

Covalently-linked insulin dimers: their metabolism and biological effects in vivo as partial competitive antagonists of insulin clearance

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Summary. The biological properties of three covalently-linked insulin dimers were studied in greyhounds. Constant infusions showed that the plasma distribution kinetics were slower for the dimers than for insulin. The metabolic clearance rates of the three dimers (10.3 ± 0.4 , 8.8 ± 0.5 , 8.2 ± 0.5 ml · min⁻¹ · kg⁻¹; mean \pm SEM) were significantly lower than that of insulin (19 ± 0.8 ml · min⁻¹ · kg⁻¹), and their hypoglycaemic effects (11.2%, 3% and 0.3%) were markedly reduced compared with their lipogenic potencies in vitro (80%, 30% and 13%, respectively). A low dose infusion of insulin or an equipotent dose of one of the dimers significantly prolonged the effects of an insulin bolus on plasma glucose but not on non-esterified fatty acids. The apparent distribution space (106.4 ± 11.9 ml/kg)

and clearance rate (14.7 ± 0.5 ml · min⁻¹ · kg⁻¹) of an insulin bolus were significantly reduced by one dimer (44.5 ± 8.4 ml/kg and 10.7 ± 2.8 ml · min⁻¹ · kg⁻¹) but not by the equipotent insulin infusion (102.7 ± 8.2 ml/kg and 16.4 ± 0.07 ml · min⁻¹ · kg⁻¹). The apparent partial competitive antagonism of insulin by the dimers that has been reported in vitro can be observed in vivo, in that antagonism of insulin metabolism was directly demonstrated with one of the dimers.

Key words: Chemically-modified insulins, insulin structure-function, bioactivity and metabolism in vivo, competitive antagonism, hypoglycaemia, non-esterified fatty acids.

For chemically-modified monomeric insulins close correlations have been reported between biological properties in vivo and receptor binding affinities or biochemical responses in vitro [1]. Moreover, insulin derivatives with modifications in or near the putative receptor binding region (A1,5,19,21 and B12,16,22–26) [2, 3] exhibited parallel reductions in their rates of metabolism and hypoglycaemic potencies, whereas those insulins modified at other residues, such as at B1 or B29, retained full or nearly full metabolism and biological expressions [4]. These studies suggest highly specific structural requirements for insulin metabolism and action.

We have previously reported that covalently-linked insulin dimers possessed unusual properties in vitro. In particular, their binding affinities for insulin receptors in various tissues were markedly higher than their lipogenic or anti-lipolytic potencies in isolated rat adipocytes [5, 6]. We have now studied three dimers in greyhounds to determine the physiological implications of these unusual features. Since the observations in vitro suggested that the dimers behaved as partial antagonists of insulin, this aspect was also investigated directly in vivo with one of the dimers.

Materials and methods

Three covalently-linked insulin dimers were prepared and kindly donated by Drs. A. Schüttler and D. Brandenburg, Deutsches Wollforschungsinstitut, Aachen, FRG [7] (N^{B1}, N^{B29}-suberoyl-insulin dimer (B1–B'29 D), N^{B1}, B^{B1}-suberoyl-insulin dimer (B1–B'1 D), and N^{B29}, N^{B29}-suberoyl-insulin dimer (B29–B'29 D)). Highly purified bovine insulin was supplied by the same group, and porcine insulin by Novo, Copenhagen. For intravenous administration, materials were in isotonic saline (0.154 mol/l) containing 0.5% human serum albumin.

Experimental protocols

Mature greyhounds of both sexes (weight 26.7–36 kg) were anaesthetised intravenously with sodium pentobarbitone (30 g/kg body weight) after an overnight fast. Body temperature was maintained by a warming pad and the dogs were artificially ventilated to a constant end-tidal CO₂ concentration of 4–5%, as measured by an infra-red capnograph (Godart, Bilthoven, The Netherlands). After 30 min for baseline sampling, dimer was infused into a saphenous vein at a single constant rate for 3.5 h at either 1.0–1.5 pmol · min⁻¹ · kg⁻¹ (low dose) or 2.8–6.2 pmol · min⁻¹ · kg⁻¹ (high dose). Sampling from a jugular vein continued for 60 min after termination of the infusion. Two or three experiments were performed at each dose with each dimer. On the assumption that each half of a dimer could be a potentially active insulin molecule, at each dose level bovine insulin was infused at approximately twice the molar rate of the dimers. During insulin infusion, dangerous hypoglycaemia was prevented by limiting the time of

the low-dose infusion ($2.7\text{--}3.6\text{ pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$) to 2 h, and by using a simple glucose clamp to maintain plasma glucose concentrations at 3 mmol/l with the high-dose infusion ($8.2\text{--}14.1\text{ pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$).

In a second set of experiments with non-anaesthetised greyhounds (after an overnight fast), either saline (0.154 mol/l) or equipotent doses of insulin or B1-B'29 D were infused in the presence of a bolus of insulin to detect interaction between insulin and the dimer. The dose of insulin that was empirically found to be equipotent with B1-B'29 D at $4.90\pm 0.46\text{ pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$ was $1.40\pm 0.08\text{ pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$ (Fig. 1). The dogs showed no outward signs of stress during the experiments, which consisted of a priming dose of $335\pm 19\text{ pmol}$ insulin or $1302\pm 153\text{ pmol}$ B1-B'29 D followed by a 90-min constant infusion (into a cephalic vein) of insulin, dimer, or saline. A bolus injection of porcine insulin 173 or 700 pmol/kg body weight was administered 30 min into the infusion. Sampling at 5-min intervals from a saphenous vein began immediately before the infusion and continued for 15 min after termination, with an additional sample 2 min after the bolus injection.

Assay methods

Plasma glucose concentration was measured by a glucose oxidase method (Yellow Springs Instruments glucose analyser, Yellow Springs, Ohio, USA); plasma non-esterified fatty acids (NEFA) were determined by the method of Dole and Meinertz [8]; and immunoreactive insulin or dimer levels were measured by a modification [9] of a double-antibody radioimmunoassay [10] (using charcoal-treated dog serum in place of human serum). An anti-insulin serum was selected that cross-reacted equally well with equal masses of insulin and of the dimers. Samples from the interaction experiments that contained a mixture of insulin and B1-B'29 D showed the same cross-reactivity with the antiserum as did equal masses of the individual materials. Bovine insulin was radiolabelled as previously described [11].

Calculations

The initial half-disappearance time of all materials studied ($t_{1/2}$) was derived graphically from a semi-logarithmic plot of the serum disappearance curve after termination of the infusion. Metabolic clearance rate (MCR) and apparent distribution space (DS) were determined from the constant-infusion data.

$$\text{MCR (ml}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}) = \frac{\text{infusion rate (pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1})}{\text{steady-state analogue level (pmol/ml)}}$$

$$\text{DS (ml/kg)} = \frac{\text{MCR (ml}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}) \times t_{1/2} \text{ (min)}}{0.693}$$

Metabolic clearance rates and apparent distribution spaces were determined from the bolus data after subtraction of background infusion values and analysis of the disappearance curves by a double exponential curve-fitting program written by Dr. M. D. Baron for use on a Z-80A-based microcomputer.

$$\text{MCR (ml}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}) = \frac{\text{dose (pmol)}}{\text{area under curve (pmol}\cdot\text{ml}^{-1}\cdot\text{min}) \times \text{dog weight (kg)}}$$

$$\text{DS (ml}\cdot\text{kg}^{-1}) = \frac{\text{dose (pmol)}}{\text{sum of 2 y-intercepts (pmol/ml)} \times \text{dog weight (kg)}}$$

Biopotencies in vivo of chemically-modified insulins have been reported significantly higher when hypoglycaemic activity has been related to the total dose of material administered than when calculated in relation to the serum steady-state level actually achieved. The latter method allows for differences in the rates at which the materials are metabolised, and correlates well with potencies in vitro when monomeric insulin analogues are studied. Unless stated otherwise, dimer biopotency in vivo has been calculated by relating hypoglycaemic response to serum steady-state level achieved [1]. An experimental protocol of primed 30-min infusion periods was originally used to determine dimer potencies. However in view of the slow kinetics of the

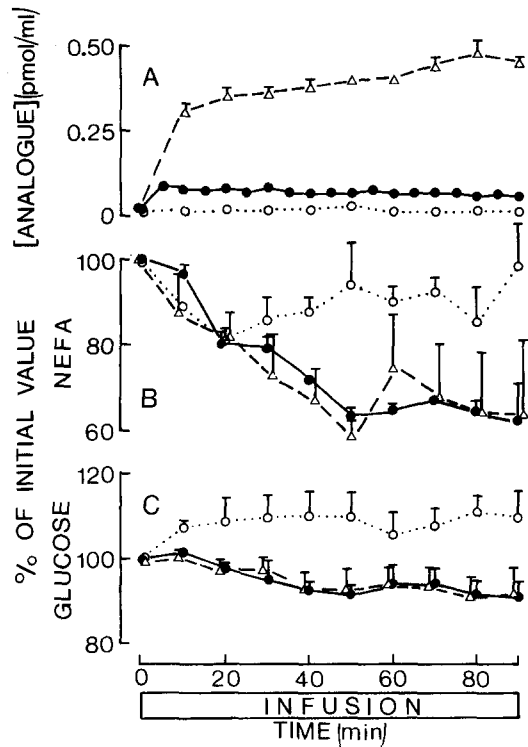


Fig. 1 A-C. Infusions of saline (0.154 mol/l) ($\circ\cdots\circ$) or equipotent doses of insulin ($\bullet\cdots\bullet$, $1.40\pm 0.08\text{ pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$) or B1-B'29 D ($\triangle\cdots\triangle$, $4.90\pm 0.46\text{ pmol}\cdot\text{min}^{-1}\cdot\text{kg}^{-1}$). Data from three experiments with each substance are means \pm SEM (when error bars are not shown variance is smaller than symbol) for A plasma immunoreactive analogue levels, B non-esterified fatty acids (NEFA) and C glucose

dimers it is possible that even with the priming doses true serum steady-state levels had not been achieved, leading to errors in the estimates. Further estimates of potencies from the experiments reported here have been undertaken as follows. On the assumption that the dose-response relationship between steady-state levels of hormone and fall in plasma glucose from baseline (SSL versus ΔG) was parallel between insulin and each of the dimers, data from the interaction experiments could be regarded as a single point bioassay for B1-B'29 D. Its biopotency was determined from the steady-state levels of the equipotent doses of insulin and B1-B'29 D, using only the last few data points of the 90-min infusion of B1-B'29 D when a true steady state level had been achieved (Fig. 1).

$$\text{Potency (\% B1-B'29 D)} = \frac{\text{SSL (insulin)}}{\text{SSL (B1-B'29 D)}} \times 100\%$$

Using this calculated potency for B1-B'29 D, the biopotency of each of the other two dimers was estimated from the two doses of the 3.5-h infusions by relating their steady state levels and the falls in plasma glucose concentration after 120 min of infusion to the respective values for B1-B'29 D. Potency of dimer

$$= \frac{\Delta G \text{ (dimer)}}{\Delta G \text{ (B1-B'29 D)}} \times \frac{\text{SSL (B1-B'29 D)}}{\text{SSL (dimer)}} \times \% \text{ B1-B'29 D}$$

Statistical analyses

For each metabolic variable calculated from either infusion or bolus data, a one-way analysis of variance was used to determine the significance of difference ($p < 0.05$), either between insulin and the dimers, or between control, insulin and B1-B'29 D in the interaction experiments. A two-way analysis of variance was used to compare the effects of insulin and dimer on plasma glucose and NEFA in the interaction experiments.

Results

Constant infusions of insulin and the three dimers, given separately, showed that the plasma distribution kinetics of the dimers were slower than those of insulin. Whereas insulin achieved a steady-state level by 20 min into the infusion, the dimers did not reach a steady state until 60–110 min during the low-dose (a representative infusion of each is shown in Fig. 2) and 100–150 min during the high-dose infusions. The mean steady-state levels achieved at each dose are shown in Figure 3A. All three dimers showed significantly reduced rates of metabolism ($p < 0.001$, Fig. 3B), which was also reflected in their prolonged half-time of disappearance from serum ($p < 0.001$, Fig. 3C). During the low-dose infusions the hypoglycaemic effects were markedly reduced for the dimers compared with insulin ($p < 0.001$, Fig. 3D). At both dose levels of dimers, B1–B'29 D was the most and B29–B'29 D the least active. This relative order of the dimers for biological potencies was also observed in vitro [5, 7]. The apparent distribution space of the dimers (77.1 ± 7.6 to 94 ± 13.7 ml/kg) did not significantly differ from that of insulin (90.4 ± 7.5 ml/kg).

Our findings in vitro that the binding potencies of the dimers were 2.5 to 6.6-fold higher than their biological potencies suggested that covalent insulin dimers were partial competitive antagonists of insulin. The most active dimer, B1–B'29 D, was selected to investigate the possibility of an interaction with insulin. Figure 4 illustrates the results of these experiments, in which an insulin bolus (700 pmol/kg) was given 30 min into a 90-min infusion of either saline or equipotent doses of insulin or dimer (1.4 and 4.9 pmol \cdot min $^{-1}$ \cdot kg $^{-1}$ respectively). The mean plasma immunoreactive analogue concentrations are shown in Figure 4, panel A. Both infusions significantly reduced plasma NEFA before the insulin bolus was given ($p < 0.05$), but did not alter the recovery of NEFA 30 min after the bolus (Fig. 4, panel B). Both infusions had little effect on plasma glucose levels before the insulin bolus (NS), but markedly prolonged the hypoglycaemic effect of the bolus until the end of the infusion ($p < 0.001$, Fig. 4, panel C). This prolongation of hypoglycaemia was found to be dose-dependent, as an infusion of insulin (0.87 pmol \cdot min $^{-1}$ \cdot kg $^{-1}$) showed a significant intermediate effect ($p < 0.05$ compared with the higher dose of insulin (1.4 pmol \cdot min $^{-1}$ \cdot kg $^{-1}$, $p < 0.1$) compared with control; data not shown). Infusion of B1–B'29 D also prolonged the hypoglycaemic effect of a smaller insulin bolus (173 pmol/kg, $p < 0.001$), during which the plasma glucose levels fell from 4.5–5.0 to 2.7–3.5 mmol/l (data not shown).

The effects of the insulin or dimer infusions on either metabolic clearance rate or apparent distribution space of the insulin bolus (700 pmol/kg) were compared after subtraction of background-infusion immunoreactive analogue levels. The apparent distribution space of the insulin bolus (106.4 ± 11.9 ml/kg) was sig-

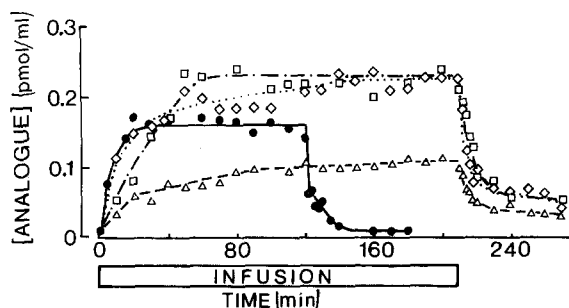


Fig. 2. Plasma distribution kinetics from a representative low-dose infusion of insulin (●—●), B1–B'29 D (△—△), B1–B'1 D (□—□), or B29–B'29 D (◇—◇). Insulin was infused for 2 h at 2.7 pmol \cdot min $^{-1}$ \cdot kg $^{-1}$ and the dimers for 3.5 h at 1.0 – 1.5 pmol \cdot min $^{-1}$ \cdot kg $^{-1}$.

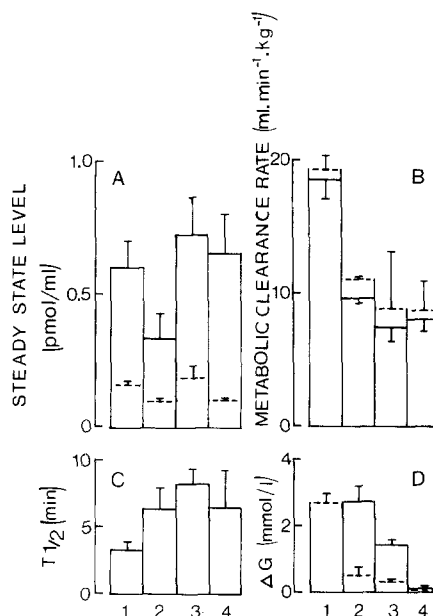


Fig. 3A–D. Results of single constant infusions of insulin (1), B1–B'29 D (2), B1–B'1 D (3) or B29–B'29 D (4). Data from two or three experiments with each at either low (broken lines) or high (solid lines) dose are means and range for A serum steady-state analogue concentration, B metabolic clearance rates, C initial half disappearance time ($t_{1/2}$, the mean values from both low and high doses are shown) and D fall in plasma glucose during 120 min infusion (ΔG). No effect on glucose levels was measured during the high-dose insulin infusions because a glucose clamp was used to prevent dangerous hypoglycaemia.

nificantly reduced by the dimer (44.5 ± 8.4 ml/kg, $p < 0.02$), but not by the equipotent insulin infusion (102.7 ± 8.2 ml/kg). The metabolic clearance rate of the insulin bolus (14.7 ± 0.5 ml \cdot min $^{-1}$ \cdot kg $^{-1}$) was also reduced by the dimer (10.7 ± 2.8 ml \cdot min $^{-1}$ \cdot kg $^{-1}$, $p < 0.1$ compared with control, $p < 0.05$ compared with insulin infusion), but not by the insulin infusion (16.4 ± 0.7 ml \cdot min $^{-1}$ \cdot kg $^{-1}$).

The plasma steady-state levels of the equipotent doses of insulin and B1–B'29 D showed that eight to nine times more dimer than insulin was required for the same biological response (Fig. 1), i.e., B1–B'29 D had a

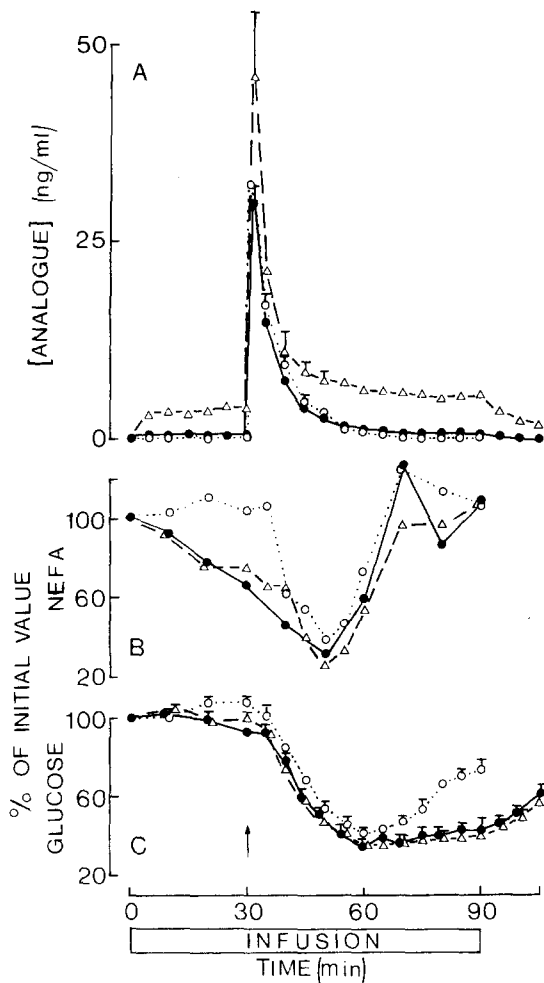


Fig. 4 A-C. Interaction experiments with infusion of either saline (○····○) or equipotent doses of insulin (●—●) or B1-B'29 D (△—△) in the presence of a bolus of insulin (700 pmol/kg) given 30 min (indicated by the arrow) into the infusion. Data from four experiments for each substance (two for NEFA) are means ± SEM (when variance is larger than symbol) for **A** immunoreactive analogue concentrations, **B** plasma NEFA, and **C** plasma glucose. Analogue concentrations in **A** are in mass rather than molar units since the samples from the B1-B'29 D infusions contained a mixture of insulin and dimer

biopotency of 11.2% on a molar basis. Using this potency and the data from the 3.5-h infusion of the three dimers, the biopotencies of the other two dimers were estimated at 3%–3.5% for B1-B'1 D and 0.3%–1.7% for B29-B'29D. These values were markedly lower than their lipogenic potencies in isolated adipocytes in vitro (80%, 30% and 13% for B1-B'29 D, B1-B'1 D and B29-B'29 D, respectively).

Discussion

The rates of metabolism of chemically-modified monomeric insulins have been reported to be directly proportional to their biological responses in vivo and to their binding potencies in vitro in isolated rat liver plasma

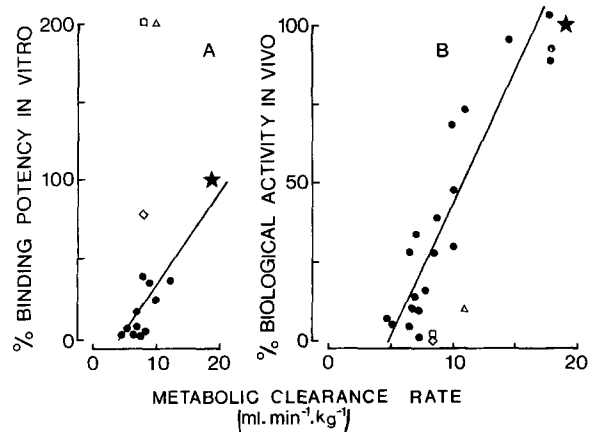


Fig. 5. Relationship between metabolic clearance rate at a steady-state level of $0.5 \text{ pmol} \cdot \text{ml}^{-1}$ and **A** percentage binding potencies in isolated liver plasma membranes or adipocytes, or **B** percentage biological activities in vivo (potencies are on a molar basis). Data for insulin (★) and several chemically-modified monomeric insulins and proinsulin (●) are from [4], with the linear regression of their data shown by the line (for A, $r=0.932$, $p<0.001$; for B, $r=0.912$, $p<0.001$). The results for B1-B'29 D, B1-B'1 D, and B29-B'29 D are shown by △, □, and ◇, respectively

membranes or adipocytes [1, 4]. Figure 5 illustrates these two relationships and demonstrates that covalently-linked insulin dimers showed marked deviations from the correlations. The most striking observation is the dissociation of degradation in vivo (i.e. metabolic clearance rates) from receptor binding affinities in vitro (Fig. 5A). Impairment in the distribution of the dimers to the site of cell surface receptors is one possible explanation, since distribution is primarily by diffusion and therefore dependent upon molecular size. Although their plasma distribution kinetics were slower than those of insulin (Fig. 2), the measured distribution spaces of insulin and the dimers were similar and must therefore be regarded as evidence against impaired distribution.

It is perhaps more likely that the dimers, even when receptor bound, are less rapidly degraded than previously studied monomeric analogues. This explanation would support the idea that the processes of internalisation and subsequent degradation are linked to biological action. The post-binding events which initiate the process of internalisation and subsequent degradation are not understood, but it is of interest that receptor-bound dimers also show reduced ability to initiate effects on lipogenesis and lipolysis in isolated adipocytes. This property would be expected to result in partial antagonism of insulin by the dimers.

It is interesting to note that the plasma immunoreactive analogue concentrations of the dimers, unlike insulin, failed to return to baseline levels 60 min after termination of the infusion (Fig. 2). With chemically-modified monomeric insulins an inverse correlation has been found between the plasma concentrations at 60 min after termination of the infusion and the rates of degrada-

tion of the materials in vivo (unpublished observations). A likely explanation is recycling of immunoreactive material back into the plasma pool.

All three of the dimers had lower hypoglycaemic effects than expected from their rates of metabolism (Fig. 5B), again suggesting partial competitive antagonism.

Partial antagonism of insulin degradation in vivo was demonstrated by the interaction experiments in which the apparent distribution space and metabolic clearance rate of insulin were reduced by B1-B'29 D but not by an equipotent dose of insulin. This is the expected result if the dimer, acting as an antagonist with a high binding affinity, reduces the number of available receptor sites without producing a commensurate biological effect. These observations are consistent with those of others who have reported reductions in the apparent distribution space and metabolic clearance rate of a bolus of iodinsulin tracer by a high-dose infusion of insulin [12].

Plasma NEFA were found to be more sensitive than glucose to the effects of a low dose of insulin as previously reported [13, 14]. Insulin has been shown to control NEFA concentration primarily by modulating output from peripheral stores [14]. On the other hand, the hepatic effect of insulin on glucose production is the predominant determinant of peripheral glucose concentration at low insulin concentrations, with a further effect in increased peripheral uptake only at high physiological levels [15, 16]. A bolus of insulin alone (173 or 700 pmol/kg) caused an immediate rapid fall in plasma NEFA and glucose. As plasma insulin concentrations rapidly decreased, recovery of both NEFA and glucose would be aided by the stimulatory action of counter-regulatory hormones, such as glucagon, catecholamines and adrenaline on glucose production in the liver and lipolysis in adipose tissue [17, 18]. A low-dose infusion of insulin (and an equipotent dose of B1-B'29 D) prolonged the hypoglycaemic effect of an insulin bolus but were unable to prevent the recovery of NEFA. This suggests that the stimulatory action of counter-regulatory hormones was stronger than the inhibitory action of insulin in peripheral tissue (i.e., on lipolysis) but not in the liver (i.e., on gluconeogenesis or glycogenolysis).

Covalently-linked insulin dimers had slower plasma distribution kinetics, reduced rates of metabolism and markedly diminished hypoglycaemic effects in vivo compared with insulin. The apparent partial competitive antagonism of insulin by dimers that has been observed in vitro was investigated in vivo and partial antagonism of insulin metabolism by one of the dimers was directly demonstrated.

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