

Oscillations in oxygen tension and insulin release of individual pancreatic *ob/ob* mouse islets

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Abstract

Aims/hypothesis. The role of beta-cell metabolism for generation of oscillatory insulin release was investigated by simultaneous measurements of oxygen tension (pO₂) and insulin release from individual islets of Langerhans.

Methods. Individual islets isolated from the *ob/ob*-mice were perfused. Insulin in the perfusate was measured with a sensitive ELISA and pO₂ with a modified Clark-type electrode inserted into the islets.

Results. In the presence of 3 mmol/l D-glucose, pO₂ was 102 ± 9 mmHg and oscillatory (0.26 ± 0.04 oscillations/min). Corresponding insulin measurements showed oscillatory release with similar periodicity (0.25 ± 0.02 oscillations/min). When the D-glucose concentration was increased to 11 mmol/l, pO₂ decreased by 30% to 72 ± 10 mmHg with maintained frequency of the oscillations. Corresponding insulin secretory rate rose from 5 ± 2 to 131 ± 16 pmol · g⁻¹ · s⁻¹ leaving the frequency of the insulin pulses unaffected. The magnitude of glucose-induced

change in pO₂ varied between islets but was positively correlated to the amount of insulin released ($r^2 = 0.85$). When 1 mmol/l tolbutamide was added to the perfusion medium containing 11 mmol/l glucose no change in average oscillatory pO₂ was observed despite a doubling in the secretory rate. When 8 mmol/l 3-oxymethyl glucose was added to perfusion medium containing 3 mmol/l D-glucose, neither pO₂ nor insulin release of the islets were changed. Temporal analysis of oscillations in pO₂ and insulin release revealed that maximum respiration correlated to maximum or close to maximum insulin release.

Conclusion/interpretation. The temporal relation between oscillations in pO₂ and insulin release supports a role for metabolic oscillations in the generation of pulsatile insulin release. [Diabetologia (2000) 43: 1313–1318]

Keywords Oscillation, metabolism, oxygen tension, insulin release, islet, glucose, tolbutamide, heterogeneity, Clark electrode, ELISA.

Insulin is released in 4–5 min pulses from isolated islets [1]. The rhythmic release of the hormone is decisive for the appearance of plasma insulin oscillations [2,3], which are important for the blood glucose lowering effect of the hormone [4, 5, 6]. Despite the importance of pulsatile insulin release, the origin of the oscillations is still not clear. Regular variations of dif-

ferent metabolic variables such as oxygen consumption, ATP:ADP ratio, lactate release and pyridine nucleotides have been measured both in intact pancreatic beta cells and in permeabilized clonal beta cells incubated in an oscillating glycolytic muscle extract [7, 8, 9, 10, 11, 12, 13]. These metabolic oscillations show similar frequencies as the insulin oscillations of isolated islets [1,9,14], which supports the concept of an oscillatory metabolism underlying pulsatile insulin release [15]. Oscillations in the cytoplasmic Ca²⁺ concentration ([Ca²⁺]_i) have also been proposed to initiate the secretory pulses. This idea was strongly supported by results from simultaneous measurements

Received: 9 March 2000 and in revised form: 19 May 2000

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of $[Ca^{2+}]_i$ and insulin release from individual islets in which oscillations in the two variables coincided [14, 16]. When it was discovered that pulsatile insulin secretion was not always accompanied by oscillatory $[Ca^{2+}]_i$ [17, 18, 19], the role of $[Ca^{2+}]_i$ as a generator of the secretory pulses became less clear. The idea of a metabolic oscillator was once again proposed although it was not known whether metabolic oscillations existed when pulsatile insulin release was not accompanied by oscillatory $[Ca^{2+}]_i$. To further investigate the role of metabolic oscillations in the generation of pulsatile insulin release we have used sensitive techniques [1,20], which enabled us to do dynamic measurements of insulin release and pO_2 from single islets of Langerhans also under conditions associated with stationary $[Ca^{2+}]_i$.

Materials and methods

Chemicals. Reagents of analytical grade and deionized water were used. Collagenase (lot no. 83963721–35), HEPES and bovine serum albumin (fraction V) were obtained from Boehringer Mannheim (Mannheim, Germany). The D-glucose, 3-oxymethyl glucose, tetramethylbenzidine and insulin-peroxidase came from Sigma (St. Louis, Mo., USA). The rat insulin standard was from Novo Nordisk (Bagsvaerd, Denmark). The IgG-certified microtitre plates were purchased from Nunc (Roskilde, Denmark). Tolbutamide was from Hoechst (Frankfurt, Germany). The mouse insulin antibodies were generated in our laboratory from guinea-pigs.

Preparation and perfusion of islets. Pancreatic islets were isolated by collagenase from 15 *ob/ob* mice [21]. Keeping and handling of the mice and experimental procedures were approved by the local animal ethics committee in accordance with NIH publication No. 85–23. Single freshly isolated islets ($n = 24$) were mounted on a cover slip coated with poly-L-lysine, which was used as the bottom of a perfusion chamber maintained at 37°C by a thermostat [14]. The islets were perfused at a rate of 150–200 μ l per min with a medium supplemented with 1 mg/ml albumin and containing (in mmol/l): NaCl 125, KCl 5.9, $MgCl_2$ 1.2, $CaCl_2$ 1.28, HEPES 25 and D-glucose 3, titrated to pH 7.4 with NaOH. After 60 min, oxygen tension was measured in the presence of 3 mmol/l D-glucose and the perfusate was collected in 20-s fractions for measurement of insulin. The time required for the perfusate to be pumped from the islet to the collection point was 120 s. This lag period has been taken into account in all calculations. In experiments where either the D-glucose concentration was increased to 11 mmol/l or 8 mmol/l 3-oxymethyl glucose was added to the perfusion medium, measurements of oxygen tension and insulin release were interrupted for 10 min after increasing the glucose concentration. After subsequent measurements for approximately 20 min, 1 mmol/l tolbutamide was added to the perfusion medium without interrupting the measurements. In experiments where 1 mmol/l tolbutamide was added to perfusion medium containing 3 mmol/l D-glucose there was no interruption in sampling.

Measurements of oxygen tension. Oxygen tension in the isolated islets was measured by a modified Clark microelectrode [20]. The tip of the microelectrode was positioned into the islets with the aid of a micromanipulator [22]. A stereomicro-

scope (Nikon, Tokyo, Japan) was used to control the penetration depth of the electrode, which was 25–50 μ m. In two experiments the tip broke and the experiments were interrupted and not analysed. In the absence of islets no changes in oxygen tension were observed when perfusing the electrode with perfusion medium, which had regular changes in the glucose or insulin concentration from 3 to 11 mmol/l and 0 to 1 pmol/l, respectively. The electrodes were polarised at –0.8 V, which gave a linear response between the oxygen tension and the electrode current. The electrical current was measured by picoampere-meters (University of Aarhus, Aarhus, Denmark). The sampling rate of the A/D converter was 4 data points per s. Averages of data points corresponding to 20 s of recordings were calculated and used for the further data presentation. The electrodes were calibrated in water saturated with $Na_2S_2O_5$ or air at 37°C before and after the experiments. The drift of the microelectrodes was less than 0.5% per h.

Measurements of insulin release. Insulin in the perfusate was assayed by a competitive ELISA with the insulin antibody immobilized directly onto the solid phase [1]. The assay showed linearity in a semilogarithmic diagram over the range of 0.1 – 100 fmol and had inter-assay and intra-assay variations of less than 10% in the specified range [1]. In one experiment the insulin assay standard curve was non-linear in the specified range and the experiment was excluded. The rate of insulin release was normalised to dry weight after freeze-drying and weighing the islets on a quartz fibre balance.

Data analysis. Frequency determination of oscillations in oxygen tension and insulin release was done by Fourier transformation on both original and autocorrelated data from 21 experiments using the Igor software (Wave Metrics, Lake Oswego, Ore., USA). In general, the relevant spectrum peak was clearly and uniquely identifiable. In all cases the corresponding area was more than three times higher than the adjacent parts of the spectrum, neglecting the extreme low frequency components derived from the drift. A sinus function was then fitted to the data. Phase shift between oxygen and insulin pulses was investigated by comparing at what time points the two variables had their peak values. The peak values were chosen in accordance with the fitted sinus function. To further investigate the temporal relation between oscillations in pO_2 and insulin release the data series of the two variables were analysed by cross-correlation. The time difference between the two oscillatory patterns was expressed in periods.

Statistical analysis. Results are presented as means \pm SEM. Differences in average oxygen tension and secretory rates were evaluated with ANOVA for repeated measurements. Linear regression analysis was used to evaluate the correlation between oxygen tension and insulin release. Paired Student's *t* test was used to evaluate the temporal differences between measurements of oxygen tension and insulin release.

Results

Oxygen tension and insulin release were measured simultaneously from individual islets of Langerhans. In the presence of 3 mmol/l D-glucose mean pO_2 was 102 ± 9 mmHg and insulin release was 5 ± 2 pmol $g^{-1} \cdot s^{-1}$ (Fig. 1, Table 1). Both oxygen tension and insulin release were oscillatory with frequencies of 0.26 ± 0.04 and 0.25 ± 0.02 oscillations/min, respec-

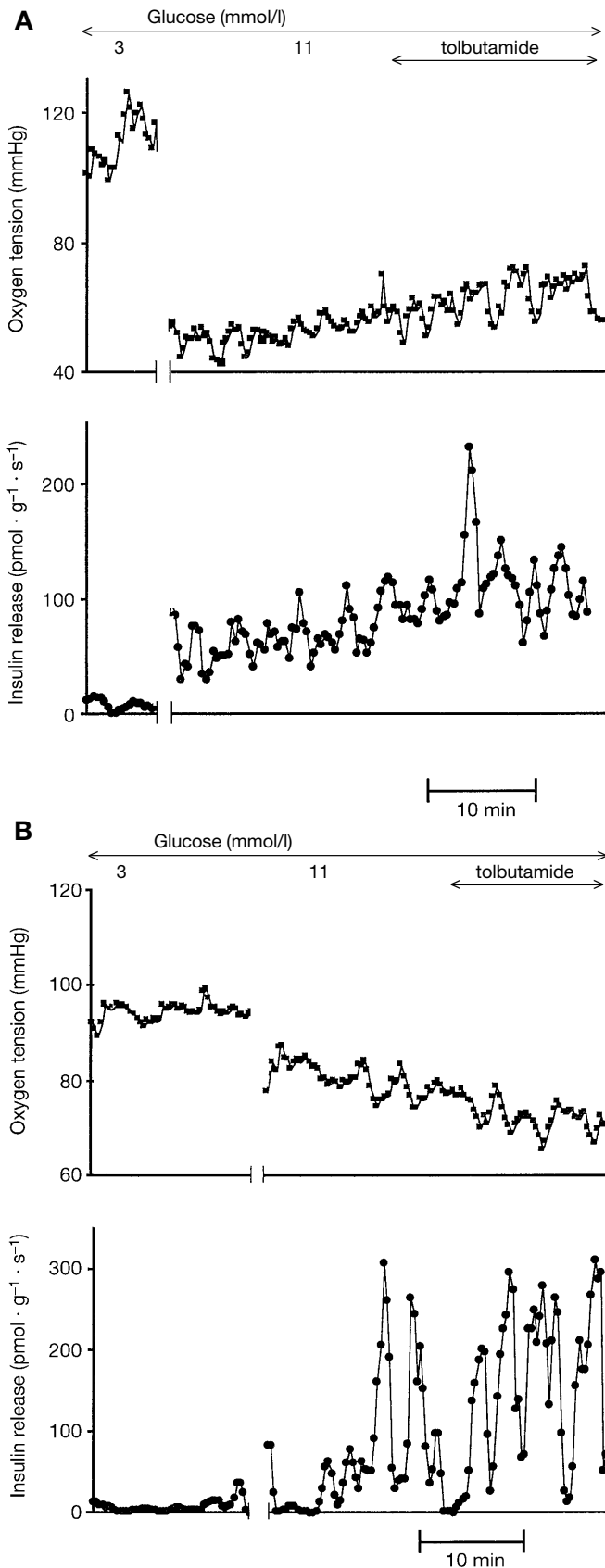


Fig. 1 A, B. Simultaneous measurements of pO_2 (top panels) and insulin release (bottom panels) in individual islets perfused in the presence of 3, 11 mmol/l D-glucose and 1 mmol/l tolbutamide. Two representative experiments out of six

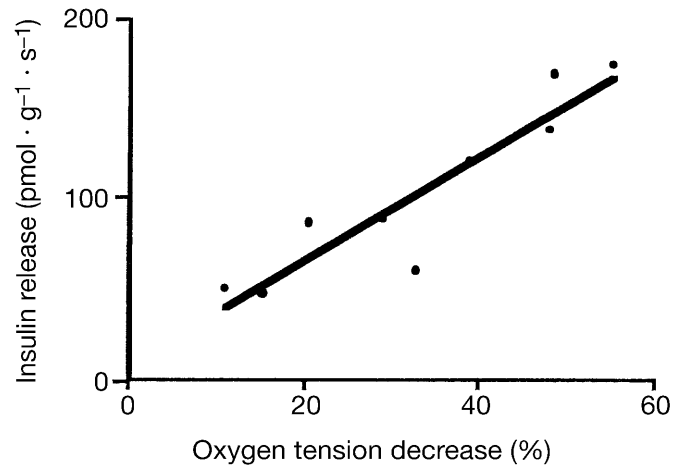


Fig. 2. Relation between glucose-induced changes in oxygen tension and insulin release. Points represent percentage change in pO_2 when the glucose concentration was raised from 3 to 11 mmol/l D-glucose compared with insulin release at 11 mmol/l D-glucose. Linear regression analysis was done on data from nine individual islets giving a first order polynomial equation $y = 287x + 9.2$ ($r^2 = 0.85$), where y represents insulin release and x decrease in oxygen tension

tively. The mean oxygen tension decreased with maintained frequency of the pO_2 oscillations when the D-glucose concentration was increased to 11 mmol/l. This was associated with an increase of the insulin release. After 10 min insulin release had increased 26-fold and pO_2 decreased by 30%. Whereas the increase in insulin release was amplitude-regulated, the decrease in oxygen tension was not associated with any change in the amplitude of the oscillations in oxygen tension (Fig. 1). Rather the pulses were superimposed on a lower average oxygen tension level.

The decrease in oxygen tension as well as the increase in insulin release caused by increasing the D-glucose concentration from 3 to 11 mmol/l varied between islets. These variations were analysed by relating the decrease in oxygen tension to the corresponding increase in insulin release for nine individual islets (Fig. 2). A linear relation ($r^2 = 0.85$) was found between the decrease in pO_2 , expressed in percentage of pO_2 at 3 mmol/l D-glucose, and the increase in insulin release when the D-glucose concentration was increased from 3 to 11 mmol/l. From the regression line the calculated value for insulin release is $9.2 \text{ pmol} \cdot \text{g}^{-1} \cdot \text{s}^{-1}$ when the pO_2 decrease is 0%, which is in agreement with the actual value at 3 mmol/l D-glucose of $5 \pm 2 \text{ pmol} \cdot \text{g}^{-1} \cdot \text{s}^{-1}$ (Table 1). The osmotic influence of increasing the sugar concentration from 3 to 11 mmol/l on insulin release and oxygen tension measurements was evaluated by adding 8 mmol/l 3-oxymethyl glucose to the perfusion containing 3 mmol/l D-glucose. No change in either oxygen tension or insulin release of the islets was observed after

Table 1. Oxygen tension and insulin release measured in isolated mouse islets in the presence of different concentrations of D-glucose and tolbutamide

D-Glucose (mmol/l)	Tolbutamide (mmol/l)	Oxygen tension		Insulin release		<i>n</i> ^c
		Mean (mmHg)	Frequency (osc/min)	Mean (pmol · g ⁻¹ · s ⁻¹)	Frequency (osc/min)	
3		102 ± 9	0.26 ± 0.04	5 ± 2	0.25 ± 0.02	12
3	1	99 ± 6	0.26 ± 0.01	30 ± 9 ^a	0.29 ± 0.01	6
11		72 ± 10 ^b	0.22 ± 0.04	131 ± 16 ^b	0.26 ± 0.03	6
11	1	75 ± 11	0.23 ± 0.02	268 ± 42 ^a	0.25 ± 0.02	6

Simultaneous measurements of pO₂ and insulin release were done in individual islets perfused in the presence of 3 and 11 mmol/l D-glucose in the presence or absence of 1 mmol/l tolbutamide.

^a*P* < 0.05 vs results in the absence of tolbutamide

^b*P* < 0.05 vs results at 3 mmol/l D-glucose

^cValues are means ± SEM calculated for the indicated number of experiments

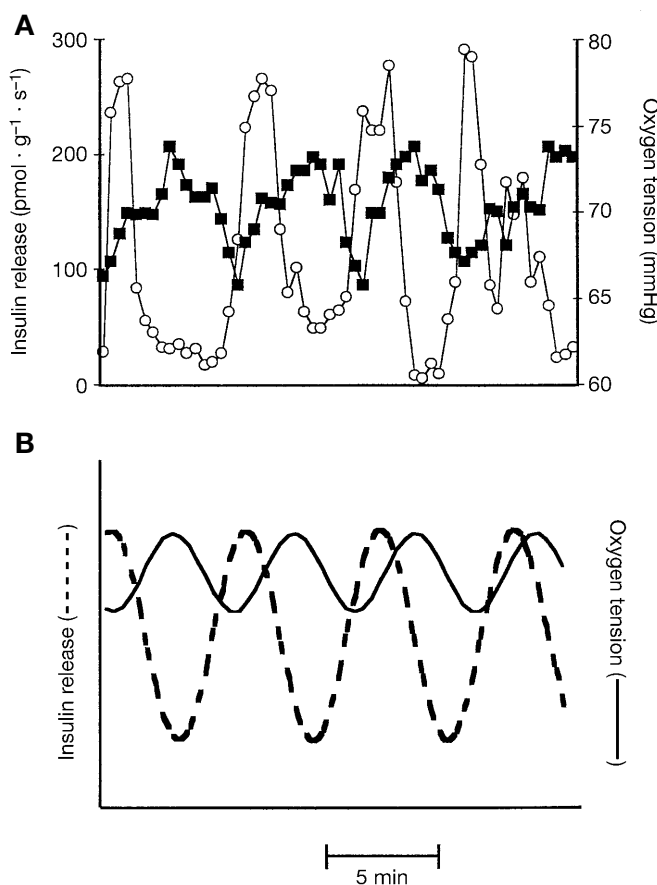


Fig. 3. **A** Simultaneous measurements of pO₂ (closed symbols) and insulin release (open symbols) from an individual mouse islet perfused in the presence of 11 mmol/l D-glucose. **B** Corresponding sinus functions are displayed for oxygen (solid line) and insulin (broken line) measurements

addition of the non-metabolisable glucose analogue (*n* = 6).

When 1 mmol/l tolbutamide was added to the perfusion medium containing 11 mmol/l D-glucose no change in pO₂ was observed despite a doubling of the secretory rate (Fig. 1, Table 1). Tolbutamide (1 mmol/l) was also added to islets perfused in the presence of 3 mmol/l glucose (Table 1). Although no

statistically significant change in pO₂ was observed, the amplitude of the insulin pulses increased sixfold.

Frequencies of oscillations in pO₂ and insulin release were equal under all conditions tested (Fig. 1, Table 1). Phase-shift analysis of 40 identified peaks from 14 different experiments showed, however, that peaks of oxygen and insulin oscillations did not coincide but were time-shifted (*p* < 0.01). Cross-correlation showed that peaks in pO₂ preceded peaks in insulin release with 0.63 ± 0.02 periods. Maximum respiration (nadir in pO₂) occurred just before maximum insulin secretion. This relation is illustrated in Figure 3 where simultaneous measurements of pO₂ and insulin release in the presence of 11 mmol/l glucose are presented.

Discussion

In our study the role of changes in pO₂ for the generation of pulsatile insulin release in single islets of Langerhans was further investigated by simultaneous measurements of pO₂ with a modified Clark electrode [20] and insulin release with a sensitive ELISA [1]. The combination of sensitive techniques has previously been used to evaluate the role of [Ca²⁺]_i for pulsatile insulin release from single islets [14,16,18,19,23].

Attempts have previously been made to correlate oscillatory metabolism and hormonal secretion by simultaneously measuring lactate and insulin release from groups of islets [10]. Both the sampling time of 3.3 min and the use of approximately 200 islets in each experiment made it, however, difficult to study the correlation between these oscillations with approximately 5-min duration. Oxygen measurements of the islet had previously required groups of islets [9,24,25,26] or large piscine islet organs [27]. Thus, oscillatory oxygen consumption and insulin release had to be studied in parallel using multiple islets and separate perfusion systems for the two variables [9]. Notably, periodic fluctuations of both variables could be observed. It is, however, difficult to draw any firm

conclusions from these previous studies about the pulsatile behaviour of isolated islets because the metabolic and secretory phenomena should preferably be studied simultaneously in connected pancreatic beta cells [28]. Nevertheless, the results from these and other metabolic studies both with clonal beta cells and isolated islets [7,8,11] provide evidence suggesting that an oscillating metabolism is an important factor for the generation of pulsatile insulin release [15].

Monitoring pO_2 from individual islets with the aid of an oxygen microsensor [12,13,24] has made it possible to observe regular fluctuations in pO_2 from individual islets. In all these studies a small oxygen electrode, with a tip diameter of 2–5 μm has been used. The electrode used by another group [12,13] has a reference electrode placed outside the electrode as described by Davies and Brink [29]. Our electrode [22] is a Clark-type electrode with the reference electrode behind the same membrane as the sensing cathode as described by Clark [30]. The shielding electrolyte around the sensing cathode stabilises the electrode against surrounding electronic disturbances. Our electrode also has a guard-electrode behind the sensing cathode, which makes the measurements extremely stable as it eliminates any oxygen coming from behind the sensing cathode from the electrolyte reservoir. Both electrodes recorded similar values for frequency and amplitude of the pulses in oxygen tension microsensor [12,13]. The discrepancy between our recordings of average oxygen tension at 11 mmol/l glucose compared with those reported at 10 mmol/l of the sugar [12] is probably because of differences in islet size rather than in the electrodes as variations in islet size affect oxygen tension measurements in individual islet [12]. With our enhanced Clark-like oxygen microsensor in combination with a sensitive ELISA for insulin [1] we made simultaneous measurements of pO_2 and insulin release from individual islets. Oscillations in pO_2 and insulin release with the same frequency were recorded. When oscillations in oxygen tension and insulin release were cross-correlated and analysed for a temporal relation, the two variables were approximately half a cycle apart. A nadir in an oscillation of pO_2 , which corresponds to maximum respiration, coincided with a peak or just before a peak of an insulin pulse. The oscillatory activity of the two variables were also present at 3 mmol/l glucose or in the presence of tolbutamide when $[Ca^{2+}]_i$ is reported to be stable [17,18,19]. This strengthens the idea that metabolic oscillations are important for oscillatory insulin and makes metabolic oscillations a more plausible candidate for the generation of pulsatile insulin release at least when $[Ca^{2+}]_i$ is non-oscillatory.

Glucose is known to modulate the amplitude of the insulin oscillations in vivo and in vitro without affecting the oscillation frequency [1,31,32]. It is evi-

dent from the pO_2 traces in this and another study [12] that the frequency of the oxygen fluctuations did not change when the glucose concentration was altered. The amplitude of the pO_2 changes did not, however, seem to change either although the corresponding measurements of insulin release showed amplitude-modulation of the insulin pulses. Rather a new level was attained from which pO_2 oscillations with similar amplitude and frequency were superimposed. This could be because the islets were perfused in our study. Under quiescent conditions oscillations in oxygen tension are more pronounced [12]. Furthermore, as pO_2 had to be measured in an open system with several diffusion-related variables it is difficult to judge whether the amplitudes of the pO_2 fluctuations seen reflect quantitatively the actual changes in islet oxygen consumption. Alternatively, glucose-induced amplification of the amplitude of pulsatile insulin release could be related to enhancement of other triggering factors, e. g. $[Ca^{2+}]_i$ or molecules derived from glucose metabolism.

The variability observed in the glucose-induced changes in the level of oxygen tension correlated with changes in the amplitude of the insulin pulses and exemplifies the close linkage between glucose metabolism and insulin release [24,25,33,34,35]. The increase in the D-glucose concentration from 3 to 11 mmol/l induced a wide range in percentage decrease in pO_2 (15–55 %) with a corresponding range in insulin release (40–190 $\text{pmol} \cdot \text{g}^{-1} \cdot \text{s}^{-1}$) in different islets. Differences in secretorial response between islets has been shown recently [36]. Metabolic and secretory inter-islet variability could be explained by differences in the proportions of beta, alpha, delta and pp cells constituting the islet [37]. In this study we obtained, however, an equal and high amount of beta cells by using islets of similar size from the *ob/ob* mouse. These islets consist of more than 90 % beta cells [22]. It is reasonable to assume that metabolic differences with correlation to secretory activity cannot only be detected in isolated beta cells [38] but also in intact islets.

The correspondence in frequencies and temporal relation between oscillations in insulin release and oxygen tension suggest a close linkage between oscillations in metabolism of the pancreatic beta cell and the generation of pulsatile insulin release.

Acknowledgements. The study was supported by grants from the Swedish Medical Research Council (12X-11203), the Swedish Diabetes Association, the Novo Nordisk Foundation, the Family Ernfors Foundation, the Gunvor and Josef Anér Foundation, the Marcus and Amalia Wallenberg Foundation and the Swedish Society for Medical Research.

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