Mitosis Detection in Breast Cancer Histology Images with Deep Neural Networks

Dan C. Cireşan, Alessandro Giusti, Luca M. Gambardella, and Jürgen Schmidhuber

IDSIA, Dalle Molle Institute for Artificial Intelligence, USI-SUPSI, Lugano, Switzerland {dan,alessandrog,luca,juergen}@idsia.ch

Abstract. We use deep max-pooling convolutional neural networks to detect mitosis in breast histology images. The networks are trained to classify each pixel in the images, using as context a patch centered on the pixel. Simple postprocessing is then applied to the network output. Our approach won the ICPR 2012 mitosis detection competition, outperforming other contestants by a significant margin.

1 Introduction

The number of mitotic figures visible in histology sections is an important indicator for cancer screening and assessment. Normally, the count is performed manually by histologists, but automating the process could reduce its time and costs (thus making it more accessible), minimize errors, and improve the comparability of results obtained in different labs.

Mitosis detection is very hard. In fact, mitosis is a complex process during which a cell nucleus undergoes various transformations. In addition, different image areas are characterized by different tissue types, which exhibit highly variable appearance. A large amount of different structures can be observed in histology images stained with *Hematosin & Eosin*, and in particular many dark-blue spots, most of which correspond to cell nuclei. Only a subset of them is in a mitotic phase and must be detected. In most stages a mitotic nucleus looks very much like a non-mitotic one, or like other dark-blue spots, to the point that a human observer without extensive training cannot differentiate them (Figure 1). As an additional complication, in later stages of the mitosis process a nucleus may appear to split in two dark-blue spots, to be counted as one single mitosis.

Our approach is conceptually very simple. We use a supervised Deep Neural Network (DNN) as a powerful pixel classifier. The DNN is a max-pooling (MP) convolutional neural network (CNN). It directly operates on raw RGB data sampled from a square patch of the source image, centered on the pixel itself. The DNN is trained to differentiate patches with a mitotic nucleus close to the center from all other windows. Mitosis in unseen images are detected by applying the classifier on a sliding window, and postprocessing its outputs with simple techniques. Because the DNN operates on raw pixel values, no human input is needed: on the contrary, the DNN automatically learns a set of visual features from the training data.

Our main contribution is a new, important, practical application of DNN, which recently produced outstanding results in image classification, segmentation and detection. Our approach is tested on a publicly available dataset. It significantly outperforms all competing techniques, with manageable computational effort: processing a 4MPixel image requires few minutes on a standard laptop. Supplementary material for this paper is available at http://bit.ly/18681Km.

Related Work. Different flavors of CNN have been used for decades to classify objects. Introduced in 1980 [6] and gradually improved over the next two decades [11,1,17], they unfold their full potential when combined with MP and made both deep and wide [3,4]. They excel on data sets ranging from handwritten characters [3] to complex cluttered images (NORB) [4], faces, and natural color images. DNN-based pattern recognition is not limited to object classification, but can be used for detection as well. Recently, DNN were used to segment images of neural tissue in Electron Microscopy [2] and natural scenes [5].

Many detection problems in biomedical images are solved by means of pixel classifiers, and are characterized by the relatively obvious appearance of the objects to be detected. Difficulties may arise due to clumping/touching objects which may be hard to separate and count [13]. Mitosis detection is different. While mitosis are normally rare and well-separated, they are very hard to differentiate from non-mitotic nuclei.

2 Methods

Given an input RGB image I, the problem is to find a set $D = \{d_1, d_2, \ldots, d_N\}$ of detections, each reporting the centroid coordinates for a single mitosis. The problem is solved by training a detector on training images with given ground truth information about the centroid of each visible mitosis. Each pixel is assigned one of two possible classes, *mitosis* or *non-mitosis*, the former to pixels at (or close to) mitosis centroids, the latter to all other pixels. Our detector is a DNN-based pixel classifier. For any given pixel p, the DNN predicts its class using raw RGB values in a square image window centered on p (Figure 1). Windows of class *mitosis* contain a visible mitosis around the window's center. Others contain off-center or no mitosis.

Deep Neural Netwok Architecture. A DNN [4] is a feed-forward net made of successive pairs of convolutional and max-pooling layers, followed by several fully connected layers. Raw pixel intensities of the input image are passed through this general, hierarchical feature extractor. The feature vector it produces is classified by the fully connected layers. All weights are optimized through minimization of the misclassification error over the training set.

Each **convolutional Layer** performs a 2D convolution of its input maps with a rectangular filter. The filter is applied in every possible position of the input map. If the previous layer contains more than one map, the activations of the corresponding convolutions are summed up, then passed through a nonlinear activation function.

One of the architectural differences between our DNN and previous CNN [11] are **max-pooling (MP) layers** [14,16] instead of sub-sampling layers. Their outputs are given by the maximum activations over non-overlapping square regions. MP layers are fixed, non-trainable layers selecting the winning features. Typical DNN also are much wider than previous CNN, with many more connections, weights and non-linearities.

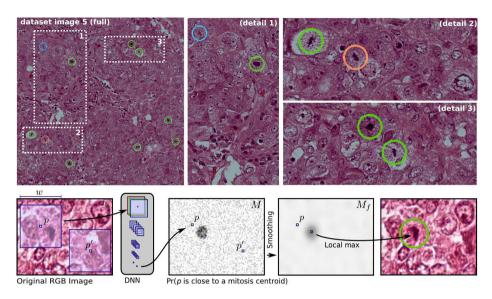


Fig. 1. Top left: one image (4 MPixels) corresponding to one of the 50 high power fields represented in the dataset. Our detected mitosis are circled green (true positives) and red (false positives); cyan denotes mitosis not detected by our approach. Top right: details of three areas (full-size results on the whole dataset in supplementary material). Note the challenging appearance of mitotic nuclei and other very similar non-mitotic structures. Bottom: overview of our detection approach.

After several pairs of convolutional and MP layers, one **fully connected layer** further mixes the outputs into a feature vector. The output layer is a simple fully connected layer with one neuron per class (two for this problem), activated by a softmax function, thus ensuring that each neuron's output activation can be interpreted as the probability of a particular input belonging to that class.

Training a Detector. Using ground truth data, we label each pixel of each training image as either mitosis (when closer than d pixels to the centroid of a mitosis) or non-mitosis (elsewhere). Then, we build a training set in which each instance maps a square window of RGB values sampled from the original image to the class of the central pixel. If a window lies partly outside of the image boundary, the missing pixels are synthesized by mirroring.

The mitosis detection problem is rotationally invariant. Therefore, additional training instances are generated by transforming windows within the training set by applying arbitrary rotations and/or mirroring. This is especially important considering that there are extremely few mitosis examples in the training set.

Processing a Testing Image. To process an unseen image I, we apply the DNN to all windows whose central pixel is within the image boundaries. Pixels outside of the image boundaries are again synthesized by mirroring. This yields a probability map M, in which each pixel is assigned a probability of being close to the centroid of a

mitosis. Ideally, we expect M to be zero everywhere except within d-pixel-radius disks centered on each mitosis. In practice, M is extremely noisy. Therefore, M is convolved with a d-pixel-radius disk kernel, which yields a smoothed probability map M_f ; the local maxima of M_f are expected to lie at the disk centers in M, i.e., at the centroids of each mitosis.

To obtain a set of detections D_I for image I, we first initialize $D_I \leftarrow \emptyset$, then iterate the following two steps until no pixel in M_f exceeds a given threshold t.

- Let p_m be the pixel with the largest value in M_f ; $D_I = D_I \cup (p_m, M_f(p_m))$.
- $-M_f(p) \leftarrow 0$ for each $p:|p-p_m| < 2d$ (non-maxima suppression).

This yields a (possibly empty) set D_I (depending on threshold t) containing the detected centroids of all mitosis in image I, as well as their respective score.

Exploiting Multiple Nets and Rotational Invariance. Because the DNN classifier is very flexible and has many degrees of freedom, it is expected to exhibit large variance and low bias [7]. In fact, in related work [2] it was observed that large nets with different architectures, even when trained on the same dataset, tend to yield significantly different outputs, especially for challenging image parts. We reduce such variance by averaging the outputs of multiple classifiers with different architectures. Moreover, we exploit rotational invariance by separately processing rotated and mirrored versions of each input image, and averaging their results.

3 Materials, Experiments and Results

Dataset and Performance Measures. We evaluate our method on the public MITOS dataset including 50 images corresponding to 50 high-power fields in 5 different biopsy slides stained with Hematosin & Eosin. A total of about 300 mitosis are visible in MITOS. Each field represents a $512\times512\mu\text{m}^2$ area, and is acquired using three different setups: two slide scanners and a multispectral microscope. Here we consider images acquired by the Aperio XT scanner, the most widespread and accessible solution among the three. It has a resolution of $0.2456\mu\text{m}$ per pixel, resulting in a 2084×2084 RGB image for each field. Expert pathologists manually annotated all visible mitosis.

We partition the 50 images into three subsets: *T1* (26 images), *T2* (9 images), and *T3* (15 images). *T3* coincides with the *evaluation images* for the 2012 ICPR Mitosis Detection Contest. Its ground truth was withheld from contestants until the end of the contest. *T3* is exclusively used for computing our performance measures once, to ensure a fair comparison with other algorithms.

Given a set of detections for dataset T3, according to the contest criteria, we count the number $N_{\rm TP}$ of True Positives (i.e. detections whose coordinates are closer than $5\mu{\rm m}(20~{\rm px})$ from the ground truth centroid), False Positives ($N_{\rm FP}$) and False Negatives ($N_{\rm FN}$). We compute the following performance measures: recall ($R=N_{\rm TP}/(N_{\rm TP}+N_{\rm FN})$), precision ($P=N_{\rm TP}/(N_{\rm TP}+N_{\rm FP})$) and F_1 score ($F_1=2PR/(P+R)$).

We randomly split the remaining 35 images, for which ground truth was available, in two disjoint sets T1 (training) and T2 (validation). Detectors trained on the former are evaluated on the latter for determining the threshold yielding the largest F-score.

Building the Detector. For images in T1 and T2, the *mitosis* class is assigned to all windows whose center pixel is closer than d=10 pixels to the centroid of a ground-truth mitosis; all remaining windows are given the *non-mitosis* class. This results in a total of roughly 66000 *mitosis* pixels and 151 million *non-mitosis* pixels. Note that, among all *non-mitosis* pixels, only a tiny fraction (i.e. those close to non-mitotic nuclei and similarly looking structures) represent interesting instances. In contrast, the largest part of the image area is covered by background pixels far from any nucleus, whose class *(non-mitosis)* is quite trivial to determine. If training instances for class *non-mitosis* were uniformly sampled from images, most of the training effort would be wasted.

Other approaches [18,8,12,20] address this issue by first detecting all nuclei, then classifying each nucleus separately as mitotic or non-mitotic. We follow a different, simpler approach, which does not need any additional ground-truth information and relies on a single trained detector. In particular, we build our training set so that the relatively rare challenging *non-mitosis* instances are well represented, whereas instances obviously belonging to class *non-mitosis* (which prevail in the input images) appear only rarely. This approach, loosely inspired by boosting techniques, allows us to spend most of the training time in learning important differences among mitotic and non-mitotic nuclei. We adopt a general approach to building such a training set, without relying on problem-specific heuristics.

- We build a small training set Sd, which includes all 66000 mitosis instances and the same number of non-mitosis instances, uniformly sampled from the 151 million non-mitosis pixels.
- We use Sd to briefly train a simple DNN classifier Cd. Because Cd is trained on a limited training set in which challenging non-mitosis instances are severely underrepresented, it tends to misclassify most non-mitotic nuclei as class mitosis.
- We apply Cd to all images in T1 and T2. Let D(p) denote the *mitosis* probability that Cd assigns to pixel p. D(p) will be large for challenging *non-mitosis* pixels.

Table 1. 13-layer architecture for network DNN1 (left) and 11-layer architecture for network DNN2 (right). Layer type: I - input, C - convolutional, MP - max-pooling, FC - fully-connected.

Laye	er Type	Maps	Filter	Weights (Connections						
		and neurons	size			Laye	er Type				Connections
0	I	3M x 101x101N	_	_	_			and neurons	size		
1	C	16M x 100x100N	2x2	208	2080000	0	I	3M x 101x101N	_	_	_
2	MP	16M x 50x50N	2x2	_	_	1	C	16M x 98x98N	4x4	784	7529536
3	C	16M x 48x48N	3x3	2320	5345280	2	MP	16M x 49x49N	2x2	_	_
4	MP	16M x 24x24N	2x2	_	_	3	C	16M x 46x46N	4x4	4112	8700992
5	C	16M x 22x22N	3x3	2320	1122880	4	MP	16M x 23x23N	2x2	_	_
6	MP	16M x 11x11N	2x2	_	_	5	C	16M x 20x20N	4x4	4112	1644800
7	C	16M x 10x10N	2x2	1040	104000	6	MP	16M x 10x10N	2x2	_	_
8	MP	16M x 5x5N	2x2	_	_	7	C	16M x 8x8N	3x3	2320	148480
9	C	16M x 4x4N	2x2	1040	16640	8	MP	16M x 4x4N	2x2	_	_
10	MP	16M x 2x2N	2x2	_	_	9	FC	100N	1x1	25700	25700
11	FC	100N	1x1	6500	6500	10	FC	2N	1x1	202	202
12	FC	2N	1x1	202	202						

- We build the actual training set, composed by 1 million instances, which includes all *mitosis* pixels (6.6% of the training instances). The remaining 95.4% is sampled from *non-mitosis* pixels by assigning to each pixel p a weight D(p).

The resulting optimized training set is used for learning two nets DNN1 and DNN2 (architectures outlined in Table 1). Because the problem is rotationally invariant, during each training epoch each patch is subject to a random rotation around its center and a 50% chance of mirroring, in order to artificially augment the training set.

Each unseen image I is processed 16 times: each of the two nets is applied to each of 8 variations of the input image, namely: rotations by $k \cdot 90^{\circ}$, k = 0, 1, 2, 3, with and without mirroring. For each variation, the resulting map is subject to the inverse transformation, to match the input image. The resulting 16 maps are averaged, yielding M, from which a set of detections D_I is determined as described in Section 2.

The whole procedure is first performed by training the nets on data from TI and detecting mitosis in T2 images. The threshold yielding the largest F_1 score (t' = 0.35) is then determined. The final detector is obtained by training the two nets on data from TI and T2, and evaluated on T3.

Training each network requires one day of computation with an optimized GPU implementation. Less than 30 epochs are needed to reach a minimum on validation data. For detecting mitosis in a single image, our MATLAB implementation required 31 seconds to apply each network on each input variation, which amounts to a total time of roughly 8 minutes per image. Significantly faster results can obtained by averaging fewer variations with minimal performance loss (see Table 2).

Performance and Comparison. Performance results on the T3 dataset are reported in Table 2. Our approach yields an F-score of 0.782, significantly higher than the F-score obtained by the closest competitor (0.718). The same data is plotted in the Precision-Recall plane in Figure 3.

The choice of the detection threshold t affects the resulting F-score: Figure 3 (right) shows that the parameter is not particularly critical, since even significant deviations from t' result in limited performance loss.

Table 2. Performance results for our approach (**DNN**) compared with competing approaches [15]. We also report the performance of faster but less accurate versions of our approach, namely: **DNN**f12, which averages the results of nets DNN1 and DNN2 without computing input variations (1 minute per image), and **DNN**f1, which is computed only from the result of DNN1 (31s per image).

method	precision recall	F ₁ score	method	precision 1	recall	F_1 score
DNN	0.88 0.70	0.782	NUS	0.63	0.40	0.490
DNNf12	0.85 0.68	0.758	ISIK [19]	0.28	0.68	0.397
DNNf1	0.78 0.72	0.751	ETH-HEILDERBERG [18]	0.14	0.80	0.374
IPAL [9]	0.69 0.74	0.718	OKAN-IRISA-LIAMA	0.78	0.22	0.343
SUTECH	0.70 0.72	0.709	IITG	0.17	0.46	0.255
NEC [12]	0.74 0.59	0.659	DREXEL	0.14	0.21	0.172
UTRECHT [20]	0.51 0.68	0.583	ВП	0.10	0.32	0.156
WARWICK [10]	0.46 0.57	0.513	QATAR	0.00	0.94	0.005

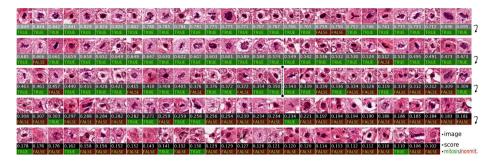
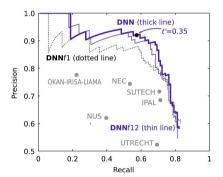


Fig. 2. All 143 detections (29 per row) on T3 with scores larger than 0.1, sorted by descending score. For each, we report the corresponding image patch, score, and whether it is a mitosis (TRUE, bright green background) or a non-mitosis (FALSE, dark red background). Vertical dotted line for score 0.35 reports the detection threshold t' determined on T2.



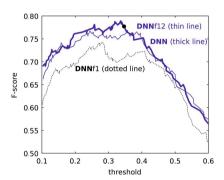


Fig. 3. Left: Performance of our approach compared to others in the PR plane. Right: sensitivity to the choice of threshold.

4 Conclusion and Future Works

We presented an approach for mitosis detection that outperformed all competitors on the first public annotated dataset of breast cancer histology images.

Future work will aim at validating our approach on larger datasets, and comparing its performance to the one of expert histologists, with the ultimate goal of gradually bringing automated mitosis detection into clinical practice.

Acknowledgments. This work was partially supported by the *Supervised Deep / Recurrent Nets* SNF grant, Project Code 140399.

References

 Behnke, S.: Hierarchical Neural Networks for Image Interpretation. LNCS, vol. 2766. Springer, Heidelberg (2003) 412

- Ciresan, D.C., Giusti, A., Gambardella, L.M., Schmidhuber, J.: Deep Neural Networks Segment Neuronal Membranes in Electron Microscopy Images. In: Neural Information Processing Systems, pp. 2852–2860 (2012) 412, 414
- Ciresan, D.C., Meier, U., Masci, J., Gambardella, L.M., Schmidhuber, J.: Flexible, High Performance Convolutional Neural Networks for Image Classification. In: International Joint Conference on Artificial Intelligence, pp. 1237–1242 (2011) 412
- Ciresan, D.C., Meier, U., Schmidhuber, J.: Multi-column Deep Neural Networks for Image Classification. In: Computer Vision and Pattern Recognition, pp. 3642–3649 (2012) 412
- Farabet, C., Couprie, C., Najman, L., LeCun, Y.: Learning Hierarchical Features for Scene Labeling. IEEE Transactions on Pattern Analysis and Machine Intelligence (in press, 2013) 412
- Fukushima, K.: Neocognitron: A self-organizing neural network for a mechanism of pattern recognition unaffected by shift in position. Biological Cybernetics 36(4), 193–202 (1980) 412
- Geman, S., Bienenstock, E., Doursat, R.: Neural networks and the bias/variance dilemma. Neural Computation 4(1), 1–58 (1992) 414
- Huang, C., Hwee, K.: Automated Mitosis Detection Based on Exclusive Independent Component Analysis. In: Proc. ICPR 2012 (2012) 415
- Irshad, H.: Automated mitosis detection in histopathology using morphological and multichannel statistics features. Journal of Pathology Informatics 4(1) (2013) 416
- Khan, A., ElDaly, H., Rajpoot, N.: A gamma-gaussian mixture model for detection of mitotic cells in breast cancer histopathology images. Journal of Pathology Informatics 4(1) (2013) 416
- LeCun, Y., Bottou, L., Bengio, Y., Haffner, P.: Gradient-Based Learning Applied to Document Recognition. Proceedings of the IEEE 86(11), 2278–2324 (1998) 412
- Malon, C., Cosatto, E.: Classification of mitotic figures with convolutional neural networks and seeded blob features. Journal of Pathology Informatics 4(1) (2013) 415, 416
- Pan, J., Kanade, T., Chen, M.: Heterogeneous conditional random field: Realizing joint detection and segmentation of cell regions in microscopic images. In: 2010 IEEE Conference on Computer Vision and Pattern Recognition, pp. 2940–2947. IEEE (2010) 412
- Riesenhuber, M., Poggio, T.: Hierarchical models of object recognition in cortex. Nat. Neurosci. 2(11), 1019–1025 (1999) 412
- Roux, L., Racoceanu, D., Loménie, N., Kulikova, M., Irshad, H., Klossa, J., Capron, F., Genestie, C., Naour, G.L., Gurcan, M.N.: Mitosis detection in breast cancer histological images An ICPR 2012 contest. Journal of Pathology Informatics 4(1) (2013) 416
- Scherer, D., Müller, A., Behnke, S.: Evaluation of Pooling Operations in Convolutional Architectures for Object Recognition. In: International Conference on Artificial Neural Networks (2010) 412
- Simard, P.Y., Steinkraus, D., Platt, J.C.: Best practices for convolutional neural networks applied to visual document analysis. In: Seventh International Conference on Document Analysis and Recognition, pp. 958–963 (2003) 412
- Sommer, C., Fiaschi, L., Heidelberg, H., Hamprecht, F., Gerlich, D.: Learning-based mitotic cell detection in histopathological images. In: Proc. ICPR 2012 (2012) 415, 416
- Tek, F.: Mitosis detection using generic features and an ensemble of cascade adaboosts. Journal of Pathology Informatics 4(1) (2013) 416
- Veta, M., van Diestb, P., Pluim, J.: Detecting mitotic figures in breast cancer histopathology images. In: Proc. of SPIE Medical Imaging (2013) 415, 416