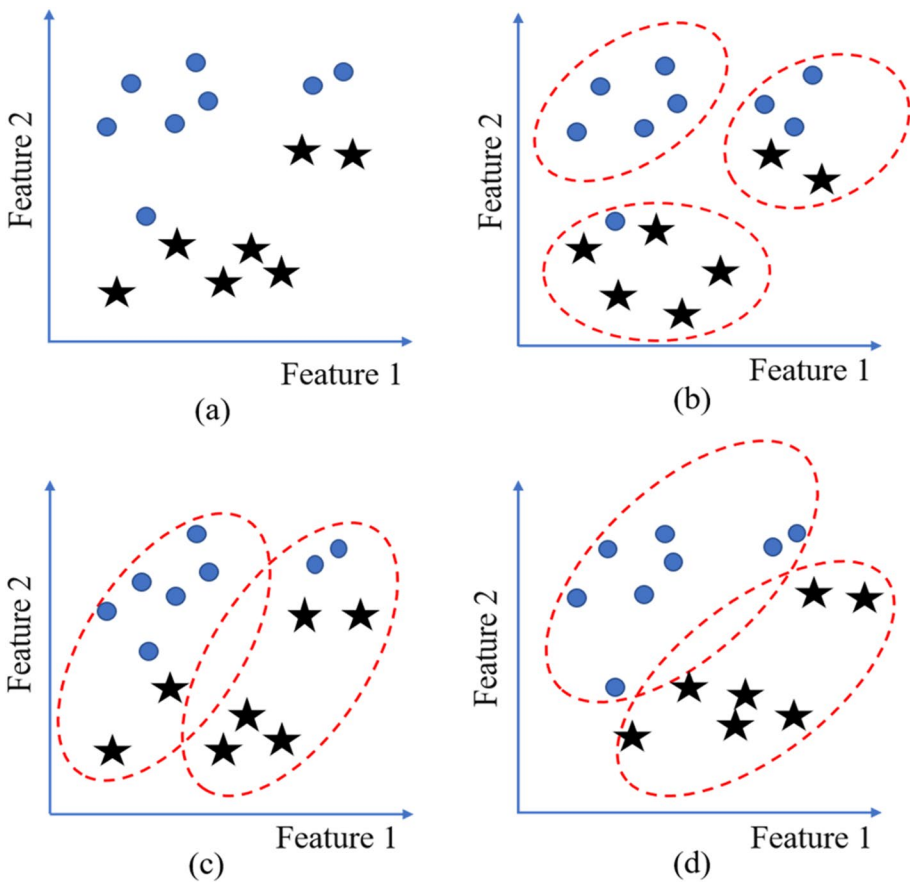


Fig. 17 Clustering (a) Dataset Sample (b) Unsupervised Clustering (c) Semi-Supervised Clustering (d) Supervised Clustering

algorithms in research communities include Hierarchical Agglomerative Clustering (HAC), Density-based Hierarchical Agglomerative Clustering (DHAC), and K-Means (Camastra and Vinciarelli 2008).

**Hierarchical clustering** Hierarchical clustering creates a tree-like structure, often called dendrograms, by assessing relationships between data points. It encompasses two approaches: agglomerative, where clusters are successively merged, and divisive, which involves iteratively splitting clusters. Unlike K-Means, hierarchical clustering does not require a predefined number of clusters. The method evaluates relationships between data elements, utilizing centroids in an optimization algorithm. The effectiveness of the clusters can be assessed using different fitness functions and criteria.

In summary, the choice between supervised and unsupervised DL DR detection hinges on factors such as the availability of labeled data, the desire for high accuracy, and the exploration of data patterns. While supervised methods aim for precision with labeled datasets, unsupervised methods offer flexibility in scenarios with limited annotations, albeit with challenges in evaluation and interpretability.

## 4 Discussion & critical analysis

DR is a prevalent eye disease and a leading cause of global blindness. Early detection is crucial to prevent vision loss, making regular patient screening imperative. This study comprehensively reviews supervised and unsupervised DL methods for early DR detection. While numerous reviews exist on automated DR detection (Alyoubi et al. 2020; A. Bilal et al. 2021a, b, c; Cleland et al. 2023; Kar et al. 2021; Mayya et al. 2021; Subramanian et al. 2022), there is a scarcity of reviews explicitly addressing the supervised and unsupervised DL techniques. Furthermore, no reviews have systematically compared the performance of unsupervised and supervised DL methods. By addressing this gap, the review study offers an illustrious understanding of the strengths and limitations of supervised and unsupervised DL techniques for DR detection. The systematic comparison presented in this review contributes to a more informed decision-making process when selecting an appropriate DL approach for early DR detection, ultimately enhancing the efficiency and accuracy of diagnostic systems. The study analyzes 103 articles retrieved from four databases, employing diverse queries, papers, years, and keyword-based filters to extract relevant manuscripts. The review explores publicly available and exclusive datasets for automated DR detection, detailing image processing techniques such as CE, noise removal, optic disc and blood vessel segmentation, green channel extraction, and more to enhance image quality.

The author utilized open access or comprehensive datasets for DR detection in the selected manuscripts. Many researchers (Z. Xiao et al. 2015; Su Wang et al. 2017; Tan et al. 2017; Takahashi et al. 2017; Takahashi et al. 2017; Fumero et al. 2011) have assembled datasets from fundus images collected at specific hospitals or through particular camera devices. The review highlights challenges associated with the use of exclusive datasets. Firstly, classification models trained on such datasets may not generalize well to different data modalities. Given the limited scope of data collected from one or two hospitals with specific devices, it is essential to ensure that the detection of DR applies to various data modalities. Therefore, collecting multimodal data is recommended, considering the diversity of medical devices used in DR diagnosis. Secondly, the small number of images in

exclusive datasets can lead to lower model performance. It is noted that exclusive datasets tend to exhibit lower accuracy and other metric performances compared to open-access datasets.

Conversely, numerous researchers (Naqvi et al. 2015; Kusakunniran et al. 2018; Budak et al. 2017; Chudzik et al. 2018; Fraz et al. 2017; X. Li et al. 2018; Shuangling Wang et al. 2015) have focused on automated DR detection using open access datasets. However, these datasets often encounter a class imbalance problem. Notably, most publicly available datasets exhibit this issue. For instance, the Kaggle dataset comprises 35,426 images categorized into Mild, Moderate, Severe, No DR, and Proliferative signs. This dataset is highly imbalanced, with the majority class containing 25,810 images, making up 73% of the total, while the minority class consists of 9,316 images. Researchers working with imbalanced datasets typically employ techniques such as downsampling or augmenting the minority class to enhance the model's performance.

Several studies (Simonyan & Zisserman, 2015; Takahashi et al. 2017) have employed Data Augmentation (DA) techniques to synthesize data points from minority classes. However, it is recommended that DA be applied during training rather than testing. Exclusive datasets comprising images from different hospitals may exhibit noisy pixels or features, making pre-processing crucial for enhancing model performance. Image resizing is a pre-processing method that can remove noisy features, and cropping is an effective technique for eliminating extraneous pixels that do not contribute to classification. Additionally, resizing images can decrease computational time by converting high-resolution images to low-resolution. Green channel extraction is another applied technique, extracting the green channel from the RGB channel and facilitating the easy identification of blood vessels, as outlined in Table 6.

Contrarily, CE serves to enhance picture quality and sharpen fundus images. Nevertheless, these techniques come with certain limitations. Similarly, image augmentation methods generate synthetic data points, potentially introducing bias in the model's performance when confronted with real-life DR detection. Image cropping may result in the loss of crucial information. Therefore, comparing the model's performance with and without pre-processing is advisable for a comprehensive evaluation. Various supervised deep-learning methods for diabetic retinopathy detection are discussed in Table 12. However, unsupervised techniques demonstrate significant potential for extracting hidden patterns.

CNNs dedicated to image-related tasks are widely used and exhibit remarkable performance records. GAN performed exceptionally well in unsupervised classification, but their application in DR is limited. Moreover, no specific model is universally suitable for DR classification. Table 14 compares both models, aiding in understanding their performance across various applications, contingent upon the data's variability and dimension. Consequently, scholars face diverse challenges in exploration and should prioritize the model's explainability.

## 5 Future scope and open challenges

There is still a need for improvement in the existing approach to enhance performance in DR detection. Thus, this section addresses the future scope and open challenges researchers should focus on to enhance DR classification performance. The challenges that need to be addressed include-

**Table 14** Comparison of Supervised and Unsupervised DL Approaches for DR Detection

| Key difference    |   | Unsupervised DL   |   |
|-------------------|---|---|---|
| <b>Objectives</b> | <b>Precision in Classification</b>      | The primary goal of supervised DL methods is to achieve high precision and accuracy in classifying input data into predefined categories. In the context of DR detection, this involves accurately categorizing retinal images into different stages of the disease | <b>Data Exploration and Pattern Discovery</b><br>Unsupervised DL methods are designed to explore data without needing labeled information. The primary goal is to discover inherent patterns, structures, or relationships within the data, often without predefined categories |
|                   | <b>Optimizing for Specific Criteria</b> | The training aims to optimize specific criteria, such as minimizing classification errors or maximizing accuracy. The model aims to replicate the human-assigned labels in the training set and generalize well to new, unseen data                                 | <b>Novel Insights and Discoveries</b><br>UL seeks to provide novel insights and discoveries within the data, potentially identifying patterns that were not preconceived or explicitly defined. This goal aligns with the exploration of unknown territories in data            |
| <b>Metrics</b>    | <b>Accuracy</b>                         | Indicates the overall correctness of the model's predictions in supervised tasks  | <b>Silhouette Score</b><br>Evaluates the cohesion and separation of clusters in unsupervised settings   |
|                   | <b>Precision</b>                        | Measures the accuracy of positive predictions, which is crucial for tasks with imbalanced classes   | <b>Adjusted Rand Index (ARI):</b><br>Evaluates the accuracy of clustering in comparison to ground truth   |
|                   | <b>Recall</b>                           | It focuses on capturing all positive instances, essential in scenarios where missing positives have high consequences   | <b>Inertia (Within-Cluster Sum of Squares)</b><br>Represents the compactness of clusters in unsupervised learning   |
|                   | <b>F1 Score</b>                         | Balances precision and recall, suitable for tasks where both false positives and false negatives are critical   | <b>Davies-Bouldin Index</b><br>Provides a measure of cluster compactness and separation   |

**Table 14** (continued)

| Key difference  | Supervised DL   | Unsupervised DL   |
|---|---|---|
| <p><b>Area Under the ROC Curve (AUC-ROC)</b></p>        | <p>Measures the model's ability to distinguish between classes, especially relevant in binary classification tasks</p>  |   |
| <p><b>Complexity</b></p>                                | <p><b>Data Labelling Complexity</b><br/>Acquiring and annotating large datasets with accurate labels for training purposes can be a time-consuming and resource-intensive process</p>                                   | <p><b>Interpretability Complexity</b><br/>Unsupervised DL models may produce complex internal representations that are challenging to interpret, limiting understanding of the learned patterns</p>   |
| <p><b>Model Complexity</b></p>                          | <p>Designing, fine-tuning, and optimizing complex deep neural networks like CNN and RNN demands expertise in architecture selection and hyperparameter tuning</p>   | <p><b>Evaluation Complexity</b><br/>Assessing the performance of unsupervised models is more complex as there may not be a clear benchmark or ground truth for comparison</p>   |
| <p><b>Overfitting and Generalization Complexity</b></p> | <p>Striking the right balance to prevent overfitting while ensuring generalization to unseen data is challenging</p>  | <p><b>Clustering and Structure Discovery Complexity</b><br/>Identifying meaningful clusters or structures within unlabelled data can be inherently complex, especially when the ground truth is unknown</p>   |
| <p><b>High Accuracy with Labelled Data</b></p>          | <p>Supervised methods, particularly Convolutional Neural Networks (CNNs), achieve high accuracy when trained on extensive labeled datasets. This accuracy is crucial in precisely identifying DR</p>                    | <p><b>Data Exploration without Labels</b><br/>Unsupervised methods, such as clustering algorithms, allow for data exploration without needing labeled information. This is beneficial when the underlying patterns in retinal images are not fully understood</p> |
| <p><b>Optimized for Annotated Data</b></p>              | <p>The supervised approach is well-suited for scenarios where datasets are annotated or labeled, providing a well-defined framework for the model to learn specific features associated with different stages of DR</p> | <p><b>Handling Unlabelled Data</b><br/>In cases where obtaining labeled data is challenging (medical imaging domain), UL methods prove valuable. They can uncover hidden structures in the data without extensive manual annotation</p>                           |

**Table 14** (continued)

| Key difference      |   | Supervised DL   |  | Unsupervised DL                        |   |
|---------------------|---|---|--|--|---|
|                     | <b>Established Frameworks</b>   | Supervised DL methods benefit from well-established frameworks like CNNs, known for their effectiveness in image classification tasks   |  | <b>Potential for Novel Discoveries</b> | Unsupervised methods have the potential to reveal novel patterns or relationships within the data, contributing to a deeper understanding of medical data   |
| <b>Cons</b>         | <b>Limited Generalization</b>   | Supervised models might struggle with generalizing to new, unseen data, primarily when the training data does not encompass the full spectrum of potential variations in retinal images                                   |  | <b>Challenge in Evaluation</b>         | Evaluating the performance of unsupervised models can be challenging due to the absence of clear ground truth labels. Metrics for assessing accuracy may be less straightforward compared to supervised methods |
|                     | <b>Dependency on Labelled Data</b>  | A significant drawback is a heavy reliance on labeled data for training. In the context of DR, acquiring a large and accurately labeled dataset can be challenging and time-consuming, specifically in the medical domain |  | <b>Sensitivity to Initialization</b>   | Specific unsupervised methods (profound clustering algorithms, can be sensitive to the initial configuration of parameters, requiring careful tuning  |
| <b>Applications</b> | A supervised algorithm can perform well with spam detection, weather forecasting, and sentiment analysis applications |   |  | <b>Limited Interpretability</b>        | Unsupervised models may lack interpretability, making understanding the underlying rationale behind their predictions for DR challenging  |
|                     |   |   |  |  | On the other hand, UL can be considered a gift for detecting anomalies, designing a recommendation engine, customer persons, and medical imaging  |

1. **Explainability and Interpretability:** The interpretability of DL models in DR detection is a pressing challenge. Enhancing the explainability of model predictions is crucial for gaining the trust of healthcare practitioners. Future studies should aim to develop models capable of providing clear and understandable concerning their decision-making processes.
2. **Integration of Multimodal Data:** Integrating data from various imaging modalities, such as OCT and fundus photography, poses a challenge. Future studies should explore methods to effectively integrate and leverage multimodal data for a more comprehensive understanding of DR progression and severity.
3. **Virtual and Augmented Reality for Training and Visualization:** The application of Virtual and Augmented Reality (VR/AR) in DR studies will evolve to enhance medical training and visualization. Future directions include the development of immersive VR/AR platforms for training healthcare professionals in DR diagnosis and creating AR tools that allow practitioners to visualize retinal structures in three-dimensional space.
4. **3D Medical Imaging for Detailed Retinal Assessment:** The future of DR detection will see advancements in 3D medical imaging techniques for more detailed and comprehensive retinal assessment. This includes the development of imaging technologies such as 3D OCT for capturing volumetric data, providing a deeper understanding of structural changes associated with DR.
5. **Wearables for Continuous Monitoring:** Wearable devices will play a pivotal role in continuously monitoring individuals at risk of DR. Future directions involve integrating wearable technologies for real-time tracking of retinal health parameters. These wearables can provide early warnings and enable proactive management.
6. **Human-AI Collaboration in Clinical Decision-Making:** Integrating AI models into clinical decision-making processes requires collaboration between healthcare professionals and AI systems. Future research should focus on developing frameworks for effective human-AI collaboration, ensuring that AI complements clinical expertise rather than replacing it.

## 6 Concluding remarks

DR stands out as a leading cause of global blindness, often remaining asymptomatic until reaching a severe stage. Early treatment of DR can effectively prevent vision loss. Consequently, various supervised DL models, such as CNN, DNN, BPNN, semi-supervised, and ensemble DL models, have been employed for automated DR detection. The superiority of DL models in image analysis within the DR detection domain is notable. However, a significant challenge persists due to the unavailability of labeled data in medical imaging.

The review delves into a literature survey on keywords associated with supervised and unsupervised methods from 2018 to 2023. One hundred and three articles were meticulously selected from four diverse databases, employing five specific filters—a process detailed further in the discussion section. Additionally, publicly and exclusively utilized datasets for DR classification studies are presented with their available links and essential details. Kaggle and DIARETDB1 emerge as the primary datasets across all included studies. Among various pre-processing techniques, green channel extraction followed by CE consistently yielded more accurate outcomes and was deemed a fundamental approach. Subsequently, the review comprehensively explores widely employed SL and UL techniques in DR detection,



covering features and classification methods. A comparison of Unsupervised and Supervised methods for DR classification is presented in Table 13.

In the specific application context, the literature underscores a notable lack of emphasis on unsupervised methods for DR classification. Supervised DL methods exhibit superior performance when extensive training data is available. However, these methods rely heavily on labeled datasets, which are invaluable for real-time training and classification but demand substantial manual labeling efforts. In instances where labeled datasets are unavailable, the efficacy of supervised DL algorithms diminishes. Most studies have predominantly employed CNN-based DL models for DR detection. Nevertheless, CNNs are more adept at handling supervised problems with annotated or labeled data, necessitating the availability of large datasets for optimal performance. This review thoroughly explores the challenges inherent in medical images and DR detection, revealing a shift towards the emergence of unsupervised, semi-supervised, and hybrid learning approaches in medical imaging and DR detection.

While the presented reviews aim to cover a comprehensive spectrum, it is conceivable that the authors may have inadvertently omitted certain vital elements. This review emphasizes that while supervised DL methods excel with extensive labeled data, the attention to unsupervised methods is relatively scant, opening avenues for future exploration. This comprehensive study is valuable for scholars and academicians in DR detection. It sets the stage for upcoming research that advances unsupervised methodologies across various medical imaging domains, especially with emerging medical diseases. Future work will concentrate exclusively on UL methodologies across all medical imaging areas, particularly addressing emerging medical diseases.

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Permission has been obtained from the authors to reprint figures 3 and 4.

## Declarations

**Competing interests** The authors declare no competing interests.

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