

Radiation dose of cardiac computed tomography – what has been achieved and what needs to be done

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Abstract This review highlights the recently introduced techniques by manufacturers and various research workers to reduce radiation dose in coronary CT. It discusses in detail the development of ECG-based tube current modulation, the application of low tube voltage protocols and prospective ECG-gating. It also briefly discusses two further methods of dose reduction, namely minimisation of the x-y anatomical coverage and adaptive statistical iterative reconstruction.

Introduction

In the October issue of *European Radiology* in 2009, Ertel and colleagues [1] described a spiral computed tomography (CT) technique employing a very high table feed (and pitch) for a fast data acquisition of the heart. The authors performed experiments in three pigs using a first-generation dual-source CT machine equipped with prototype software allowing pitch factors up to 3.0. The high-pitch mode delivered good image quality of the pig hearts, similar to that obtained from a standard spiral low-pitch data acquisition technique. Most importantly, the corresponding effective radiation dose of a high-pitch cardiac CT study in their first experiments was only 2.0 mSv.

In the November issue of *European Radiology* in 2009, Lell and colleagues [2] could extend these initial results to a first feasibility study employing the high-pitch mode in a series of 25 patients and using a second-generation dual-source CT machine. Data were acquired synchronized to the electrocardiogram (ECG), and starting at 60% of the R-R interval with a pitch of 3.2 or 3.4.

Again, image quality of the heart and coronary arteries using the high-pitch mode was good to excellent, along with a very small rate of segments having a non-diagnostic image quality. Importantly, the average estimated effective radiation dose of the high-pitch mode was 0.88 mSv and 1.0 mSv, depending on the protocol used.

These two studies nicely illustrate the most recent achievement in radiation dose lowering algorithms, enabling a cardiac CT study for the non-invasive evaluation of the coronary arteries with a radiation dose of around (or even below) 1 mSv. Confirmation of these results was published thereafter in a number of studies [3, 4], also demonstrating the high diagnostic performance of the high-pitch mode for coronary imaging when compared to the reference standard modality catheter coronary angiography [5, 6]. In this editorial, we want to briefly summarize and highlight the most amazing achievements that were made over the last few years in regard to the radiation dose of cardiac CT, resulting in a tremendous reduction in radiation exposure to the patients undergoing this non-invasive imaging test.

Summary of radiation dose reducing techniques

The recent years showed an overall increase in the use of CT for imaging of the heart and coronary arteries. For example in the United States, around 2.3 million CT

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coronary angiography examinations are currently performed annually [7]. The downside of this increased use of the radiation-associated cardiac imaging test is the increase in the collective radiation dose, which might pose a risk to the population [8]. It is obvious that the strategy to lower the overall radiation burden to the population must be twofold: First, the radiation dose of the individual CT study should be lowered to a level that is as low as reasonably achievable; and second, the total number of CT studies must be controlled by strict adherence to common guidelines and recommendations.

With ECG-gated cardiac CT, radiation dose is closely related to the table feet, or pitch value. The pitch for spiral CT coronary angiography studies as e.g. employed with 64-slice CT machines is typically low, ranging from 0.2 to 0.5. This indicates that the table is advanced by less than one detector width during each gantry rotation. Thus, this technique exposes the same anatomic area to X-ray radiation during consecutive rotations of the gantry, which results in a relatively high radiation dose. With retrospectively ECG-gated cardiac single-source 64-slice CT, radiation dose values of up to 21 mSv have been reported for coronary imaging [9], while average effective doses of this technique are in the range of 15 mSv [8, 10–12] (Fig. 1).

ECG-based tube current modulation

An important approach for lowering the dose of retrospectively ECG-gated cardiac CT is ECG-based tube current modulation. With this technique, the tube current outside the diastole is lowered to 25% of the nominal value. Thus, the effective radiation dose of retrospectively ECG-gated CT coronary angiography can be considerably lowered, with a drop of effective dose to around 10 mSv [10–14] (see Fig. 1).

Another approach for radiation dose reduction with retrospective ECG-gating is *MinDose* (Siemens Healthcare), representing a technique that lowers the tube current outside the diastole to only 4% of the nominal value [15]. With this algorithm, which is particularly efficient at lower heart rates, the radiation dose of a CT coronary angiography study can be further lowered down to around 8 mSv (see Fig. 1).

Low tube voltage

The next step in reducing radiation dose of CT coronary angiography was the application of low tube voltage protocols [16, 17]. Lowering the tube voltage represents an important radiation dose reduction approach because the radiation dose varies with the square of the tube voltage [18]. Lowering the tube voltage has the additional advantage of the higher attenuation levels for iodinated contrast

medium as a result of a greater photoelectric effect and decreased Compton scattering [16]. This effect can be also used for lowering the contrast medium volume while obtaining the same attenuation within the vessels. With reduction of the tube voltage from the standard 120 kV to 100 kV (Fig. 2a), another lowering of the average effective radiation dose of retrospectively ECG-gated cardiac CT with ECG-controlled tube current modulation to around 6.5 mSv was achieved [16, 17] (see Fig. 1). It must be noted, however, that lowering of the tube voltage should be done according to the body physiognomy of the patient (e. g. only in patients with a body mass index below 25 kg/m² [16]).

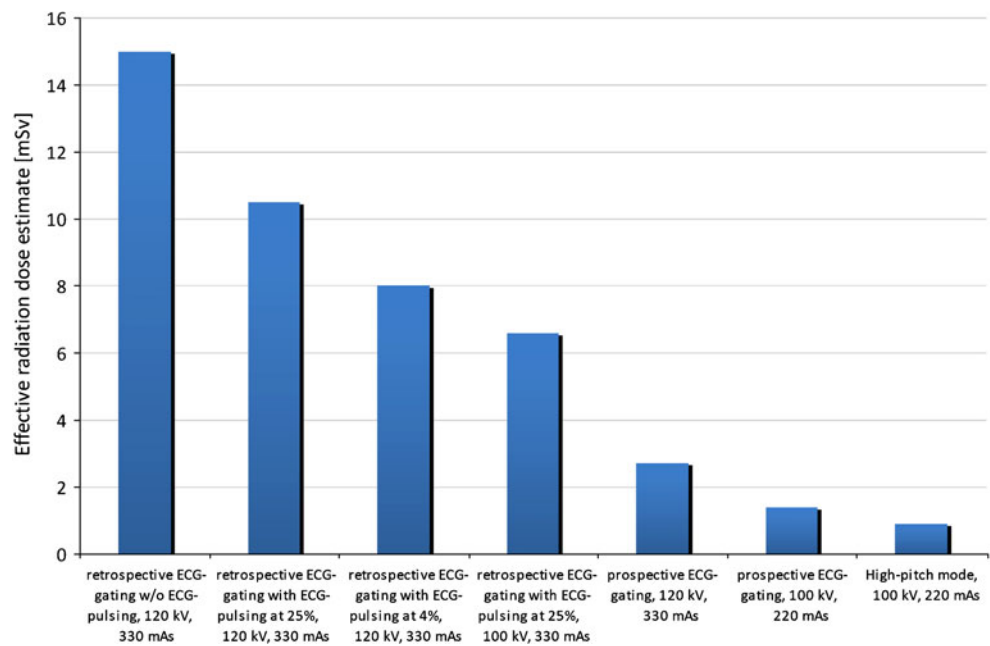
Prospective ECG-gating

The next quantum leap in radiation dose reduction of cardiac CT was the reintroduction of prospective ECG-gating, or the step-and-shoot mode. Prospective ECG-gating is characterized by turning on the X-ray tube only at a predefined time point of the cardiac cycle, usually in diastole, while keeping the patient table stationary. The X-ray exposure time of this technique is short, and thus, low radiation doses ranging between 1.5 to 4 mSv have been reported with this technique, depending on the use of a standard 120 kV or a low tube voltage protocol at 100 kV [19] (see Fig. 1). Importantly, this radiation dose saving technique can be reliably and accurately employed with various CT machines, including single-source and dual-source CT scanners, as well as broader detector systems with 256- or 320-slices [20–24] (Fig. 2b). With this approach, cardiac CT can be even used for the accurate diagnosis of congenital heart disease in infants and children [25]. Of note, however, is the requirement of a stable sinus rhythm with a relatively low heart rate (i.e., below 65 or 70 bpm) for being eligible for this technique.

ECG-gated high-pitch mode

One of the most recent advents in radiation dose saving algorithms for cardiac CT is – as discussed already above [1, 2] – the ECG-gated high-pitch mode (Fig. 2c). With this mode, data is acquired in a spiral mode while the table runs with a high pitch of maximally 3.4, equaling a table feed of 46 cm/s. When using the high-pitch mode, the entire heart can be scanned within one single cardiac cycle, usually during diastole. The effective radiation dose of the high-pitch mode for a cardiac CT study is as low as 1 mSv [3–6] (see Fig. 1), and around 2 to 4 mSv for an ECG-gated CT angiography study of the entire chest [3, 26]. This can be explained by the fact that using high-pitch imaging, ‘superfluous’ X-rays exposing the entire width of the detector as it enters and leaves the entire arc of projections

Fig. 1 Bar graph illustrating the average effective radiation doses of cardiac CT applying the various radiation dose reducing algorithms



are applied only once at the beginning and end of the spiral path [1, 2, 6]. With prospective ECG-gating (or step-and-shoot mode), such ‘superfluous’ exposure occurs for each acquired slice, which explains the further reduction of radiation dose to the patient with the high-pitch mode. Again, it must be noted, that a stable sinus rhythm with a relatively low heart rate (i.e., below 63 bpm) is required for being eligible for this technique.

Additional means to lower the radiation dose

Various additional means exist to further lower the radiation dose of cardiac CT. Among these, limiting the cranio-

caudal coverage length, use of bowtie filters, and statistical iterative reconstruction algorithms will be highlighted in this brief review. Of note, these radiation reducing approaches can be used in addition to the dose-saving algorithms outlined above, which will result in additional lowering of the radiation burden to the patient.

The region undergoing radiation exposure in the cranio-caudal is the largest contributor to radiation absorption. The CT scout (or topogram) is quite inaccurate for determining the precise extent of the coronary arteries. An alternative is to use images from the coronary calcium scoring to set the upper limit above the apex of the left anterior descending artery and the lower limit inferior to the posterior descend-

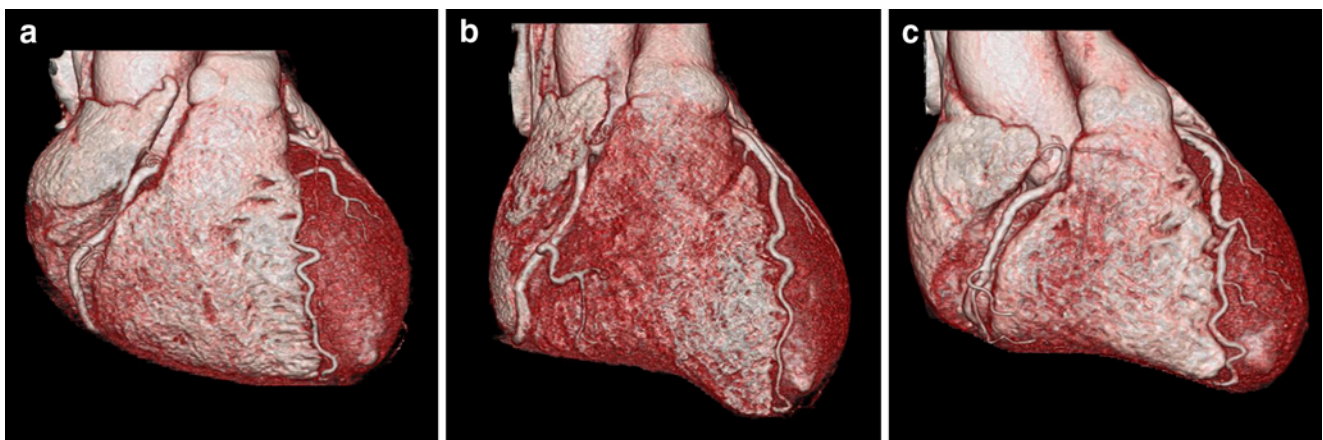


Fig. 2 Examples of image quality and radiation exposure with different cardiac CT protocols. (a) 65-year-old woman with a BMI of 22.1 kg/m² and a heart rate of 81 bpm. CT was performed using retrospective ECG-gating with ECG-pulsing at a full tube current window from 30–80% of the R-R interval and a tube voltage of 100 kV. Radiation dose estimate was 6.2 mSv. (b) 55-year-old man

with a BMI of 28.0 kg/m² and a heart rate of 70 bpm. CT was performed using prospective ECG-gating and a tube voltage of 120 kV. Radiation dose estimate was 2.5 mSv. (c) 51-year-old man with a BMI of 23.9 kg/m² and a heart rate of 61 bpm. CT was performed using a high-pitch CT protocol at a tube voltage of 100 kV. Radiation dose estimate was 1 mSv

ing artery, leaving sufficient margins to allow for movement [27]. This simple approach helps to further reduce the radiation dose by about 16% [28].

Another technique that might be underused is to restrict the x-y field of view. Bowtie filters allow for smaller radiation exposure by limiting the scatter of the X-ray towards the detectors. Thus, bowtie filters allow less X-rays out of the central part of the X-ray tube, as less are required to expose the detectors. Use of bowtie filters have potential to reduce the radiation exposure to the patient by up to 40% [27].

Statistical iterative reconstruction algorithms are an alternative to the classic reconstruction technique of CT, i. e., filtered back projection. This technique incorporates statistical modelling to reduce image noise, which may permit preserved image quality with reduced tube current, thereby permitting lower radiation dose. As a matter of fact, first experience with statistical iterative reconstruction for coronary artery imaging has shown a 44% reduction in the median radiation dose when compared to CT protocols using filtered back projection for image reconstruction [29].

Outlook and conclusion

This brief overview was intended to demonstrate and highlight the many steps that were undertaken in the past years for lowering the radiation exposure to patients undergoing cardiac CT. Employing these techniques, the effective radiation dose of a CT coronary angiography study can be reduced from around 15 to as low as 1 mSv in selected patients. It is important to note that the current effective radiation doses from cardiac CT are at the level or even below those reported for the reference standard modality catheter coronary angiography. In addition, it is also lower than that of a standard chest or abdominal CT study. Thus, the achievements in radiation dose reduction in cardiac CT must be considered tremendous, and similar success stories in radiation dose lowering techniques for CT of other body regions are still be awaited.

Nevertheless, still a number of issues and problems need to be addressed and solved in the near future. Considerable problems continue to be present for the CT imaging of coronary artery stents. While CT stent imaging can be now performed – similar to the imaging of the native coronary arteries – at a low radiation dose, the in-stent visualization still is limited [30, 31], and a routine application of CT for the follow-up of coronary stent patency cannot be recommended so far.

Another important issues is the question on how we will assure that all these radiation dose lowering protocols for cardiac CT are used by the increasingly large radiological community performing cardiac imaging. In parallel, cardiac

imagers must strictly adhere to the appropriate indications for cardiac CT. For example, use of this modality in asymptomatic subjects for screening purposes (as part of so-called check-up examinations) should be disallowed. Otherwise, all our efforts to lower the radiation dose of individual CT studies will be thwarted by an increasing total number of imaging tests. When the latter cannot be prevented, the collective radiation dose to the population undergoing X-ray-based cardiac imaging might continue to increase even further.

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