

NARRATIVE REVIEW



# Clinical targeting of the cerebral oxygen cascade to improve brain oxygenation in patients with hypoxic–ischaemic brain injury after cardiac arrest

Ryan L. Hoiland<sup>1,2,3,4,5\*</sup> , Chiara Robba<sup>6,7</sup>, David K. Menon<sup>8</sup>, Giuseppe Citerio<sup>9</sup>, Claudio Sandroni<sup>10</sup> and Mypinder S. Sekhon<sup>1,4,5,11</sup>

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## Abstract

The cerebral oxygen cascade includes three key stages: (a) convective oxygen delivery representing the bulk flow of oxygen to the cerebral vascular bed; (b) diffusion of oxygen from the blood into brain tissue; and (c) cellular utilisation of oxygen for aerobic metabolism. All three stages may become dysfunctional after resuscitation from cardiac arrest and contribute to hypoxic–ischaemic brain injury (HIBI). Improving convective cerebral oxygen delivery by optimising cerebral blood flow has been widely investigated as a strategy to mitigate HIBI. However, clinical trials aimed at optimising convective oxygen delivery have yielded neutral results. Advances in the understanding of HIBI pathophysiology suggest that impairments in the stages of the oxygen cascade pertaining to oxygen diffusion and cellular utilisation of oxygen should also be considered in identifying therapeutic strategies for the clinical management of HIBI patients. Culprit mechanisms for these impairments may include a widening of the diffusion barrier due to perivascular oedema and mitochondrial dysfunction. An integrated approach encompassing both intra-parenchymal and non-invasive neuromonitoring techniques may aid in detecting pathophysiologic changes in the oxygen cascade and enable patient-specific management aimed at reducing the severity of HIBI.

**Keywords:** Hypoxic–ischaemic brain injury, Cardiac arrest, Cerebral blood flow, Neuromonitoring, Brain tissue oxygenation, Cerebral oxygen delivery, Oxygen cascade

## Introduction

In patients resuscitated from cardiac arrest, hypoxic–ischaemic brain injury (HIBI) is the primary cause of mortality [1, 2] and is associated with significant disability in survivors [1]. The pathophysiology of HIBI includes three phases: (1) global brain ischaemia occurring in the

interval between circulatory arrest and the start of cardiopulmonary resuscitation (CPR) (no-flow); (2) global brain hypoperfusion occurring during CPR (low-flow); and (3) brain reperfusion after the return of spontaneous circulation (ROSC) [2]. A significant degree of HIBI occurs as a secondary injury after ROSC and part of this injury is associated with brain tissue hypoxia [3].

Observational studies have demonstrated a relationship between reductions in cerebral oxygen delivery (CDO<sub>2</sub>) due to arterial hypotension [4], anaemia [5], and hypocapnia [6] with adverse neurologic outcome following resuscitation. As such, significant focus has been placed on the post-resuscitation optimisation of CDO<sub>2</sub>

\*Correspondence: ryanleohiland@gmail.com

<sup>1</sup> Division of Critical Care Medicine, Department of Medicine, Faculty of Medicine, Vancouver General Hospital, University of British Columbia, Vancouver, BC, Canada

Full author information is available at the end of the article

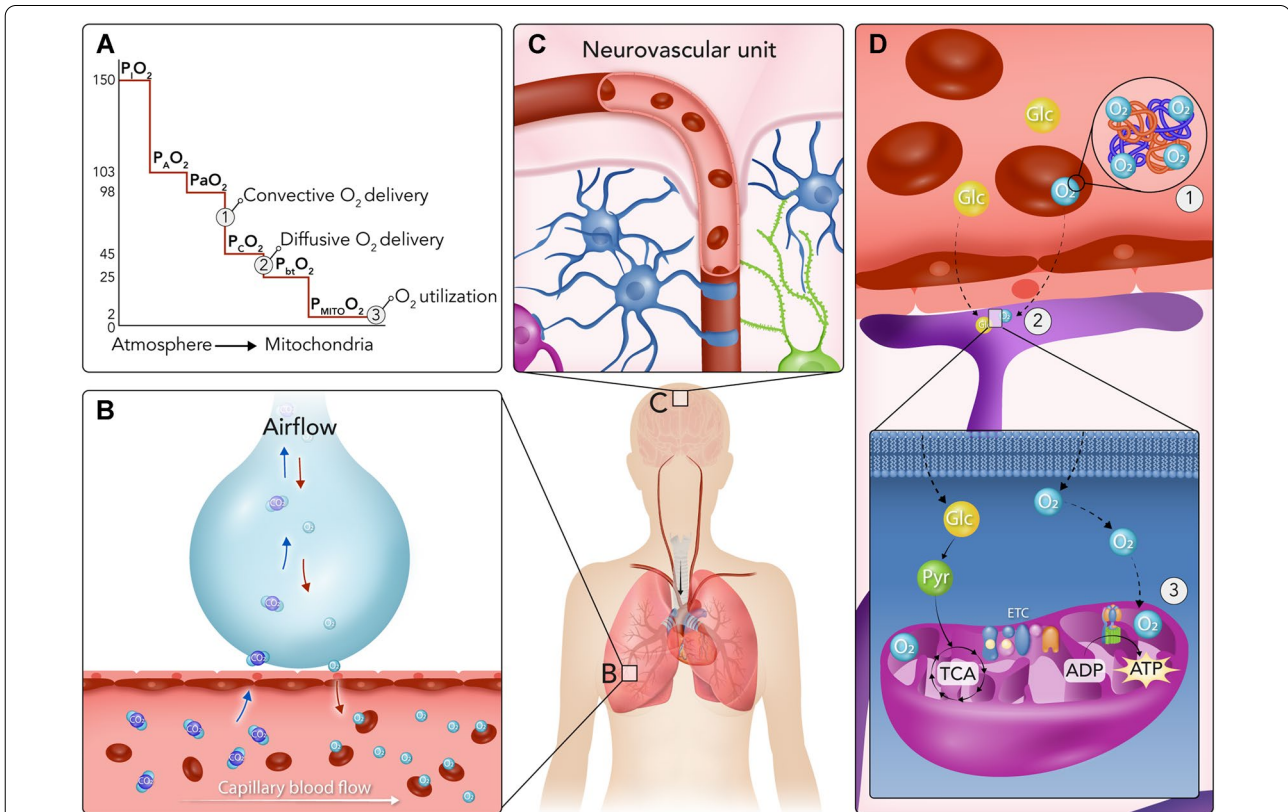
Claudio Sandroni and Mypinder S. Sekhon are co-last authors.

[2], although the mechanisms by which brain tissue hypoxia may persist after ROSC appear to be more complex [3].

The oxygen cascade encompasses oxygen transport from the atmosphere to mitochondria (Fig. 1). It requires integrating cardiorespiratory, microcirculatory, and cellular systems, and involves three key stages: (1) convective oxygen delivery, (2) diffusion of oxygen, and (3) cellular utilisation of oxygen. The lack of improved neurologic outcomes in HIBI trials attempting to optimise post-resuscitation CDO<sub>2</sub> [7–15] (Table 1) may be explained by

### Take-home message

The successful treatment of hypoxic–ischaemic brain injury will likely require a multi-pronged approach that aims to resolve dysfunction within each step of the oxygen cascade, including convective oxygen delivery, oxygen diffusion, and oxygen utilisation. Further, the timing of interventions after resuscitation from cardiac arrest and patient-specific pathophysiology must be considered in future studies.



**Fig. 1** The oxygen cascade and oxygen delivery to the brain. **A** The oxygen cascade is a multi-step process involving the movement of oxygen from the atmosphere to the mitochondria. Oxygen transport depends upon both convective and diffusive oxygen delivery along the oxygen cascade and subsequent utilisation by the mitochondria. **B** Air is drawn into the lungs, where the partial pressure of inspired oxygen (P<sub>I</sub>O<sub>2</sub>) is ~150 mmHg. Subsequent mixing with residual volume renders an alveolar partial pressure of oxygen (P<sub>A</sub>O<sub>2</sub>) of ~103 mmHg, where at the alveolar–capillary junction oxygen then diffuses from the alveoli to the blood whilst carbon dioxide diffuses from the blood to the alveoli. This diffusion process is associated with a slight reduction in the partial pressure of arterial oxygen (P<sub>a</sub>O<sub>2</sub>) to approximately 98 mmHg. Thereafter, blood is pumped to the body by the heart. Importantly, cardiovascular (e.g., MAP), respiratory (e.g., PaO<sub>2</sub>/PaCO<sub>2</sub>), humoral (e.g., haemoglobin concentration, [Hb]), and microcirculatory (e.g., cerebrovascular resistance) factors influence CBF, which is determined by the integration of these physiologic factors and more [16]. Panel **C** depicts the neurovascular unit which is the anatomical and functional integration of cerebral microvasculature, perivascular glial cells and neurons, which ultimately maintains homeostasis in the brain parenchyma. **D** Convective oxygen delivery, denoted as (1), is determined by arterial oxygen content (CaO<sub>2</sub>) and cerebral blood flow (CBF). (2) Following oxygen delivery to the cerebral capillary network, where the partial pressure of capillary oxygen (P<sub>c</sub>O<sub>2</sub>) approximates 45 mmHg, oxygen diffusion from the cerebral vasculature to the cerebral parenchyma occurs. This diffusion process is determined by factors including the surface area for diffusion (A), the thickness of the diffusion barrier (T), and the pressure gradient for diffusion (ΔP<sub>O<sub>2</sub></sub>), and results in a brain tissue partial pressure of oxygen (P<sub>bt</sub>O<sub>2</sub>) that is typically greater than 20 mmHg. Oxygen must then traverse the cytoplasm to reach the mitochondria, where the partial pressure of mitochondrial oxygen (P<sub>MITO</sub>O<sub>2</sub>) is 2–3 mmHg (estimation based upon measures of myoglobin saturation) [17]. (3) Finally, energetic homeostasis requires successfully utilising oxygen through aerobic mitochondrial respiration and generating adenosine triphosphate (ATP)

**Table 1 Randomised-controlled trials manipulating physiologic parameters contributing to convective cerebral oxygen delivery**

Citation	n	Population	Low target	High target	Duration	CPC 1-2 or GOSE $\geq$ 5-8 (low vs. high)	Brain biomarkers (low vs. high)	Other (low vs. high)
<b>Mean arterial pressure</b>								
Jakkula et al. [11]	120	Witnessed OHCA Shockable rhythm	65-75 mmHg	80-100 mmHg	36 h from ICU admission or until extubation	6 months post-arrest (62 vs 68%; $P=0.4444$ )	NSE @48 h post-arrest (20.6 vs 22.0 $\mu\text{g/L}$ ; $P=0.522$ )	NA
Ameloot et al. [8]	107	OHCA Any rhythm	65 mmHg	85-100 mmHg	36 h from ICU admission	180 days post-arrest (43 vs 27%; $P=0.15$ )	NSE @48 h post-arrest (42 vs 59 $\mu\text{g/L}$ ; $P=0.69$ )	MRI voxels with ADC $< 650.10^{-6}$ $\text{mm}^2/\text{s}$ (12 vs 16%; $P=0.09$ )
Grand et al. [9]	49	OHCA Any rhythm	65 mmHg	72 mmHg	ICU admission onwards	180 days post-arrest (50 vs 43%; $P=0.65$ )	NSE @48 h (20 vs 18 $\mu\text{g/L}$ ; $P=0.79$ )	Thrombomodulin @48 h (8.2 vs 8.3 ng/mL; $P=0.61$ )
Kjaergaard et al. [7]	789	OHCA Any rhythm	63 mmHg	77 mmHg	ICU admission onwards	90 days post-arrest (68 vs 66%; $P=0.56$ )	NSE @48 h (18 vs 18 $\mu\text{g/L}$ ; $P=$ not specified)	NA
<b>Arterial carbon dioxide tension</b>								
Eastwood et al. [56]	1700	OHCA	35-45 mmHg	50-55 mmHg	24 h from hospital admission	6 months post-arrest (43.5 vs. 44.6%; $P=0.76$ )	NA	NA
Eastwood et al. [10]	83	IHCA/OHCA Any rhythm	35-45 mmHg	50-55 mmHg	24 h from ICU admission	6 months post-arrest (46 vs 59%; $P=0.26$ )	No statistical test per- formed on 48 h NSE data	NA
Jakkula et al. [11]	120	Witnessed OHCA Shockable rhythm	34-36 mmHg	44-46 mmHg	36 h from ICU admission or until extubation	6 months post-arrest (71 vs 59%; $P=0.20$ )	NSE @48 h (18.8 vs 22.5 $\mu\text{g/L}$ ; $P=0.40$ )	NA
<b>Arterial oxygen tension and peripheral pulse oximetry</b>								
Jakkula et al. [11]	120	Witnessed OHCA Shockable rhythm	75-113 mmHg	150-188 mmHg	36 h from ICU admission or until extubation	6 months post-arrest (69 vs 61%; $P=0.368$ )	NSE @48 h (22.4 vs 20.6 $\mu\text{g/L}$ ; $P=0.649$ )	NA
Young et al. [15]*	166	IHCA/OHCA Any rhythm	$\text{SpO}_2 < 97$	No specific limit	Admission to discharge or 28 days post randomi- sation	180 days post-arrest (44.9 vs 31.9%; $P=0.15$ )	NA	NA
Schmidt et al. [12]	789	OHCA Any rhythm	68-75 mmHg	98-105 mmHg	ICU admission onwards	90 days post-arrest (68 vs 66.1%; $P=0.69$ )	NSE @48 h post-arrest (17 vs 18 $\mu\text{g/L}$ ; $P=$ not specified)	NA
Bernard et al. [13]	425	OHCA Any rhythm	$\text{SpO}_2$ 90-94	$\text{SpO}_2$ 98-100	Until arrival to ICU (ended after first arterial blood gas)	Hospital discharge (36.6 vs 41.9%; $P=0.27$ )	NA	Survival to hospital discharge (38.3 vs 47.9%; $P=0.05$ )

ADC apparent diffusion coefficient, CPC cerebral performance category, GOSE Glasgow Outcome Scale-Extended, ICU intensive care unit, IHCA in-hospital cardiac arrest, OHCA out-of-hospital cardiac arrest, MRI magnetic resonance imaging, NA not applicable, NSE neuron-specific enolase,  $\text{SpO}_2$  peripheral oxygenhemoglobin saturation

\*Post hoc sub-analysis of the ICU-ROX randomised control trial

a disproportionate focus on solely optimising convective CDO<sub>2</sub> without consideration of abnormalities in oxygen diffusion or utilisation. Further, integrating contemporary advances in our understanding of cerebrovascular physiology in health may provide improved contextualisation of the abnormalities seen in HIBI pathophysiology and help inform future clinical trial design. As such, we provide a review with three aims: (1) to review the cerebrovascular pathophysiology in humans with HIBI after cardiac arrest placed within the context of each stage of the oxygen cascade; (2) to review the utility of neuromonitoring techniques which assess the stages of the oxygen cascade; and (3) to highlight the clinical implications of dysfunction of the oxygen cascade for clinical management of HIBI patients and future research.

**Stage 1: convective oxygen delivery**

Convective CDO<sub>2</sub> encompasses the circulatory system's delivery of oxygen from the pulmonary vasculature to the brain (Fig. 1). Convective CDO<sub>2</sub> is the product of cerebral blood flow (CBF) and arterial oxygen content (CaO<sub>2</sub>), with the latter determined by arterial oxygen saturation (SaO<sub>2</sub>), haemoglobin (Hb) concentration, and, to a lesser extent, the partial pressure of arterial oxygen (PaO<sub>2</sub>) (Fig. 2). The physiologic components of convective CDO<sub>2</sub> are summarised by Eq. 1

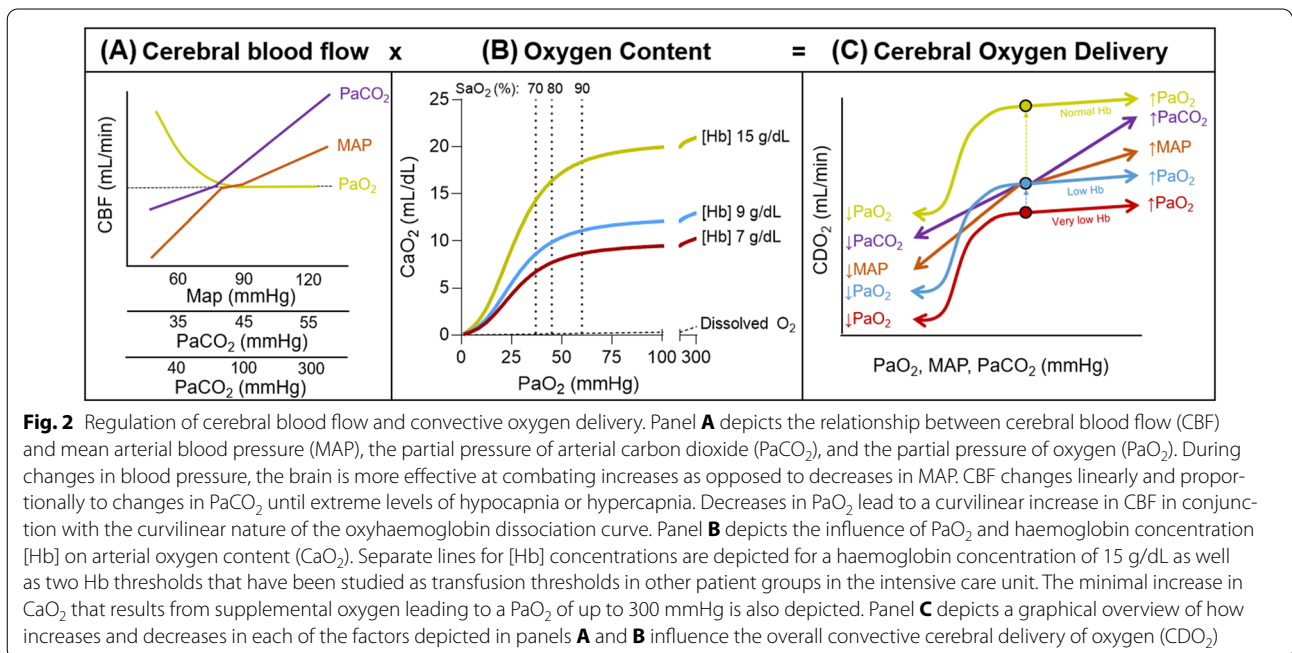
$$CDO_2 = CBF \cdot [(1.34 \cdot SaO_2 \cdot [Hb]) + 0.003 \cdot PaO_2]. \tag{1}$$

CBF is inversely proportional to cerebrovascular resistance (CVR) and proportional to cerebral perfusion pressure (CPP), which is the difference between the mean arterial pressure (MAP) and intracranial pressure (ICP).

**Cerebral blood flow**

Cerebrovascular resistance is increased following HIBI, which may be due to mechanisms encompassing cerebral endothelial dysfunction [18], pericyte constriction and death [19], oxidative stress, microvascular thrombosis in the setting of disseminated intravascular coagulopathy [20], and/or peri-vascular oedema resulting in microvascular collapse [21]. Worsening neurologic outcome with arterial hypotension [4] or sustained hypocapnia [6] suggests that reduced CBF during this period is injurious. Multiple physiologic mechanisms regulate CBF during physiologic perturbations [16, 22]. For the purposes of this review, clinically relevant CBF regulatory mechanisms include cerebral autoregulation [23] and cerebrovascular carbon dioxide reactivity [22, 24] (Fig. 2A).

Cerebral autoregulation refers to intrinsic cerebral vasomotor responses that 'buffer' the influence of changes in MAP on CBF [23]. Pial arteriolar constriction and dilation in response to increases and decreases in MAP, respectively, were described as early as the 1930s [25, 26]. Thereafter, the notion that CBF is maintained constant between an MAP of 50–150 mmHg (i.e., Lassen's curve) became very popular [27]. However, recent evidence [28–31] supports early critiques of Lassen's curve [32] and it has been re-established that autoregulation only



**Fig. 2** Regulation of cerebral blood flow and convective oxygen delivery. Panel A depicts the relationship between cerebral blood flow (CBF) and mean arterial blood pressure (MAP), the partial pressure of arterial carbon dioxide (PaCO<sub>2</sub>), and the partial pressure of oxygen (PaO<sub>2</sub>). During changes in blood pressure, the brain is more effective at combating increases as opposed to decreases in MAP. CBF changes linearly and proportionally to changes in PaCO<sub>2</sub> until extreme levels of hypocapnia or hypercapnia. Decreases in PaO<sub>2</sub> lead to a curvilinear increase in CBF in conjunction with the curvilinear nature of the oxyhaemoglobin dissociation curve. Panel B depicts the influence of PaO<sub>2</sub> and haemoglobin concentration [Hb] on arterial oxygen content (CaO<sub>2</sub>). Separate lines for [Hb] concentrations are depicted for a haemoglobin concentration of 15 g/dL as well as two Hb thresholds that have been studied as transfusion thresholds in other patient groups in the intensive care unit. The minimal increase in CaO<sub>2</sub> that results from supplemental oxygen leading to a PaO<sub>2</sub> of up to 300 mmHg is also depicted. Panel C depicts a graphical overview of how increases and decreases in each of the factors depicted in panels A and B influence the overall convective cerebral delivery of oxygen (CDO<sub>2</sub>)



preserves CBF over a narrow plateau in health, which is not uniformly flat but often has a gradual upward slope [16, 30]. The magnitude by which MAP may be altered without a concomitant change in CBF ranges from approximately 10 to 20 mmHg (Fig. 2A) [30] and largely depends upon the rapidity of the change in MAP [33]. Importantly, the cerebral vasculature is more proficient at buffering increases rather than decreases in MAP in health, thereby rendering the brain vulnerable to ischaemia during hypotension [29, 33]. In health, the lower limit of autoregulation approximates 70 mmHg [16, 33, 34] and is highly variable; however, this limit is higher in HIBI patients [34–37], indicating a greater vulnerability for cerebral hypoperfusion. Using invasive neuromonitoring, the average lower limit of autoregulation has been observed to approximate 85 mmHg in HIBI patients, with significant inter-individual variability (range 60–100 mmHg) [38]. Clinically, this suggests that HIBI patients may experience cerebral hypoperfusion at standard MAP targets (i.e., > 65 mmHg) [39].

Authors have previously suggested that MAP augmentation may be an effective treatment strategy in the post-resuscitation setting [38, 40]. However, the neutral results of randomised control trials investigating MAP augmentation [7–9, 14], and lack of influence of MAP augmentation on neurologic outcome demonstrated in a recent meta-analysis [41], have led investigators to call into question the effectiveness of such an approach. Such discordance between the perceived importance of augmenting MAP and the lack of benefit for neurologic outcome demonstrated in clinical trials may be explained by dysfunction in the latter stages of the oxygen cascade (see [Stage 2: oxygen diffusion](#) & [Stage 3: oxygen utilisation](#)) and by individualised perfusion thresholds that may reflect patient-specific cerebrovascular physiology [42]. In addition to the potential influence of MAP augmentation on CDO<sub>2</sub>, MAP augmentation has been associated with improved renal function [8] and reduced myocardial injury [43]. Nevertheless, an ongoing multicenter international randomised control trial (STEP CARE: NCT05564754) will provide further insights into the impact of higher MAP targets on neurologic recovery in HIBI patients.

Another key regulator of CBF is PaCO<sub>2</sub> [24]. In health, changes in PaCO<sub>2</sub> cause directionally concordant changes in CBF. For every 1-mmHg change in PaCO<sub>2</sub> above or below normal values, CBF increases by ~4–8% or decreases by ~1–4%, respectively (Fig. 2A) [44, 45]. Cerebrovascular CO<sub>2</sub> reactivity regulates CBF throughout the cerebral vasculature [44, 46, 47], with the grey matter having a two- to three-fold higher cerebrovascular CO<sub>2</sub> reactivity than the white matter [24, 48–50]. In healthy humans, normal cerebrovascular

PaCO<sub>2</sub> reactivity, as measured with transcranial Doppler ultrasound [i.e.,  $\Delta$  middle cerebral artery blood velocity (cm/s)/ $\Delta$ PaCO<sub>2</sub> (mmHg)], has been demonstrated to range from approximately 2.5–3.6 cm/s/mmHg [44, 51, 52]. However, in patients resuscitated from cardiac arrest, studies by Buunk et al. and [53] Bisschops et al. [54] reported values of 1.85 and 1.34 cm/s/mmHg PaCO<sub>2</sub>, respectively. These data suggest that cerebrovascular CO<sub>2</sub> reactivity may be impaired in HIBI. Clinically, impaired CO<sub>2</sub> reactivity may limit the ability of hypercapnia to improve convective CDO<sub>2</sub>. This may help explain why initial small clinical trials [10, 11] and the recently published TAME trial [55] did not demonstrate differences in neurologic outcome in HIBI patients with mild hypercapnia versus normocapnia. TAME randomised 1700 out-of-hospital cardiac arrest patients to mild hypercapnia (PaCO<sub>2</sub> 50–55 mmHg) vs normocapnia (PaCO<sub>2</sub> 35–45 mmHg) for 24 h post-ROSC. The primary outcome was favourable neurological outcome, defined as a Glasgow Outcome Scale-Extended  $\geq$  5. The trial did not demonstrate a difference in the favourable outcome rate of patients undergoing mild hypercapnia versus normocapnia (43.5% vs 44.6%, relative risk (RR) 0.98; 95% confidence interval (CI) 0.87–1.11;  $P=0.76$ ).

#### Arterial oxygen content

Maintenance and augmentation of arterial oxygen content have been extensively studied in critically ill patients in general, but only recently in HIBI [11–13, 56, 57]. Reductions in CaO<sub>2</sub>, secondary to anaemia or hypoxaemia (PaO<sub>2</sub> < 60 mmHg) [22, 58] (Fig. 2B), increase CBF in health [22]. Specifically, a 1% reduction in CaO<sub>2</sub> leads to a 2% increase in CBF [22]. The magnitude of this CBF response is sufficient to maintain convective CDO<sub>2</sub> in health [22]. Whether HIBI alters this relationship is unknown. Hypoxaemia is associated with higher mortality in HIBI patients [59, 60]. However, the recent BOX trial comparing normal (e.g., PaO<sub>2</sub> = 98–105 mmHg) versus restrictive arterial oxygen tension (e.g., PaO<sub>2</sub> = 68–75 mmHg) did not demonstrate a difference in neurologic outcome [12], which may indicate that CDO<sub>2</sub> is maintained in HIBI during modest reductions in PaO<sub>2</sub> that remain above 60 mmHg.

Observational evidence suggests that severe hyperoxaemia (e.g., PaO<sub>2</sub> > 300 mmHg) [59–63] is associated with worse outcomes after cardiac arrest, although specific harmful PaO<sub>2</sub> thresholds are not well established [64]. A recent post hoc analysis of the TTM2 trial found that the best cut-off point associated with 6-month mortality for hyperoxaemia was 195 mmHg (RR 1.006, 95% CI 0.95–1.06) [60]. It has been suggested that hyperoxaemia may increase the production of reactive oxygen species worsening HIBI [65]. However, a post hoc analysis of

COMACARE showed no difference in markers of cerebral lipid peroxidation between HIBI patients with a targeted PaO<sub>2</sub> of 75–112 mmHg and 150–187 mmHg [66]. Further research is needed to elucidate the influence of moderate levels of oxygen supplementation on CDO<sub>2</sub> in HIBI, and if individualised PaO<sub>2</sub> goals are needed.

In addition to the influence of hyperoxaemia in the intensive care unit (ICU) setting, the influence of blood oxygen levels in the acute post-ROSC setting on convective CDO<sub>2</sub> must be considered. The recent EXACT trial demonstrated that a modest reduction in blood oxygen levels (SpO<sub>2</sub> 97%) versus standard of care (SpO<sub>2</sub> 99%) did not significantly influence survival to hospital discharge (odds ratio [OR] 0.68 [95% CI 0.46–1.00]; *P*=0.05) [13]. Further, there were no apparent differences in 12-month neurologic outcome in the patients that survived to hospital discharge or 12-month survival in all patients [13]. An important consideration is the extent to which PaO<sub>2</sub> can improve the partial pressure of brain tissue oxygen (PbtO<sub>2</sub>) (see “[Parenchymal brain tissue oxygenation](#)”). Nonetheless, the findings of the EXACT trial do not support the use of lower oxygen targets in the pre-hospital phase following ROSC.

Whilst the CBF response during PaO<sub>2</sub>-dependent reductions in CaO<sub>2</sub> (i.e., hypoxaemia) is sufficient—to a certain extent—to maintain CDO<sub>2</sub>, the CBF response to acute anaemia (e.g., decreased CaO<sub>2</sub> from acute haemorrhage) is insufficient to maintain CDO<sub>2</sub> (Fig. 2C) [67]. Therefore, acute anaemia may contribute to brain tissue hypoxia in HIBI patients [5] and worsen neurologic outcome after cardiac arrest [5, 68–70]. In an observational study on 118 patients with HIBI, higher mean haemoglobin concentration in the first 48 h and 7 days following cardiac arrest was associated with lower adjusted odds of unfavourable neurologic outcome at hospital discharge (OR 0.69/10 unit decrease in Hb, 95% CI 0.54–0.88, *P*<0.01) [68].

Clinical interventions aimed at optimising convective CDO<sub>2</sub> continue to be a focus of active research in HIBI (Fig. 3). Conceptually, studies on the potential utility of MAP augmentation, mild hypercapnia, hyperoxaemia, and red blood cell transfusion are logical (Fig. 3A). However, their clinical efficacy has not been established (Table 1), suggesting that HIBI pathophysiology is more complex than dysregulation of only convective CDO<sub>2</sub>. Importantly, consideration of intracranial pressure and compliance in individual patients may be crucial in selecting the correct clinical interventions to augment convective CDO<sub>2</sub>. For example, in HIBI patients with elevated ICP, mild hypercapnia may lead to cerebral vasodilation, increased cerebrovascular blood volume [71], and intracranial hypertension [72, 73]. Similarly, such patients may also experience dangerous elevations

in ICP with compensatory vasodilatory responses in the setting of severe hypoxaemia or reduced CPP. Thus, assessment of ICP (see “[Neuromonitoring: intracranial pressure](#)” below) is a key physiologic variable which must be accounted for in optimising convective CDO<sub>2</sub> strategies after ROSC.

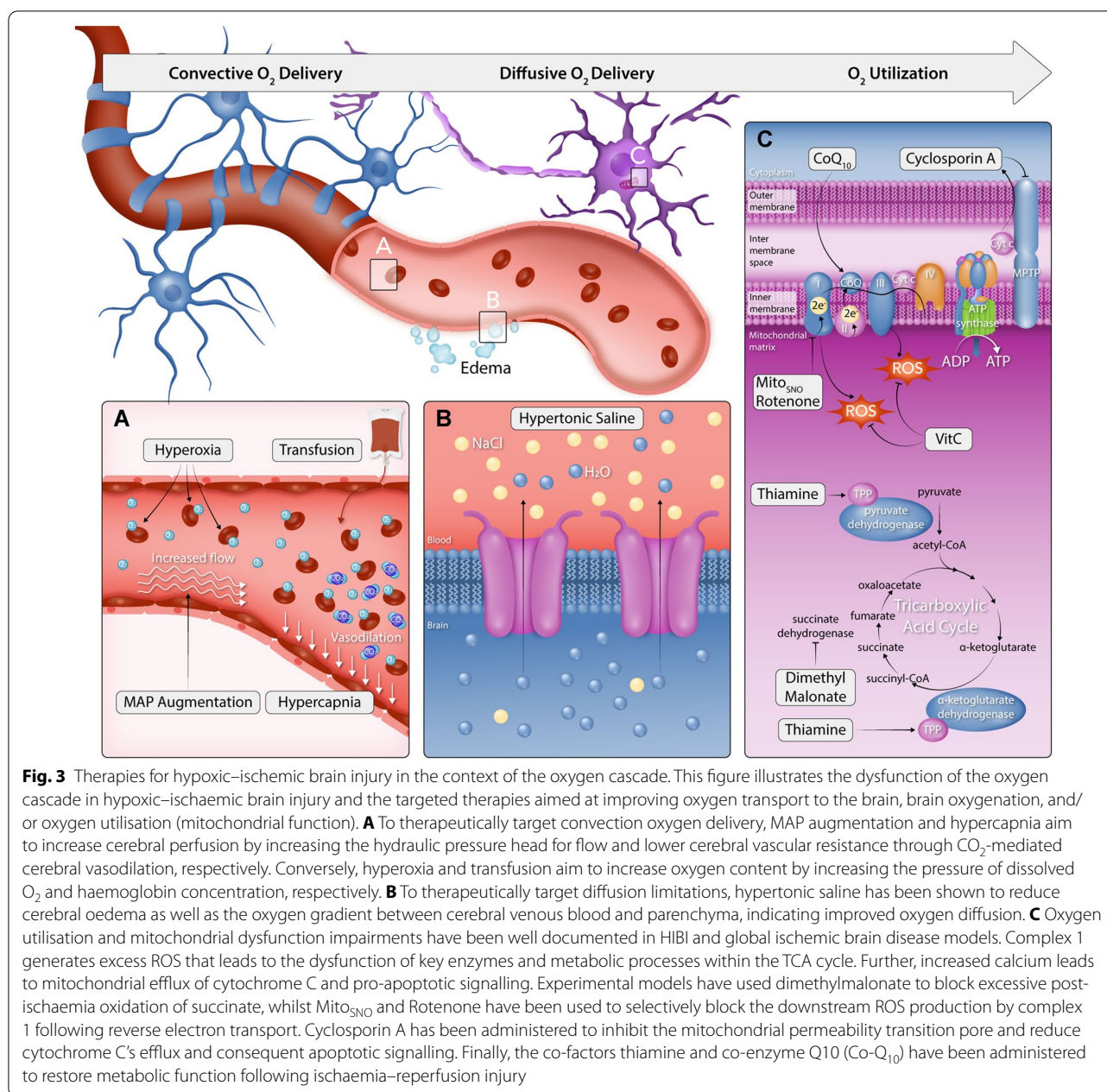
## Stage 2: oxygen diffusion

In a normal resting state, approximately 25% of oxygen carried to the brain diffuses into brain tissue. Consequently, normal cerebral venous haemoglobin oxygen saturation approximates 70–75% [74]. This relationship can be altered by reductions in CBF [45], when additional oxygen must be extracted from haemoglobin to maintain a constant cerebral metabolism. The diffusion of oxygen from the cerebral vasculature into brain tissue is governed by the biophysical principles of Fick’s law of diffusion, outlined in Eq. (2)

$$\text{Diffusion} \propto \frac{A}{T} \cdot D \cdot \Delta P_{O_2}. \quad (2)$$

Specifically, the diffusion of oxygen is proportional to the surface area for diffusion (*A*), the diffusion coefficient (*D*), and the pressure gradient from the vasculature to tissue ( $\Delta P_{O_2}$ ). Most important to consider in the context of HIBI is that oxygen diffusion into the brain is inversely proportional to the thickness (*T*) of the diffusion barrier. However, it may be more appropriate to conceptualise this as the length of the diffusional path oxygen must take to successfully enter brain tissue. This barrier includes the cerebrovascular endothelium, vessel wall, and interstitial tissue, and the path length for diffusion may increase due to a multitude of factors including cerebral oedema. Further, regional microvascular shutdown due to microthrombosis or endothelial oedema may make areas of the brain dependent on oxygen that has to diffuse from distant capillaries that remain patent, with substantial increases in the path length for oxygen diffusion.

The concept of impaired oxygen diffusion from the blood into brain tissue (i.e., a diffusion limitation) as a pathophysiologic component of brain tissue hypoxia in acute brain injuries was first demonstrated by Menon et al. [21] in humans with traumatic brain injury. This study showed that the difference between the cerebral venous partial pressure of oxygen (PvO<sub>2</sub>) and brain tissue oxygen tension (PbtO<sub>2</sub>), termed the PvO<sub>2</sub>–PbtO<sub>2</sub> gradient, was greater in patients with brain tissue hypoxia [21]. By acutely reducing CBF with a brief period of hypocapnia, the authors observed smaller increases in the cerebral oxygen extraction fraction in patients with brain tissue hypoxia compared to those with brain tissue normoxia, indicating the presence of impaired oxygen diffusion (7 ± 5% vs 16 ± 6%; *P*<0.05) [21]. Similar



observations have been made in humans with HIBI. Specifically, patients with post-resuscitation brain tissue hypoxia exhibit larger cerebral PvO<sub>2</sub>–PbtO<sub>2</sub> gradients than those with brain tissue normoxia (39 mmHg [SD 11] vs 16 mmHg [SD 6];  $P < 0.001$ ) [75]. Moreover, increasing CPP was associated with a decrease in the PvO<sub>2</sub>–PbtO<sub>2</sub> gradient in patients with brain tissue normoxia, whereby each 1 mmHg increase in CPP led to a 0.36 mmHg (95% CI 0.18–0.54,  $P < 0.001$ ) decrease in the PvO<sub>2</sub>–PbtO<sub>2</sub> gradient, indicating intact oxygen diffusion. Conversely, no relationship was observed between varying CPP and

the PvO<sub>2</sub>–PbtO<sub>2</sub> gradient in patients with brain tissue hypoxia (coefficient – 0.29, 95% CI – 0.17 to 0.11;  $P = 0.73$ ), indicating a diffusion limitation [75].

There may be differential pathophysiologic phenotypes of HIBI, whereby some patients exhibit “perfusion-dependent” physiology (i.e., PbtO<sub>2</sub> increases in response to augmented perfusion) [76]. In contrast, other patients exhibit “diffusion-limited” physiology (i.e., PbtO<sub>2</sub> is unresponsive to augmented perfusion due to impaired oxygen diffusion) [76]. Clinically, HIBI patients exhibiting diffusion limitation would not exhibit increased brain



tissue oxygenation with treatment approaches that aim to optimise convective  $\text{CDO}_2$  (e.g., MAP augmentation), rendering such interventions ineffective. Conversely, patients with intact diffusion of oxygen would likely exhibit improved brain tissue oxygen tension with convective  $\text{CDO}_2$  augmentation. Identifying these phenotypes in real time for bedside clinicians is a clear next step to facilitate individualised management paradigms in the post-resuscitation setting.

Research on interventions aimed at optimising oxygen diffusion is still in its preliminary phase. Diffusion limitation is associated with peri-vascular oedema on electron microscopy in humans [21, 77], which may be responsive to osmotherapy [78, 79]. Hypertonic saline reduces the  $\text{PvO}_2$ – $\text{PbtO}_2$  gradient and improves  $\text{PbtO}_2$  in HIBI patients with brain tissue hypoxia without significant changes in the other key physiologic variables, such as ICP, CPP, and MAP [3] (Fig. 3B). The decrease in the  $\text{PvO}_2$ – $\text{PbtO}_2$  gradient and concurrent improvement in  $\text{PbtO}_2$  provides preliminary evidence that osmotherapy may enhance oxygen diffusion into brain tissue by reducing the thickness of the diffusional barrier (Eq. 2). Although promising, considerable work remains to characterise this physiology further and evaluate its potential clinical efficacy.

### Stage 3: oxygen utilisation

At the cellular level, oxygen utilisation relies upon intact mitochondrial function and metabolic pathways. The main substrate used by the brain is glucose; however, alternative metabolic substrates such as lactate and ketones may be preferentially metabolised by the injured brain [80]. Clinical trial evidence has shown that intensive glycaemic control (4–6 mmol/L) in critically ill patients is associated with increased mortality [81], and can cause metabolic crisis in patients with acute brain injury [82]. As such, it is imperative to avoid hypoglycaemia (<4 mmol/L) which may expose the injured brain to neuroglycopenia, and there is arguably a case for maintaining high normal blood sugar levels to optimise glucose delivery to the brain. The cerebral metabolic rate of oxygen ( $\text{CMRO}_2$ ) of the grey matter is higher than that of the white matter [83]. Neurons and glia are heavily distributed in grey matter and require adequate adenosine triphosphate to support the generation of action potentials, post-synaptic ion fluxes, and maintenance of resting potentials [84]. Conversely, the sub-cortical white matter, comprised largely of myelinated axons, requires less oxygen for basal metabolic consumption [85]. This heterogeneity in metabolism leads to regional differences in the requirements for sufficient  $\text{CDO}_2$  and vulnerability to ischaemia [86].  $\text{CMRO}_2$  can be calculated as per the Fick principle (Eq. 3) [74]

$$\text{CMRO}_2 = \text{CBF}(\text{CaO}_2 - \text{CvO}_2). \quad (3)$$

Alterations to cerebral metabolic function occur following cerebral ischaemia [87] (Fig. 3C). A historical study demonstrated that  $\text{CMRO}_2$  decreased to approximately 50% of normal in humans resuscitated from cardiac arrest [88]. Interestingly, measures of the ratio of the cerebral venous-to-arterial differences of oxygen and carbon dioxide (i.e.,  $\text{Cv-aCO}_2/\text{Cv-aO}_2$ ), a global estimate of the balance between aerobic and anaerobic metabolism, indicate that low CBF may not necessarily lead to anaerobic metabolism in HIBI [89]. It remains unclear whether reductions in  $\text{CMRO}_2$  with HIBI are a regulated and adaptive response to maintain cerebral flow-metabolism coupling during the hypoperfusion that ensures following cardiac arrest. However, the evidence to date indicates that a higher  $\text{CMRO}_2$  is associated with survival [90]. Important considerations for the interpretation of reduced cerebral metabolism include that: (1) global  $\text{CMRO}_2$  may not reflect regional physiologic differences of susceptible anatomic foci that are injured in HIBI, (2) reductions in metabolism could be the result of a down regulation of metabolism or irreversible cell death, and (3) sedative administration in the ICU setting will influence  $\text{CMRO}_2$  independent from HIBI-related pathophysiologic processes.

Mechanistic explanations for cerebral metabolic dysfunction in HIBI include an impairment in glycolysis [87] stemming from essential co-factor (e.g., thiamine) depletion and dysfunction of key enzymes (e.g., pyruvate dehydrogenase) [91, 92]. Further, animal models have demonstrated an accumulation of succinate during ischaemia followed by rapid oxidation of succinate and reactive oxygen species generation consequent to reverse electron transport at complex 1 [93]. Interestingly, plasma succinate levels are higher in HIBI that do not survive than in HIBI survivors [94]. This reactive oxygen species generation further exacerbates mitochondrial dysfunction whereby intracellular calcium accumulation induces cytochrome C release from mitochondria [95] and initiates apoptotic signalling following global ischaemia [96]. Importantly, reductions in antioxidant defences [97] and increased oxidative stress [66, 98] are associated with mitochondrial dysfunction in HIBI. The influence of anaesthetic administration on  $\text{CMRO}_2$  during intensive care management must also be considered [99]. For example, whilst propofol [100] and midazolam [101] reduce both CBF and  $\text{CMRO}_2$ , and thus maintain coupling between blood flow and metabolism, other anaesthetic agents, such as volatile anaesthetics, may lead to uncoupling of CBF and  $\text{CMRO}_2$  [99].



To improve the balance between  $\text{CDO}_2$  and  $\text{O}_2$  utilisation, moderate therapeutic hypothermia has been ubiquitously employed in post-resuscitation care [102, 103]. Yet, supporting evidence has been conflicting and the most recent and comprehensive TTM2 trial showed no benefit of hypothermia in HIBI [104]. Although therapeutic hypothermia has demonstrated some potential benefit in patients presenting with non-shockable rhythms [105], the precise patient population who may benefit from therapeutic hypothermia has not been yet identified [106]. Given the considerable systemic side effects of sustained hypothermia, alternate treatments to optimise  $\text{O}_2$  utilisation and mitochondrial function are being investigated.

The administration of metabolic co-factors, antioxidants, and other treatments targeting mitochondrial function has gained interest as potential therapeutic strategies. For example, high-dose thiamine administration in a pre-clinical HIBI model reduced neurologic injury [92]; however, two recent phase-2 randomised control trials investigating the efficacy of high-dose thiamine administration (NCT03450707 and NCT02974257) were terminated early for futility. Administration of co-enzyme  $\text{Q}_{10}$ , an essential co-factor in the electron transport chain, has demonstrated a potential benefit in patients undergoing therapeutic hypothermia (35 °C for 24 h) [107]. However, another recent randomised control trial showed no difference in cerebral metabolism, neurological biomarkers, or clinical outcomes compared to placebo despite increased plasma co-enzyme  $\text{Q}_{10}$  levels in the treatment group [108]. Regarding antioxidants, pre-clinical studies indicate that vitamin C reduces reactive oxygen species following cardiac arrest [18] and improves outcomes [18, 109]. A phase-2 randomised control trial (NCT03509662) investigating the efficacy of Vitamin C administration in HIBI patients is underway. Finally, cyclosporine [110–112], an inhibitor of the mitochondrial permeability transition pore, did not confer improved survival to hospital discharge when given at the onset of advanced cardiovascular life support [113].

Pre-clinical studies have illuminated additional intriguing therapeutic targets [114], but human studies have yet to show significant clinical benefits from mitochondrial-targeted therapies. For example, increasing *S*-nitrosylation of mitochondrial complexes/enzymes improves outcome following cardiac arrest [98], presumably by reducing reverse electron transport-mediated generation of reactive oxygen species by complex 1 [93, 115] and/or protecting mitochondrial enzymes from irreversible oxidation during ischaemia–reperfusion [116]. Further, the administration of antioxidants reduces cerebral lipid peroxidation [97] and may provide a modest benefit to cerebral perfusion and metabolism [117]. However,

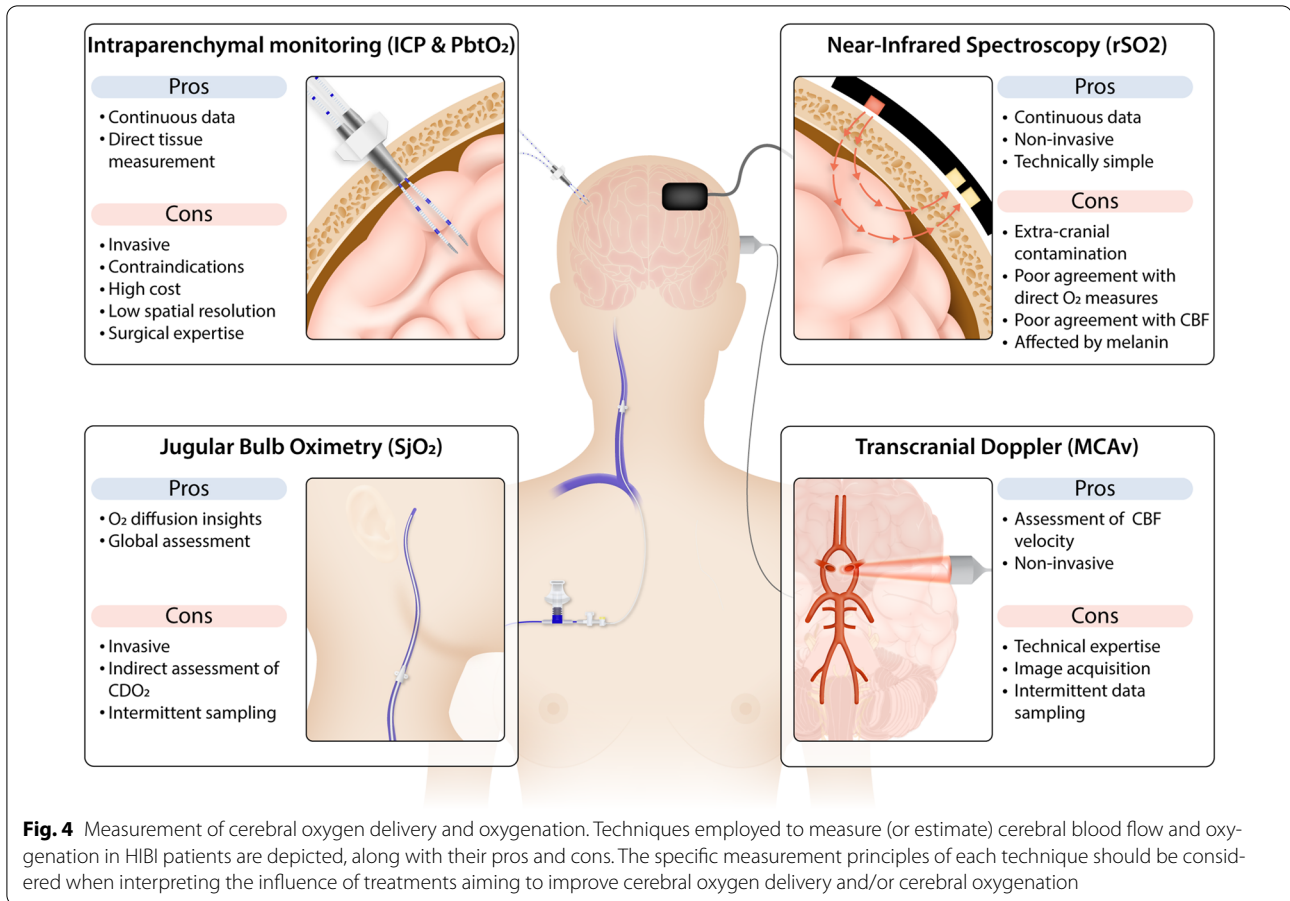
the applicability of these therapies in human patients remains to be determined. Given the complexity of the cellular pathophysiology in HIBI, the concept of rational polytherapy has emerged as a therapeutic strategy [114]. In this instance, simultaneous administration of multiple agents to reverse pathophysiologic processes at the cellular level has been advocated [114]. However, considerable work remains for translation of this approach into humans with HIBI.

### Assessing the $\text{O}_2$ cascade through neuromonitoring

Key considerations for the interpretation of neuromonitoring techniques with relevance to the oxygen cascade are presented below (Fig. 4). Currently, most published literature on HIBI patients includes neuromonitoring techniques focussing on convective  $\text{CDO}_2$  or oxygen diffusion. However, studies including techniques assessing oxygen utilisation are underway. A prospective interventional study examining surrogates of mitochondrial function (cerebral lactate/pyruvate ratio) using intraparenchymal microdialysis (NCT05390060) may shed light on the utilisation stage of the oxygen cascade in HIBI.

### Intracranial pressure

Coupled with measuring arterial blood pressure, ICP monitoring enables the continuous quantification of CPP, a key determinant of CBF and convective  $\text{CDO}_2$ . Monitoring of ICP has traditionally been employed in traumatic brain injury management, but investigators have also started monitoring ICP in HIBI patients [3, 38, 75, 118]. There appears to be considerable patient heterogeneity regarding the burden of intracranial hypertension in HIBI, with the spectrum of disease severity encompassing normal ICP to fulminant cerebral oedema and brain death [119]. A recent prospective interventional study on a consecutive sample of HIBI patients demonstrated a mean ICP of 14 mmHg (SD 11) [119]. In this cohort, the percentage of time with ICP > 20 mmHg was 22% (range 0–100) during the monitoring period [119]. Importantly, these HIBI patients also exhibited limited compliance of the intracranial compartment presumably due to mild cerebral oedema. Therefore, HIBI patients with ‘normal’ ICP may remain at risk of developing intracranial hypertension if not managed with ICP lowering interventions [120]. Indeed, pre-clinical studies have shown that the administration of osmotherapy can attenuate cerebral oedema in HIBI [78, 79] and decrease brain injury biomarker release [121]. Monitoring ICP allows measurement of autoregulation indices, specifically the pressure reactivity index [38, 118] which may be used to estimate individualised optimal perfusion pressures.



However, the clinical utility of these indices for patient management has yet to be determined [122]. Although ICP monitoring is an intriguing modality for use in HIBI, its invasive nature limits widespread implementation to guide HIBI management. An important limitation of the available literature describing ICP monitoring in HIBI is that it has largely been conducted in patients who present from non-cardiac causes of arrest (e.g., non-shockable rhythms) [118, 120]. In patients presenting with shockable rhythms, whose arrest is most often due to acute coronary occlusion, the consequent need for anti-platelet or anticoagulant therapy may preclude the implementation of invasive neuromonitoring. Considerable work remains to clarify the role of ICP monitoring in patients with HIBI and its indications and efficacy as part of critical care management after the return of spontaneous circulation.

#### Jugular venous bulb oximetry

Jugular venous bulb oximetry (SjvO<sub>2</sub>) measures the oxygen saturation of haemoglobin distal to the sigmoid sinus via an intravascular catheter placed retrograde in the dominant jugular vein. In a state of normal oxygen

diffusion, SjvO<sub>2</sub> can represent global cerebral haemodynamics by reflecting the overall balance between convective CDO<sub>2</sub> and oxygen utilisation. However, when oxygen diffusion is abnormal in HIBI, increased SjvO<sub>2</sub> may indicate underlying pathophysiologic processes, such as fulminant cerebral oedema, mitochondrial dysfunction [123], or widespread brain tissue death.

Increased SjvO<sub>2</sub> is correlated to adverse neurologic outcome [124] and increased serum levels of neuron-specific enolase (NSE) [125], a biomarker of neuron cell body injury [126]. Richter et al. conducted a retrospective study of 40 out-of-hospital-cardiac-arrest patients in whom SjvO<sub>2</sub> was intermittently sampled over 72 h after hospital admission [125]. They divided the participants into three study groups stratified by mean SjvO<sub>2</sub> (Group 1: low SjvO<sub>2</sub> < 55%; Group 2: SjvO<sub>2</sub> 55–75%; Group 3: SjvO<sub>2</sub> > 75%). The authors found that 27/40 (68%) patients had mean SjvO<sub>2</sub> > 75%, with the remaining exhibiting SjvO<sub>2</sub> between 55 and 75% and none below 55% [125]. Further, they found that HIBI patients exhibiting SjvO<sub>2</sub> 55–75% had lower NSE levels compared to those with SjvO<sub>2</sub> > 75% at 72 h (9 [interquartile range (IQR) 7–13] vs 46 [IQR 14–65] ng/mL; *P* < 0.01)

[125]. Other studies integrating S<sub>iv</sub>O<sub>2</sub> monitoring as part of a comprehensive neuromonitoring platform have found worse neurologic outcome in patients with elevated S<sub>iv</sub>O<sub>2</sub> post-ROSC [75, 124].

Currently, the clinical utility of routine S<sub>iv</sub>O<sub>2</sub> monitoring is unclear in HIBI. S<sub>iv</sub>O<sub>2</sub> may provide insights into in vivo pathophysiology and help distinguish between HIBI patients with intact (low-normal S<sub>iv</sub>O<sub>2</sub>) or abnormal oxygen diffusion (high S<sub>iv</sub>O<sub>2</sub>). Whether or not increased S<sub>iv</sub>O<sub>2</sub> in HIBI represents a sign of disease severity or could be a therapeutic goal remains to be seen and requires further study.

### Parenchymal brain tissue oxygenation

The placement of a parenchymal brain tissue oxygen probe enables continuous assessment of brain tissue oxygen tension (i.e., PbtO<sub>2</sub>) within the sub-cortical white matter of the frontal lobe. A recent study by Sekhon et al. aimed to quantify the burden of brain tissue hypoxia in HIBI [38]. This prospective interventional study of invasive neuromonitoring found that patients spent ~40% (range 6–100%) of monitoring duration with a PbtO<sub>2</sub> that is indicative of brain tissue hypoxia (less than 20 mmHg) [38]. Balu et al. demonstrated that a PbtO<sub>2</sub> < 18 mmHg is associated with poor neurologic outcome in HIBI [118]. In a matched cohort study, Fergusson et al. stratified HIBI patients based on those who underwent management guided by PbtO<sub>2</sub> (*n* = 21) versus standard of care (no PbtO<sub>2</sub>, *n* = 44) [119]. They observed that patients undergoing PbtO<sub>2</sub> monitoring had a higher rate of favourable neurological outcome (cerebral performance category 1 or 2) than those without (44% vs 18%, *P* = 0.03). However, the small sample size and the post hoc design limit the strengths of this study [119].

Physiologically, PbtO<sub>2</sub> reflects the balance between both convective CDO<sub>2</sub> and O<sub>2</sub> diffusion into the brain tissue and cerebral metabolism. A prospective study on HIBI patients undergoing PbtO<sub>2</sub> monitoring demonstrated an association between increasing MAP and increased PbtO<sub>2</sub> ( $R^2 = 0.71$ , *P* < 0.001) [38]. However, the slope of the relationship between MAP and PbtO<sub>2</sub> for each patient was heterogeneous [38]. This suggested diverse pathophysiologic HIBI phenotypes regarding coupling or uncoupling of convective CDO<sub>2</sub> and O<sub>2</sub> diffusion into the brain [75, 76] (see also the section “[Stage 2: oxygen diffusion](#)”). Therefore, the relationship between PbtO<sub>2</sub> and other physiologic variables (e.g., MAP) provides insight into the functionality of oxygen diffusion into the brain.

Identifying patient-specific phenotypes with PbtO<sub>2</sub> is clinically important, since patients exhibiting an uncoupling between convective CDO<sub>2</sub> and PbtO<sub>2</sub> would not likely benefit from MAP augmentation or other

convective CDO<sub>2</sub> focussed interventions [76]. Conversely, patients with intact O<sub>2</sub> diffusion likely would benefit. As such, patient identification and selection stratified by physiologic phenotyping are key considerations for research using PbtO<sub>2</sub> monitoring in HIBI. Future work in this area is needed to better understand the impact of post-resuscitation brain tissue hypoxia on neurologic outcome in HIBI, aid in determining methods to identify brain tissue hypoxia non-invasively and determine whether interventions that resolve brain tissue hypoxia are clinically efficacious.

An important limitation of PbtO<sub>2</sub> monitoring that must be considered is the potential for confounding of the PbtO<sub>2</sub> recording by dissolved oxygen within the cerebral vasculature. Whilst the catheter is thought to solely reflect tissue oxygen tension, it is likely unable to discriminate between the dissolved tension of oxygen within the brain parenchyma and within the microvasculature. Rosenthal et al. administered normobaric hyperoxia in humans undergoing multi-modal neuromonitoring following traumatic brain injury. The PaO<sub>2</sub> increased from 127 (103–150) to 441 mmHg (363–518) and PbtO<sub>2</sub> increased from 22.9 (17.2–28.6) to 77 mmHg (58.1–96). This increase in PbtO<sub>2</sub> occurred despite a reduction in CBF from 23.9 (16.5–31.2) to 18.5 mL/100 g/min (12.2–24.8) [127]. That PbtO<sub>2</sub> increased with normobaric hyperoxia despite a reduction in CBF and CDO<sub>2</sub> likely indicates an independent effect of PaO<sub>2</sub> on the recorded value of PbtO<sub>2</sub>. This notion has been supported by additional research [128].

### Transcranial Doppler ultrasound

Transcranial Doppler ultrasound (TCD) may have a dual role in HIBI management and research: (1) measuring middle cerebral blood velocity to estimate CBF and (2) non-invasively estimating ICP. Thus, TCD provides estimates of physiologic variables that determine convective CDO<sub>2</sub> (CBF and ICP). A linear relationship exists between CBF and flow velocities within the blood vessels insonated with TCD (e.g., middle cerebral artery), provided that the diameter of the vessel remains constant [129]. As such, TCD has been used as an indirect and non-invasive surrogate of CBF in HIBI [89, 90, 130–133]. Hoedemaekers et al. conducted a prospective observational study in 20 HIBI patients using TCD to estimate cerebral perfusion. The authors observed that the middle cerebral artery blood velocity of patients with HIBI (66 [59.5–73] years of age) was lower than healthy controls (28 ± 4.5 years of age) at 24 h (26 [18.6–40.4] vs. 59.1 cm/s [52.8–69], *P* < 0.001) but increased significantly at 72 h (63.9 cm/s [48.3–73.1]). Notwithstanding the potential influence of age on the lower CBF [134] observed in this study [89], these data suggest a dynamic nature of

cerebral haemodynamics over time in HIBI. An ongoing clinical trial (NCT04000334) is assessing the feasibility of using TCD for goal-directed haemodynamic management in HIBI.

The second key role of TCD for neuromonitoring in HIBI is the non-invasive estimation of ICP [135]. An important TCD-derived variable for this is the pulsatility index (PI). The PI is calculated as the difference between the peak systolic and diastolic flow velocities, divided by the mean flow velocity and a PI above 1.2 suggests intracranial hypertension. A recent multicentre study in neurocritically ill patients evaluating the accuracy of ICP prediction based on diastolic flow velocity and mean arterial pressure demonstrated a good negative predictive value in ruling out intracranial hypertension [136]. A high PI and low diastolic blood velocity in patients with HIBI are associated with poor neurological outcome [133]. Cardim et al. conducted an agreement study between invasively monitored ICP and non-invasive surrogates, including TCD in HIBI patients [135]. The authors found a linear relationship between ICP measured with intra-parenchymal monitoring and non-invasive ICP ( $R=0.3$ ,  $P=0.01$ ) measured with TCD. The area under the receiver-operating characteristic (ROC) curve of TCD for predicting intracranial hypertension (ICP > 20 mmHg) was 0.91 (95% CI 0.83–1.00). Although useful and risk-free, the need for technical expertise, potential inter-observer error, and difficulties acquiring high-fidelity continuous recordings may limit the widespread use of TCD to guide management in HIBI. Further studies are needed to better establish the utility of TCD in HIBI patient management [130].

### Near-infrared spectroscopy

Near-infrared spectroscopy (NIRS) monitors the regional saturation of oxygen ( $rSO_2$ ). Simply requiring the bilateral application of adhesive oximetry pads to a patient's forehead, NIRS is non-invasive and does not require high technical expertise to use. The NIRS-dependent  $rSO_2$  value represents an estimate of the oxygen saturation of haemoglobin within the cerebrovascular compartment and assumes a 25:75 or 30:70 ratio of cerebral arteriole to venule blood volume in the interrogated region [137]. In other words,  $rSO_2$  should approximate the sum of  $0.25 \cdot SaO_2$  and  $0.75 \cdot SvO_2$ . The advantages of NIRS include its non-invasive application and its low-risk profile. NIRS can be implemented quickly in the post-ROSC setting compared to other neuromonitoring devices. However, technical and methodological limitations hinder the widespread use of NIRS for clinical decision-making. Specifically, contamination of the  $rSO_2$  signal by cutaneous blood, non-adherence of the monitoring pads to skin, and ambient light interference

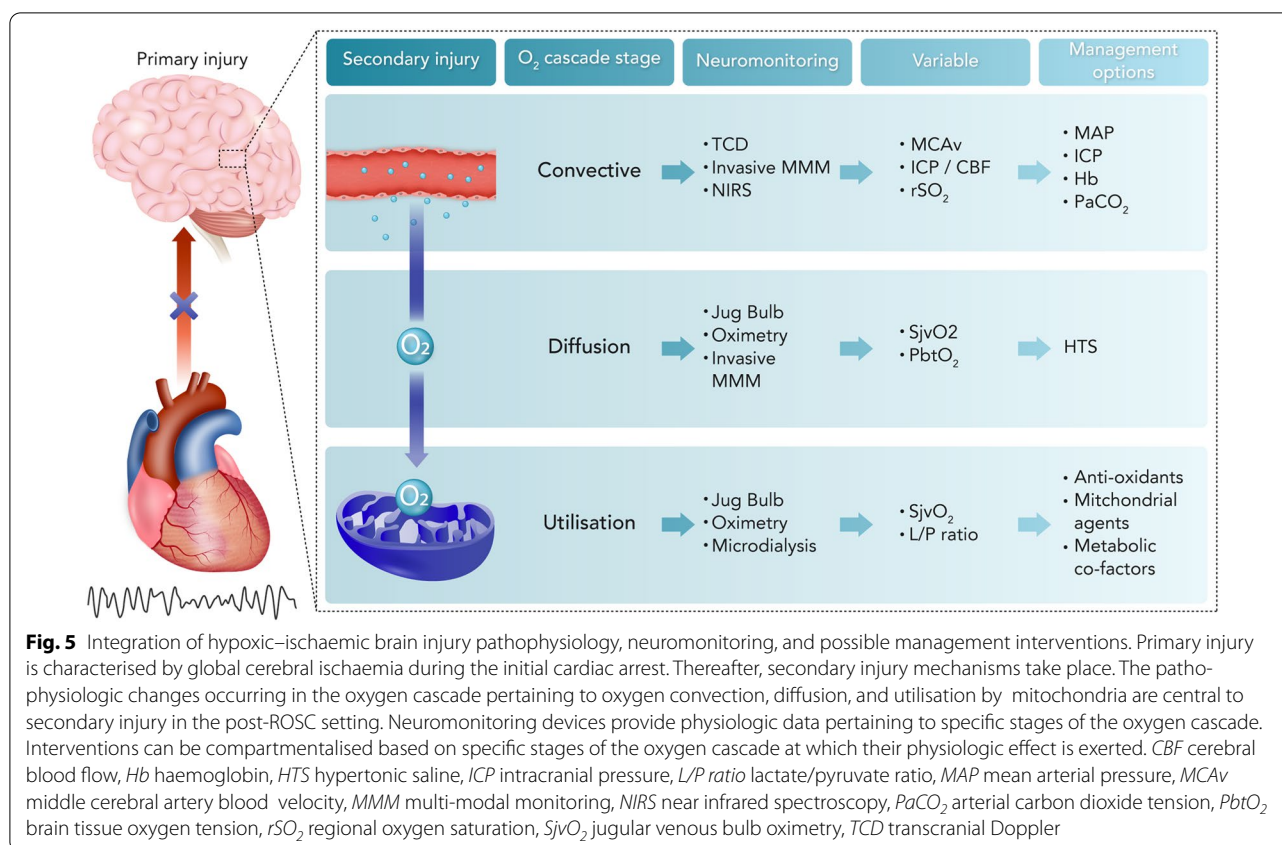
present challenges to the accuracy of NIRS [138]. Further, pathophysiologic considerations in HIBI, such as diffusion limitation, may also limit the accuracy of NIRS. In this instance, the uncoupling between  $CDO_2$  and brain tissue oxygenation precludes the normal assumption of NIRS that haemoglobin saturation within the cerebrovascular compartment is reflective of brain tissue oxygen tension [139]. For example, in patients with HIBI, NIRS does not change concordantly with  $PbtO_2$  during MAP augmentation [38], nor does it change concordantly with CBF in health and in patients with HIBI [140]. Further, poor agreement has been shown between NIRS-derived cerebral autoregulation indices compared to established indices generated with parenchymal neuromonitoring [140].

### Clinical implications

The restoration of adequate  $CDO_2$  in HIBI has intuitive importance; however, key clinical considerations remain regarding the implementation of  $CDO_2$ -based patient management strategies for therapeutic benefit. At present, clinical interventions that only target a single stage of the oxygen cascade are unlikely to provide therapeutic efficacy (Table 1). Therefore, combined approaches are likely required to simultaneously assess convective  $CDO_2$ , diffusion of oxygen, and oxygen utilisation, to ensure these critical stages of the oxygen cascade function optimally. In this regard, a stepwise approach to patient management that applies multiple interventions for the purpose of targeting each stage of the oxygen cascade represents a promising path forward (Fig. 5). For example, optimising convective  $CDO_2$  (stage 1) with CBF augmenting interventions should be sought prior to or in parallel with improving oxygen diffusion (stage 2) and cellular oxygen utilisation (stage 3). Potential candidate interventions for each stage of the oxygen cascade are described in Fig. 5. Such an approach would necessitate multi-modal neuromonitoring to assess the function of each stage of the oxygen cascade and their response (or lack thereof) to intervention.

The above approach may lay the foundation for 'personalised' post-resuscitative care but requires recognising differing pathophysiologic patient phenotypes to apply the appropriate interventions [76]. Unfortunately, no widely implementable technique is presently available to identify these phenotypes at the bedside to provide clinicians with immediately actionable real-time data. The development of non-invasive techniques to identify patient-specific pathophysiology is an essential avenue for future research. An impairment of oxygen diffusion may explain why not all HIBI patients benefit from augmented convective  $CDO_2$  [7, 8, 14, 55, 76]. Studies to date have only targeted convective  $CDO_2$





or implemented singular interventions [7–14, 56]. It is becoming increasingly clear that no single treatment can resolve HIBI, and bundle-based management interventions are likely needed [114]. Translational studies should focus on establishing the biological plausibility of oxygen cascade-based therapeutic strategies. Clinical trial design will likely require platform-based adaptive or factorial design methodologies to assess the clinical efficacy of combined interventions.

Finally, the timing of the restoration of oxygen delivery to the injured brain is likely key. The longer the delay between resuscitation and the implementation of interventions aimed at restoring CDO<sub>2</sub>, the less likely it is that the restoration of CDO<sub>2</sub> will confer a clinical benefit. This is analogous to the stroke literature's well-defined “time is brain” concept. The specific timing of when and by what magnitude the efficacy of CDO<sub>2</sub> restoration is diminished after the return of spontaneous circulation in HIBI is unknown but is clearly an important variable when designing future clinical trials.

## Conclusions

The successful treatment of HIBI will likely require a multi-pronged approach. A greater understanding of the factors that lead to dysfunction within the oxygen

cascade in HIBI is needed to develop strategies to optimise adequate CDO<sub>2</sub> and cellular utilisation. Given the complexity of HIBI pathophysiology, it is likely that optimisation of cerebral oxygen cascade will need to be paired with other neuroprotective strategies to confer clinical efficacy for patients. Key variables such as the timing of implementation for clinical interventions after resuscitation from cardiac arrest and patient-specific pathophysiology must be considered in future studies to effectively determine the efficacy of CDO<sub>2</sub> restoring interventions as part of HIBI resuscitation in the intensive care setting.

## Author details

<sup>1</sup> Division of Critical Care Medicine, Department of Medicine, Faculty of Medicine, Vancouver General Hospital, University of British Columbia, Vancouver, BC, Canada. <sup>2</sup> Division of Neurosurgery, Department of Surgery, Faculty of Medicine, University of British Columbia, Vancouver, BC, Canada. <sup>3</sup> Centre for Heart, Lung, and Vascular Health, School of Health and Exercise Sciences, Faculty of Health and Social Development, University of British Columbia Okanagan, Kelowna, BC, Canada. <sup>4</sup> International Collaboration on Repair Discoveries, University of British Columbia, Vancouver, BC, Canada. <sup>5</sup> Collaborative Entity for REsearching Brain Ischemia (CEREBRI), University of British Columbia, Vancouver, BC, Canada. <sup>6</sup> Anesthesia and Intensive Care, San Martino Polyclinic Hospital, IRCCS for Oncology and Neurosciences, Genoa, Italy. <sup>7</sup> Department of Surgical Sciences and Integrated Diagnostics, University of Genoa, Genoa, Italy. <sup>8</sup> Department of Medicine, University Division of Anaesthesia, University of Cambridge, Cambridge, UK. <sup>9</sup> School of Medicine and Surgery,

University of Milan-Bicocca, Monza, Italy. <sup>10</sup> Department of Intensive Care, Emergency Medicine and Anaesthesiology, Fondazione Policlinico Universitario "Agostino Gemelli", IRCCS, Università Cattolica del Sacro Cuore, Rome, Italy. <sup>11</sup> Djavad Mowafaghian Centre for Brain Health, University of British Columbia, Vancouver, BC, Canada.

## Declarations

### Conflicts of interest

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