Development and evaluation of a gold nanoparticle-based immunochromatographic strip test for the detection of canine parvovirus

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Abstract

Canine parvovirus (CPV) is the leading viral cause of enteritis in dogs and occurs mainly in 6- to 8-week-old pups. Rapid diagnosis of CPV under field conditions is now possible due to commercially available immunochromatographic (IC) assays. However, these commercial kits are somewhat expensive because they utilize a minimum of two monoclonal antibodies (mAbs) targeting different epitopes as capture and detector antibodies. Using only a single mAb for both capture and detection purpose may reduce the sensitivity of the assay. In the present study, efforts were made to develop an economical assay that can be utilized for diagnosis of CPV under Indian conditions with a high level of confidence. Rabbit polyclonal antibodies (pAbs) generated against recombinant truncated VP2 proteins of CPV were used as capture antibodies because they can be produced economically, while a commercial anti-CPV mAb was used as the detector antibody. The detection limit of the test strip was 6.6×10^5 TCID₅₀/ml, and it specifically detected CPV-2, CPV-2a and CPV-2b while displaying no cross-reactivity with other common canine enteric pathogens. The relative sensitivity/specificity of pAb based strip test was 71%/92% and 71%/100% in relation to the hemagglutination test and a commercial IC kit, respectively, with substantial agreement. In addition, two commercially available mAbs targeting different epitopes were also used for development of another IC assay, which showed sensitivity, and specificity of 82%/87% and 90%/98% in relation to the hemagglutination test and commercial kit. Hence, the present strip test based on a combination of mAb and pAb provides an acceptable alternative for onsite and cost-effective diagnosis of CPV infection.

Introduction

Canine parvoviral enteritis is a highly contagious and fatal viral disease that is responsible for neonatal death in pups [1, 2]. The etiological agent, canine parvovirus 2 (CPV-2), is a small, non-enveloped, negative-sense ss-DNA virus with a genome of 5.2 kb in length that encodes two non-structural (NS1 and NS2) and two structural (VP1 and VP2) proteins [3]. VP2 is the major capsid protein, which plays a crucial role in determining antigenicity, host range and tissue tropism [4]. This virus, which initially emerged in 1970s and spread globally thereafter, is now considered endemic in the dog population, with the existence of different antigenic variants, viz., CPV-2a, CPV-2b, CPV-2c, new CPV-2a/2b [5–7].

Due to the acute and highly contagious nature of the disease, an early and prompt diagnosis is essential in order to adopt biosecurity measures for preventing the spread of the disease to the susceptible population, and

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also to initiate supportive treatment to reduce morbidity and mortality. Hence, a simple, cost-effective, field-based test is essential for rapid diagnosis of canine parvoviral enteritis. Several diagnostic assays have been developed for the detection of CPV; however, each of these assays has its own merits and demerits in terms of cost, sensitivity, specificity and convenience that may render them unsuitable for widespread field use [8]. The diagnostic assays frequently employed for the detection of CPV-2 are hemagglutination (HA) test, virus isolation, enzyme-linked immunosorbent assay (ELISA; SNAP Parvo, Idexx USA) and polymerase chain reaction (PCR).

A range of commercial immunochromatographic (IC)-strip-based assays are available for rapid detection of CPV-2 under field conditions [9, 10]. Most of these kits are not produced in India and must be imported from other countries, which increases the cost per test. These strip tests are based on the sandwich principle, using either a single monoclonal antibody (mAb) or two different CPV-specific mAbs as detector and capture antibodies. Although not described in the literature, the use of the same mAb for both capture and detection in these IC assays may limit the sensitivity of detection in cases of low fecal CPV load, as the capture and detector mAbs would compete for the same epitope. This could be the reason behind the poor sensitivity displayed by these assays, especially during late stage of the infection, when fecal shedding is significantly reduced [9, 11]. Alternatively, employing two different mAbs in these strip-based assays is an expensive proposition, limiting its practical usability on a wider scale. Furthermore, binding of one mAb (detector) to an epitope has the potential of affecting certain other spatially unrelated epitopes in a way that could alter the binding of the second mAb [12]. Utilizing a polyclonal antibody (pAb) instead of an mAb as the capture antibody in the IC test may hold promise, as using mAbs as detector antibodies may result in alteration of only some of the original epitopes, leaving the rest of the epitopes unaltered and accessible to the polyclonal capture antibodies. Furthermore, pAbs are generally less expensive and faster to produce than mAbs.

Considering the importance of developing an indigenous and economical kit that utilizes homemade biological reagents, the present study was undertaken to explore the combination of an mAb and pAbs as detector and capture antibodies, respectively, for the development of an IC test for rapid detection of CPV. Furthermore, for economical production of pAbs in the laboratory, recombinant structural proteins of CPV were expressed in truncated form for higher yield using a prokaryotic system. The use of recombinant proteins eliminates the risk of handling live virus in the laboratory for production of pAbs.

Materials and methods

Clinical samples

A total of 97 fecal swabs ($n = 97$), collected in duplicate from dogs of different age groups (both vaccinated and unvaccinated) showing symptoms of gastroenteritis were collected from the Referral Veterinary Polyclinic located at the Indian Veterinary Research Institute, Izatnagar Bareilly, UP, India, during the years 2015 and 2016 and processed as described earlier [13]. The clinical samples were tested for the presence of CPV using a hemagglutination (HA) test (HA titers ≥ 32 were considered positive for CPV) and a commercially available IC-based Rapid CPV Ag Test Kit (Bionote, Republic of Korea).

Cloning, bacterial expression, and purification of truncated CPV VP2 proteins (CPV-tVP2)

Two overlapping fragments corresponding to the N-terminal end and most of the C-terminal end of the VP2 gene were targeted separately for amplification (N-region, nt 10-770; C-region, nt 750-1641) using genomic DNA from cell-culture-adapted CPV-2a (BE-1; NCBI GenBank accession number KJ364524). The primers CPV-NF (5-ACACAGAATTCAGGAGCAGTTCAACCAGAC-3) and CPV-NR (5-ATCTAGATTCTCGAGTGTTCC TGTAGCAAATTCATC-3) were used for amplification of the N-terminal region, and the primers CPV-CF (5-ACTGCAGCGAATTCAGGTGATGAATTTGCTACAG-3) and CPV-CR (5-GGGCTCGAGTGGATTCCAAGTATGAGAG-3) were used for amplification of the partial C-terminal region. The resulting PCR products were gel purified, ligated with pET32b vector, and used to transform chemically competent *E. coli* BL21 strain Rosetta (DE3) pLysS cells (Novagen, Germany) following standard procedures. Expression of recombinant CPV-tVP2 protein was optimized by evaluating the different combinations of IPTG concentration, temperature, and time for induction, as described earlier [14]. A overnight-grown bacterial culture was harvested by centrifugation and lysed in a buffer containing 8 M urea, 100 mM NaH_2PO_4 and 10 mM Tris-Cl, pH 8.0, prior to sonication. Both recombinant CPV-tVP2 proteins were purified by affinity chromatography using Ni-NTA resin (QIAGEN, Inc., Hilden, Germany) under denaturing conditions as described by the manufacturer. The purified CPV-tVP2 proteins were electro-transferred onto the nitrocellulose membrane (MDI, India) in order to test their immunoreactivity by Western blotting. The membrane was probed with a known anti-CPV dog serum (1:100 dilution) collected from healthy vaccinated dogs,

and following incubation with anti-dog HRPO conjugate, the proteins on the membrane were detected using an enzymatic reaction.

Generation of anti-CPV-tVP2 rabbit pAbs

Two healthy young male New Zealand white rabbits were injected intramuscularly with a mixture of 100 µg of each of the purified recombinant CPV-tVP2 proteins mixed in equal proportion with Freund's complete adjuvant (Sigma, USA). Rabbits were boosted three times at an interval of two weeks each with same antigen mixed with Freund incomplete adjuvant (Sigma, USA). Serum was harvested after bleeding the animals on the tenth day following the last injection. Blood serum was collected and reactivity was determined by dot-blot assay using CPV-tVP2 protein and A-72 infected CPV as per the standard procedure. The total immunoglobulin G (IgG) from the CPV-tVP2 specific rabbit hyperimmune serum was separated using a protein A affinity column (Thermo Scientific, USA) following the procedure described by the manufacturer. The purified rabbit IgG fraction was quantified using a spectrophotometer and stored at -80°C for subsequent use.

Preparation of colloidal gold nanoparticle conjugate

Determination of the optimum pH and antibody concentration for gold conjugation

The CPV-specific mAb (Thermo Scientific, USA) was conjugated to 30-nm colloidal gold nanoparticles (GNPs) (Sigma, USA) under various conditions of pH and antibody concentration using NaCl flocculation assay and UV-Vis absorbance assay as described earlier [15, 16] with slight modifications. Briefly, the pH of 100 µl of GNPs was adjusted from 6 to 9 in a microtiter plate in increments of 0.5 by adding 0.1 N K_2CO_3 and testing the pH with Hi-media pH indicator strips (Hi-media, India). Anti CPV mAb (1 mg/ml) at different concentrations (0, 5, 10, 20 and 30 µg/ml) was added to each well containing GNPs at different pH values. The mixtures were allowed to react for 15 min at room temperature with manual shaking, and 20 µl of 10% NaCl was then added to each well, and gentle shaking was continued for another 15 min. The solution was monitored visually for any color change (GNPs flocculation) and absorbance was measured using a microplate reader (Thermo Scientific, USA) at 580 nm and 600 nm to calculate the stability index ($\text{SI} = \text{OD}_{\lambda_{\text{max}}} / \text{OD}_{580}$) and polydispersity index ($\text{PI} = \text{OD}_{600} / \text{OD}_{\lambda_{\text{max}}}$). Average values were calculated from three repeated experiments. The optimal coverage of colloidal gold with mAbs was further verified by UV-Vis spectrophotometry, differential light scattering (DLS), transmission electron microscopy (TEM), and dot-blot assay, using standard method.

Preparation of mAb-colloidal gold conjugate

Briefly, 1 mL of colloidal gold suspension was adjusted to the optimized pH using 0.1 N K_2CO_3 and the optimal amount of anti-CPV mAb was then added with constant stirring. The adsorption of mAbs on the surface of the GNPs was allowed to take place at room temperature with constant stirring for 30 min. Unreactive sites on GNPs were blocked by addition of 0.01 M PBS, pH 7.2, containing 10% bovine serum albumin (BSA) at room temperature with continuous stirring for 15 min. The solution was centrifuged at 8000 rpm for 30 min at 4°C , and the soft pellet was washed with 0.01 M PBS, pH 7.2, with centrifugation at 8000 rpm for 30 min at 4°C to remove unbound antibodies from the solution. Finally, the pellet was resuspended with one tenth of the original volume in 0.01 M PBS, pH 7.2, containing 1% BSA and subsequently stored at 4°C for future use.

Preparation of an mAb/pAb-based lateral flow immunochromatographic test strip

The colloidal gold conjugate was coated onto the conjugate pad (MDI, India) by manual pipetting (10 µl of conjugate per strip) and allowed to air dry. A nitrocellulose membrane (MDI, India) was charged with test and control antibodies by manual pipetting or using an Easy Printer (MDI, India). Different concentrations (1, 2 and 5 mg/ml) of anti-CPV-tVP2 rabbit polyclonal IgG and goat anti-mouse pAbs (Genei, India) were used for coating on the test and control line, respectively. After coating, the membrane was air dried at 37°C for 2 h and then assembled with other pads. The distance between test and control line was kept at around 5 mm. Other variables that could potentially influence the performance of the IC test were also optimized, and these are presented in Table 1.

Table 1 Optimization of IC test with minor variables

Variables	Optimum
Membrane pore size (5, 8 and 10 µm)	8 and 10 µm
Sample volume and running buffer	Sample volume = 60–80 µl Sample running buffer = 10 mM phosphate buffer, pH 7.2 with SDS
Concentration of anti-CPV-tVP2 rabbit pAbs on test line (1, 2 and 5 mg/ml)	2 mg/ml
Concentration of goat anti-mouse pAbs on control line (1, 2 and 5 mg/ml)	1 mg/ml
Completion time (5, 10 and 20 min)	10 min

Preparation of an mAb/mAb-based lateral flow immunochromatographic test strip

The procedure described in the previous section was essentially followed, except instead of anti-CPV-tVP2 pAb, commercially procured anti-CPV mAb (VMRD, USA) was used as the capture antibody (1 mg/ml) for coating on the test line.

Assay procedure

Upon interaction of CPV antigen with mAb-gold conjugate, a CPV-mAb-gold complex formed, which migrated onto the nitrocellulose membrane and subsequently reacted with immobilized capture antibodies (anti-CPV-tVP2 pAbs or anti CPV mAbs) on the test line, whereas unbound anti-CPV monoclonal gold conjugate ran over the test line and then reacted with the goat anti-mouse antibody at the control line to form a second visible purple-red band. The sample was considered positive if two distinct purple-red lines appeared, one in the test region and the other in the control region, negative when no line appeared in the test region, and invalid if the control line failed to appear.

Estimation of the sensitivity and specificity of the IC strip test

The analytical sensitivity of the mAb/pAb and mAb/mAb-based test strips were determined using a serially diluted live attenuated strain of CPV (TN-4; NCBI GenBank accession number KX219741) with 10^7 TCID₅₀/ml. The standard CPV and known A-72-cell-adapted CPV-2a and CPV-2b isolate (CPV-2a isolate BE-1, NCBI GenBank accession number KJ364524; CPV-2b isolate PALAM1CPV2b/CAD/2010, NCBI GenBank accession number KX181847.1) were tested as positive controls, whereas a mock-infected A-72 cell culture supernatant, fecal swabs from healthy dogs showing no apparent clinical signs of canine parvoviral disease, and phosphate-buffered saline were used as negative controls.

The cross-reactivity of the IC test with other pathogens was tested using standard antigens from canine adenovirus 1 (CAV-1), canine distemper (CD) virus vaccine strain, *Salmonella* Typhimurium, *Clostridium perfringens* type A and *Leptospira canicola* (vaccine antigen) on test strips. The specific bacterial and viral agents were obtained from the institute repository. To determine the stability of the IC strips, assembled strips from the one batch were stored at 4 °C and tested repeatedly with known CPV-positive and negative samples every 15 days for a period of 3 months.

To determine the performance of IC test with clinical samples, 97 fecal swabs were tested simultaneously using the IC test, an HA test, and a commercial Rapid CPV Ag Test Kit (Bionote, Korea). The relative sensitivity and specificity of test were determined using Medcalc

epidemiological calculator software at a confidence level of 95%. Kappa statistics were used to determine the strength of the agreement of the results between the two tests.

Results

Expression of recombinant tVP2 protein and generation of anti-CPV-tVP2 rabbit pAbs

Optimal expression of both proteins was observed at 8 h post-induction using 1 mM IPTG at 37 °C. A fair level of purification was achieved for both 6xHis-tagged recombinant CPV-tVP2 proteins using Ni-NTA resin, as indicated by 12% SDS-PAGE analysis. The observed molecular weight was close to the predicted molecular weight of 51 kDa and 54 kDa for the N and C terminal protein, respectively, as indicated by Western blot analysis using CPV-positive sera from vaccinated animals (Fig. 1).

A dot-blot showed appreciable reactivity of rabbit anti-CPV-tVP2 polyclonal serum against the CPV-tVP2 protein and the A-72-adapted virus (Fig. 1). A fairly high concentration (2.5 mg/ml) of total IgG fraction was obtained by purification from the rabbit hyperimmune serum. The purity of the IgG was sufficiently high, as determined by SDS-PAGE analysis (data not shown).

Fig. 1 (A) Western blot image showing the reactivity of N- and C-region tVP2 proteins against a positive serum from a vaccinated dog. (B) Dot-blot showing the reactivity of PBS (1), CPV-tVP2 protein (2) and A-72-grown CPV (3) against rabbit anti-CPV-tVP2 polyclonal serum

Preparation of colloidal gold conjugate

Based on findings of UV-Vis absorbance and flocculation assays, it was observed that GNPs at pH 8.0 adsorbed with anti-CPV mAb ranging in concentration from 10 to 20 $\mu\text{g/ml}$ provided satisfactory conjugation (Fig. 2). Optimal coupling of mAbs on the GNP surface was observed in the form of an increase in the absorbance peak and the average diameter of the GNPs detected by UV-Vis measurement and DLS/particle size analysis, respectively. The UV-Vis measurement of GNPs before and after conjugation with mAbs indicated a marginal shift (5 nm) in the absorbance peak from its λ_{max} value (526 nm) (Fig. 3). Likewise, DLS findings revealed an increase in the average diameter of GNPs from 36.6 to 48.5 nm following mAb addition, suggestive of antibody coupling (Fig. 3). TEM imaging revealed that the GNPs coupled with mAb had halos around the gold particles due to the adsorption of antibodies (Fig. 3). Additionally, it was observed that the colloidal gold conjugate displayed immune reactivity to a standard CPV antigen (Fig. 3).

Evaluation of IC test performance in detection of clinical samples

The strip test was validated by testing fecal samples collected from pups suspected of CPV infection in comparison with the HA test and a commercial CPV Ag kit (Fig. 4). Out of a total of 97 fecal samples examined, 34, 41, 29 and 37 samples gave positive results in the HA test, the commercial CPV Ag test, and mAb-pAb- and mAb-mAb-based IC tests, respectively. The relative sensitivity/specificity of the new strip test based on mAb-pAb in comparison to HA and the commercial IC kit was recorded as 71%/92% and 71%/100%, respectively, with substantial agreement ($\kappa = 0.736\text{--}0.757$) (Table 2). However, the relative sensitivity and specificity of the new IC test based on mAb-mAb combination was 82%/87% (substantial agreement; $\kappa = 0.687$) and 90%/98% (almost perfect agreement; $\kappa = 0.892$) in relation to the HA and commercial strip test, respectively (Table 3). In addition, the results of IC test based on either combination (mAb or pAb as capture antibodies) and the commercial IC test were almost uniformly positive, with fecal samples showing HA titers greater than 256 (Table 4).

Discussion

Canine parvovirus is the number one cause of viral enteritis in dogs and is responsible for significant morbidity and mortality [17]. An accurate and rapid diagnosis of the virus at very early stages of infection is pivotal in controlling the disease. The SNAP Parvo Test (Idexx, USA) is used by clinicians worldwide as an in-house test for rapid detection of

Fig. 2 (A) Determination of optimum pH for producing a stable gold conjugate. The image shows the SI and PI values of the colloidal gold conjugate at different pH values after addition of 10% NaCl. The colloidal GNPs were most stable and least polydisperse at pH 8.0. (B) Determination of the optimum concentration of mAbs for coupling of GNPs depicted by a curve showing the absorbance at 580 nm vs. the mAb concentration (SI). The image shows that the stability of the gold particles increased with increasing amounts of anti-CPV mAbs and remained constant after 20 $\mu\text{g/ml}$. Hence, the optimal amount of mAbs required to stabilize the GNPs against 10% NaCl is 20 $\mu\text{g/ml}$. (C) Determination of the optimum pH and antibody concentration using a flocculation assay, i.e. visual recording of any color change in GNPs from red to blue/violet after addition of 10% NaCl. The image reveals that a pH range of 7.5–8.5 and an mAb concentration of 10–30 $\mu\text{g/ml}$ may be sufficient for stability of the conjugate. Thus, the optimum pH and mAb concentration were chosen as 8.0 and 20 $\mu\text{g/ml}$, respectively

Fig. 3 (A) UV/Vis spectra of colloidal GNPs and the anti-CPV mAb-colloidal GNP conjugate, showing an increase in the absorbance wavelength of GNPs (526 to 531 nm) after mAb coupling. Blue line, colloidal gold solution; red line, gold-mAb conjugate. (B) DLS spectrum of (1) colloidal GNPs and (2) anti-CPV mAb-gold conjugate visible in the form of an increase in the average diameter of

GNPs from 36.6 to 48.5 nm after mAb coupling. (C) TEM image of (1) colloidal GNPs and (2) anti CPV-mAb-gold conjugate visible in the form of a halo around gold particles, indicating the adsorption of mAbs on the GNPs. (D) Dot-blot showing the reactivity of prepared mAb-gold conjugate against (1) cell-culture adapted CPV and (2) commercial CPV vaccine antigen

Fig. 4 Images of IC test showing (A) no reactivity with either PBS or mock-infected DMEM medium, (B) positivity in the form of the appearance of two visible red color bands at the test and control lines, detected by employing mAb/pAb and (C) mAb/mAb at the test and control line in prototype IC tests. (SP, sample pad; CP, conjugate pad; AP, absorbent pad; T, test line C, control line)

Table 2 Determination of the relative sensitivity and specificity of the new prototype strip test (mAbs/pAbs) in comparison to HA and commercial antigen kit

Prototype strip test (pAb as capture antibodies) vs HA test	HA test		Total	Prototype strip test (pAb as capture antibodies) vs commercial kit	Commercial kit		Total
	+	–			+	–	
Prototype strip test				Prototype strip test			
+	24	05	29	+	29	0	29
–	10	58	68	–	12	56	68
Total	34	63	n = 97	Total	41	56	n = 97
Sensitivity = 71% (95% CI: 52.52–84.90%)				Sensitivity = 71% (95%CI: 54.46–83.87%)			
Specificity = 92% (95%CI: 82.44–97.37%)				Specificity = 100% (95%CI: 93.62–100.00%)			
Kappa value = 0.757 (substantial agreement)				Kappa value = 0.736 (Substantial agreement)			

Table 3 Determination of the relative sensitivity and specificity of the new prototype strip test (mAb/mAb) in comparison to HA and commercial antigen kit

Prototype strip test (mAb as capture antibodies) vs HA test	HA test		Total	Prototype strip test (mAb as capture antibodies) vs commercial kit	Commercial kit		Total
	+	–			+	–	
Prototype strip test				Prototype strip test			
+	28	08	36	+	36	01	37
–	06	55	61	–	04	56	60
Total	34	63	n = 97	Total	40	57	n = 97
Sensitivity = 82% (95% CI: 65.47%–93.24%)				Sensitivity = 90% (95%CI: 76.34%–97.21%)			
Specificity = 87% (95% CI: 76.50%–94.35%)				Specificity = 98% (95%CI: 90.61%–99.96%)			
Kappa value = 0.687 (Substantial agreement)				Kappa value = 0.892 (Almost perfect agreement)			

Table 4 Number of fecal samples screened by prototype and commercial IC test displaying positive results with their respective HA titers

HA Titer	Prototype strip test (mAb/pAb)	Prototype strip test (mAb/mAb)	Commercial Rapid CPV Ag kit
<32	5	8	12
32	2	2	5
64	0	2	2
128	1	2	2
256	3	3	3
≥512	18	20	17

canine parvovirus. This is a fecal CPV antigen test based on enzyme-linked immunosorbent assay (ELISA) technology [18]. Although it is very specific, its sensitivity has been reported to be widely variable, from as low as 18.4% [19] to as high as 81.8% [20]. With the development of colloidal-gold-based rapid IC assays, testing of samples under field conditions with a fair level of confidence is now possible. However, because of the high cost, the diagnosis of CPV infection using existing IC tests is not affordable, especially in developing countries like India, for testing a large population of dogs. In the existing setting, two mAbs (as detector and capture antibodies) targeting different epitopes of CPV are required for high sensitivity of the IC assays, which

also increases the cost per test [19, 21]. However, antibody-induced conformational changes of epitopes might also limit the sensitivity of IC tests utilizing two heterologous mAbs as capture and detector antibodies [12]. Use of the same mAb as both the capture and detector antibody in the sandwich format can potentially reduce the cost but simultaneously may decrease the sensitivity of the IC assay.

It is known that in comparison to mAbs, pAbs are less expensive to generate (one-fifth the cost of mAbs) and can be produced much more rapidly (the turnaround time is less than half of that for mAbs) with little technical skill [22]. Thus, it was hypothesized that inclusion of pAbs, which is more economical and can detect multiple epitopes simultaneously, may replace at least one mAb in the sandwich format of an IC test and thereby reduce the overall cost. As preparation of a colloid gold conjugate employing pAbs for use as the detector is not desirable because of their heterogeneity, in the present work, a commercial anti-CPV mAb was used for conjugate preparation, and rabbit anti-CPV-tVP2 pAbs were employed to coat the test line. One existing commercial IC kit for rapid detection of canine parvovirus (Witness Parvo; Synbiotic, USA) also uses a CPV-specific mAb for detection and a pAb for capture. There are also several published reports indicating the successful use of pAbs as capture antibodies in IC assays [23].

In most IC assays, the analyte (pathogen) is detected based on the accumulation of GNPs at the immobilized

capture antibody site using sandwich-type immunoreactions [24, 25]. The key factors influencing the analyte detection limit or sensitivity of the sandwich IC assay include the size of the GNPs and the conjugation procedure, which mainly includes buffer pH and antibody concentration.

The available literature generally supports the use of GNPs in the range of 20–40 nm for preparation of the conjugate for IC tests [24, 26]. In the present work, a conjugate prepared with 30-nm GNPs displayed sufficient stability and immune reactivity towards the CPV antigen (Fig. 3). The degree of stabilization of colloidal gold conjugate is directly proportional to the SI and inversely proportional to the PI [15]. The ideal pH and mAb concentration required for proper coverage of GNPs were determined on the basis of SI and PI values and further confirmed by flocculation assay, which indicated that a pH ranging from 7.5 to 8.5 (average, 8.0) with an mAb concentration of 10–30 µg/ml was sufficient to prevent a color change from red to violet following addition of 10% NaCl (Fig. 2). From the flocculation experiment, the minimum protective amount (MPA) of mAb required to prevent the color change in GNPs from red to blue/violet was found to be 10 µg/ml (Fig. 2); however, the optimum amount of antibody needed for proper coverage of the GNP surface was determined on the basis of the stability index, which corresponds to 20 µg/ml (Fig. 2). This is in agreement with previous reports in which it was recommended to use a twofold excess of antibody for proper coverage of the GNP surface [24].

The optimal coverage of GNPs was also ensured by using several established methods, which revealed an increase in wavelength of the absorbance peak (526 to 531 nm) and the average diameter of GNPs (36.6 to 48.5 nm) as well as the appearance of a halo effect in TEM images after addition of mAbs (Fig. 3). This is suggestive of antibody coupling on GNPs and consistent with an earlier report [16].

Truncated recombinant proteins have been shown to be applicable for use in diagnosis of many infections [27, 28]. Therefore, in the current study, we used two CPV-tVP2 proteins covering almost the full length of the VP2 capsid protein of CPV as a source of antigen to raise rabbit pAbs, and to the best of our knowledge, this is the first IC assay in which CPV-tVP2-specific pAbs are used as capture antibodies for detection of CPV. The VP2 capsid protein contains most of the immunogenic epitopes near the N-terminal region [29]. However, to cover an almost full-length VP2 gene, two almost equal fragments (N = 760 bp and C = 891 bp) were selected for ease of expression.

The minimum detection limit recorded with the newly developed mAb/pAb-based prototype IC assay was 6.6×10^5 TCID₅₀/ml, a level that is marginally higher than the value (3.13×10^5 TCID₅₀/ml) reported for the commercial IC based kit to detect CPV in fecal samples. This could be acceptable, considering its economical benefit in addition

to its ability to detect CPV, especially at early stages of disease when viral loads are typically high ($>10^8$ CCID₅₀). The CPV standard and its antigenic variants (CPV-2a and CPV2b) gave positive results within 10 min with the new IC test, while other canine enteric pathogens tested in present study gave negative results, indicating the specificity of the strip test. The IC test results were reproducible when testing positive and negative specimens after up to 3 months of storage at 4 °C, which is consistent with an earlier report in which antibody colloidal gold conjugate was reported to be stable for at least 2 months at 4 °C [30]. Previous studies have already shown that in-clinic IC tests rarely detect the attenuated parvovirus vaccine strain, due to the very low level of vaccine virus shed in the feces, providing the user a level of confidence that a positive test result with these tests always indicates the presence of wild-type pathogenic virus regardless of recent vaccination [31]. However, these in-clinic tests, including our newly developed one, do not differentiate between the wild and vaccine strains of CPV-2.

Because there is no gold standard assay to detect CPV in fecal samples, the prototype IC test was compared separately with the HA test and a commercial CPV antigen kit using a panel of 97 clinical samples from animals suspected of having a CPV infection (Fig. 4). The relative sensitivity/specificity of the mAb/pAb-based strip test in comparison to the HA and commercial IC kit was 71%/92% and 71%/100%, respectively. This is in accordance with earlier findings which revealed that HA test is slightly more sensitive but less specific than IC tests [9]. Similar findings have also been reported for a commercial IC kit (Witness Parvo; Synbiotic, USA), where the relative sensitivity and specificity in comparison to the HA test was 63% and 93%, respectively [32]. The lower sensitivity observed with prototype IC test may be due to the nonspecific hemagglutination in fecal samples with HA titers up to 512. It is not essential for the IC test to be more sensitive than the HA test, as both of these field-based tests have their distinct merits.

Interestingly, with use of pAb as capture antibodies, a very high level of specificity was observed in comparison to the HA and commercially available kit. This finding is supported by a previous report that indicated that pAbs frequently have better specificity than mAbs because they are produced by a large number of B cell clones, each generating antibodies to a specific epitope [22]. There was substantial agreement ($\kappa = 0.736$ – 0.757) observed between the new IC test and the HA and commercial kit results (Table 2). Hence, the above results confirmed that the mAb/pAb-based IC test has similar specificity but lower sensitivity than the HA and commercial kits (Table 2). It was also demonstrated that pAb reactive with CPV can be produced economically by using recombinant truncated structural proteins. However, as reported by Turiso et al. [29], the use of recombinant proteins in their native form

can generate antibodies with high affinity, which will be, evaluated in future studies.

Comparing the results obtained with the mAb/mAb-based prototype strip test in relation to the HA test revealed high sensitivity (82%) and moderate specificity (87%), with substantial agreement and high sensitivity/specificity (90/98%) (almost perfect agreement) in relation to the commercial kit (Table 3). The use of two different anti-CPV mAbs as detector and capture antibodies in new prototype strip test gave almost identical results (minimum detection limit, 3.12×10^5 TCID₅₀/ml) in relation to the commercial CPV antigen kit (3.13×10^5 TCID₅₀/ml). Additionally, it appeared that a high viral load (HA titer ≥ 256) in clinical samples was needed to capture the gold-mAb-CPV complexes, which is evident from the correlation between HA titers with IC positivity and is consistent with earlier findings [32] (Table 4).

The present study provides an important proof of concept for development of an economical mAb/pAb-based IC test for on-site diagnosis of parvoviral enteritis in dogs with very high specificity. An mAb/mAb-based variation of this assay showed very high sensitivity and comparable specificity. The availability of both the assays will provide flexibility to choose either high sensitivity or specificity as required. This prototype test (mAb/pAb) may present the new choices for CPV diagnosis, considering its economical benefit and high specificity. Consequently, in cases where the IC result is negative but the index of suspicion is high, it is recommended to send the sample for further laboratory examination using highly sensitive molecular assays. Given the ongoing need for a simple, and economical point-of-care test for CPV diagnosis, it is warranted to screen a larger number of clinical samples using this prototype test for further validation.

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Compliance with ethical standards

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Conflict of interest The authors declare no conflict of interest.

Ethical approval All applicable guidelines for the care and use of animals were followed (Institutional Animal Ethical Committee approval Lr. no. (F.1-53/2012-13-J.D.Res dated 05.10.2013). The consent of the animal owners was sought for collecting rectal swabs from dogs.

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